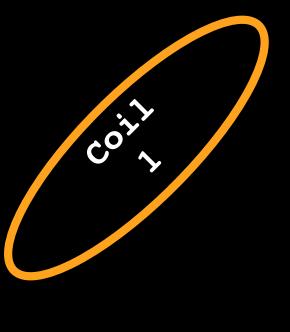
Image Reconstruction Parallel Imaging

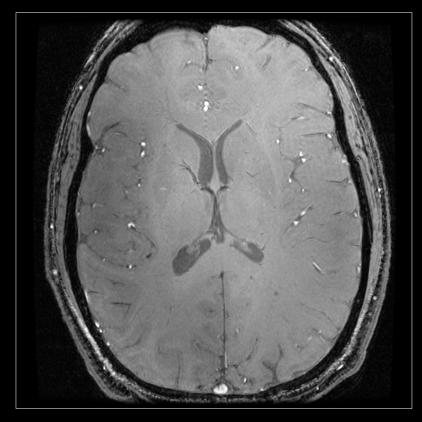
M229 Advanced Topics in MRI Kyung Sung, Ph.D. 5/11/2023

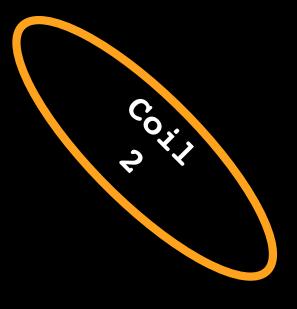
Today's Topics

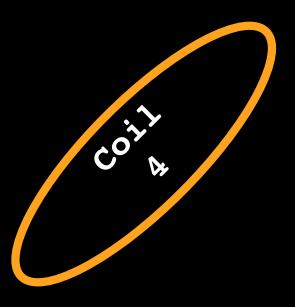
- Multicoil reconstruction
- Parallel imaging
 - Image domain methods:
 - SENSE
 - k-space domain methods:
 - SMASH
 - GRAPPA

Multi-coil Arrays



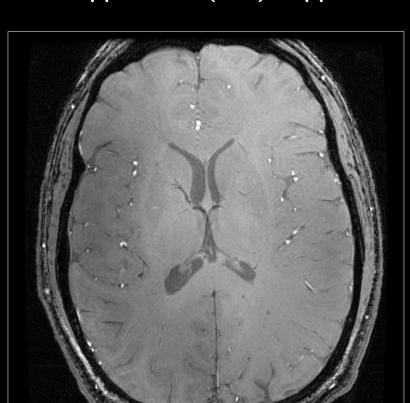


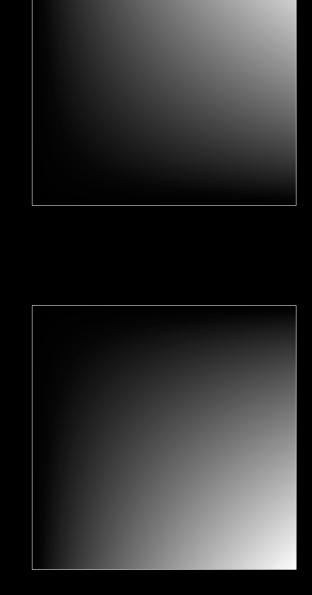




Multi-coil Sensitivity







Multi-coil Reconstruction

Each coil has a complete image of whole
 FOV and an amplitude and phase sensitivity

$$C_l(\vec{x})$$
 $l = 1, 2, ... L$

Coils are coupled, so noise is correlated

$$E[n_i n_j] = \Psi$$

Received data from coil I:

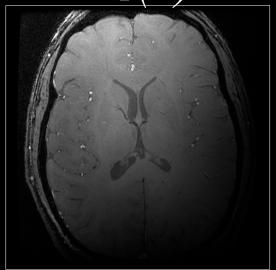
$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x}) + n_l(\vec{x})$$

• Given $m_l(x)$, how do we reconstruct m(x)?

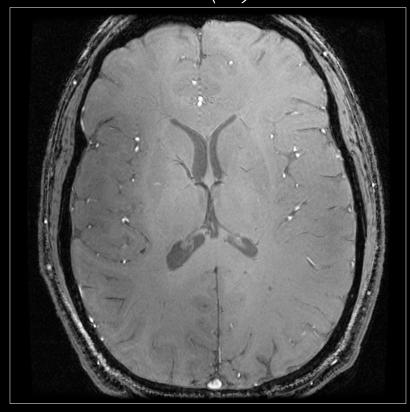
 $m_1(x)$

Multi-coil Images

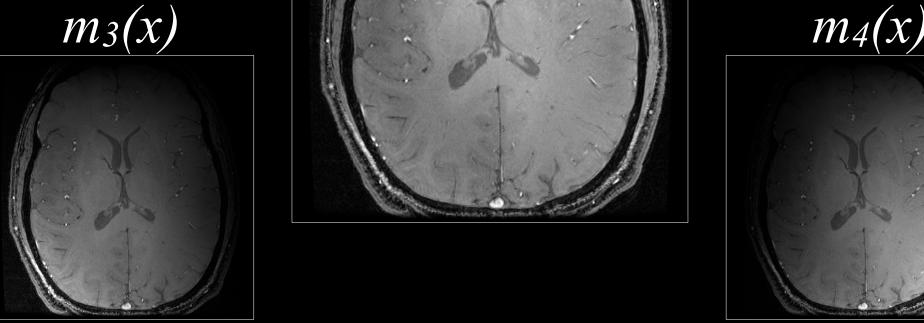
 $m_2(x)$

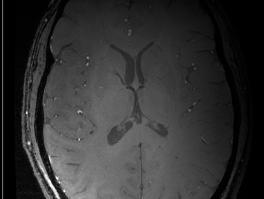


 $m_s(x)$



 $m_4(x)$







Multi-coil Reconstruction

For a particular voxel x

$$\begin{pmatrix} m_{1}(\vec{x}) \\ m_{2}(\vec{x}) \\ \vdots \\ m_{L}(\vec{x}) \end{pmatrix} = \begin{pmatrix} C_{1}(\vec{x}) \\ C_{2}(\vec{x}) \\ \vdots \\ \vdots \\ C_{L}(\vec{x}) \end{pmatrix} m(\vec{x}) + \begin{pmatrix} n_{1}(\vec{x}) \\ n_{2}(\vec{x}) \\ \vdots \\ n_{L}(\vec{x}) \end{pmatrix}$$

OR

$$m_s(ec{x}) = Cm(ec{x}) + n$$
 L x 1 L x 1

Minimum Variance Estimate

$$\hat{m}(\vec{x}) = (C^* \Psi^{-1} C)^{-1} C^* \Psi^{-1} m_s(\vec{x})$$
 1 x 1 1 x L L x 1

Covariance (variance)

$$COV(\hat{m}(\vec{x})) = C^* \Psi^{-1} C$$

What if Ψ is σ^2 I?

$$\hat{m}(\vec{x}) = (C^*C)^{-1}C^*m_s(\vec{x})$$

Intensity Phase Correction

Approximate Solution

• Often we don't know $C_l(x)$, but

$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x})$$

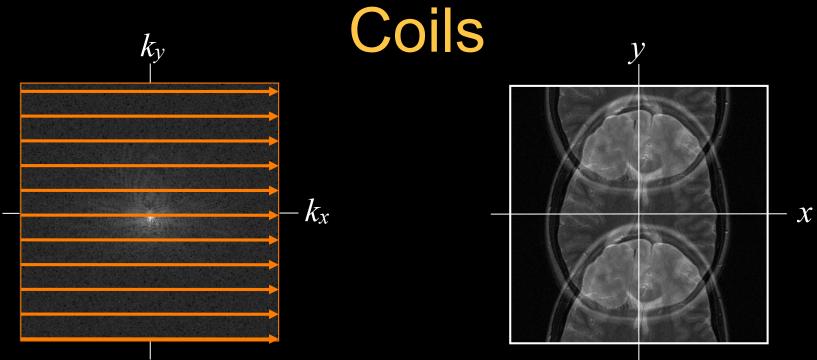
Approximate solution:

$$\hat{m}_{SS}(\vec{x}) = \sqrt{\sum_{l} m_l^*(\vec{x}) m_l(\vec{x})}$$

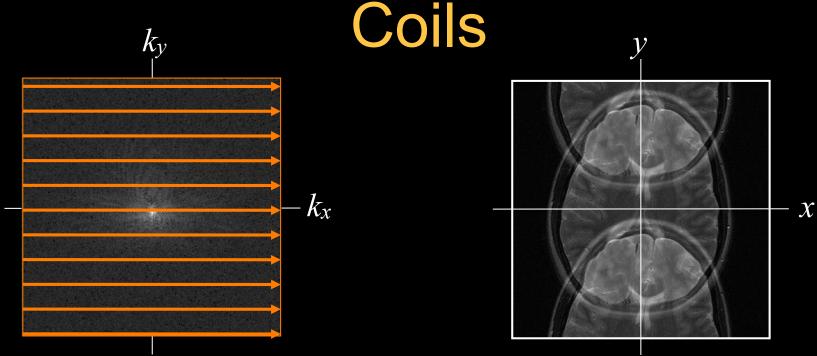
For SNR > 20, within 10% of optimal solution

PB Roemer et al. MRM 1990

Accelerate Imaging with Array Coils



Accelerate Imaging with Array Coils



- Parallel Imaging
 - Coil elements provide some localization
 - Undersample in k-space, producing aliasing
 - Sort out in reconstruction

Parallel Imaging

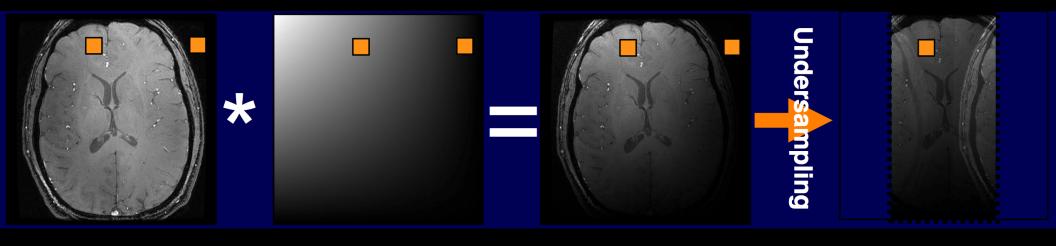
- Many approaches:
 - Image domain SENSE
 - k-space domain SMASH, GRAPPA
 - Hybrid ARC

- We will focus on two:
 - SENSE: optimal if you know coil sensitivities
 - GRAPPA: autocalibrating / robust

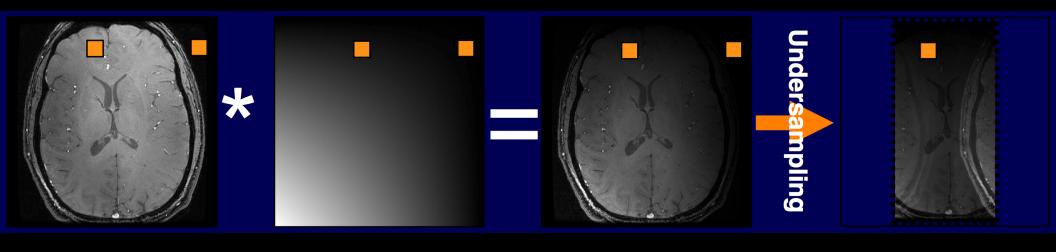
Parallel Imaging (SENSE)

Cartesian SENSE

$$m_1(\vec{x_1}) = C_1(\vec{x_1})m(\vec{x_1}) + C_1(\vec{x_2})m(\vec{x_2})$$



$$m_2(\vec{x_1}) = C_2(\vec{x_1})m(\vec{x_1}) + C_2(\vec{x_2})m(\vec{x_2})$$



$$\begin{pmatrix} m_{1}(\vec{x_{1}}) \\ m_{2}(\vec{x_{1}}) \\ \vdots \\ m_{L}(\vec{x_{1}}) \end{pmatrix} = \begin{pmatrix} C_{1}(\vec{x_{1}}) & C_{1}(\vec{x_{2}}) \\ C_{2}(\vec{x_{1}}) & C_{2}(\vec{x_{2}}) \\ \vdots \\ C_{L}(\vec{x_{1}}) & C_{L}(\vec{x_{2}}) \end{pmatrix} \begin{pmatrix} m(\vec{x_{1}}) \\ m(\vec{x_{2}}) \end{pmatrix} + \begin{pmatrix} n_{1}(\vec{x_{1}}) \\ n_{2}(\vec{x_{1}}) \\ \vdots \\ n_{L}(\vec{x_{1}}) \end{pmatrix}$$

$$C_{L}(\vec{x_{1}}) & C_{L}(\vec{x_{2}}) \end{pmatrix}$$
Source
$$Voxels$$

Aliased Images Sensitivity at Source Voxels

OR
$$2 \times 1$$

$$m_s = Om + n$$
 L x 1 L x 2 L x 1

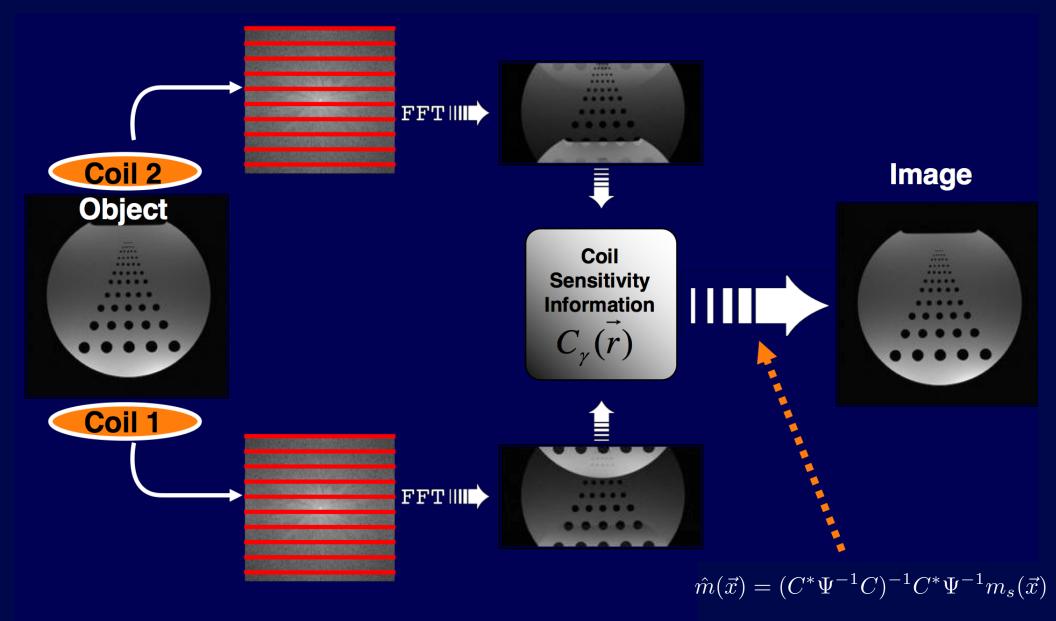
$$\hat{m}(\vec{x}) = (C^* \Psi^{-1} C)^{-1} C^* \Psi^{-1} m_s(\vec{x})$$
2 x 2 2 x L L x 1

L aliased reconstruction resolves 2 image pixels

For an N x N image, we solve (N/2 x N) 2 x 2 inverse systems

For an acceleration factor R, we solve (N/R x N) R x R inverse systems

SENSE Reconstruction



Unwrap fold over in image space

SNR Cost

- How large can R be?
- Two SNR loss mechanisms
 - Reduced scan time
 - Condition of the SENSE decomposition
- SNR Loss

$$SNR_{SENSE} = \frac{SNR}{g\sqrt{R}}$$

Geometry Reduced Factor Scan Time

Geometry Factor

 Covariance for a fully sampled image (variance of one voxel):

$$\chi_F = \frac{1}{n_F} (C_F^* \Psi^{-1} C_F)^{-1}$$

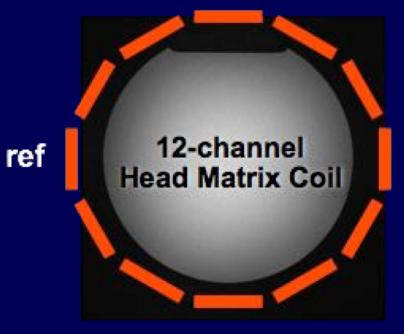
Covariance for a reduced encoded image:

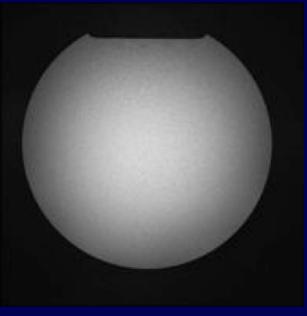
$$\chi_R = \frac{1}{n_R} (C_R^* \Psi^{-1} C_R)^{-1}$$

Geometry Factor

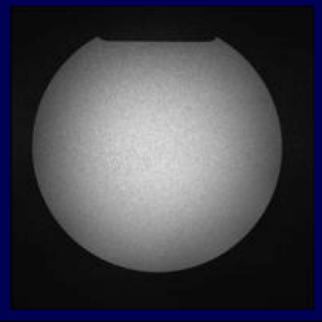
- g-factor is critical since it depends on:
 - Acceleration
 - Spatial position
 - Aliasing direction
 - Coil geometry
- Minimizing g-factor drives system design
- Sense coils are different from traditional array coils

Parallel Imaging Tradeoffs

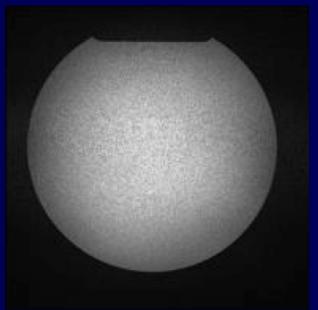




PAT x 2



PAT x 3

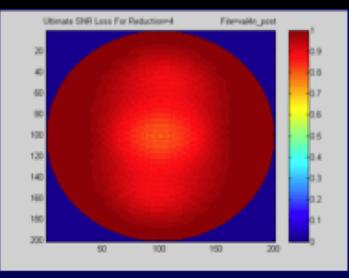


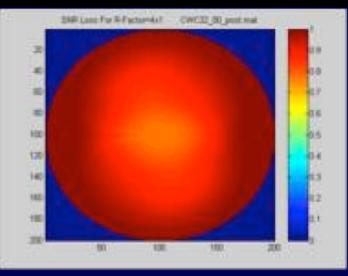
 f_p = acceleration factor

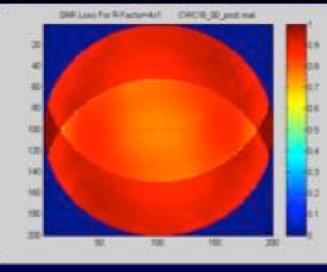
g = coil geometry factor

PAT x 4

1/g-factor Map for R=4



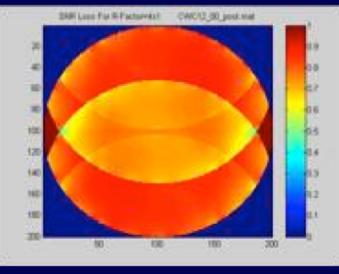




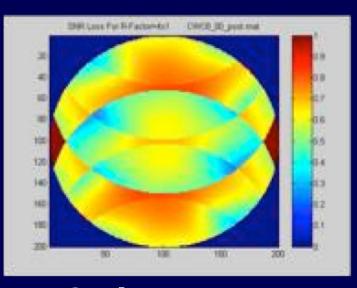
∞ elements

32 elements

16 elements



12 elements



8 elements

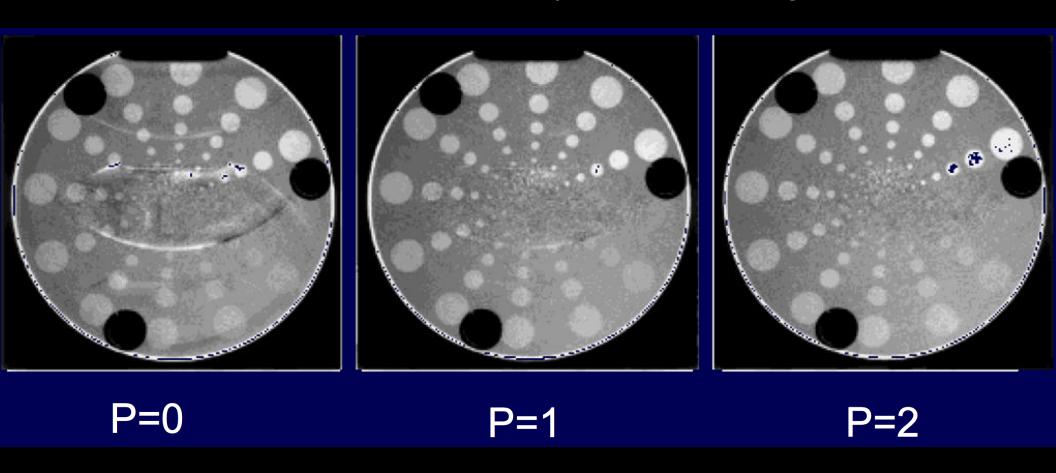
Relative SNR Scale g-map

aliased

Rate 1 2.4 SENSE

Dependence on Coil Sensitivity

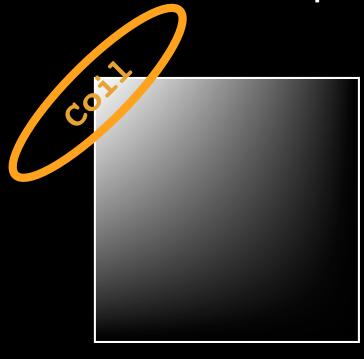
 Images reconstructed using coil sensitivity maps with different order P of polynomial fitting



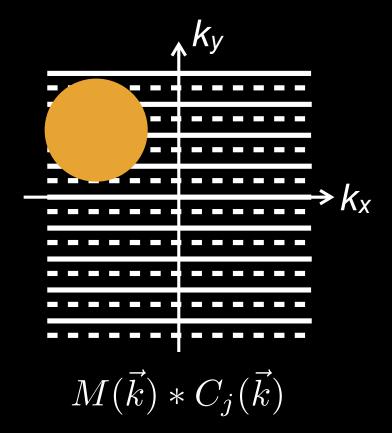
Parallel Imaging (GRAPPA)

GRAPPA

- Coil sensitivities are
 - Smooth in image space
 - Local in k-space

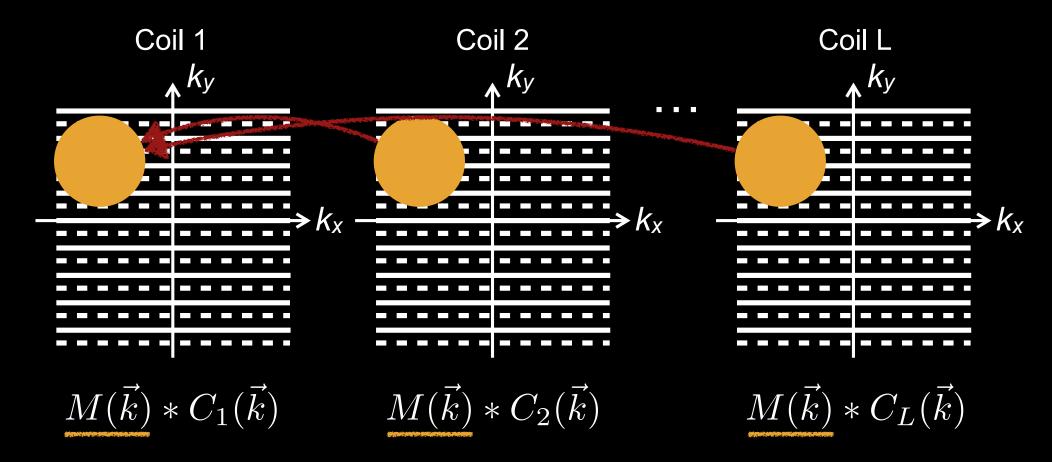


$$m(\vec{x})C_j(\vec{x})$$



GRAPPA

Missing information is implicitly contained by adjacent data

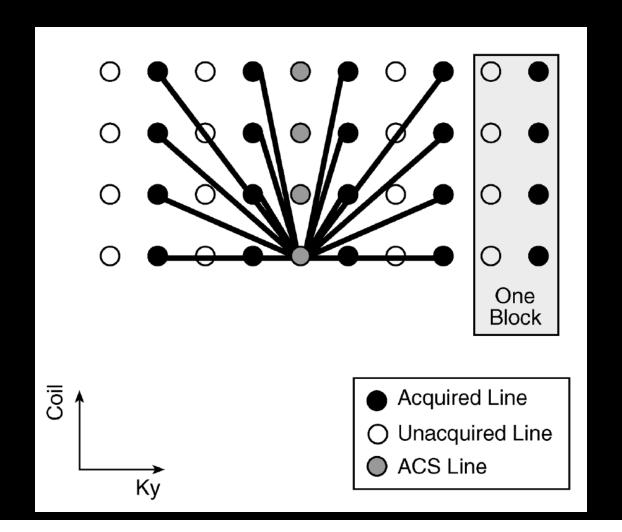


GRAPPA Reconstruction

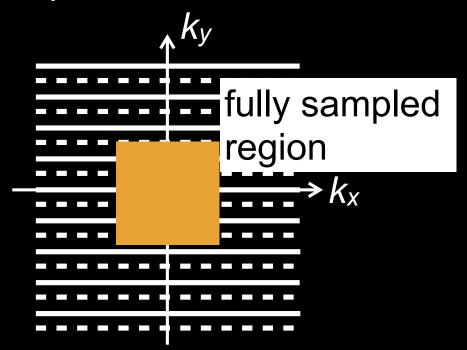
 How do we find missing data from these samples?

$$\hat{m}_k(k_x,k_y) = \sum_{i,j,k} a_{i,j,k} \cdot m_k(k_x + i\Delta k_x,k_y + j\Delta k_y)$$
 missing data for each coil neighborhood data for each coil

$$\hat{m}_k(k_x, k_y) = \sum_{i,j,k} a_{i,j,k} \cdot m_k(k_x + i\Delta k_x, k_y + j\Delta k_y)$$

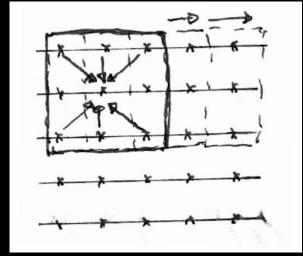


- Assume there is a fully sampled region
- We have samples of what the GRAPPA synthesis equations should produce



Invert this to solve for GRAPPA weights

- Calibration area has to be larger than the GRAPPA kernel
- Each shift of kernel gives another equation



Here, 3x3 kernel, 5x5 calibration area gives 9 equations

$$\hat{m}_k(k_x, k_y) = \sum_{i,j,k} a_{i,j,k} \cdot m_k(k_x + i\Delta k_x, k_y + j\Delta k_y)$$

Write as a matrix equation

GRAPPA Coefficients

$$\underline{M_{k,c}} = M_A \cdot a_k$$

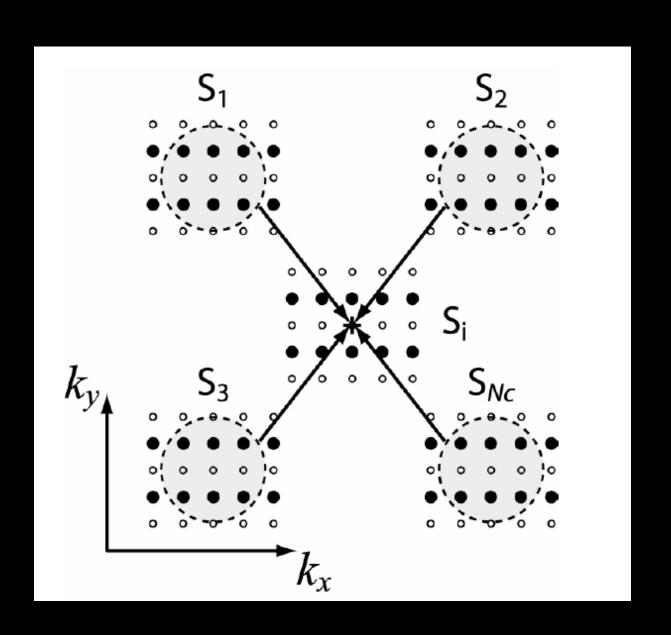
Calibration Neighborhood

Data Data

GRAPPA weights are:

$$a_k = (M_A^* M_A + \lambda I)^{-1} M_A^* M_{k,c}$$

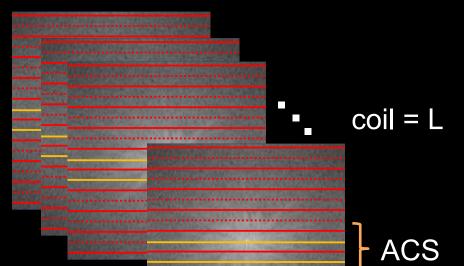
GRAPPA - Synthesis



Auto-Calibration Parallel Imaging







$$\sum_{l=1}^{L} S_{l}^{ACS}(k_{y} - m\Delta k_{y}) = \sum_{l=1}^{L} n(l, m) S_{l}(k_{y})$$

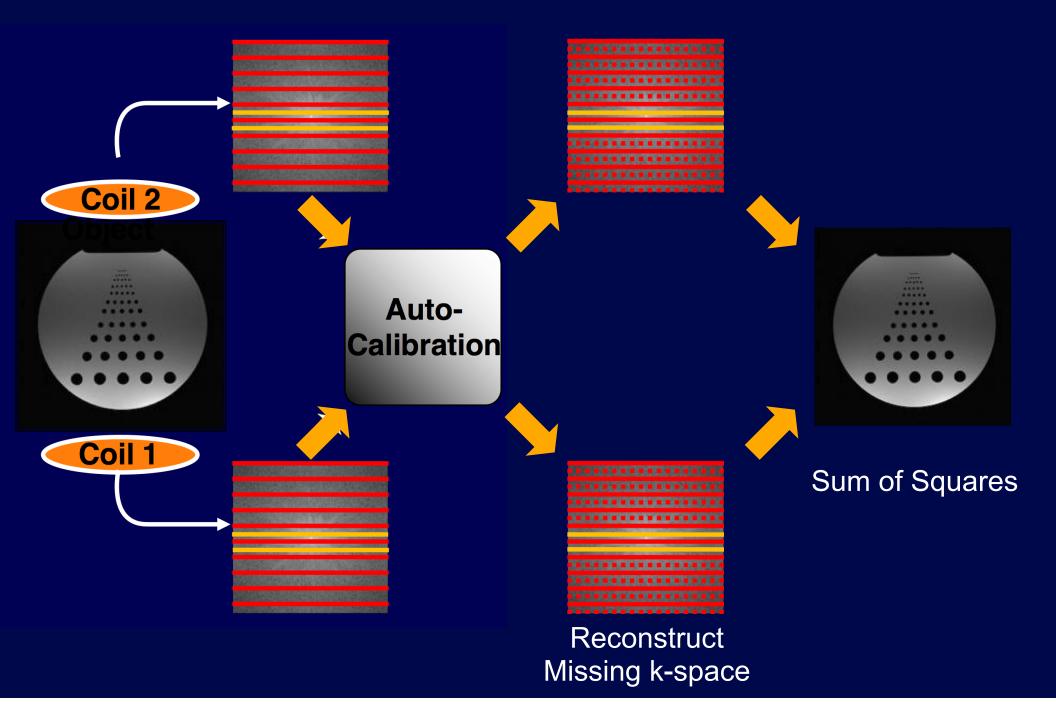
GRAPPA formula to reconstruct signal in one channel

$$S_{j}(k_{y}-m\Delta k_{y})=\sum_{l=1}^{L}\sum_{b=0}^{N_{b}-1}n(j, b, l, m)S_{l}(k_{y}-bA\Delta k_{y})$$

A: Acceleration factor n(j,b,l,m): GRAPPA weights

Griswold et al. MRM, 47(6):1202-1210 (2002)

GRAPPA Reconstruction

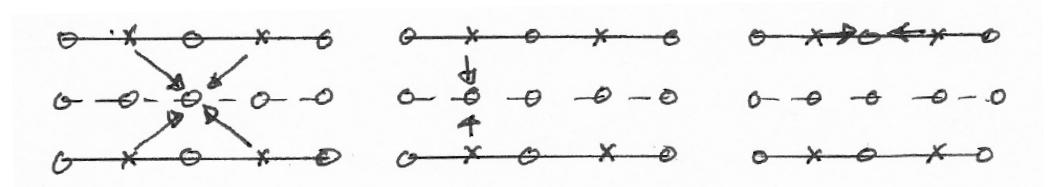


GRAPPA

- Compute GRAPPA weights from calibration region
- Compute missing k-space data using the GRAPPA weights
- Reconstruct individual coil images
- Combine coil images

Considerations of GRAPPA

- Calibration region size
- GRAPPA kernel size
- Sample geometry dependence



GRAPPA

- Compute GRAPPA weights from calibration region
- Compute missing k-space data using the GRAPPA weights
- Reconstruct individual coil images
- Combine coil images

Summary

- Parallel imaging utilizes coil sensitivities to increase the speed of MRI
- Cases for parallel imaging
 - Higher patient throughput,
 - Real-time imaging/Interventional imaging
 - Motion suppression
- Cases against parallel imaging
 - SNR starving applications

Summary

- Many approaches:
 - Image domain SENSE
 - k-space domain SMASH, GRAPPA
 - Hybrid ARC

- We will focus on two:
 - SENSE: optimal if you know coil sensitivities
 - GRAPPA: autocalibrating / robust

Further Reading

- Multi-coil Reconstruction
 - http://onlinelibrary.wiley.com/doi/10.1002/ mrm.1910160203/abstract
- SENSE
 - http://www.ncbi.nlm.nih.gov/pubmed/10542355
- SMASH
 - http://www.ncbi.nlm.nih.gov/pubmed/9324327
- Parallel Imaging Overview
 - http://www.ncbi.nlm.nih.gov/pubmed/17374908

Thanks!

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