

# Imaging Sequences II

M219 - Principles and Applications of MRI

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2/26/2024

# Course Overview

- 2024 course schedule
  - [https://mrrl.ucla.edu/pages/m219\\_2024](https://mrrl.ucla.edu/pages/m219_2024)
- Assignments
  - Homework #3 is due on 3/6
- Final exam
  - 3/18 at 2-4pm
- TA office hours, Weds 4-6pm
- Office hours, Fridays 10-12pm

# Gradient Echoes & Contrast

# Gradient Echo Sequences

- Spoiled Gradient Echo
  - SPGR, FLASH, T1-FFE
- Balanced Steady-State Free Precession
  - TrueFISP, FIESTA, Balanced FFE

# Principal GRE Advantages

- Fast Imaging Applications
  - **Why?** *Can use a shorter TE/TR than spin echo*
  - **When?** Breath-held, realtime, & 3D volume imaging
- Flexible image contrast
  - **Why?** Adjusting TE/TR/FA controls the signal
  - **When?** Characterize a tissue for diagnosis
- Bright blood signal
  - **Why?** Inflowing spins haven't "seen" numerous RF pulses
  - **When?** Cardiovascular & angiographic applications

# Principal GRE Advantages

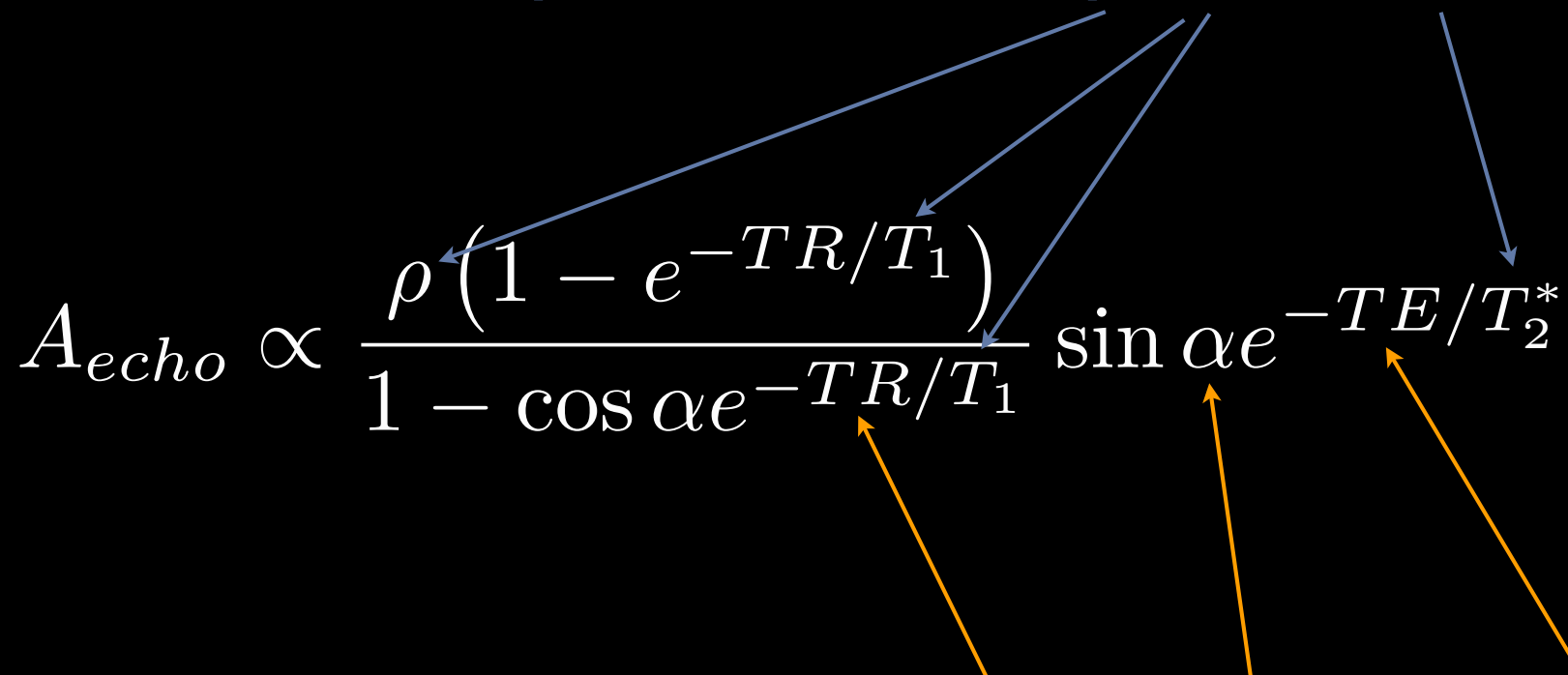
- Low SAR
  - **Why?** Imaging flip angles are (typically) small
  - **When?** When heating risks are a concern
- Quantitative
  - **Why?** Multi-echo acquisition are practical.
  - **When?** Flow quantification & Fat/Water mapping
- Susceptibility Weighted Imaging
  - **Why?** No refocusing pulse.
  - **When?**  $T_2^*$ -weighted (hemorrhage) imaging
- More...

# Principal GRE Disadvantages

- Off-resonance sensitivity
  - **Why?** No refocusing pulse
    - Field inhomogeneity, Susceptibility, & Chemical shift
- $T_2^*$ -weighted rather than  $T_2$ -weighted
  - **Why?** No re-focusing pulse
    - Spin-spin dephasing is not reversible with GRE
- Larger metal artifacts than SE
  - **Why?** No refocusing pulse.
    - Large field inhomogeneities aren't corrected with GRE

# Spoiled Gradient Echo Contrast

Contrast depends on tissue's  $\rho$ ,  $T_1$  and  $T_2^*$ .

$$A_{echo} \propto \frac{\rho (1 - e^{-TR/T_1})}{1 - \cos \alpha e^{-TR/T_1}} \sin \alpha e^{-TE/T_2^*}$$


Contrast adjusted by changing TR, flip angle, and TE



# Spoiled Gradient Echo Contrast

## Gradient Echo Parameters

Type of Contrast	TE	TR	Flip Angle
Spin Density	Short	Long	Small
T <sub>1</sub> -Weighted	Short	Intermediate	Large
T <sub>2</sub> *-Weighted	Intermediate	Long	Small

# T<sub>2</sub>\*-weighted Gradient Echo MRI

FLASH – TE=4.8ms; TR=200ms



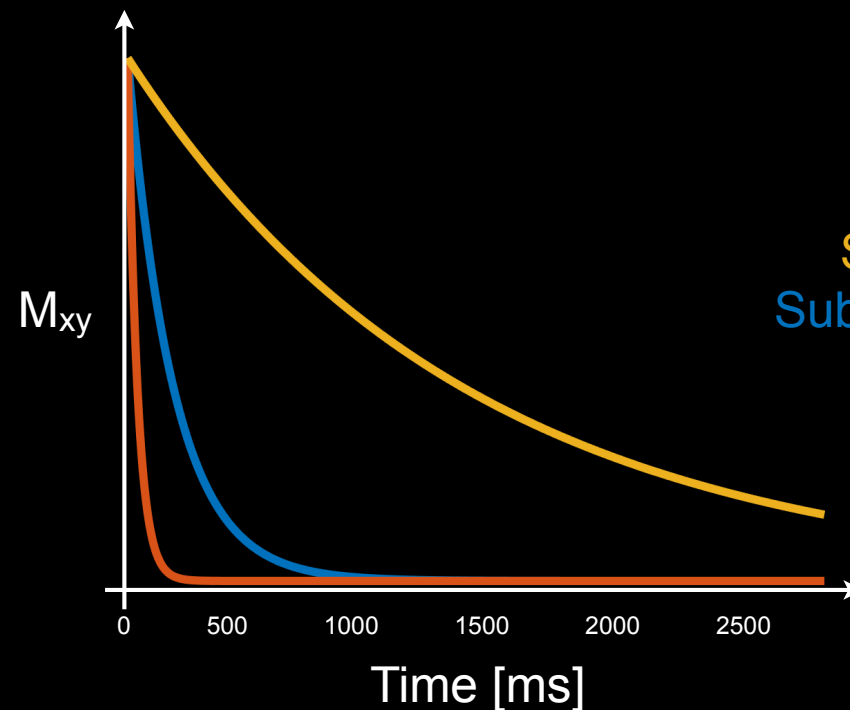
FLASH – TE=14.2ms; TR=200ms



FLASH – TE=24ms; TR=200ms

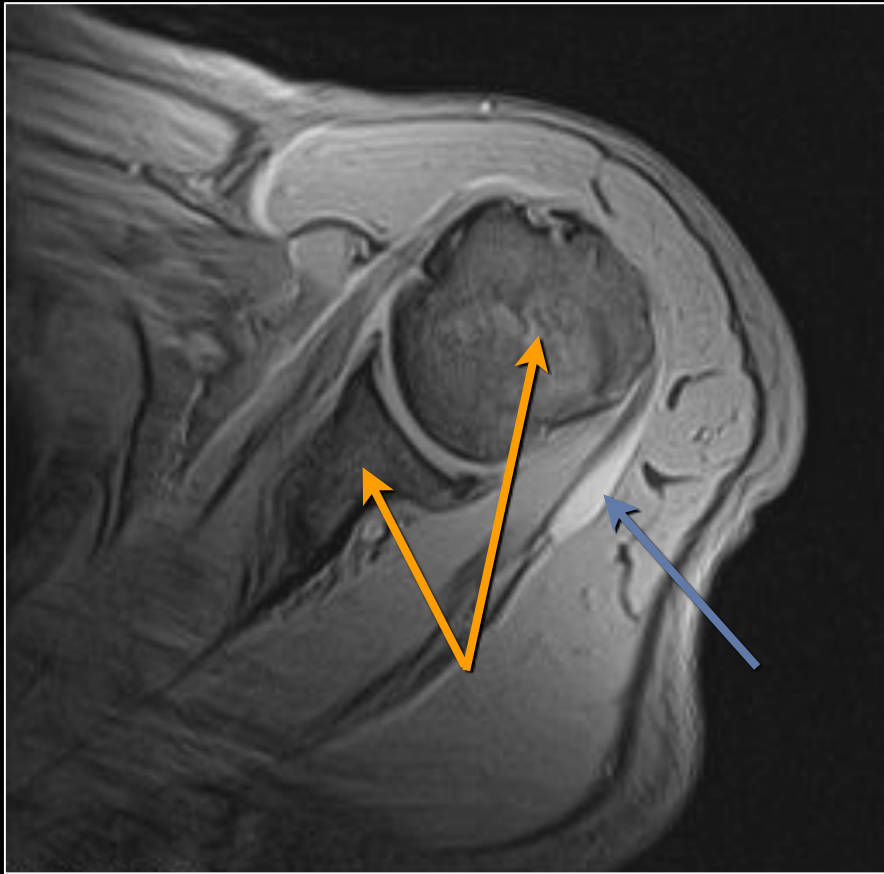


FLASH – TE=49ms; TR=200ms

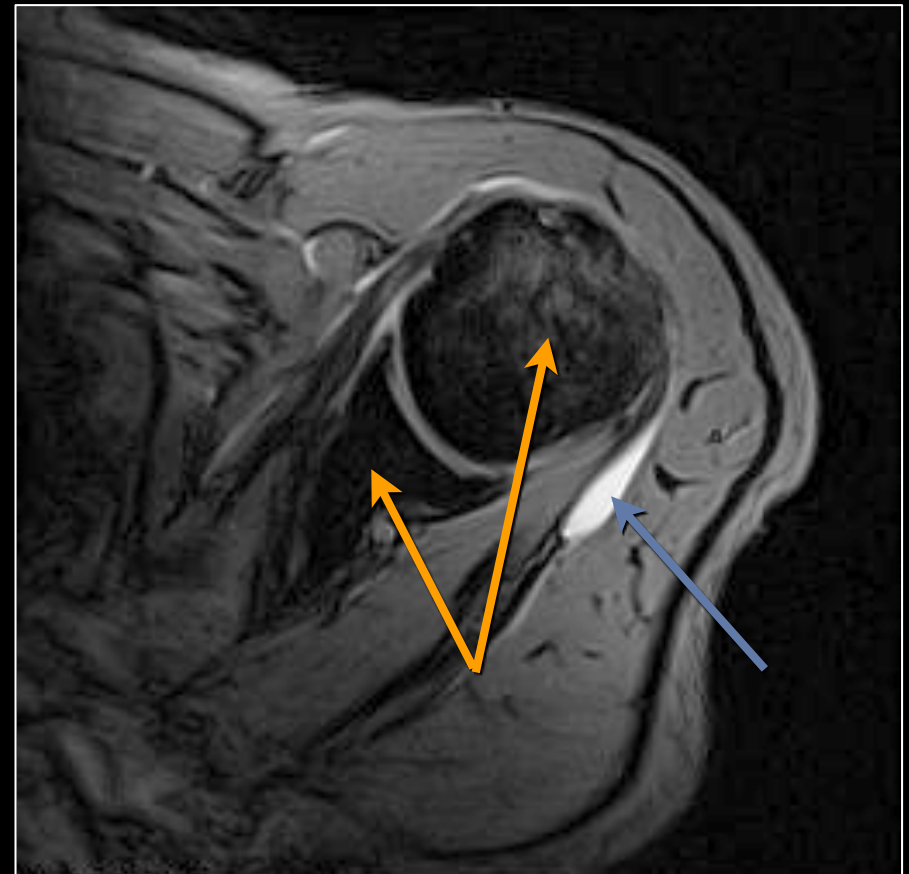


Synovial Fluid T<sub>2</sub>~1210ms  
Subcutaneous Fat T<sub>2</sub>~165ms  
Muscle T<sub>2</sub>~35ms

# $T_2^*$ -weighted Gradient Echo MRI



**TE=9ms**



**TE=30ms**

**Susceptibility Weighting (darker with longer TE)**  
**Bright fluid signal (long  $T_2^*$  is "brighter" with longer TE)**

Images Courtesy of Brian Hargreaves

# Gradient vs Spin Echo Contrast

## Gradient Echo Parameters

Type of Contrast	TE	TR	Flip Angle
Spin Density	<5ms	>100ms	<10°
T <sub>1</sub> -Weighted	<5ms	<50ms	>30°
T <sub>2</sub> *-Weighted	>20ms	>100ms	<10°

## Spin Echo Parameters

Type of Contrast	TE	TR	Flip Angle
Spin Density	10-30ms	>2000ms	90+180
T <sub>1</sub> -Weighted	10-30ms	450-850ms	90+180
T <sub>2</sub> -Weighted	>60ms	>2000ms	90+180

# Signal Equation

$$s(t) = \int_x \int_y M(x, y) e^{-i2\pi(k_x(t) \cdot x + k_y(t) \cdot y)} dx dy$$

- With off-resonance:

$$s(t) = \int_x \int_y M(x, y) e^{-i\omega_E(x,y)t} e^{-i2\pi(k_x(t) \cdot x + k_y(t) \cdot y)} dx dy$$

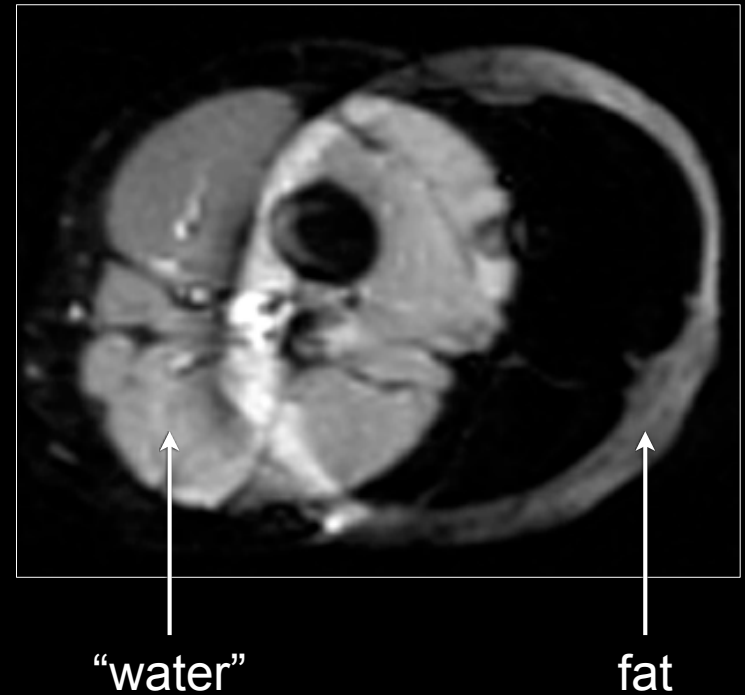
- B0 inhomogeneity
- Susceptibility
- Chemical shift

To the Board

# Gradient Echoes & Fat

# Chemical Shift - Type 1

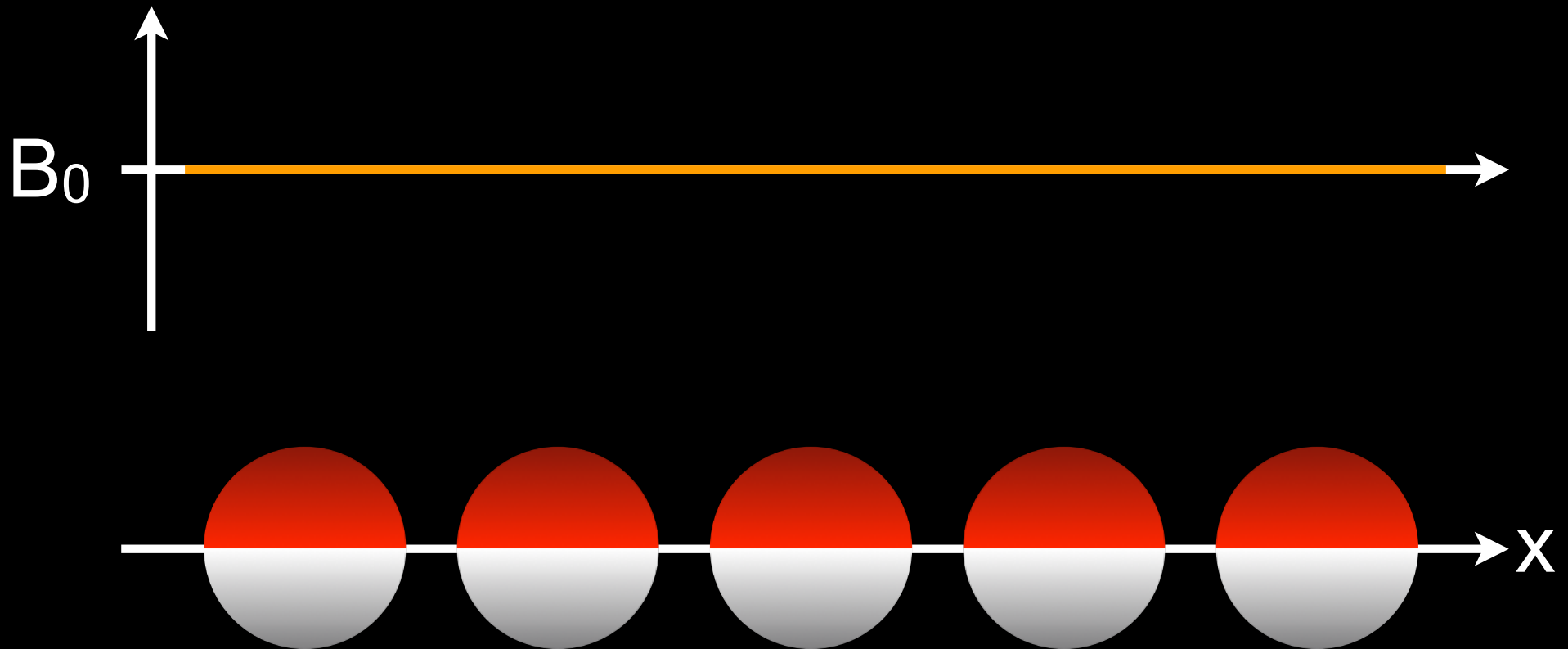
- Fat and water have different Larmor frequencies
  - ~220Hz different at 1.5T
  - ~440Hz different at 3.0T
- Spatial position is related to spin frequency in MRI.
  - Fat is more spatially mis-registered @ 3T



Chemical Shift – Fat ( $-CH_2$ ) is ~220Hz *lower* at 1.5T



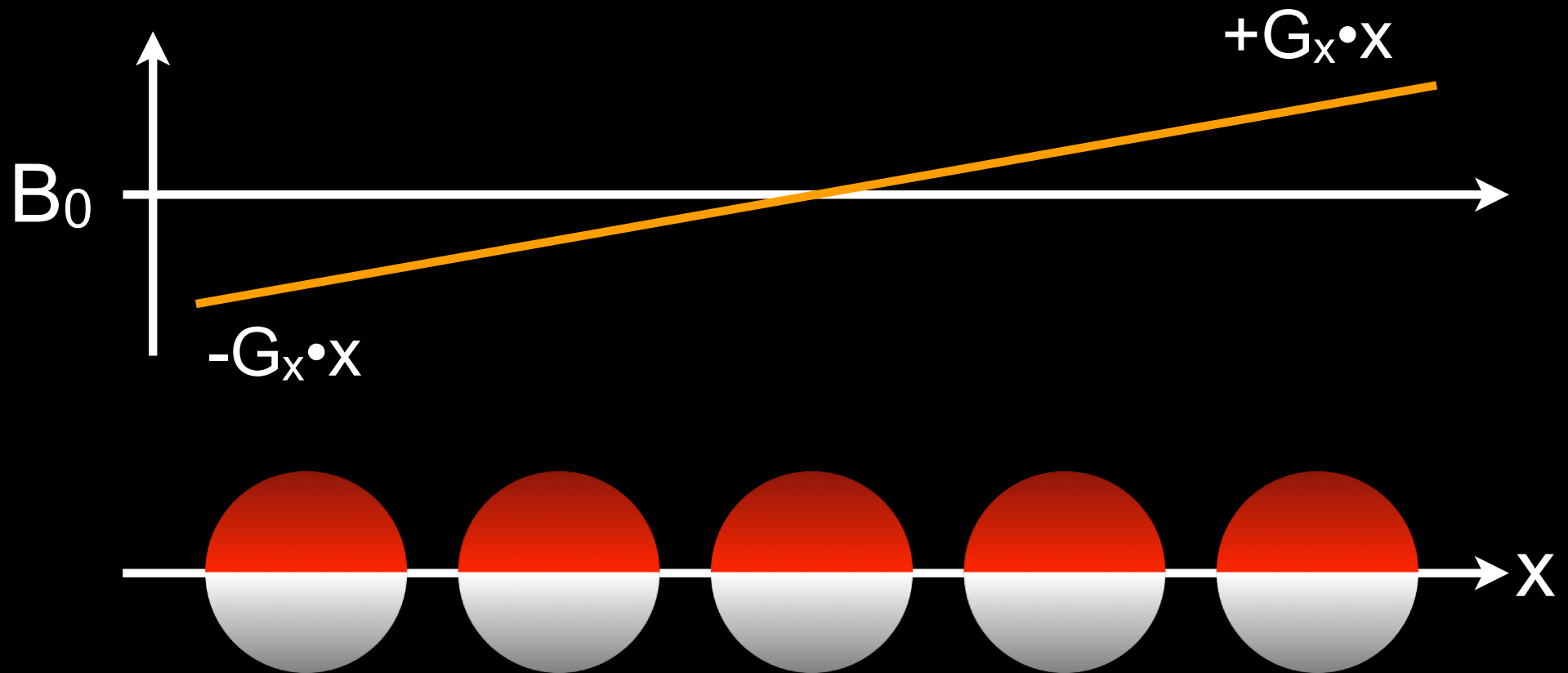
# GRE & Fat/Water Frequency



## Water Spins in a *Uniform* Field

Water spins precess at the same Larmor frequency in a uniform  $B_0$  field.

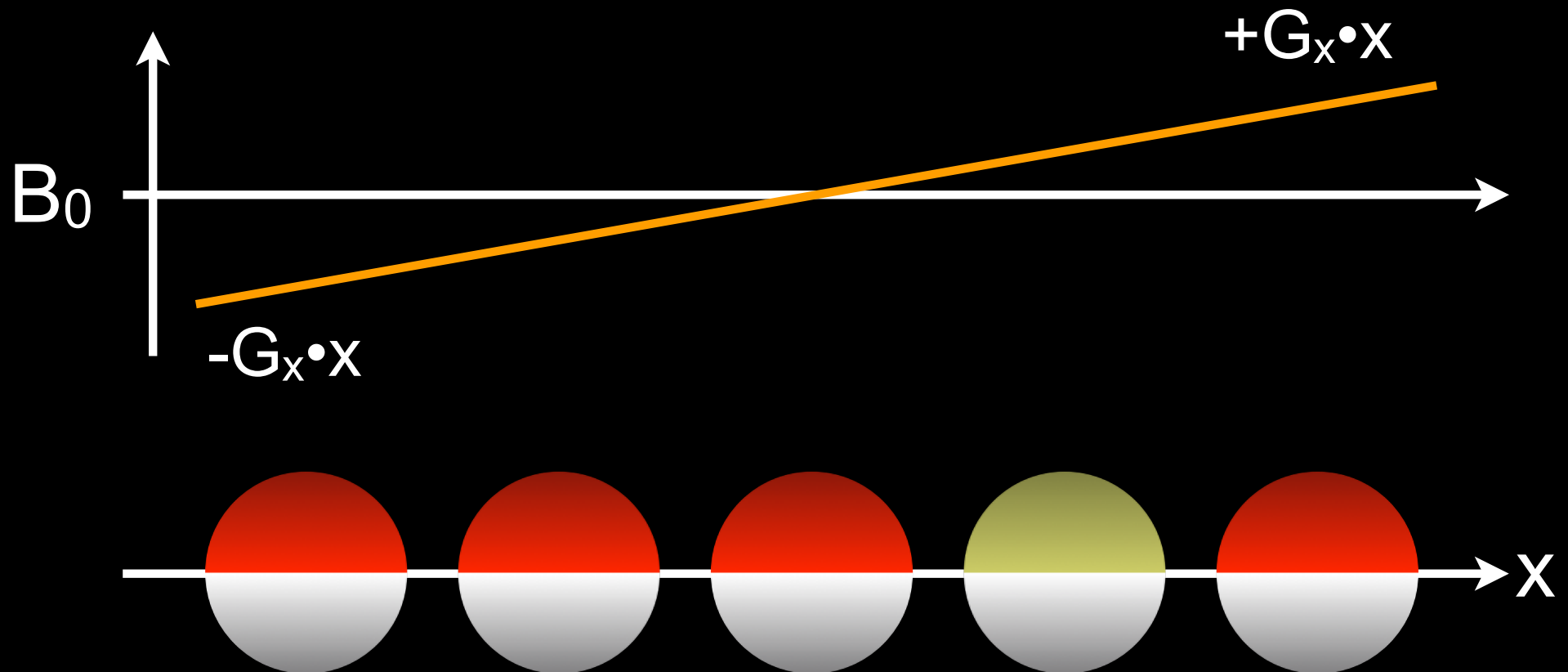
# GRE & Fat/Water Frequency



## Water Spins in a *Gradient* Field

Water spins precess at **different** Larmor frequencies in a non-uniform  $B_0$  field.

# GRE & Fat/Water Frequency

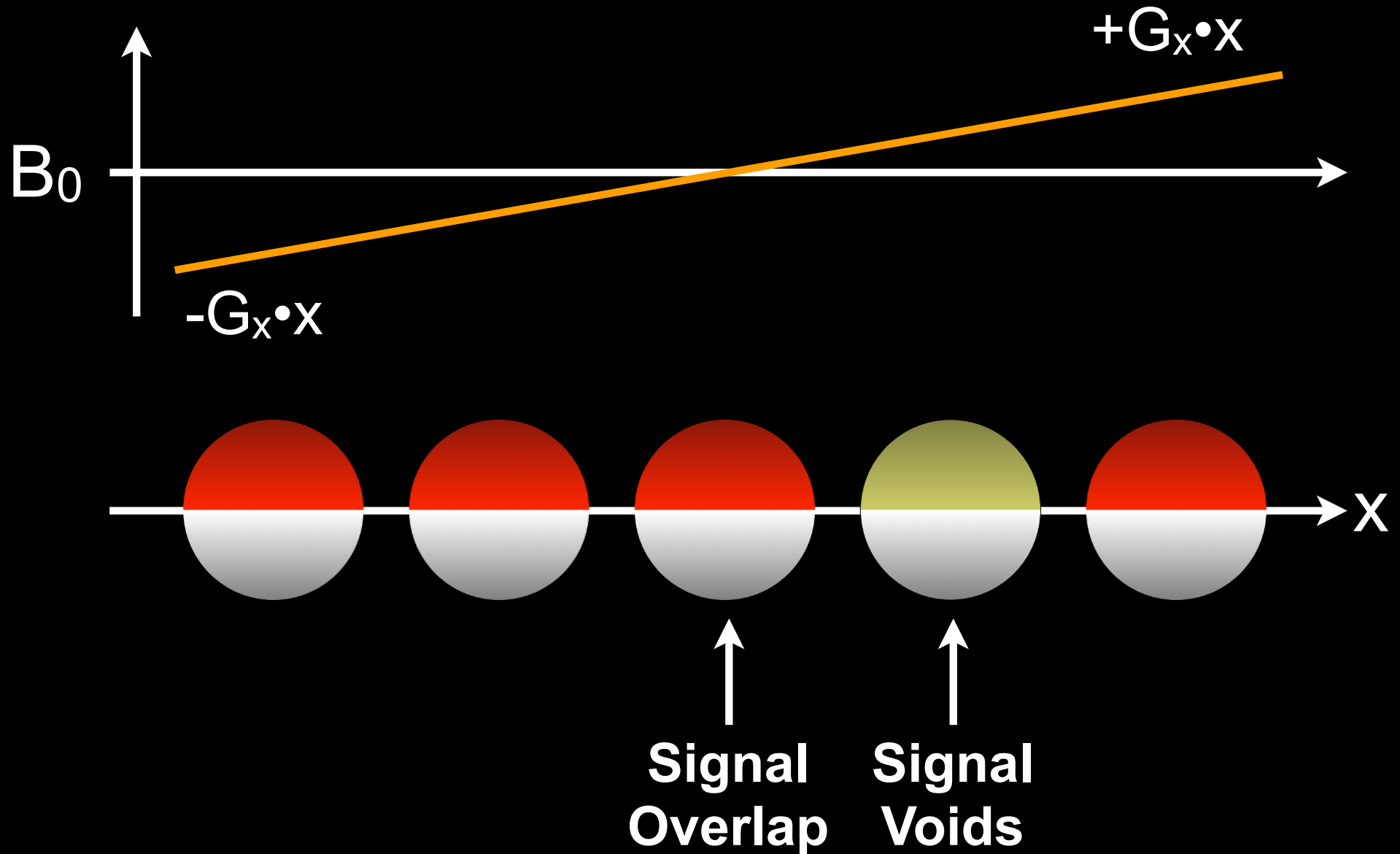


**Water & Fat Spins in a Gradient Field**

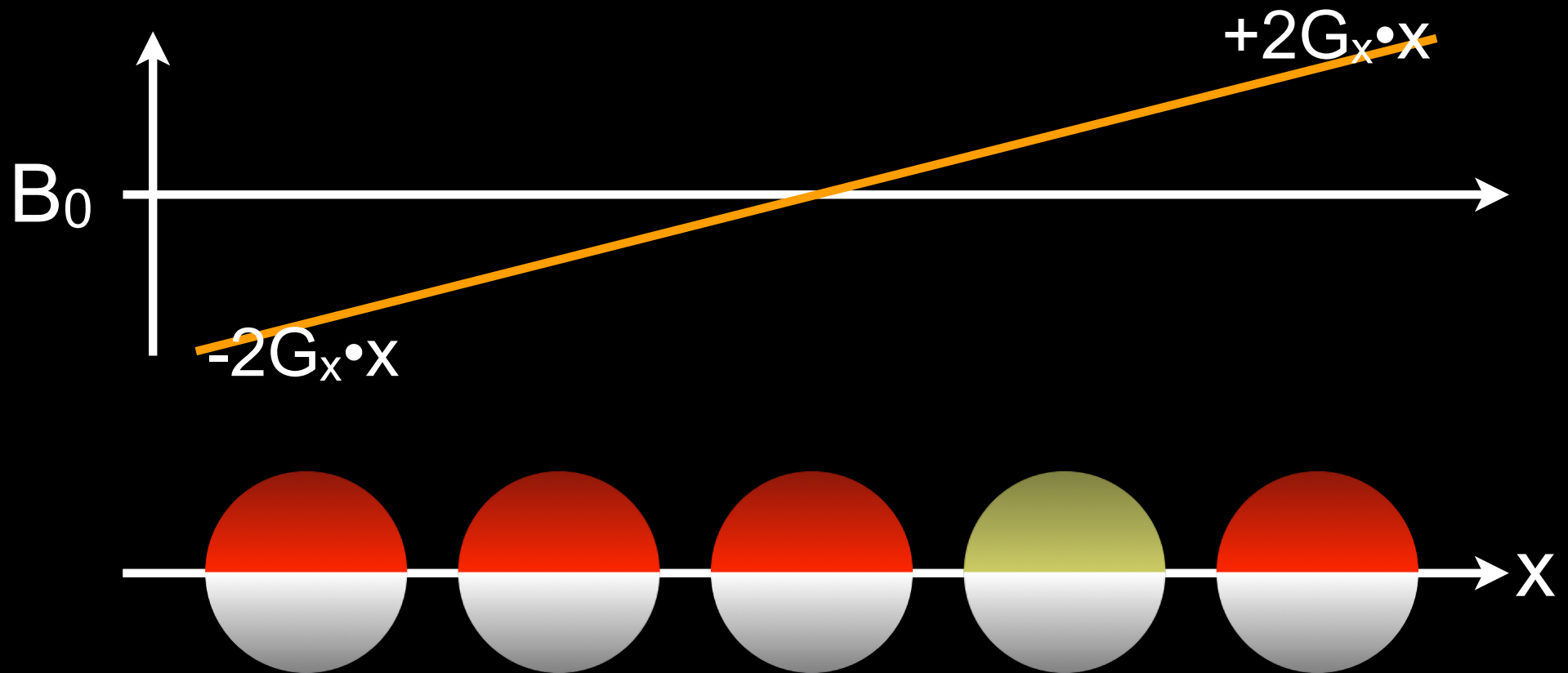
**Fat Spins ~220Hz slower than water @ 1.5T**

Spatial *position* is inferred from Larmor frequency.  
Chemical (frequency) shift produces an apparent spatial shift.

# GRE & Fat/Water Frequency

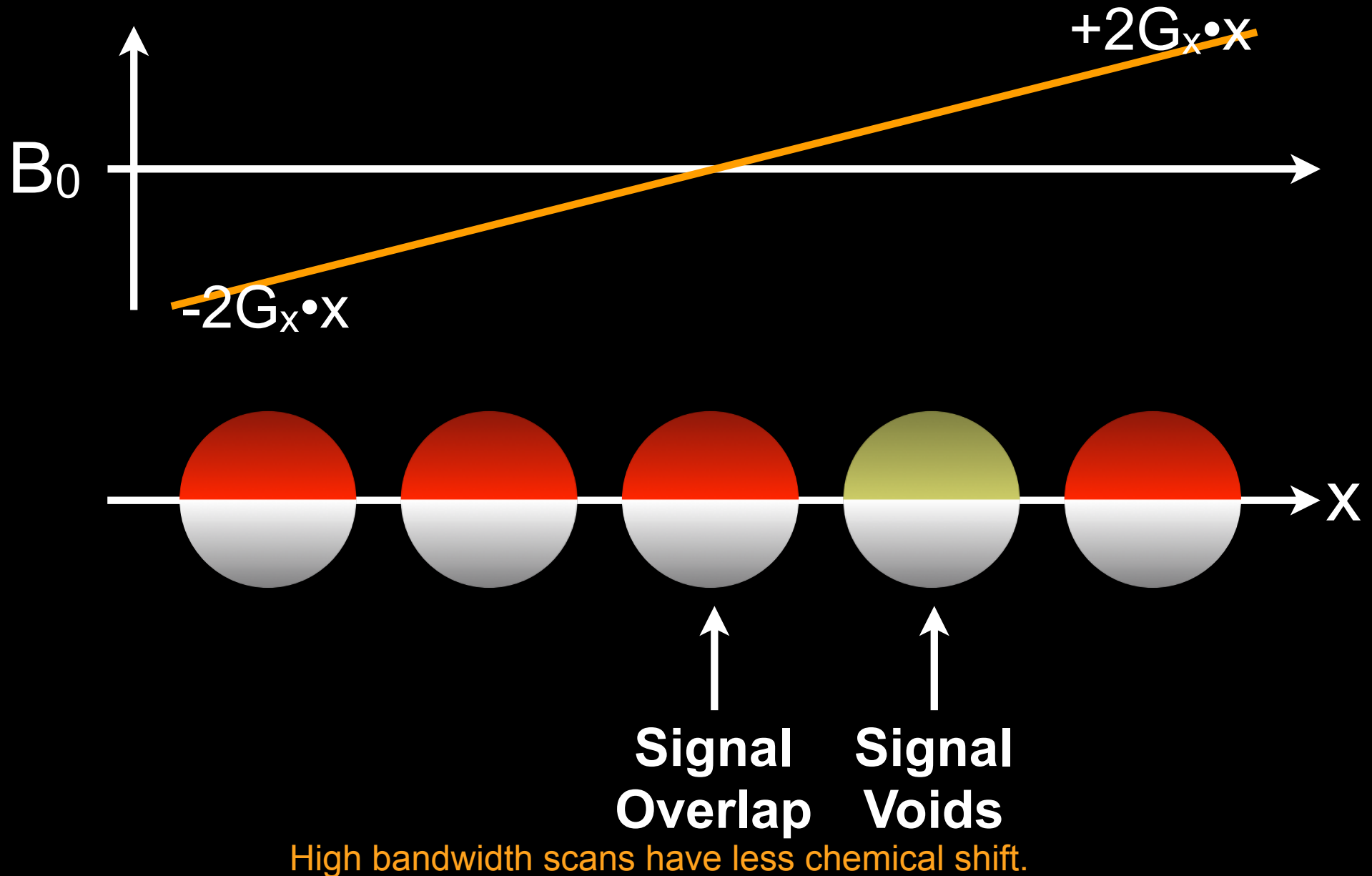


# GRE and Bandwidth



Higher bandwidths use stronger gradients and result in larger frequency differences along  $x$ . Chemical shift (frequency) is fixed for  $B_0$ , therefore chemical shift ( $\Delta x$ ) is a smaller percentage.

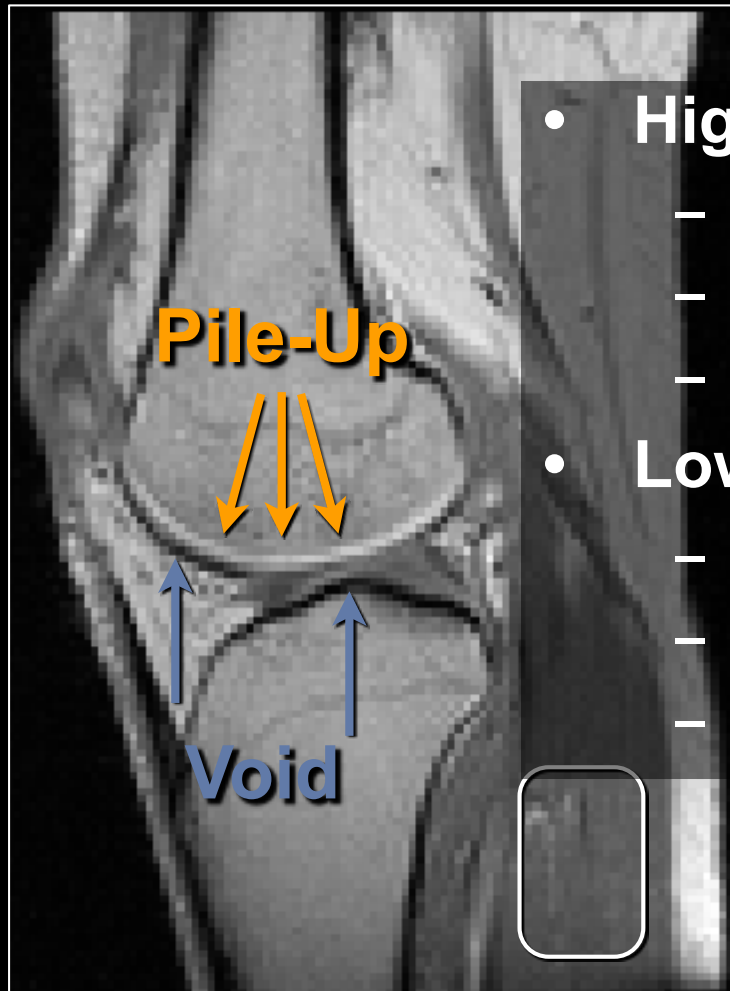
# GRE and Bandwidth



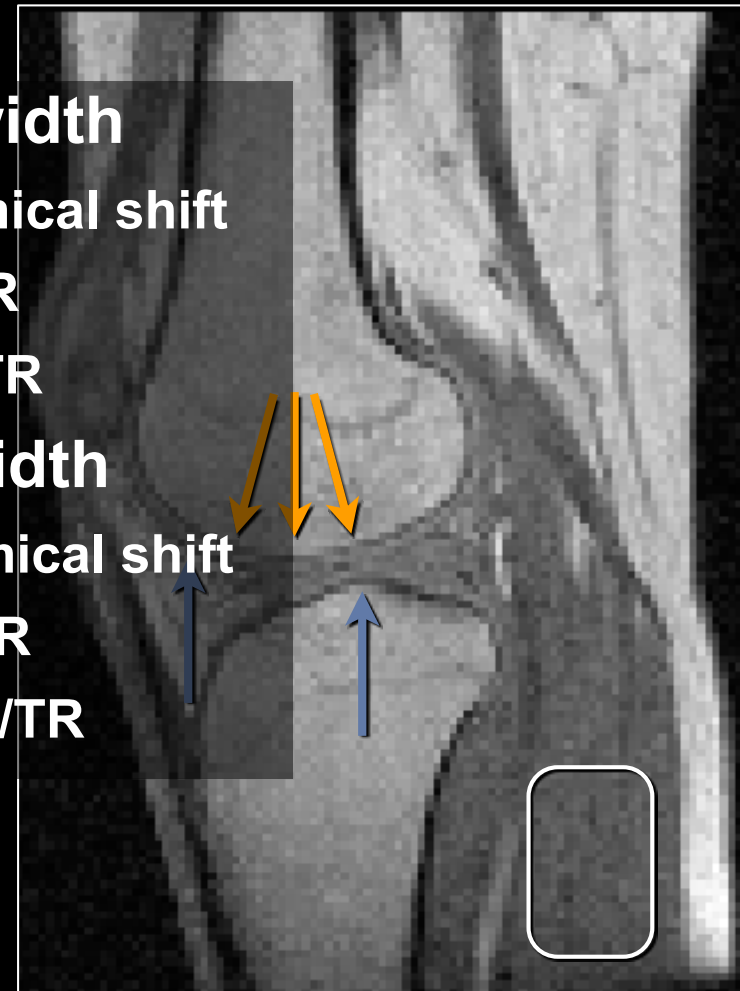
# GRE, Fat/Water & Bandwidth

Low Bandwidth

High Bandwidth



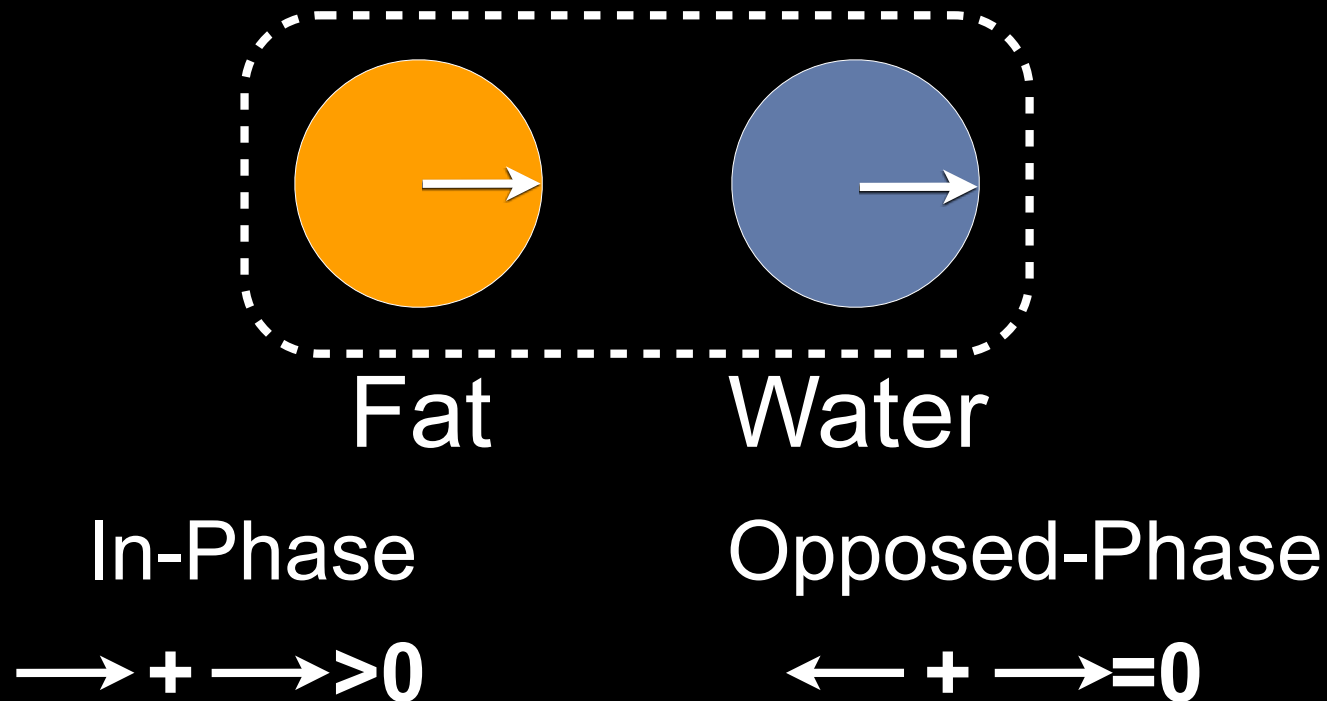
- High Bandwidth
  - Less chemical shift
  - Lower SNR
  - Short TE/TR
- Low Bandwidth
  - More chemical shift
  - Higher SNR
  - Longer TE/TR



Acquisition **bandwidth** is related to the **speed** with which an echo is acquired. If the **bandwidth** (speed) is high, then there is less time for chemical shift, less time for signal acquisition (lower SNR), and a shorter TE/TR.

# Chemical Shift - Type 2

- Pixels are frequently a mixture of fat and water
- Pixel intensity is the vector sum of fat and water

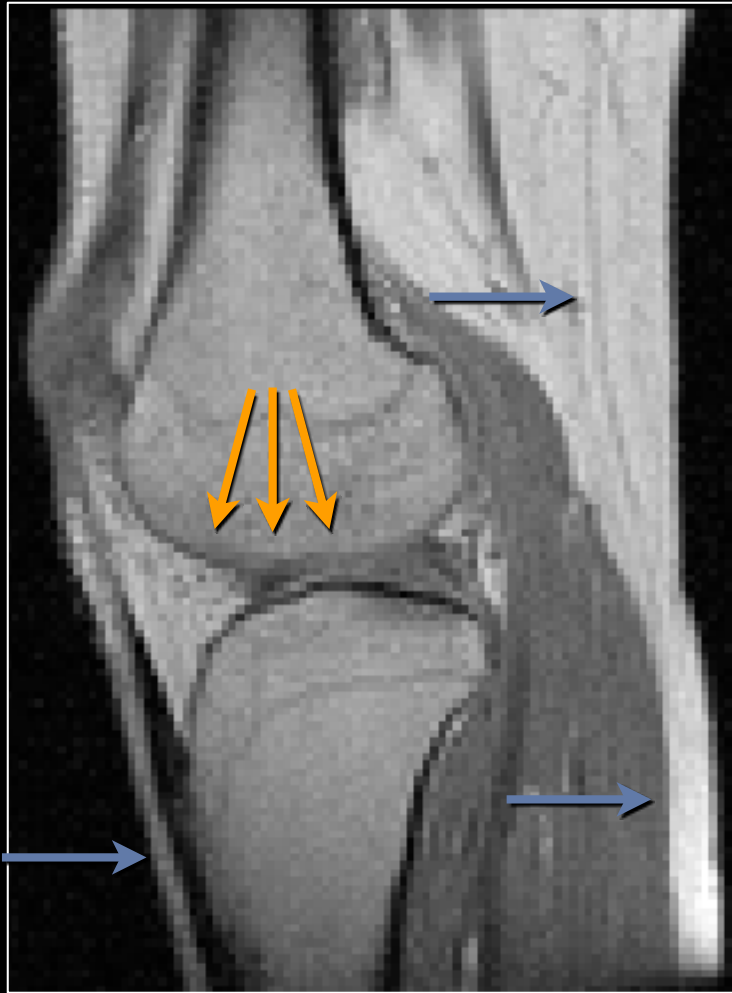


**The TE controls the phase between fat and water.**

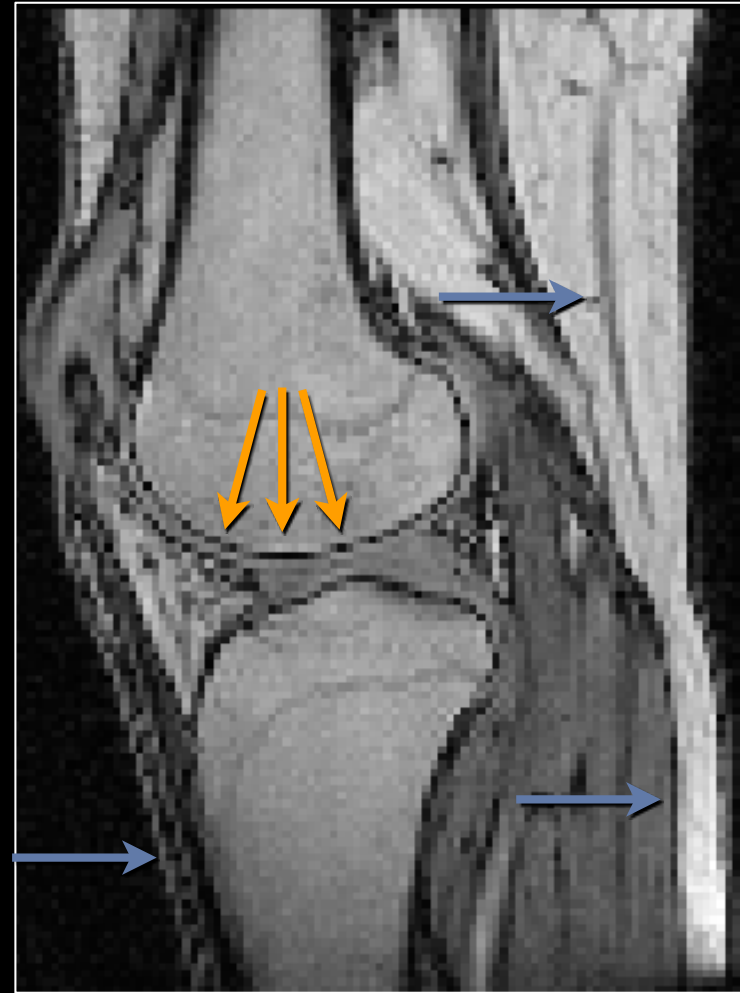


# GRE and Fat/Water Phase

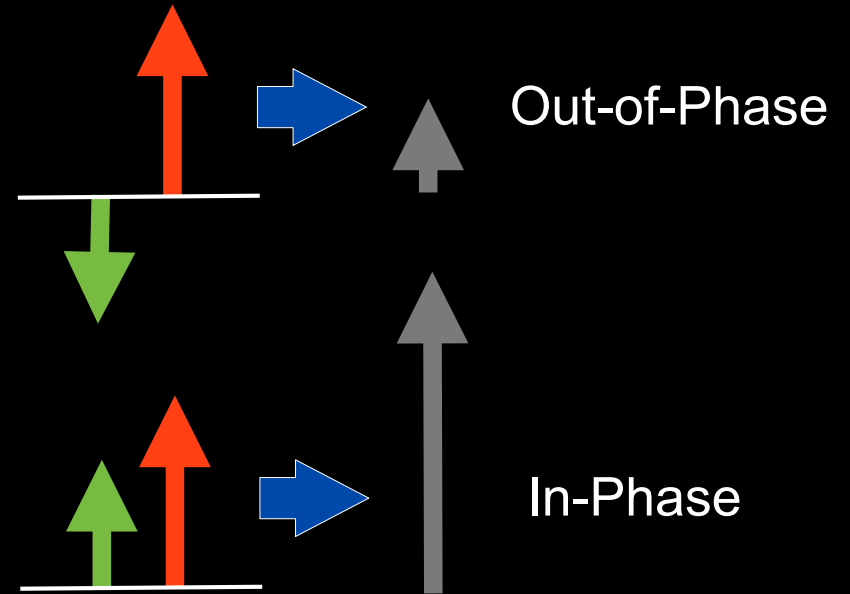
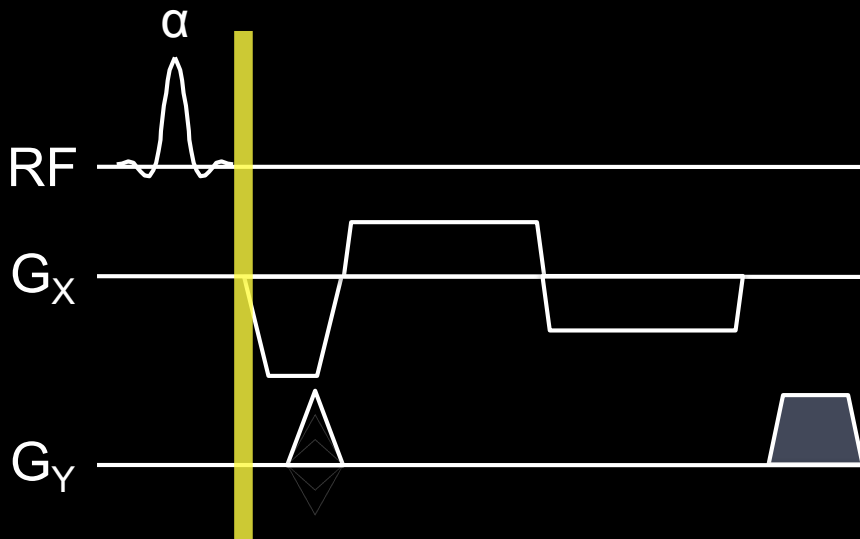
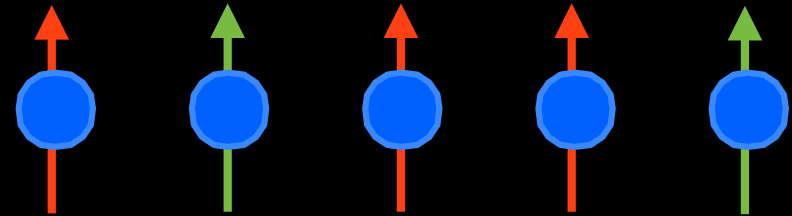
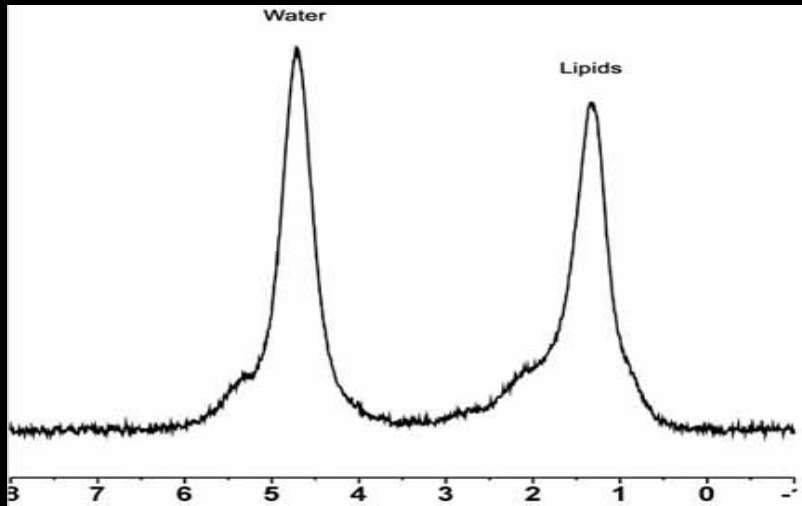
**In-Phase**



**Opposed-Phase**

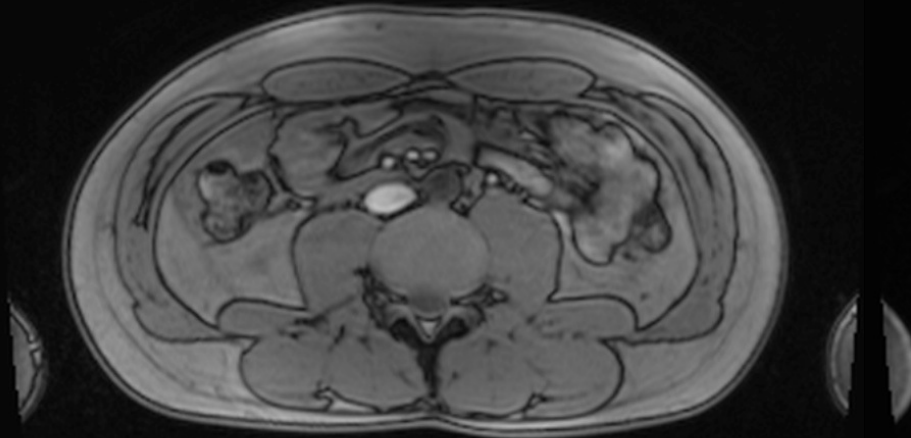


# Dual-Echo Acquisition

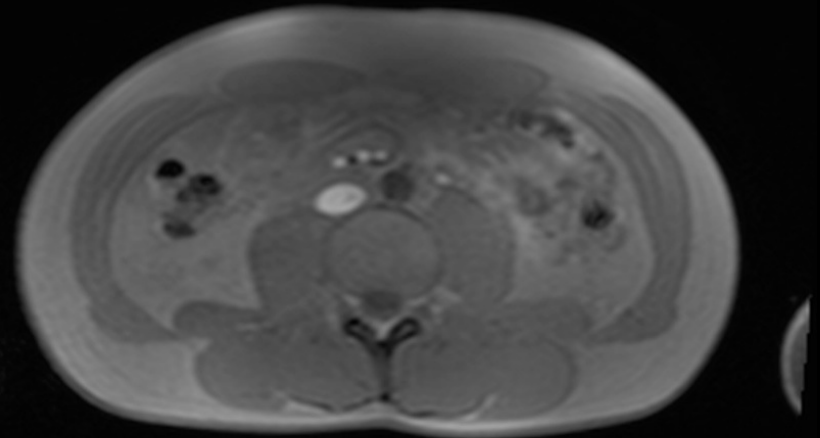


# In-phase and Out-of-phase

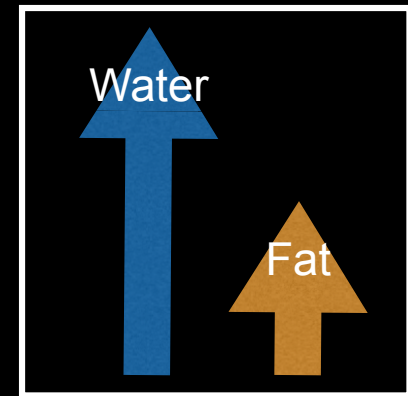
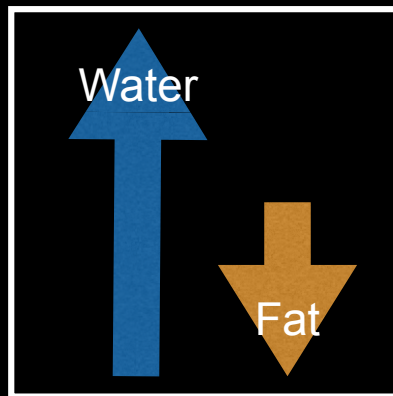
Example: 3 T abdominal scan



Out-of-phase (3 T), TE = 1.3 ms

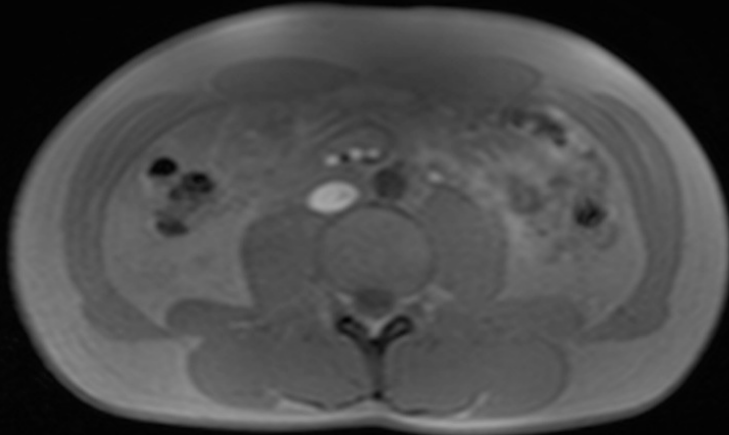


In-phase (3 T), TE = 2.6 ms

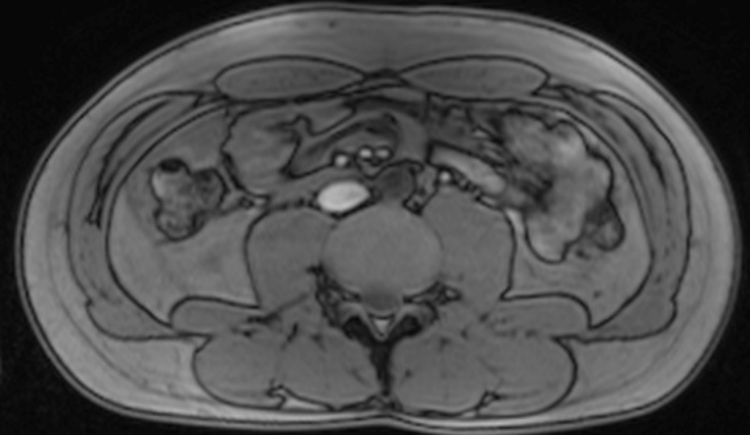


# 2-Point Dixon

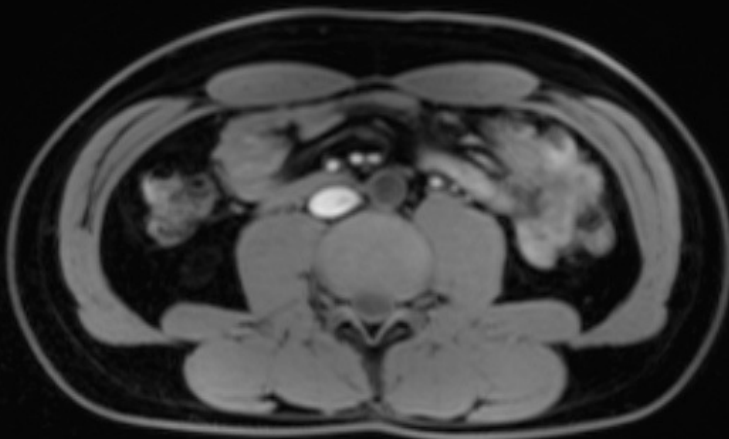
Example: 3 T abdominal scan



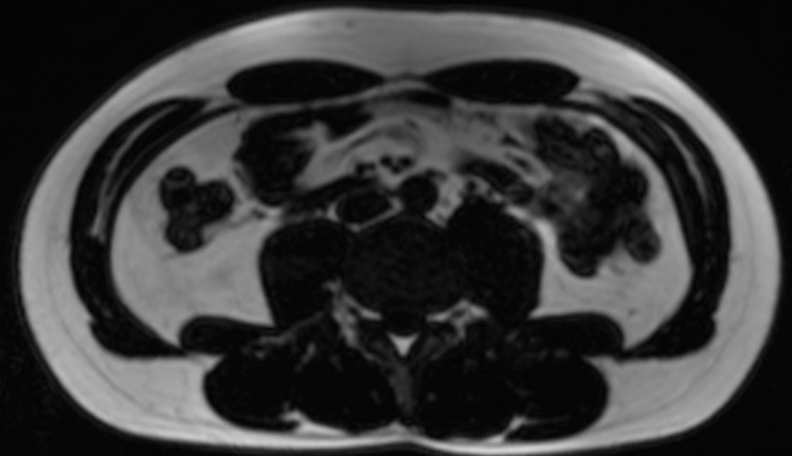
In-phase (3T), TE = 2.6 ms



Out-of-phase (3T), TE = 1.3 ms



Water



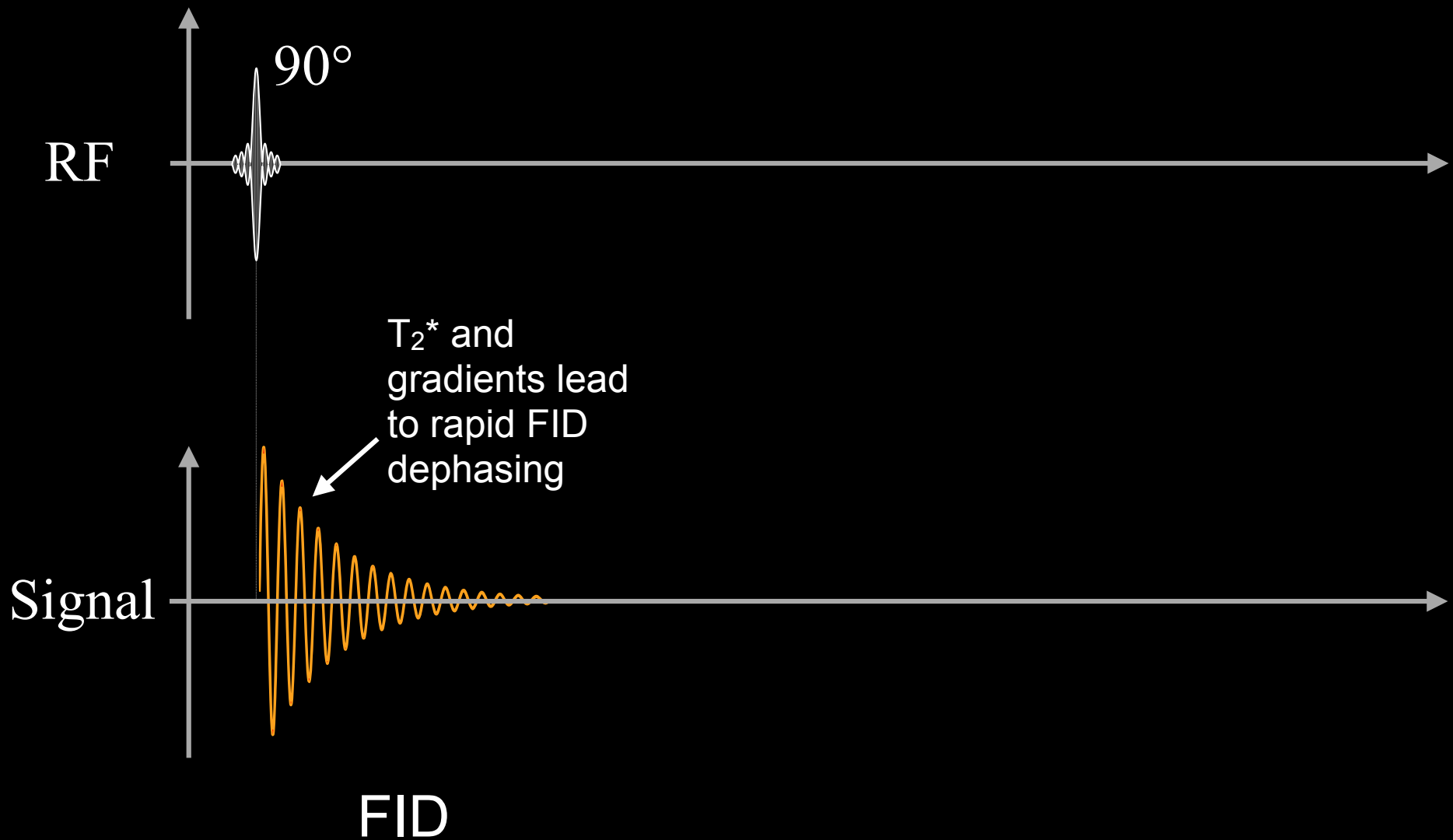
Fat

# Gradient Echo – Summary

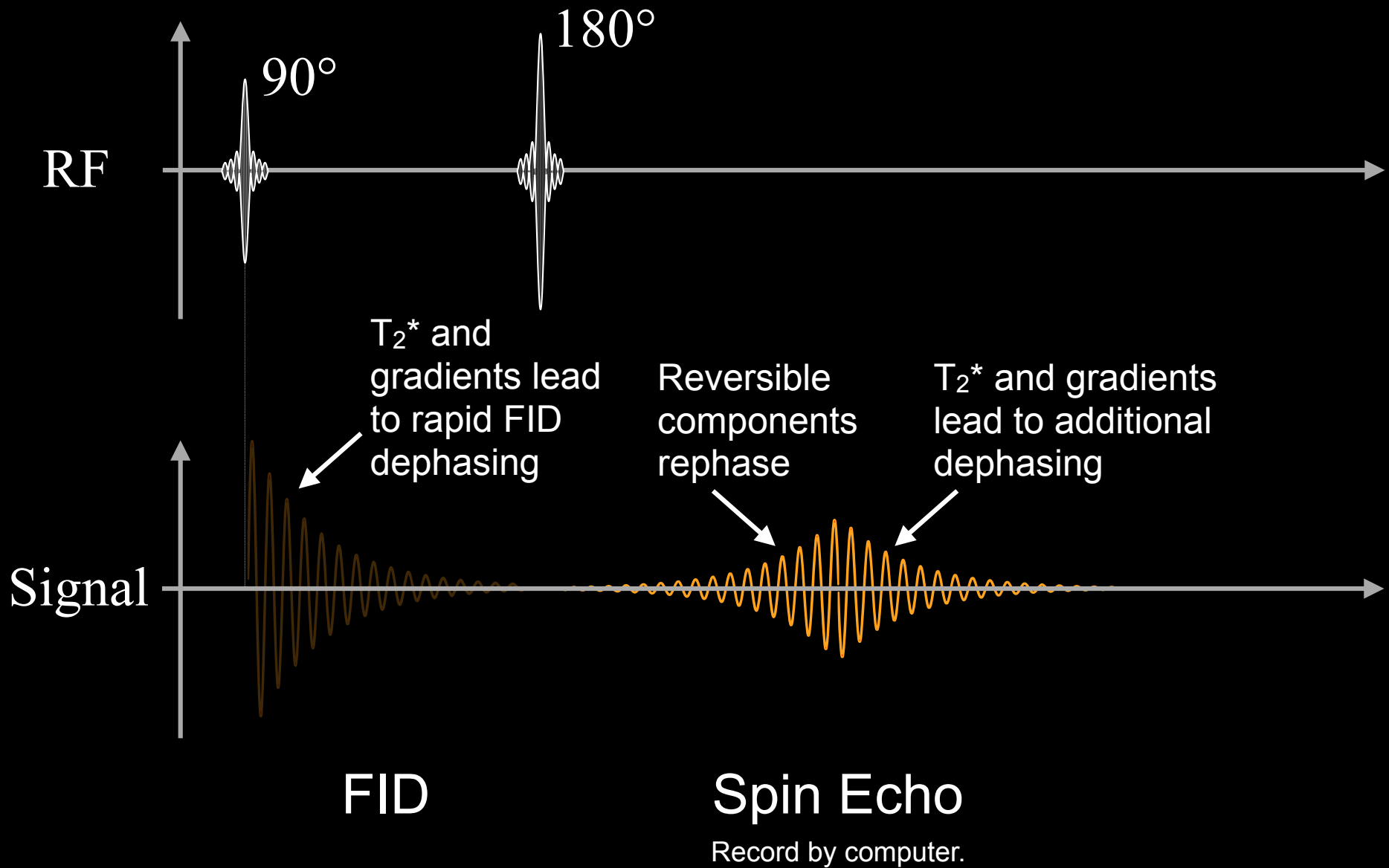
- Advantages
  - Fast Imaging Applications
  - Flexible contrast ( $T_1$  or  $T_2^*$ )
- Disadvantages
  - Off-resonance sensitivity
  - $T_2^*$ -weighted rather than  $T_2$ -weighted

# Spin Echo Imaging

# Free Induction Decay

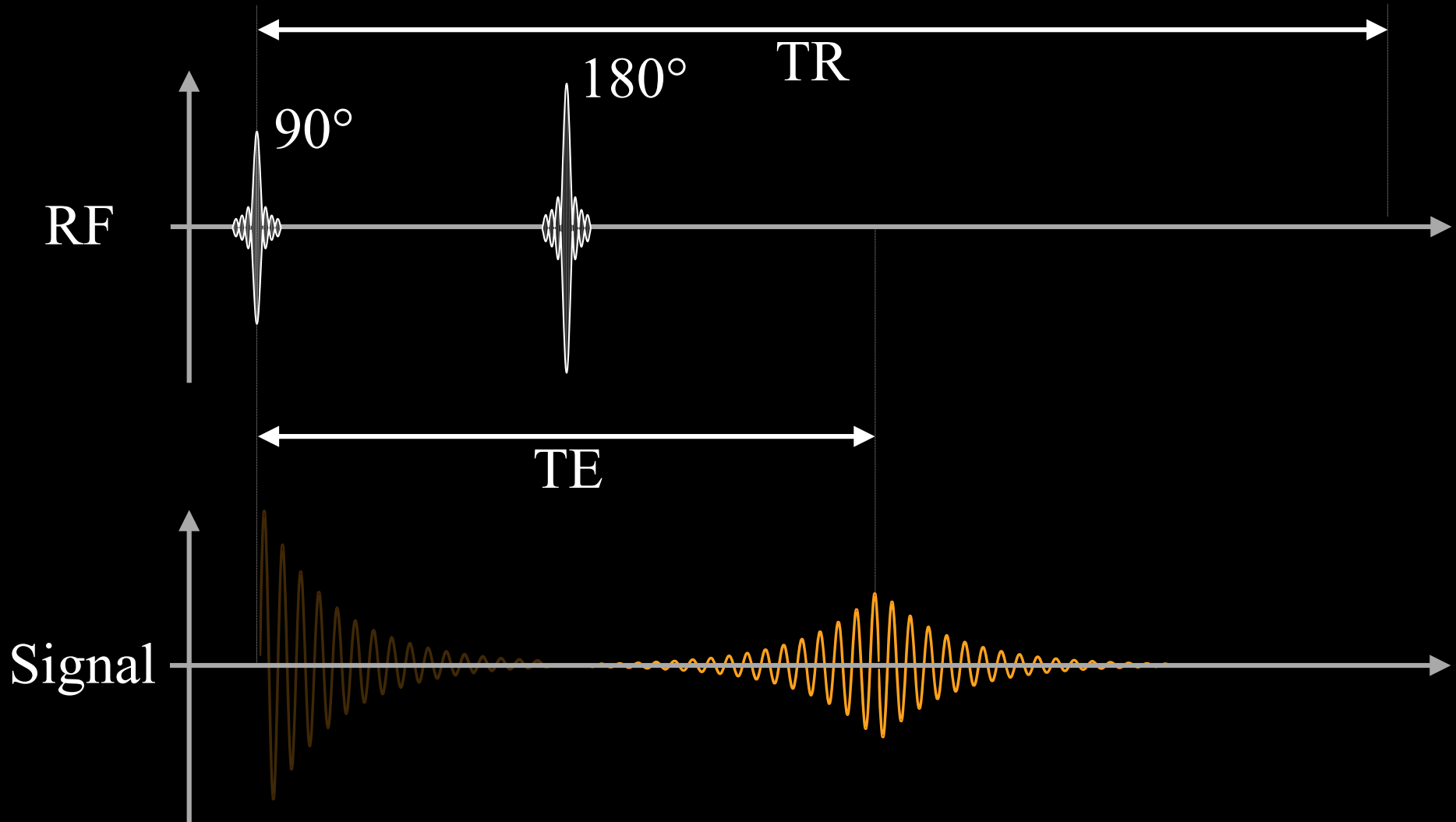


# Spin Echo





# Spin Echo



Signal

RF

$90^\circ$

$180^\circ$

TR

TE

FID

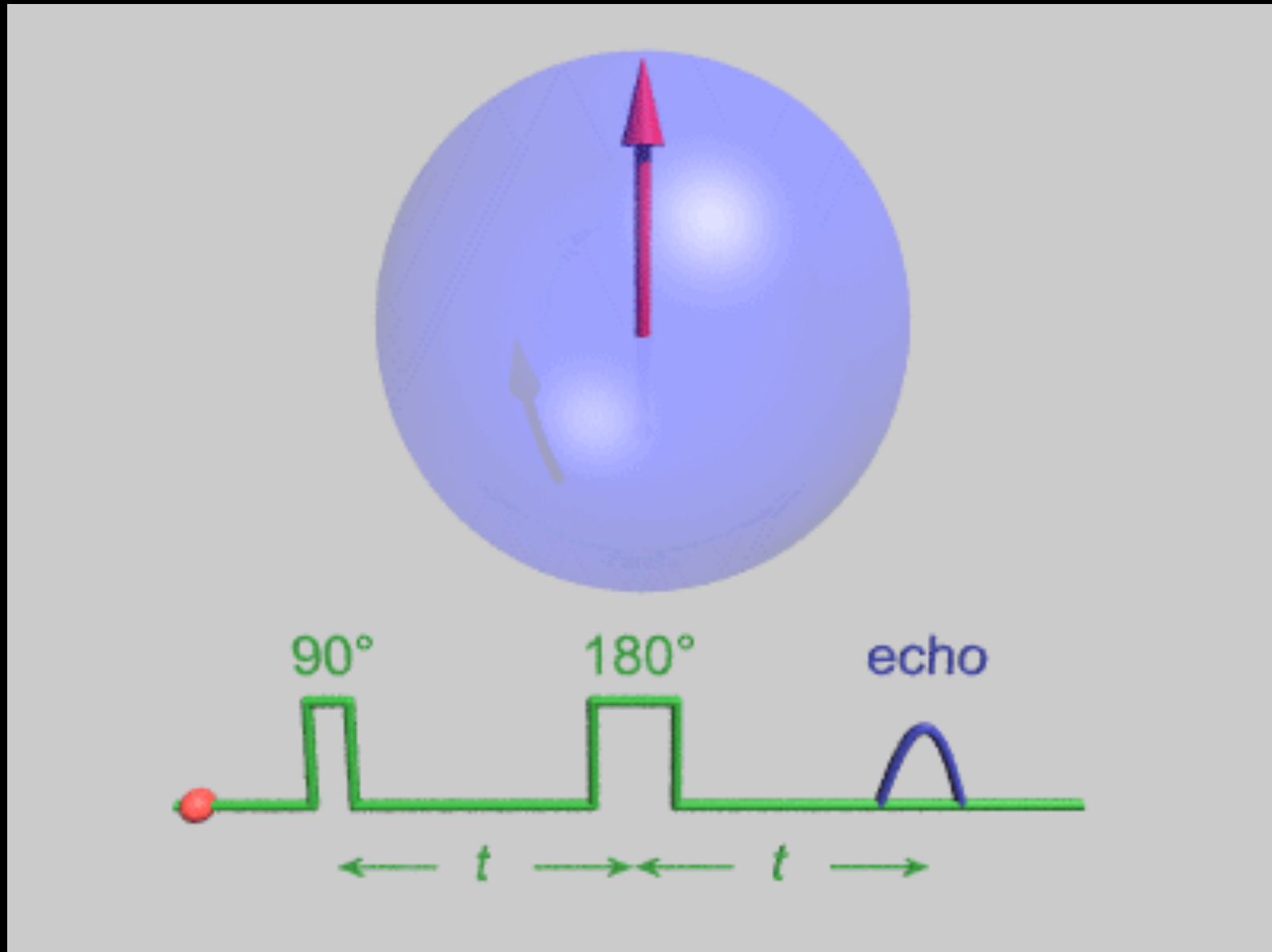
Spin Echo

Record by computer.

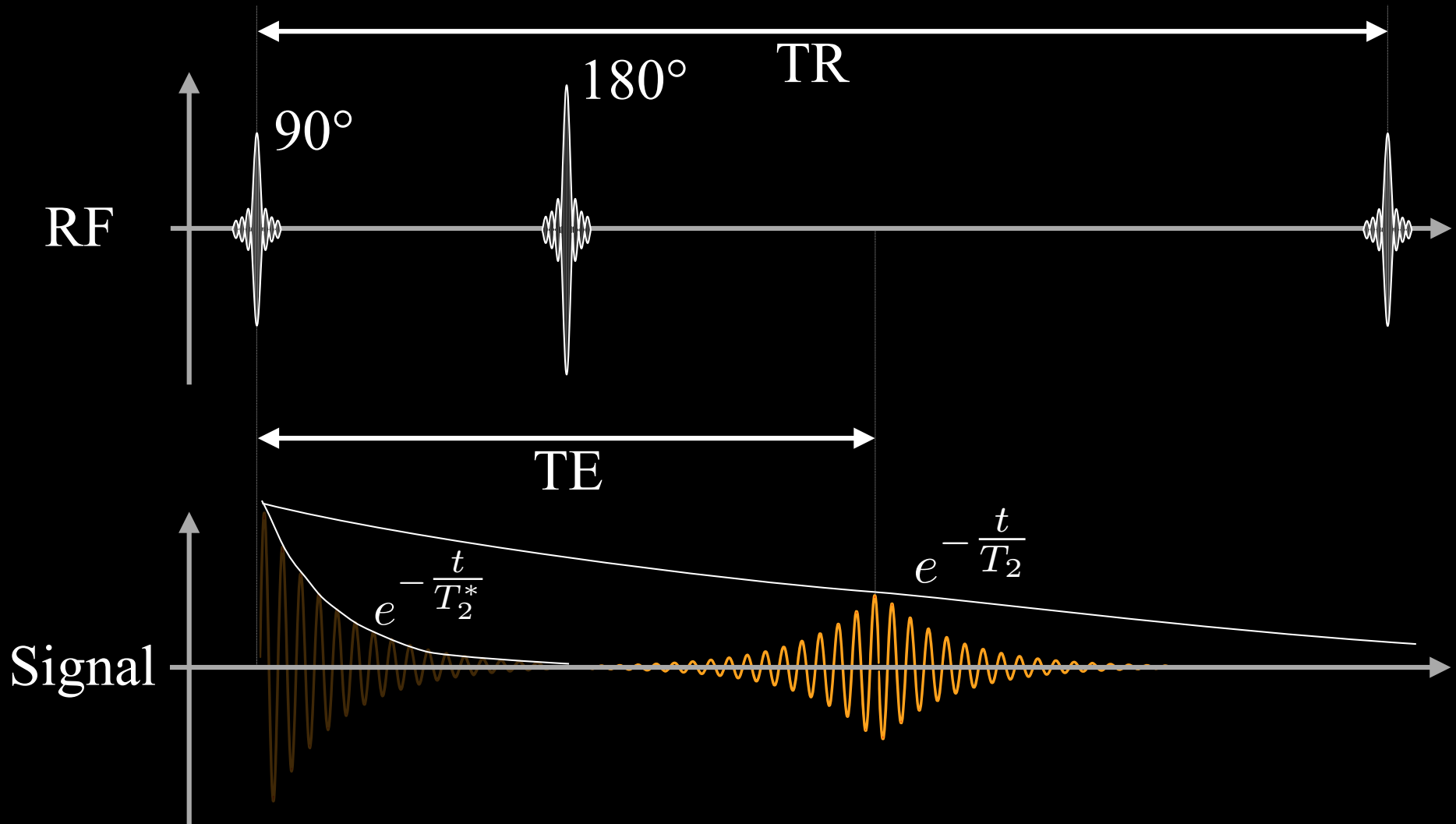
# Refocusing Pulses

- Typically, 180° RF Pulse
  - Provides optimally refocused  $M_{XY}$
  - Largest **spin echo** signal
- Refocus spin dephasing due to
  - imaging gradients
  - local magnetic field inhomogeneity
  - magnetic susceptibility variation
  - chemical shift

# Spin Echo - Refocusing



# Spin Echo - Contrast



How do you adjust the TR?  
How do you adjust the TE?

# Spin Echo Contrast

$$A_{Echo} \propto \rho \left( 1 - e^{-TR/T_1} \right) e^{-TE/T_2}$$

Longer TR  
minimizes  
T1 contrast

Short TE  
minimizes  
T2 contrast

Intermediate TR  
maximizes  
T1 contrast

Intermediate TE  
maximizes  
T2 contrast

# Spin Echo Contrast

$$A_{Echo} \propto \rho \left( 1 - e^{-TR/T_1} \right) e^{-TE/T_2}$$

Longer TR  
minimizes  
T1 contrast

Short TE  
minimizes  
T2 contrast

Intermediate TR  
maximizes  
T1 contrast

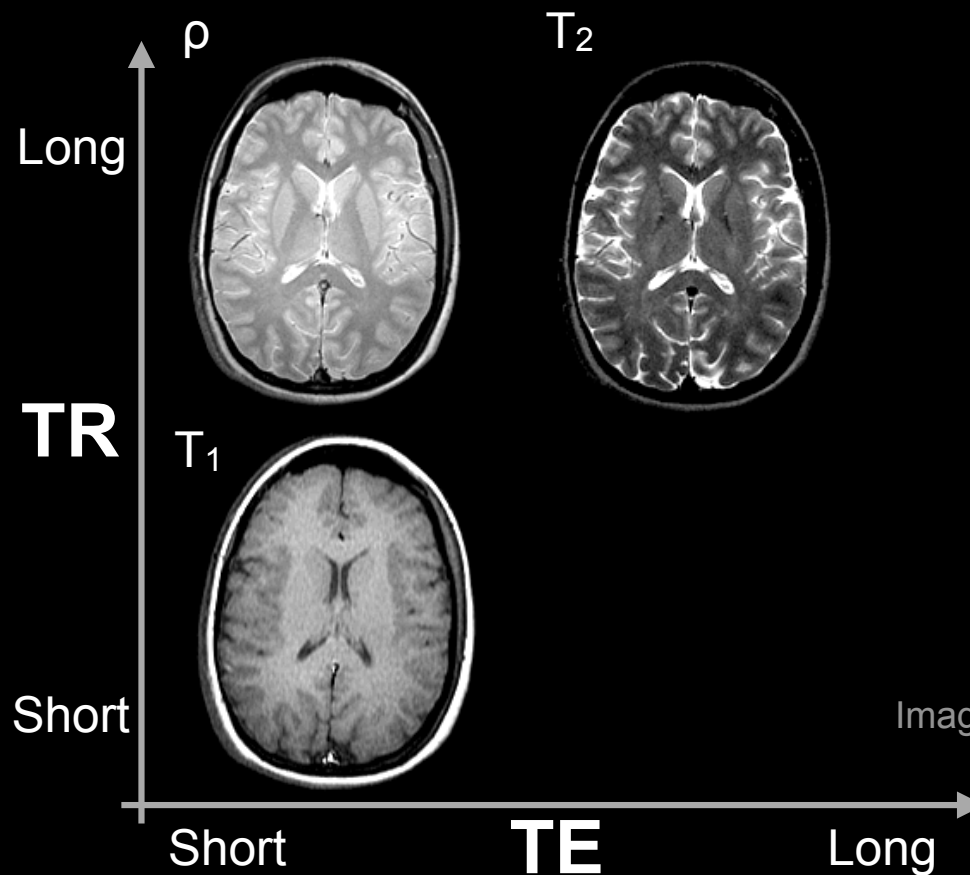
Intermediate TE  
maximizes  
T2 contrast

## Spin Echo Parameters

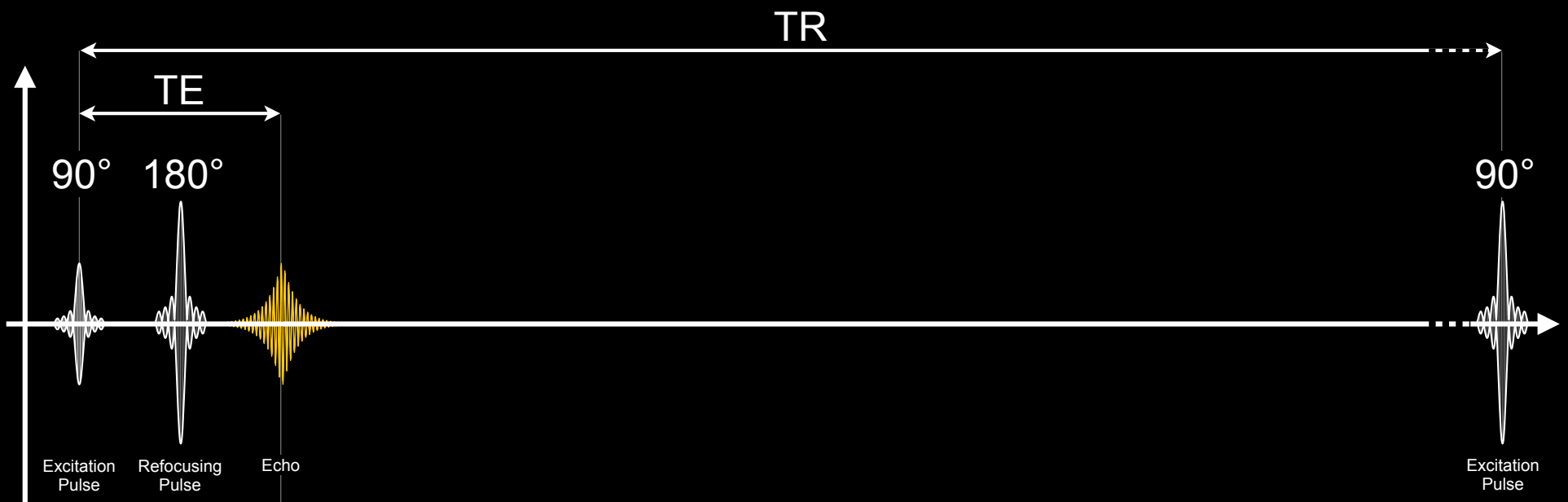
	TE	TR
<b>Spin Density</b>	Short	Long
<b>T<sub>1</sub>-Weighted</b>	Short	Intermediate
<b>T<sub>2</sub>-Weighted</b>	Intermediate	Long

# Spin Echo Contrast

	TE	TR
Spin Density	Short	Long
T <sub>1</sub> -Weighted	Short	Intermediate
T <sub>2</sub> -Weighted	Intermediate	Long



# Spin Echo

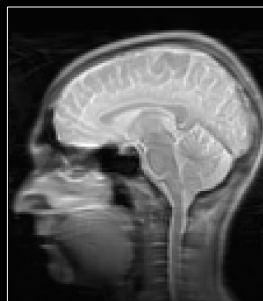
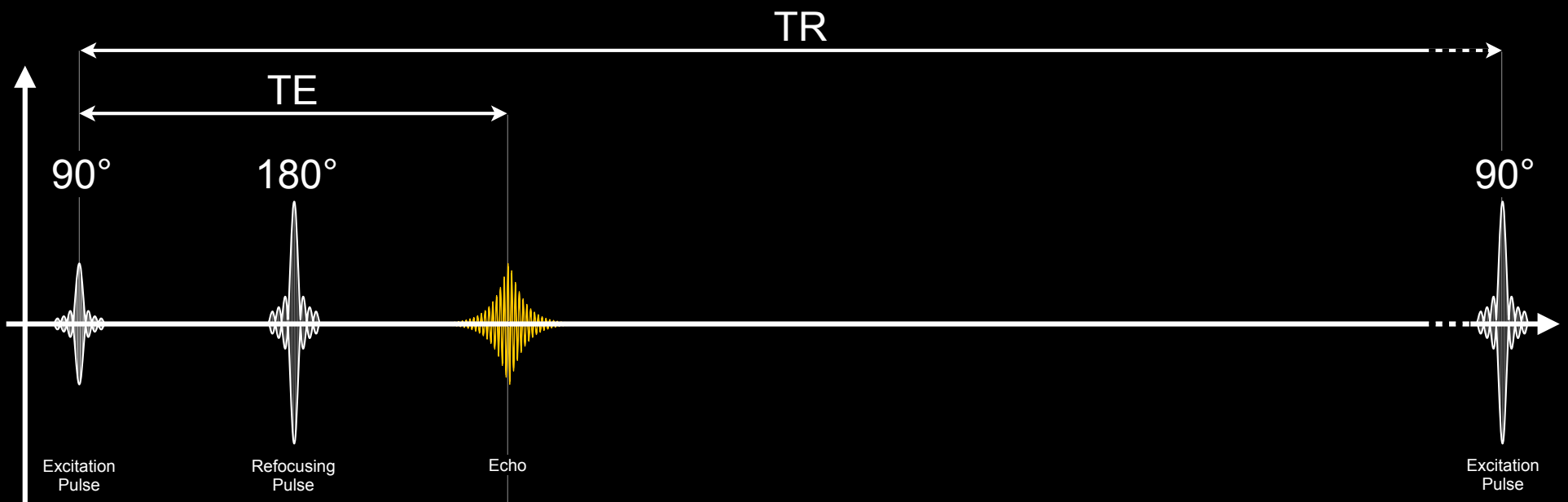


TE=12ms

Spin Echo: TR=6500ms (ETL=12)



# Spin Echo



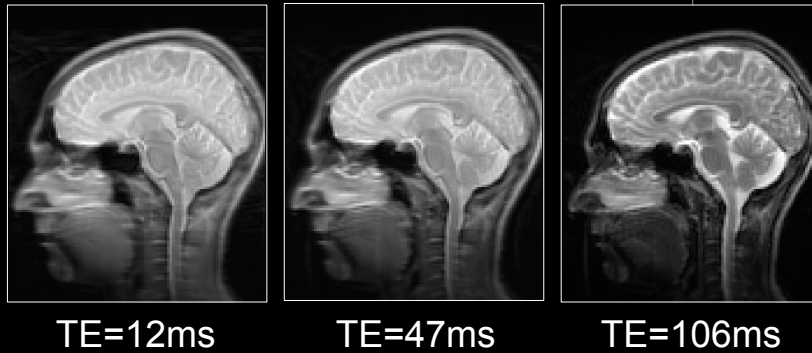
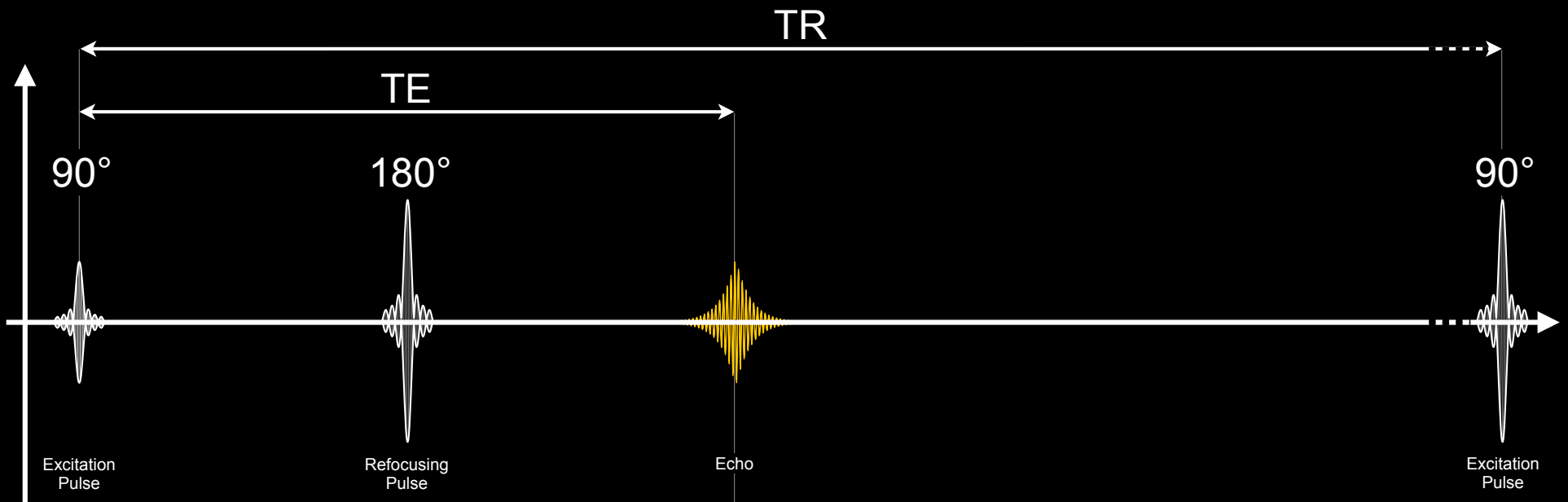
TE=12ms



TE=47ms

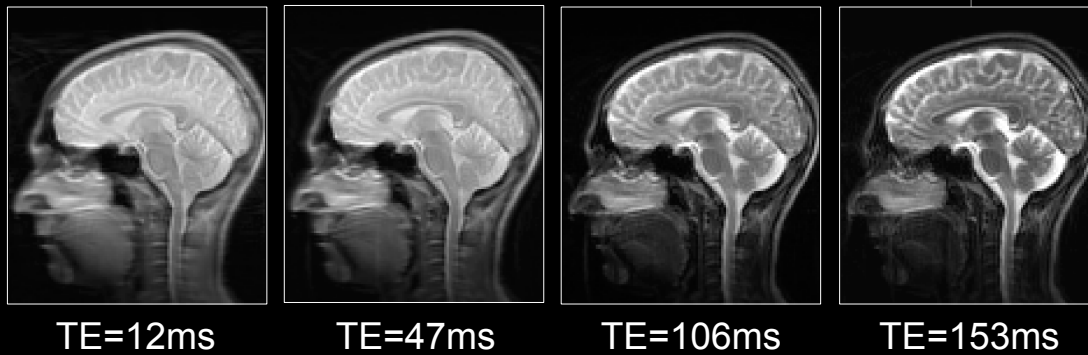
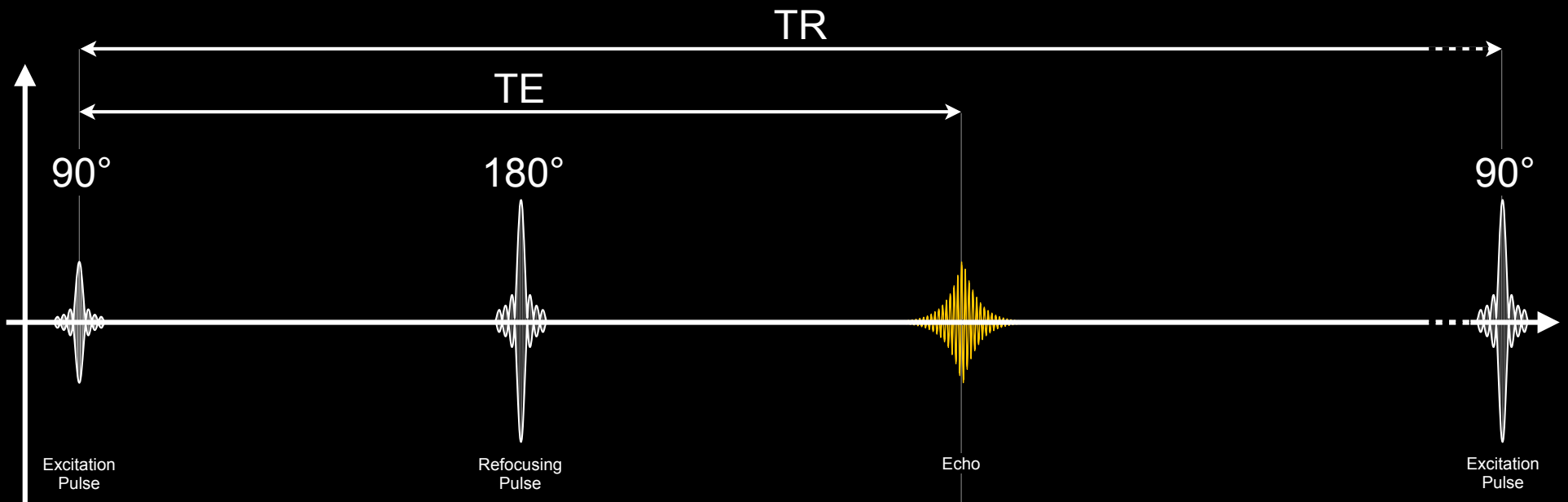
Spin Echo: TR=6500ms (ETL=12)

# Spin Echo



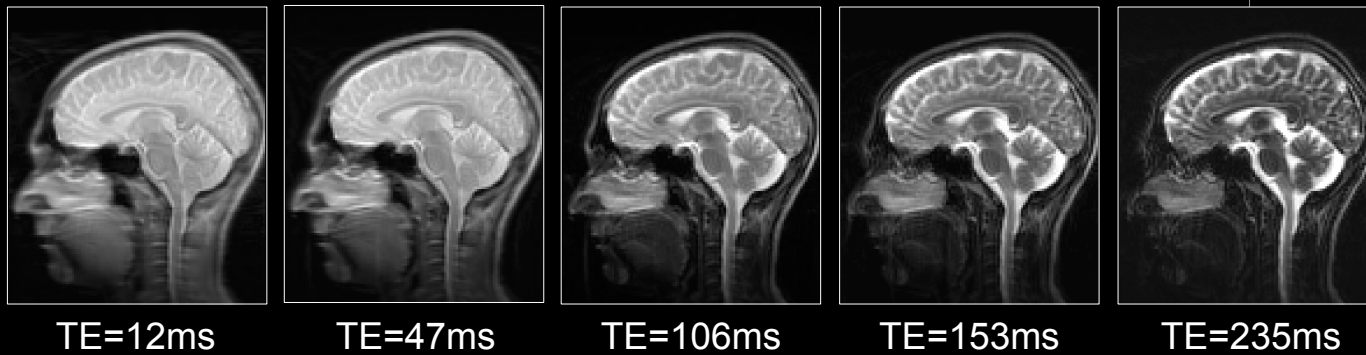
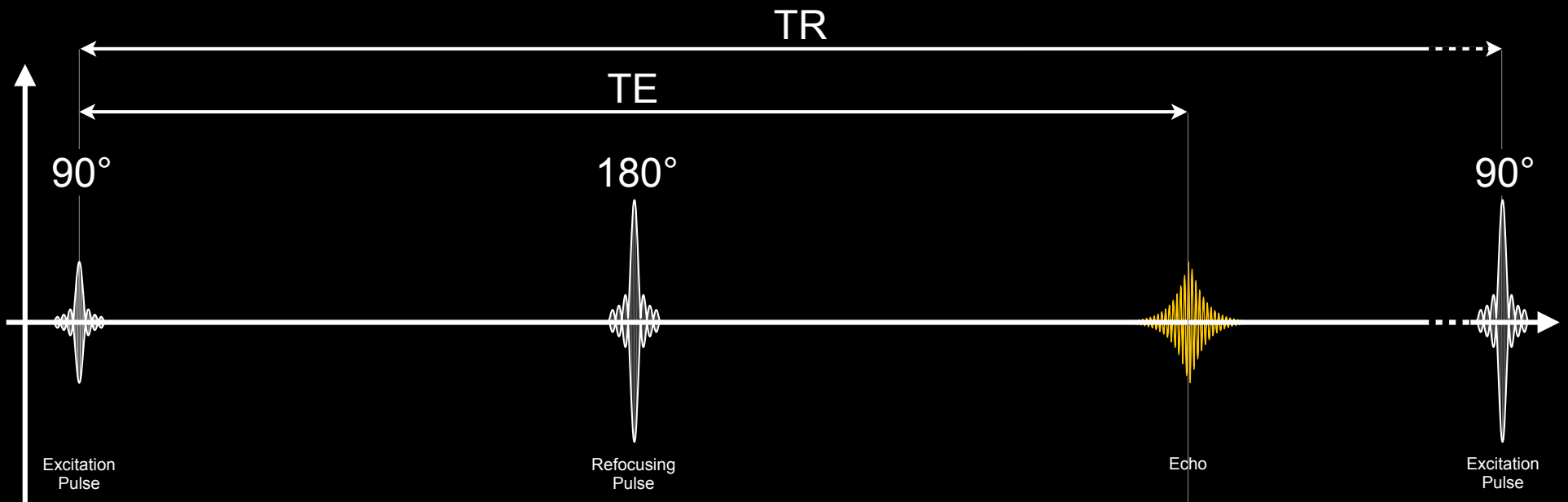
Spin Echo: TR=6500ms (ETL=12)

# Spin Echo



Spin Echo: TR=6500ms (ETL=12)

# Spin Echo



Spin Echo: TR=6500ms (ETL=12)

# Spin Echo

- Advantages
  - Insensitive to off-resonance
    - Re-focusing rephrases spin dephasing
  - Great for  $T_1$ ,  $T_2$ ,  $\rho$  contrast (not  $T_2^*$ )
  - High SNR
- Disadvantages
  - TR can be long
    - Leads to long scan time
  - SAR can be high
    - Lots of 90s and 180s lead to patient heating

# Questions?

- Related reading materials
  - Nishimura - Chap 7

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