

MRI Systems I: B0 and Bulk Magnetization

M219 - Principles and Applications of MRI

Kyung Sung, Ph.D.

1/10/2024

Course Overview

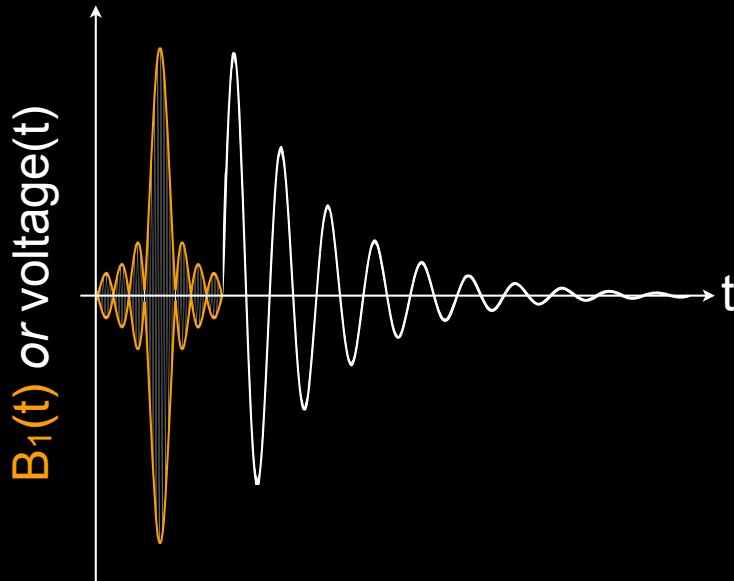
- Course website
 - <https://mrrl.ucla.edu/pages/m219>
- 2024 course schedule
 - https://mrrl.ucla.edu/pages/m219_2024
- Assignments
 - Homework #1 will be out on 1/15 (due on 1/29)
- Office hours, Fridays 10-12pm
 - In-person (Ueberroth, 1417B)
 - Zoom is also available

What is MRI?

- Magnetic
 - We need a big magnet
- Resonance
 - Excitation energy has to be on-resonance
- Imaging
 - We can make pretty pictures

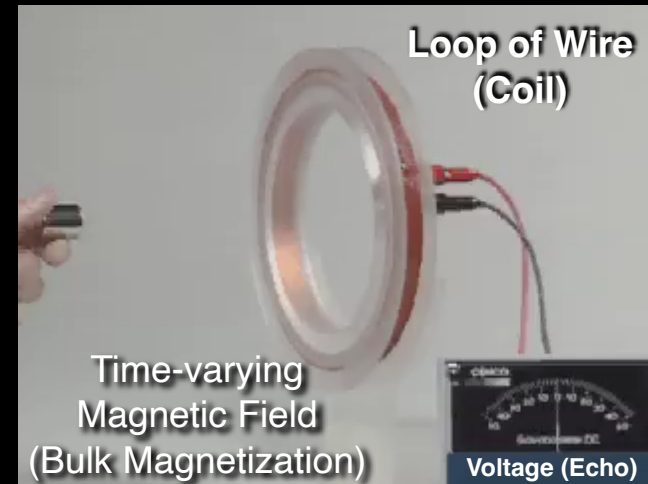
What is MRI?

MRI follows a classic excitation-reception paradigm.



Excitation
(RF Pulse)

Reception
(FID or **Echo**)



Faraday's Law of Induction

MRI encodes spatial information and image contrast in the echo.

Requirements for MRI

- NMR Active Nuclei
 - e.g. ^1H in H_2O
- Magnetic Field (B_0): Polarizer
- RF System (B_1): Exciter
- Coil: Receiver
- Gradients (G_x, G_y, G_z): Spatial Encoding

MRI Hardware

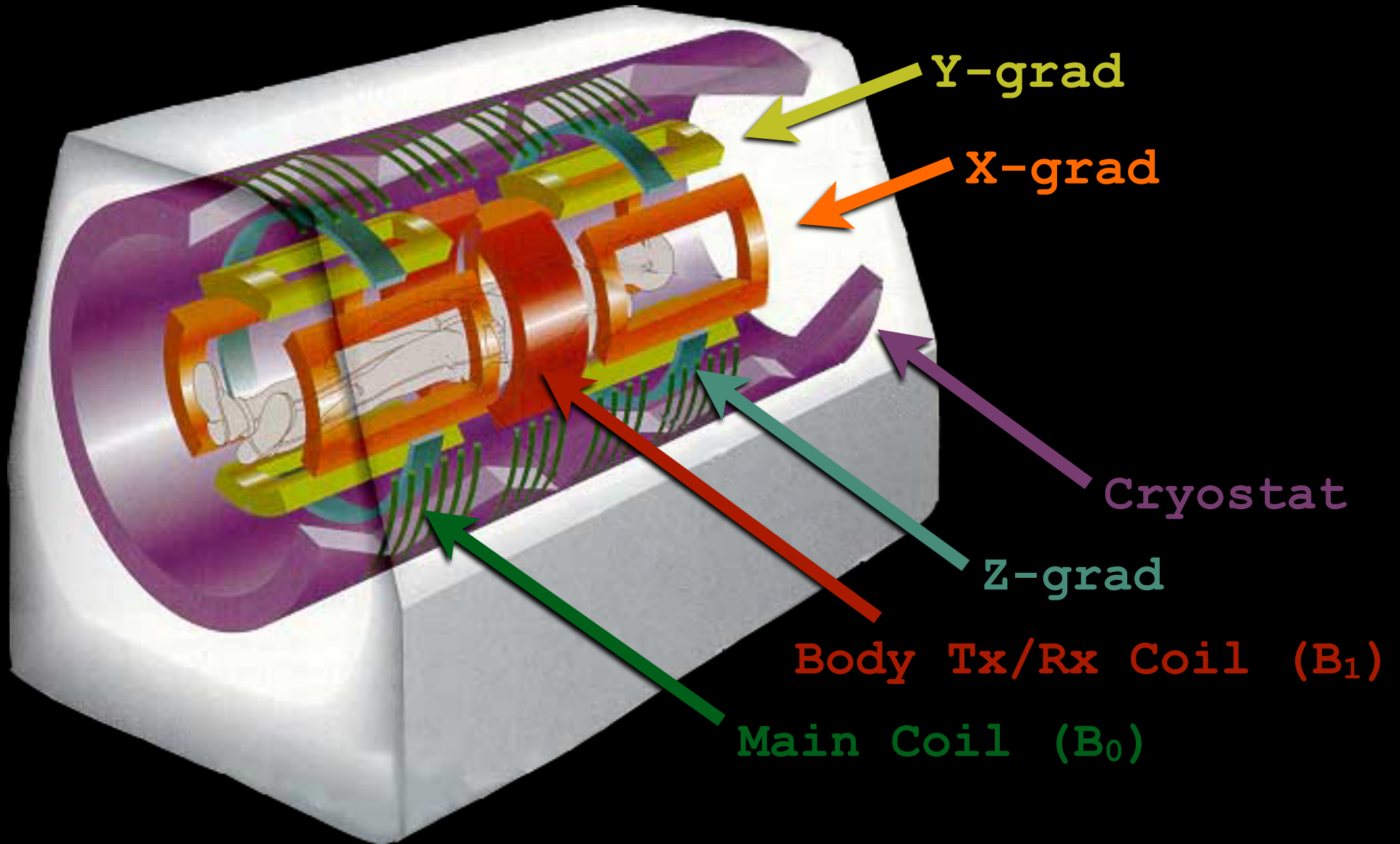


Image Adapted From: <http://www.ee.duke.edu/~jshorey>

MRI Advantages

Soft Tissue Contrast



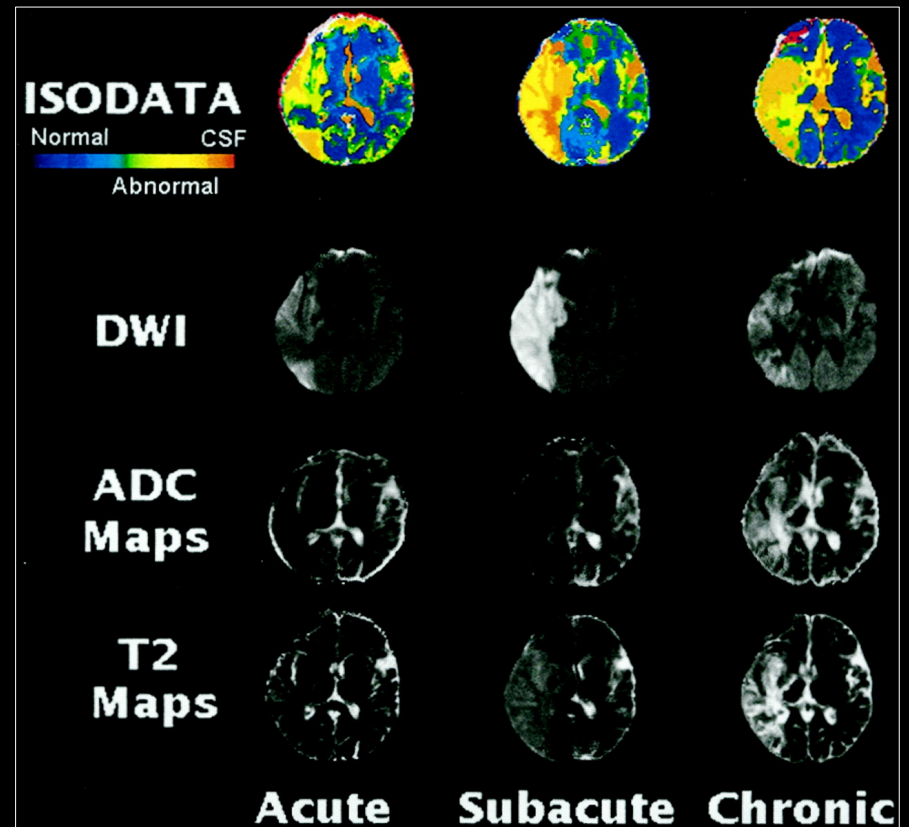
Tissue Characterization

- **Routine**

- T₁, T₂, T₂^{*}, proton weighted
- Perfusion
- Diffusion
- Contrast enhancement
 - Tumor evaluation

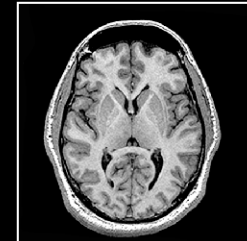
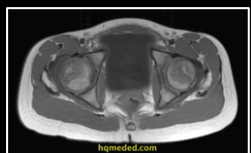
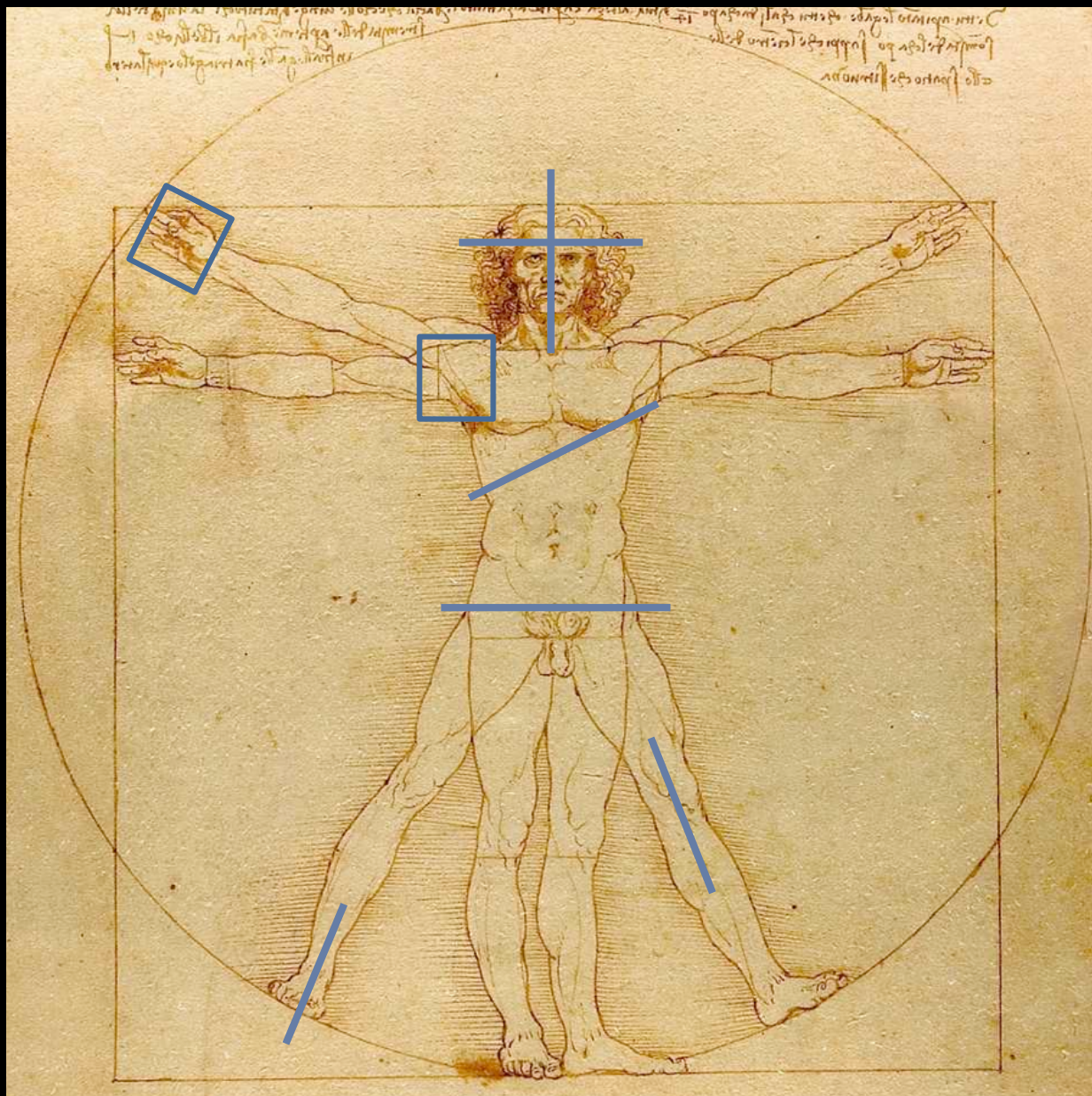
- **Advanced**

- T1- and T2-mapping
- Fat/Water & Iron quantification
- Spectroscopy (molecular)
- Susceptibility weighted imaging (SWI) for blood products and calcium
- Non-contrast angiography



Demonstration of the multiparametric ISODATA segmentation methodology and corresponding DWI (b=1000 s/mm²), ADC map, and T2 map at different times after stroke. *Jacobs M A et al. Stroke. 2001;32:950-957*

Arbitrary Imaging Planes



No Ionizing Radiation

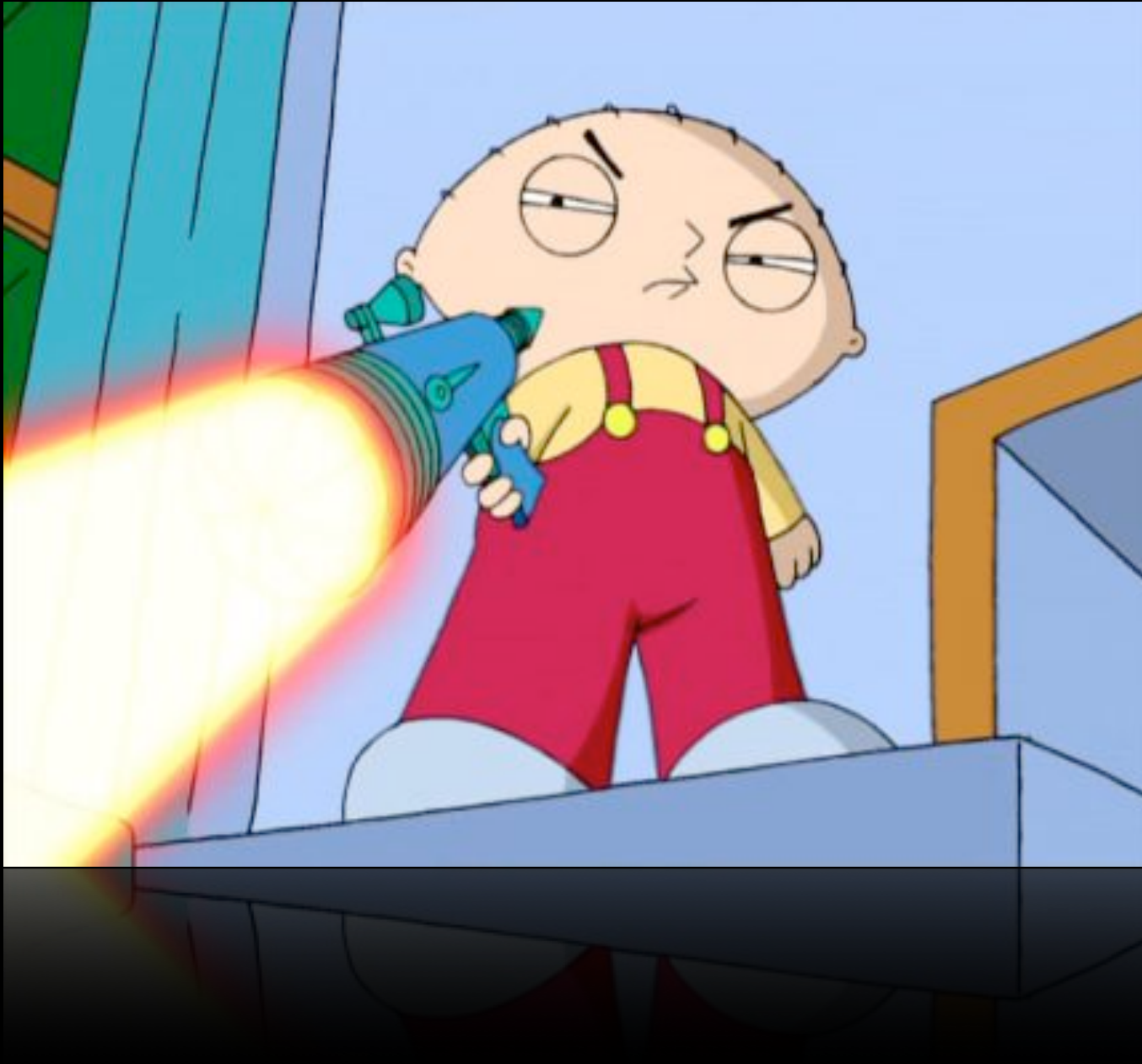
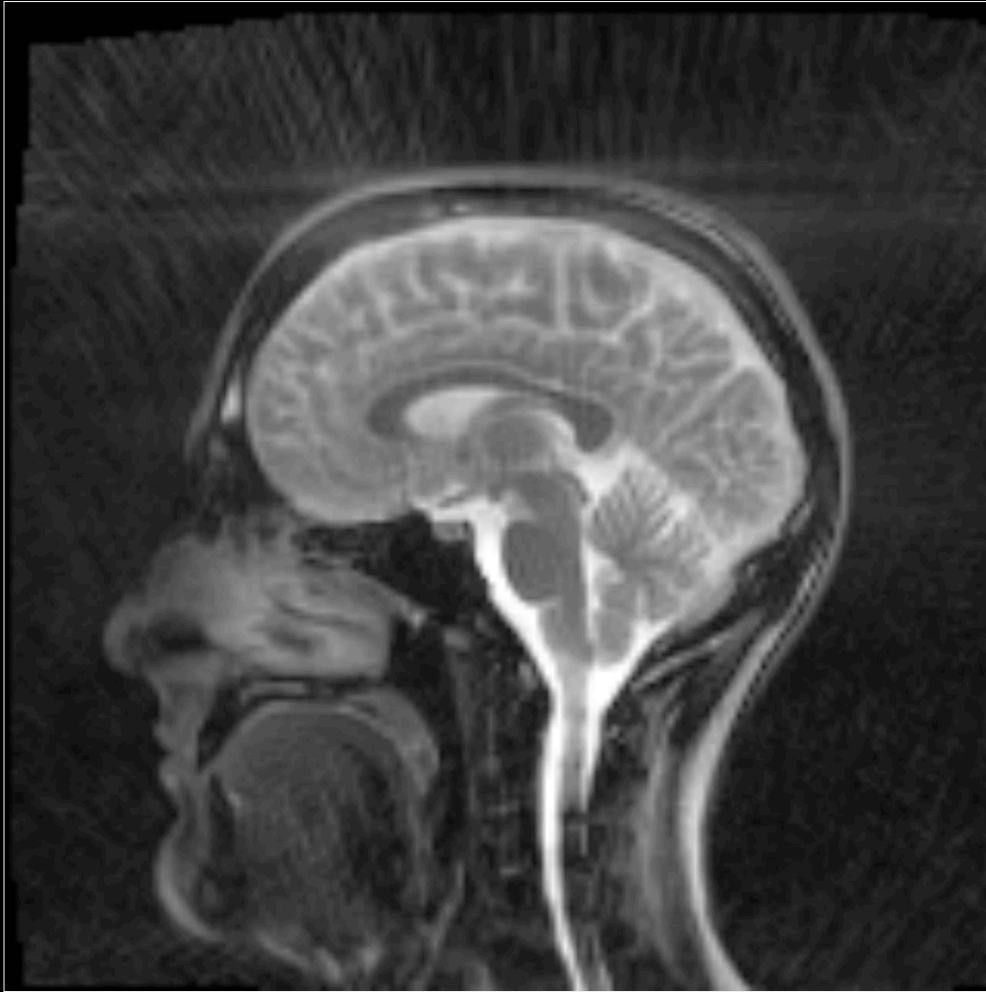


Image Physiologic Motion



Nuclear Spin

Classical View

Atoms having odd #
of protons and/or
neutrons



Spin angular
momentum

$$\vec{S} = \hbar \vec{I}$$

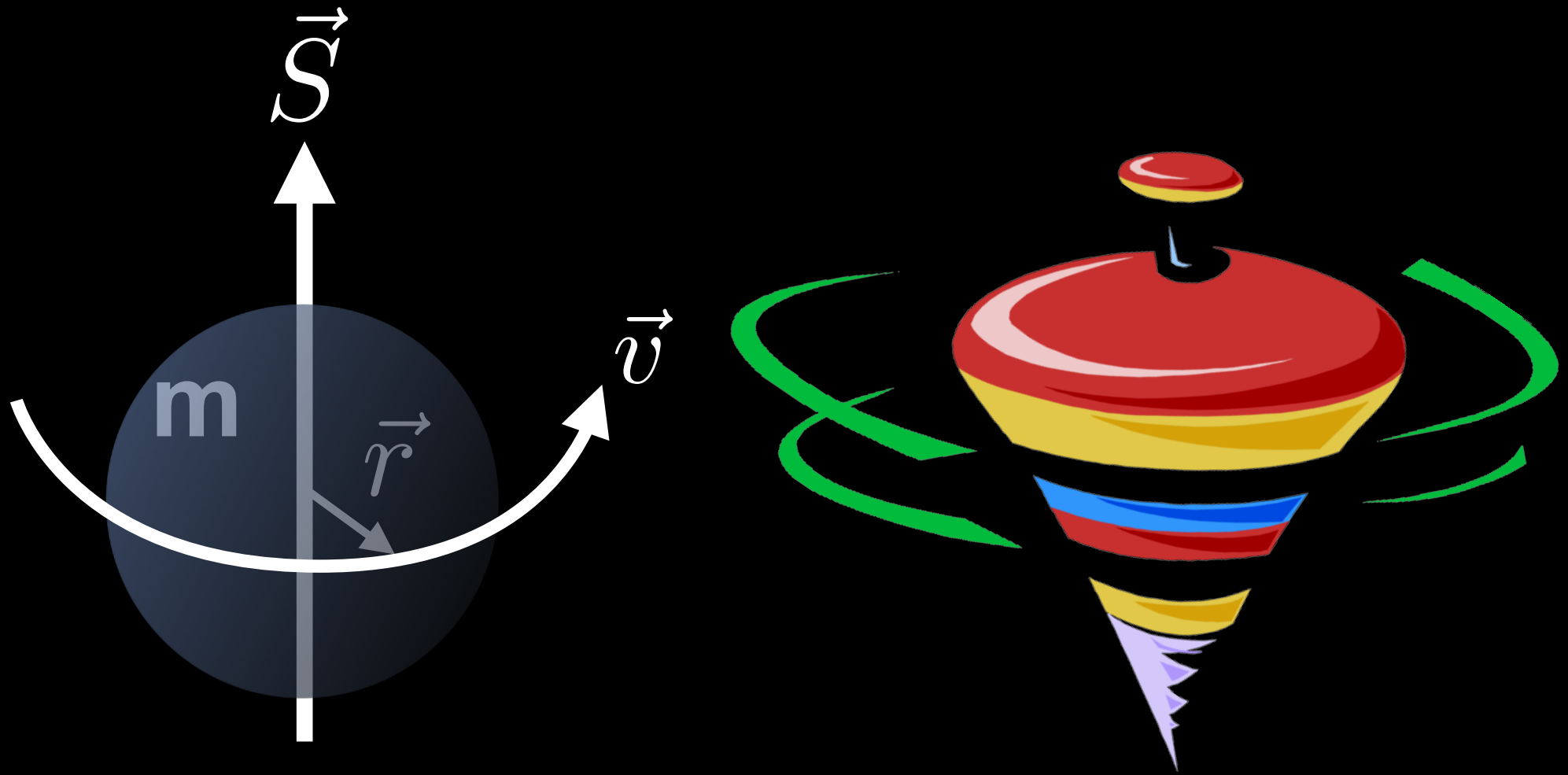
Planck's constant

Spin quantum #

- Nuclei with an odd mass number have **half-integral spin**
 - Spin-1/2 – ^1H , ^{13}C , ^{15}N , ^{19}F , ^{31}P
 - Spin-3/2 – ^{23}Na
- Nuclei with an even mass number and an even charge number have **zero spin**
 - ^{12}C and ^{16}O

Spin Angular Momentum

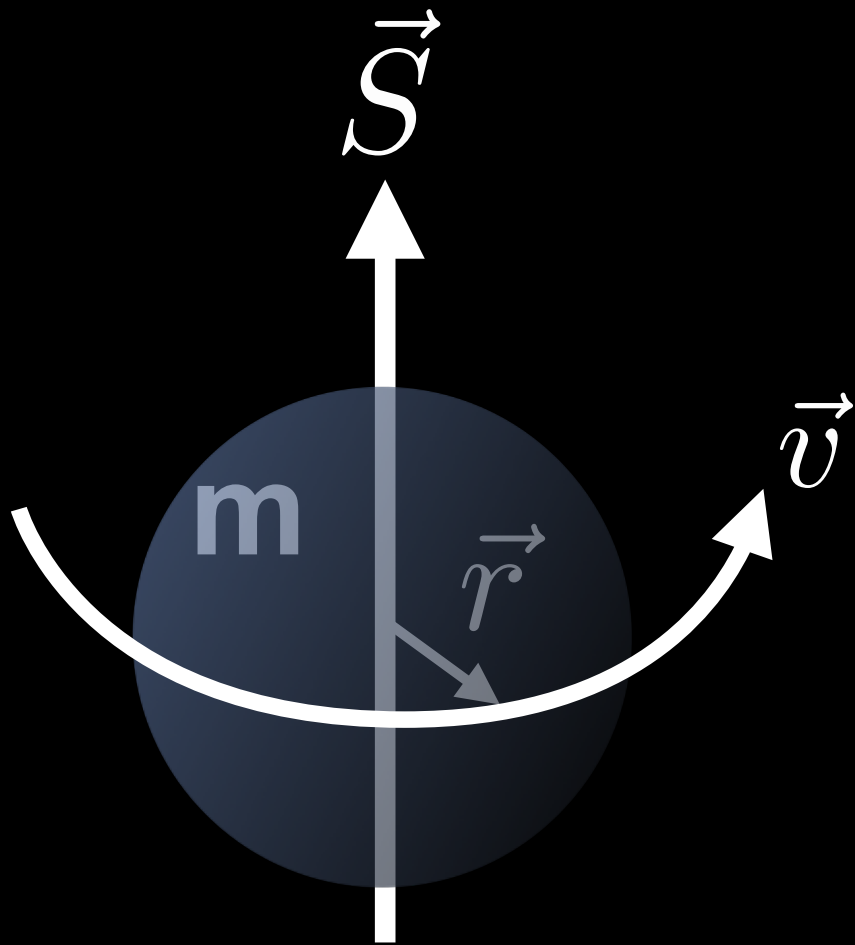
Spin + Mass \implies Spin Angular Momentum $\implies \vec{S}$ [$\text{kg}\cdot\text{m}^2\text{s}^{-1}$]



Hydrogen nuclei have spin angular momentum.

Spin Angular Momentum

Spin + Mass \implies Spin Angular Momentum $\implies \vec{S}$ [kg·m²s⁻¹]



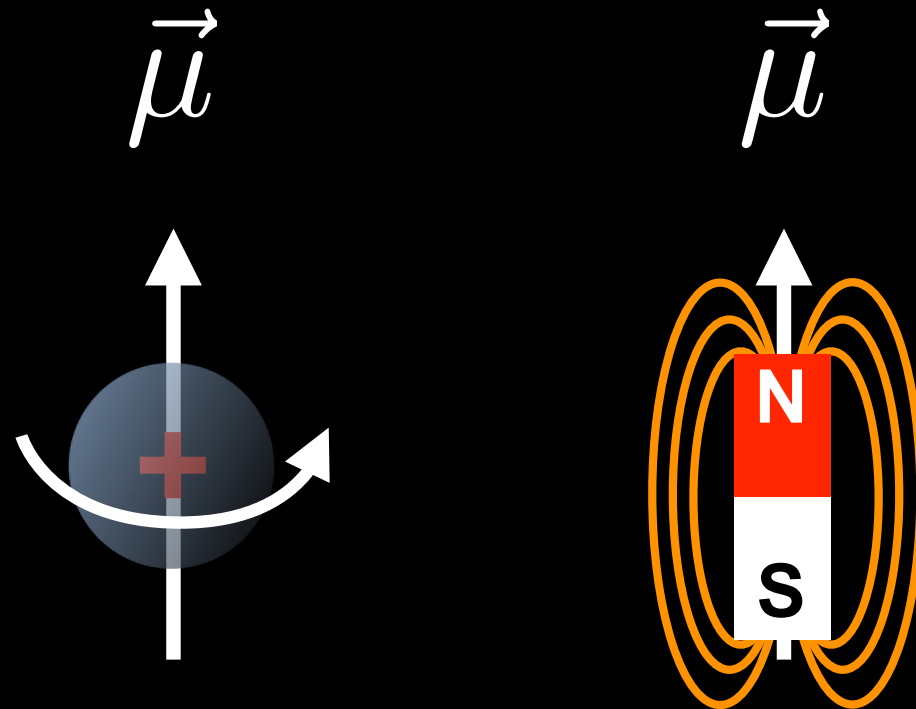
$$\begin{aligned}\vec{S} &= \vec{r} \times \vec{p} \\ &= \vec{r} \times m\vec{v}\end{aligned}$$

Hydrogen nuclei have spin angular momentum.

Magnetic Dipole Moments

Spin + Charge \Rightarrow Magnetic Moment $\Rightarrow \vec{\mu}$ [$\text{J}\cdot\text{T}^{-1}$ or $\text{kg}\cdot\text{m}^2/\text{s}^2/\text{T}$]

“a measure of the strength of the system's net magnetic source”
--http://en.wikipedia.org/wiki/Magnetic_moment



Hydrogen nuclei have magnetic dipole moments.

Gyromagnetic Ratio

- Gyromagnetic Ratio
 - Physical constant
 - Unique for each NMR active nuclei
 - Ratio of the magnetic moment to the angular momentum

$$\vec{\mu} = \gamma \vec{S} = \gamma \hbar \vec{I}$$

- Governs the frequency of *precession*
- Gamma vs. Gamma-bar

$$\gamma = \gamma / 2\pi$$

NMR Active Nuclei

Isotope	Spin [I]	Natural Abundance	Gyromagnetic Ratio [MHz/T]	Relative Sensitivity	Absolute Sensitivity
¹H	1/2	0.9980	42.57	1	9.98E-01
² H	1	0.0160	6.54	0.015	2.40E-04
¹² C	0	0.9890	---	---	---
¹³ C	1/2	0.0110	10.71	0.016	1.76E-04
¹⁴ N	1	0.9960	3.08	0.001	9.96E-04
¹⁵ N	1/2	0.0040	-4.32	0.001	4.00E-06
¹⁶ O	0	0.9890	---	---	---
¹⁷ O	5/2	0.0004	-5.77	0.029	1.16E-05
¹⁹ F	1/2	1.0000	40.05	0.83	8.30E-01
²³ Na	3/2	1.0000	11.26	0.093	9.30E-02
³¹ P	1/2	1.0000	17.24	0.066	6.60E-02

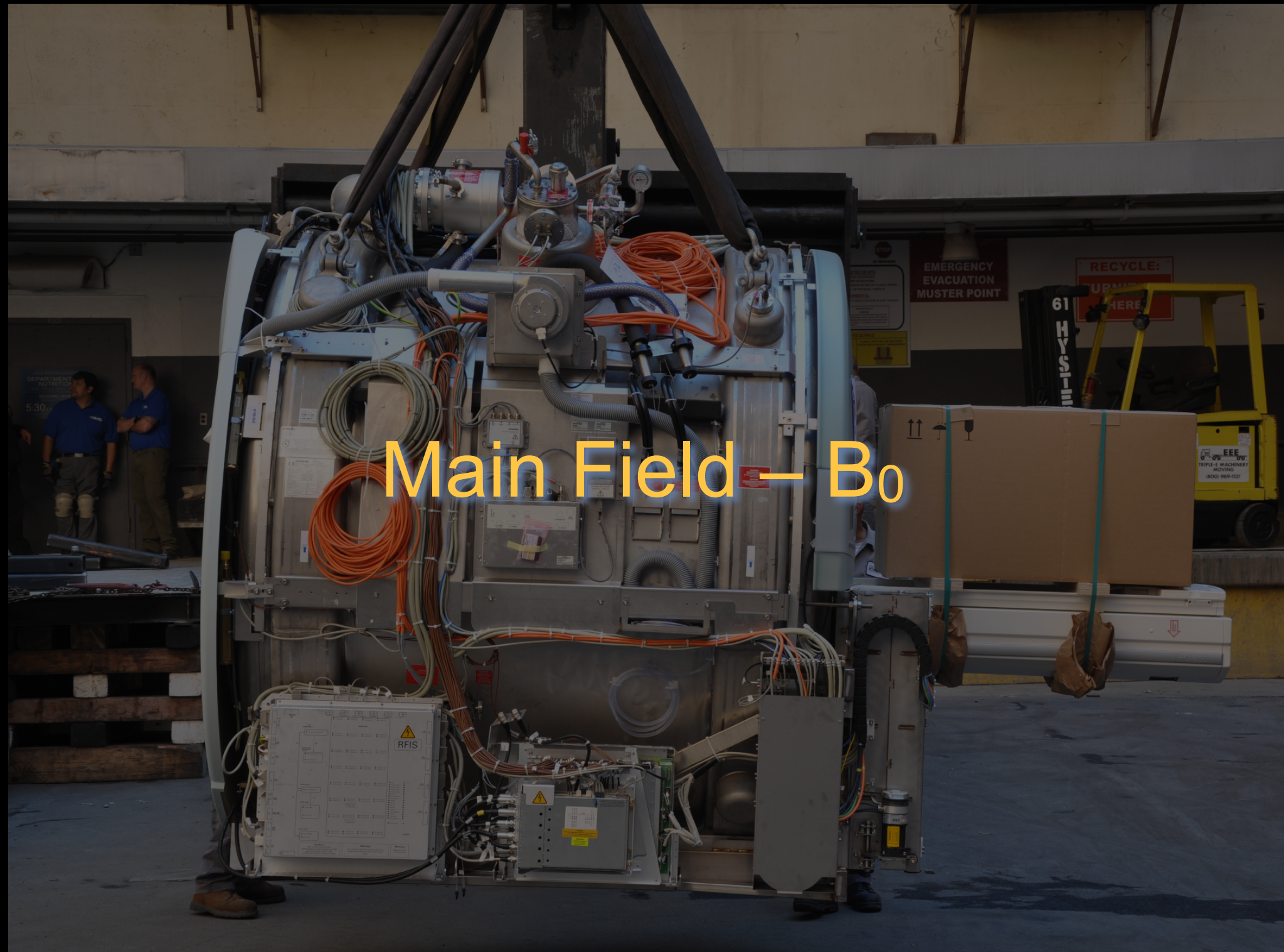
The **relative** sensitivity is at constant magnetic field and equal number of nuclei.

– Using a factor of $\gamma^{\frac{11}{4}} I(I+1)$; ¹H is the reference standard.

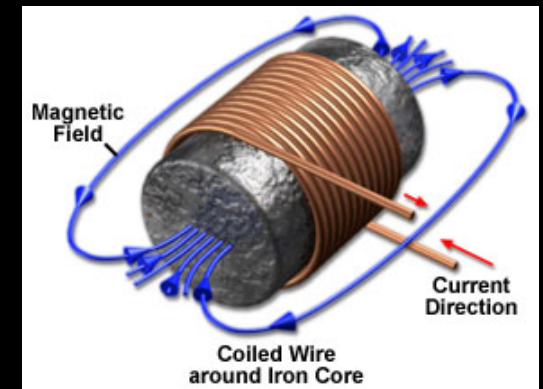
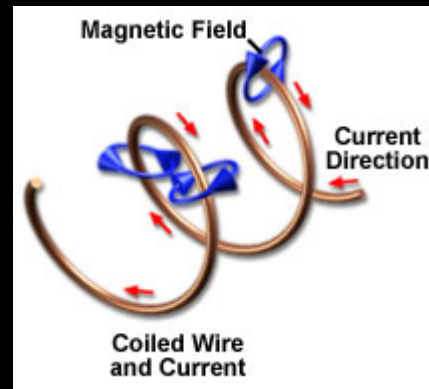
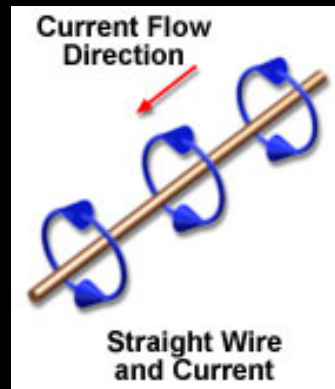
The **absolute** sensitivity is the relative sensitivity multiplied by natural abundance.



Main Field — B_0



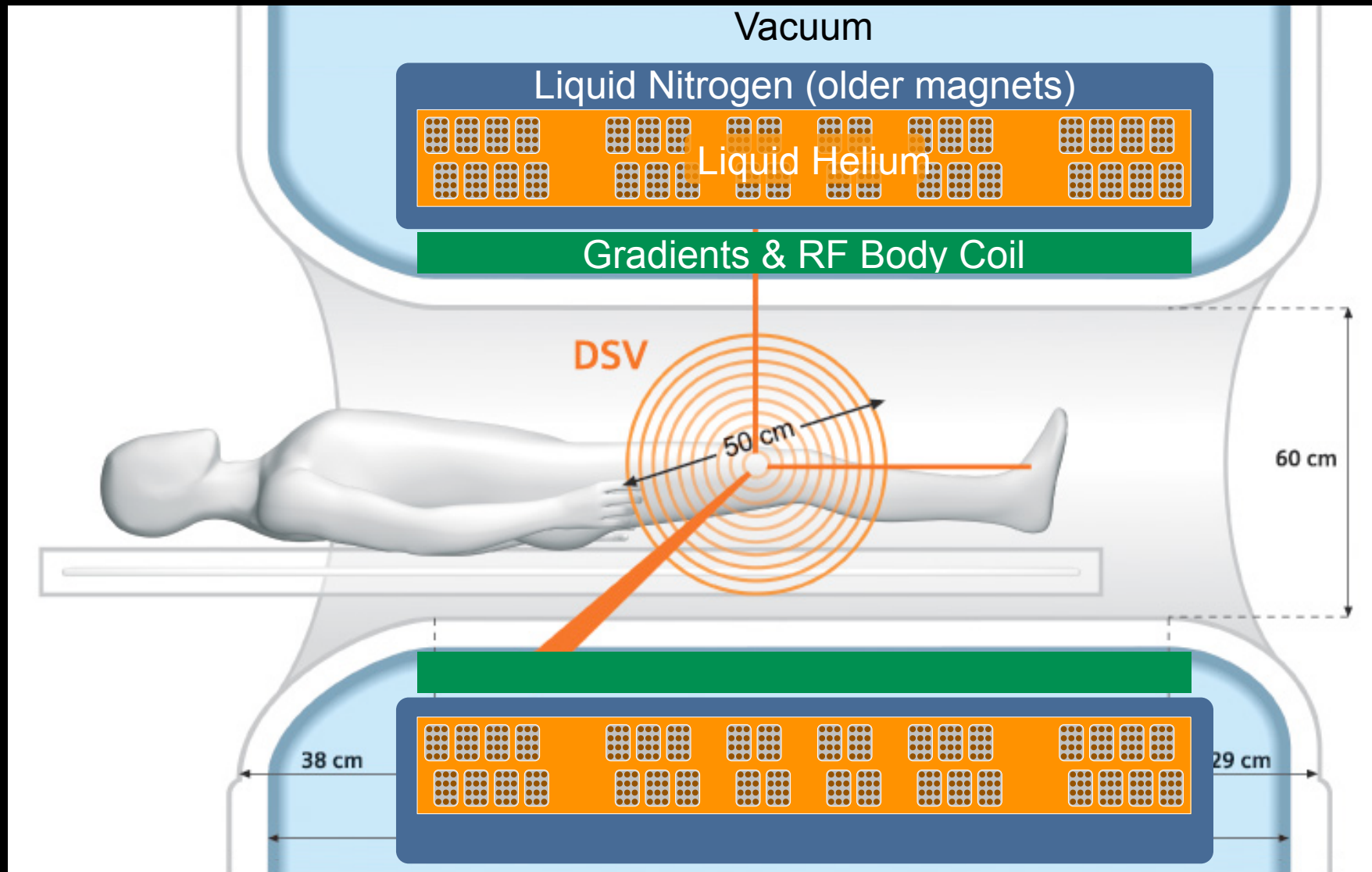
Currents & Magnetic Fields



Left-hand Rule

Electromagnet – A current in a wire generates a magnetic field.

Superconducting Electromagnet



MRI scanners are superconducting electromagnets.

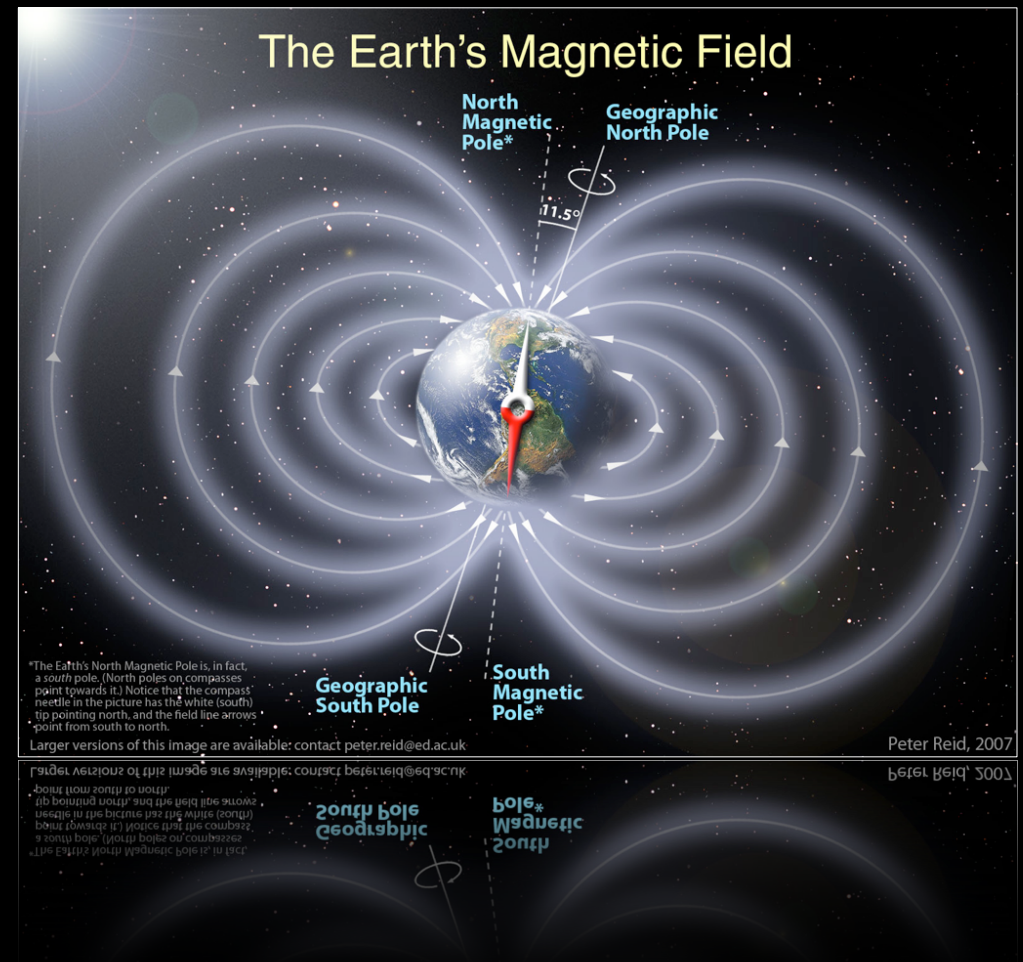
B₀ Field

- B₀ field is:
 - Spatially uniform (over a volume of interest)
 - ~50cm @ isocenter
 - Temporally stable
 - $B_0(t) = B_0(t=0)e^{-(R/L)/t}$
 - Decays <1ppm/hour
 - Oriented along the z-axis (\vec{k})
 - Long axis of the scanner.

$$\vec{B}_0 = B_0 \vec{k}$$

Main Field (B_0) – Strength

- Earth's magnetic field
 - 0.5 Gauss
- Refrigerator magnet
 - 10-100 Gauss
- B_0 Field
 - 0.5T = 5000 Gauss
 - 1.5T = 15000 Gauss
 - 3.0T = 30000 Gauss



B_0 Strength - Advantages

- $\uparrow B_0 \Rightarrow \uparrow$ Polarization ($|\vec{M}|$) = \uparrow SNR
 - \uparrow Polarization, therefore more \vec{M} for imaging.
 - $\text{SNR} \propto B_0^{7/4}$ (\uparrow Polarization + \uparrow Larmor Frequency)
 - \uparrow Spatial resolution
 - \uparrow Temporal resolution
 - \downarrow Scan time

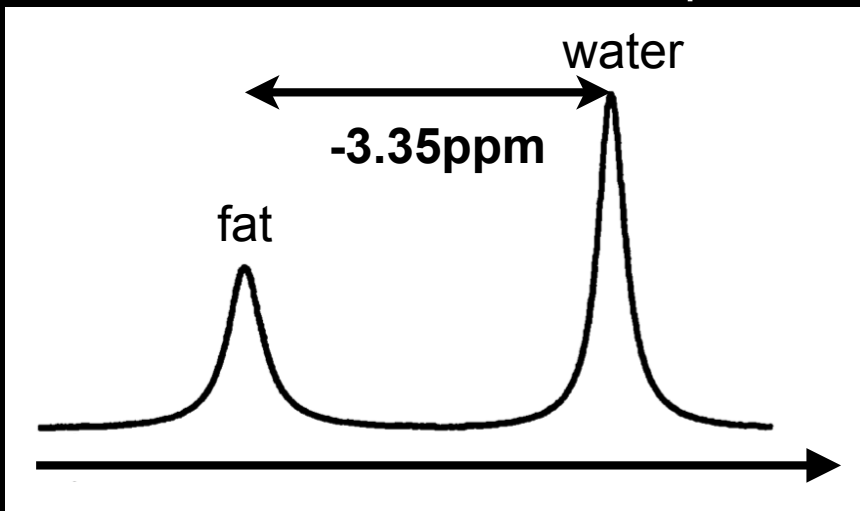
B_0 Strength - Disadvantages

- $\uparrow B_0 \Rightarrow \uparrow$ Specific Absorption Ratio (SAR)
 - Energy absorbed by body [W/kg]
 - $SAR \propto B_0^2$
- $\uparrow B_0 \Rightarrow \uparrow$ Cost
 - ~\$1,000,000 per Tesla
 - More shielding

Higher B_0 leads to higher SAR for patients and higher costs.

B_0 Strength - Disadvantages

- $\uparrow B_0 \Rightarrow \uparrow$ Chemical shift (Δf)
 - $\uparrow \Delta f$ between fat and water
 - Fat and water have different Larmor frequencies
 - ~220Hz different at 1.5T
 - ~440Hz different at 3.0T
 - Fat is more spatially mis-registered @ 3T
 - Good for spectroscopy...

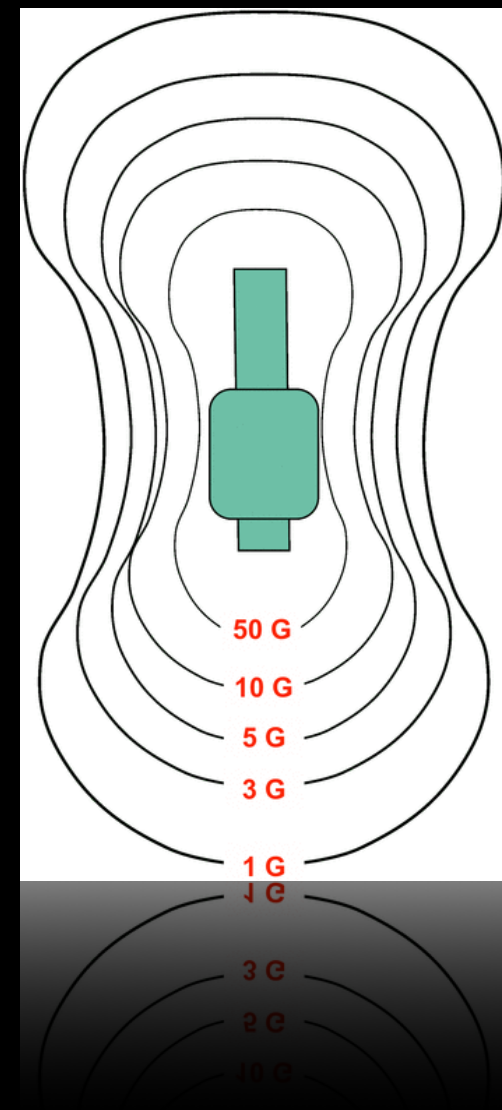


$$B = B_0 (1 - \delta)$$
$$\delta_{-\text{CH}_2} = 3.35\text{ppm}$$

Chemical Shift – Fat ($-\text{CH}_2$) is ~220Hz lower at 1.5T

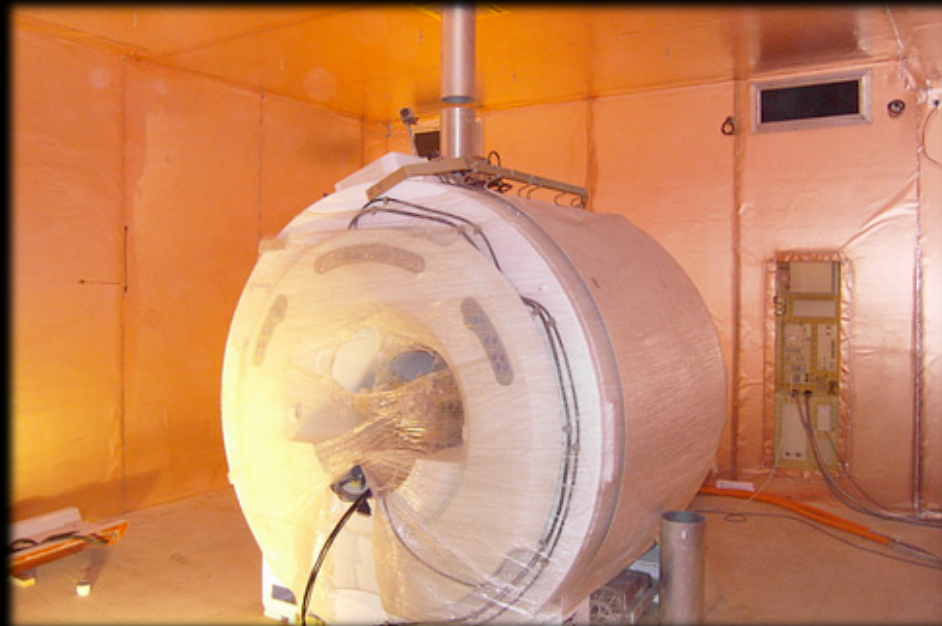
Main Field (B_0) – Shielding

- **Problem**: The B_0 field extends well beyond the scanner.
- **Shielding** reduces B_0 foot print
 - Reduces install cost
 - Reduces interference
- **Passive Shielding**
 - Iron room shielding
 - Heavy, not cheap
- **Active Shielding**
 - Super-conducting coils that oppose (shield) B_0 fringe field
- **“Five Gauss Line”**
 - Threshold beyond which ferromagnetic objects are strictly prohibited
 - $5\text{G}=0.5\text{mT}$

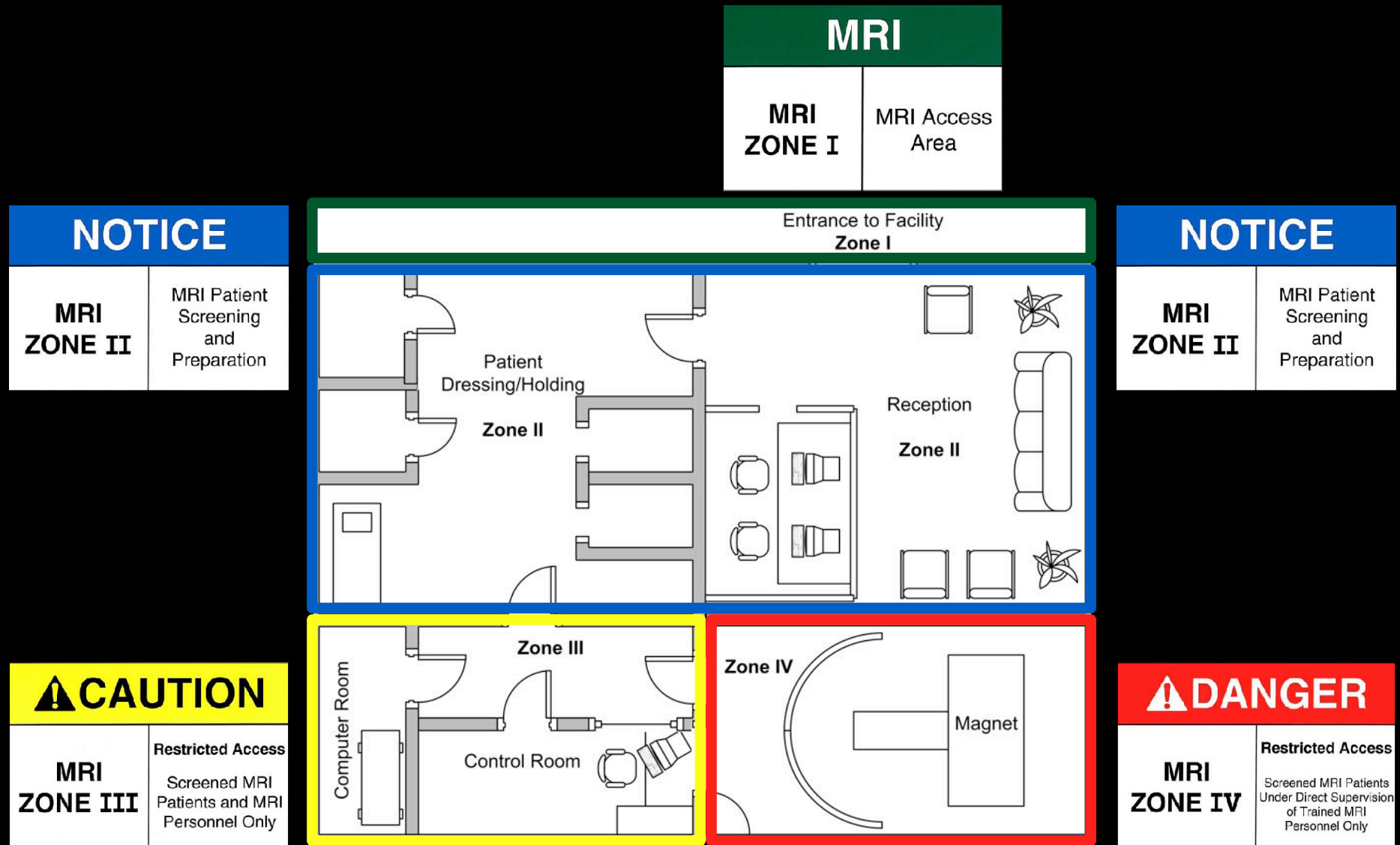


RF Shielding

- RF fields are close to FM radio
 - ^1H @ 1.5T \Rightarrow 63.85 MHz
 - ^1H @ 3.0T \Rightarrow 127.71 MHz
 - KROQ \Rightarrow 106.7 MHz
- Need to shield local sources from interfering
- Copper room shielding required



MRI Zones



B₀ Hardware Anatomy



Superconducting Electromagnets

- MRI scanners are **superconducting electromagnets**
 - B-field is generated by flowing electricity
 - Permanent magnet MRI are uncommon

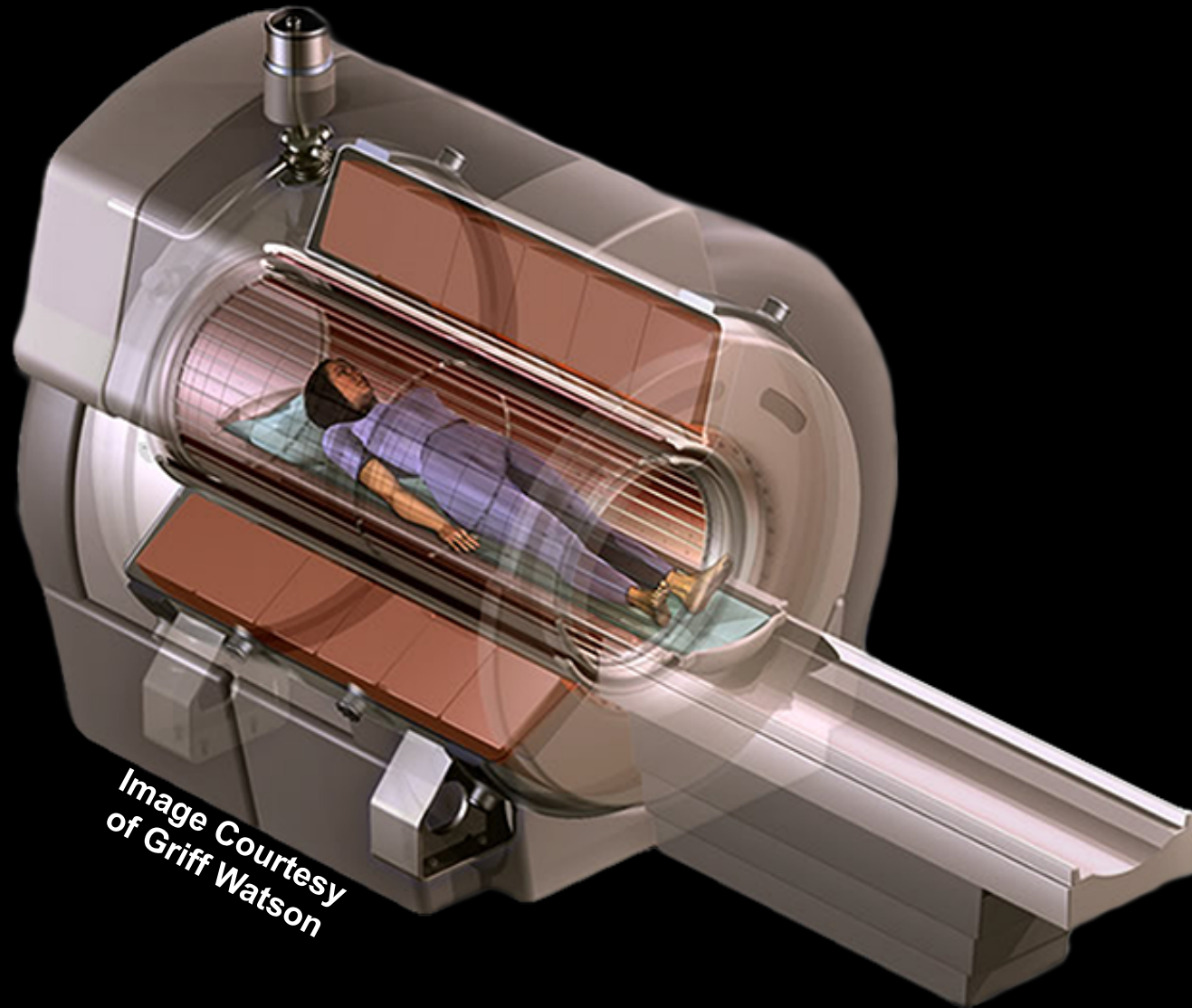
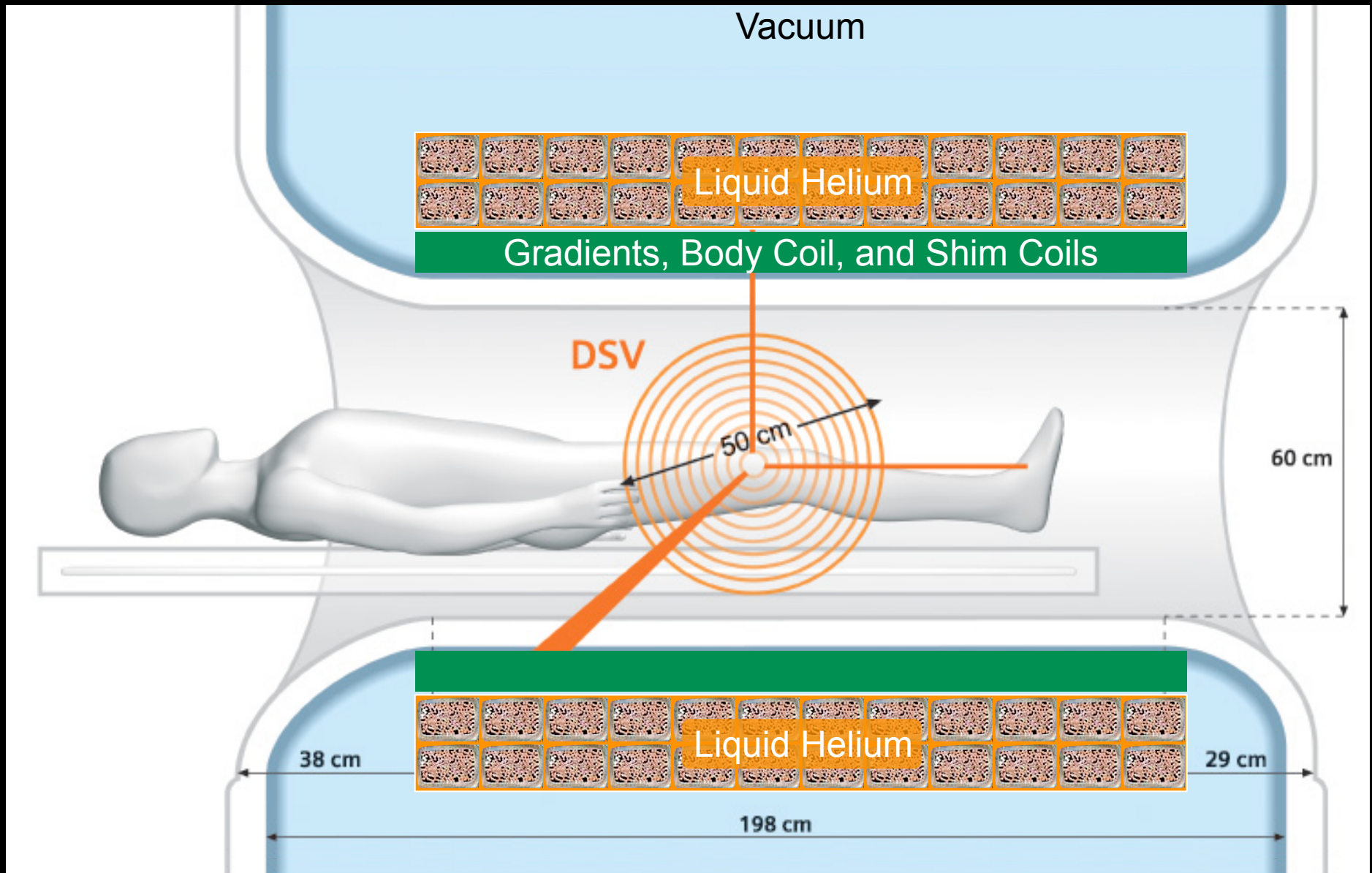
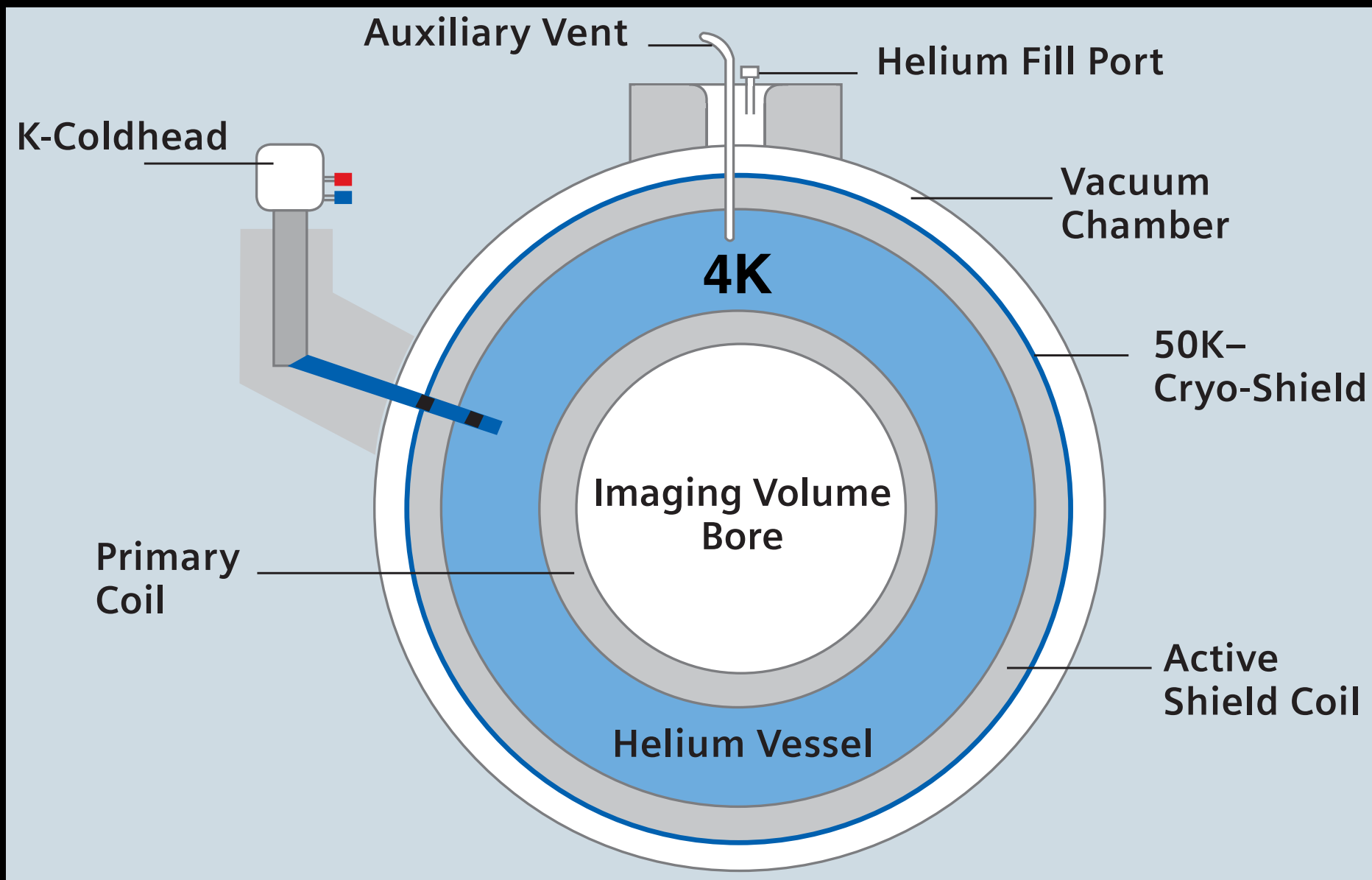


Image Courtesy
of Griff Watson

Superconducting Magnet

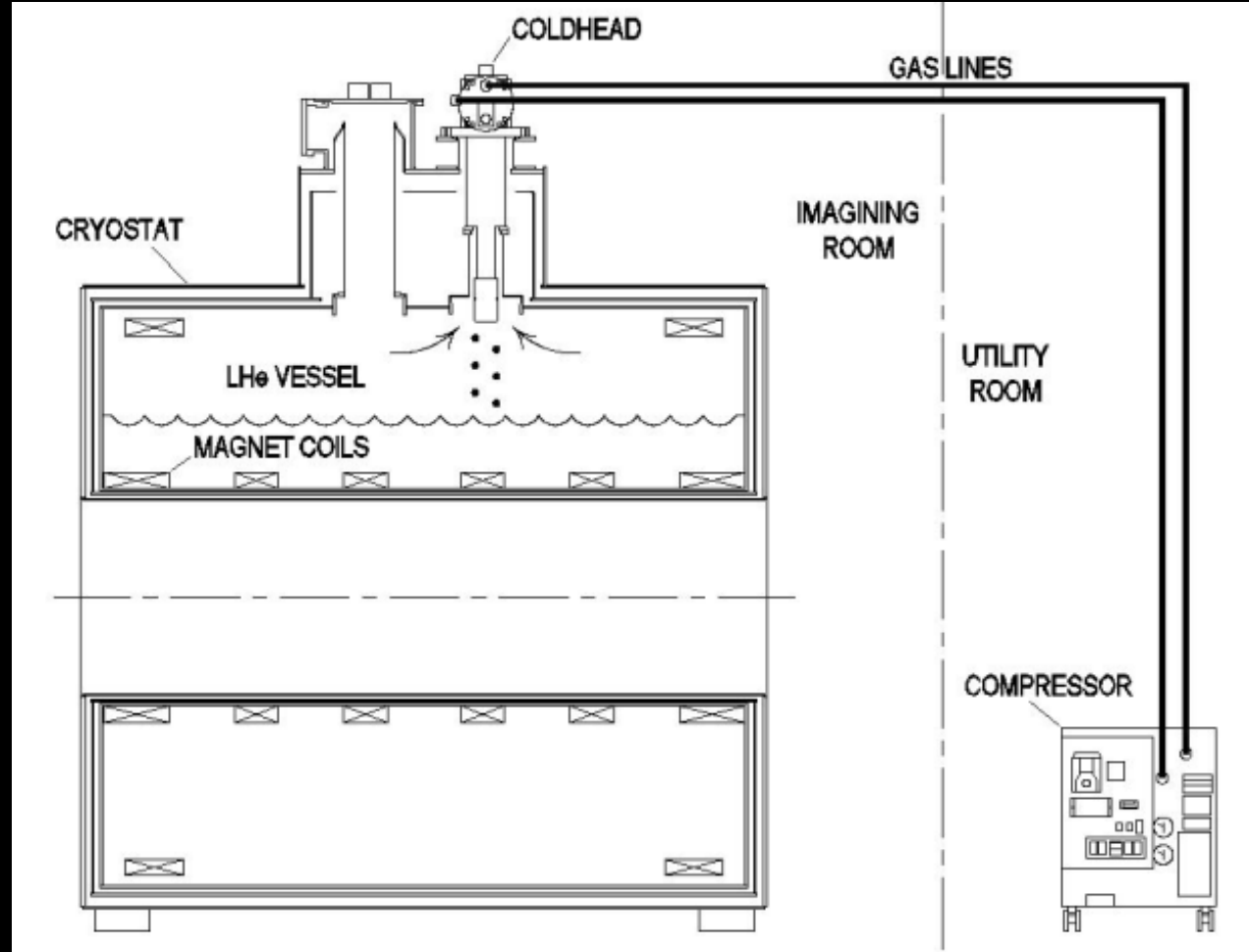
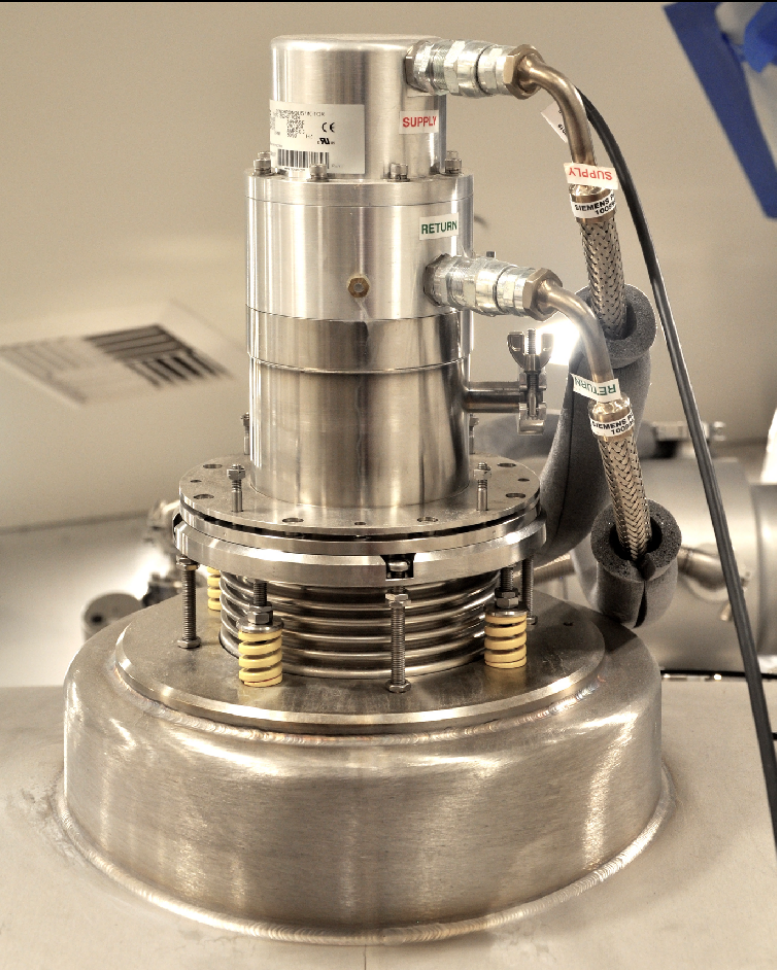


Superconducting Electromagnets



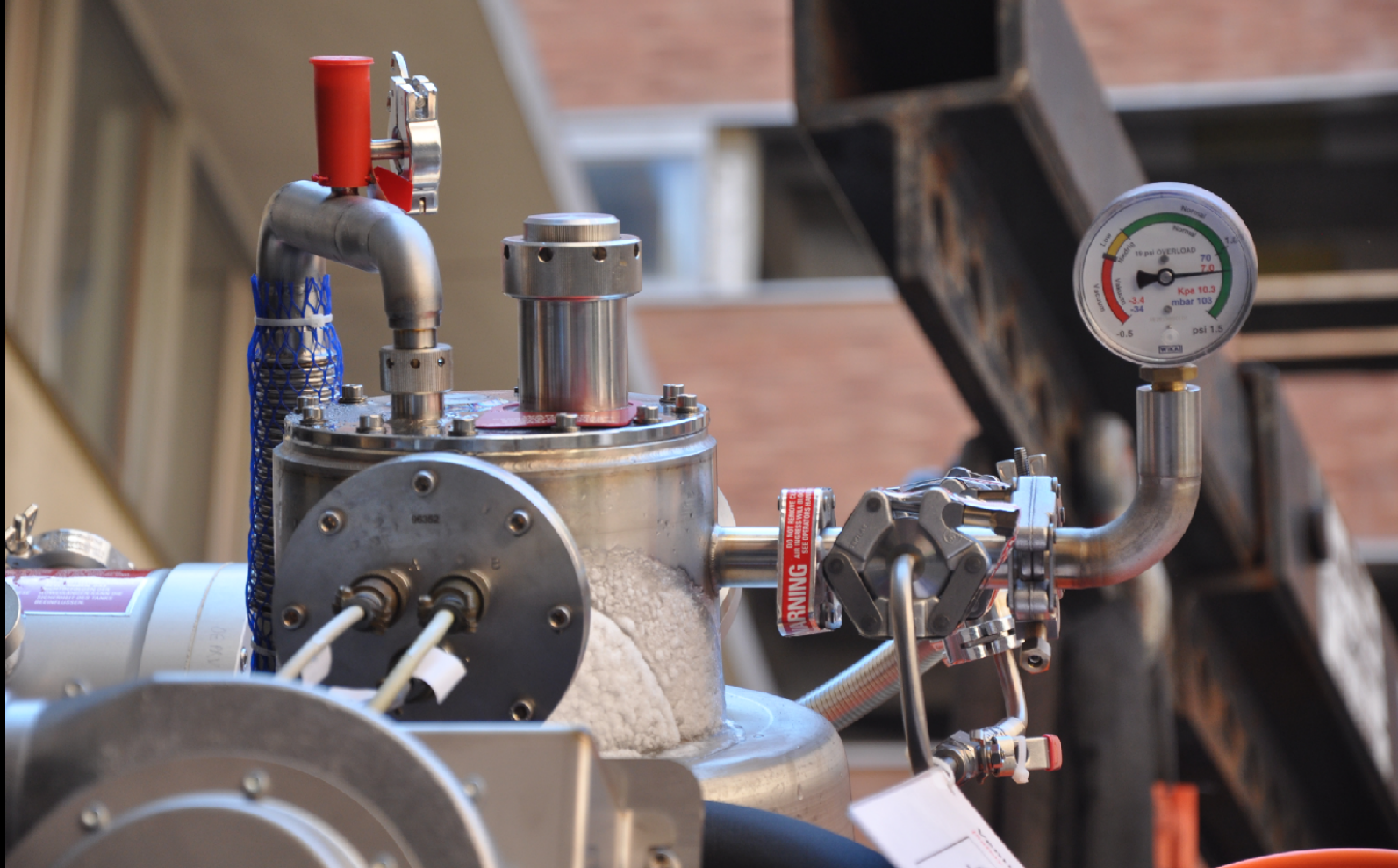
www.siemens.com/magnetom-world (Magnetom Flash 2/2008)

Coldhead (Cryocooler)



Re-condenses helium vapor and returns liquid helium to vessel.

Helium Fill Port



Helium boils off at 0 to 0.03 L/hour.
\$10-\$25 per liter of liquid Helium.

Zero Boil-off and Low Volume (~20L vs 2000L) systems are emerging.

Liquid Helium

- **Where does helium come from?**
 - Extracted from natural gas
 - Strategic helium reserve
 - **Helium that escapes to atmosphere is lost forever.**
- **Zero boil-off design**
 - Captures and re-compresses cryogen
 - Saves 700-1300L per year



Main Field (B_0) - Principles

- B_0 is a strong magnetic field
 - >1.5T
 - Z-oriented

$$\vec{B}_0 = B_0 \vec{k}$$

- B_0 generates bulk magnetization (\vec{M})
 - More B_0 , more

$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n$$

- B_0 forces \vec{M} to precess
 - Larmor Equation

$$\omega = \gamma B$$

Main Field (B_0) - Principles

- B_0 is a strong magnetic field
 - >1.5T
 - Z-oriented

$$\vec{B}_0 = B_0 \vec{k}$$

- B_0 generates bulk magnetization (\vec{M})
 - More B_0 , more

$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n$$

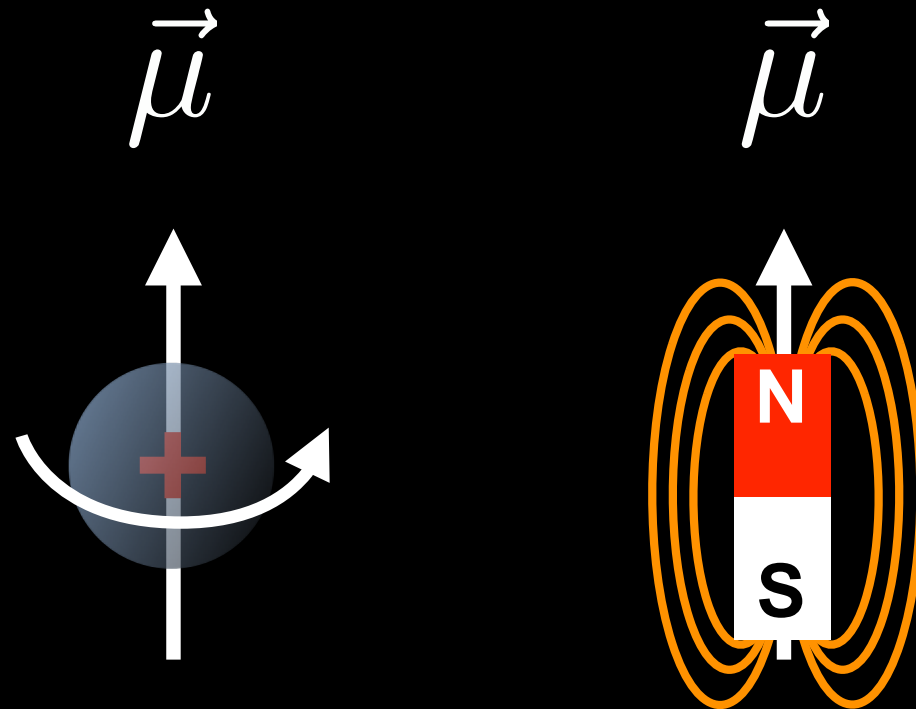
- B_0 forces \vec{M} to precess
 - Larmor Equation

$$\omega = \gamma B$$

Magnetic Dipole Moments

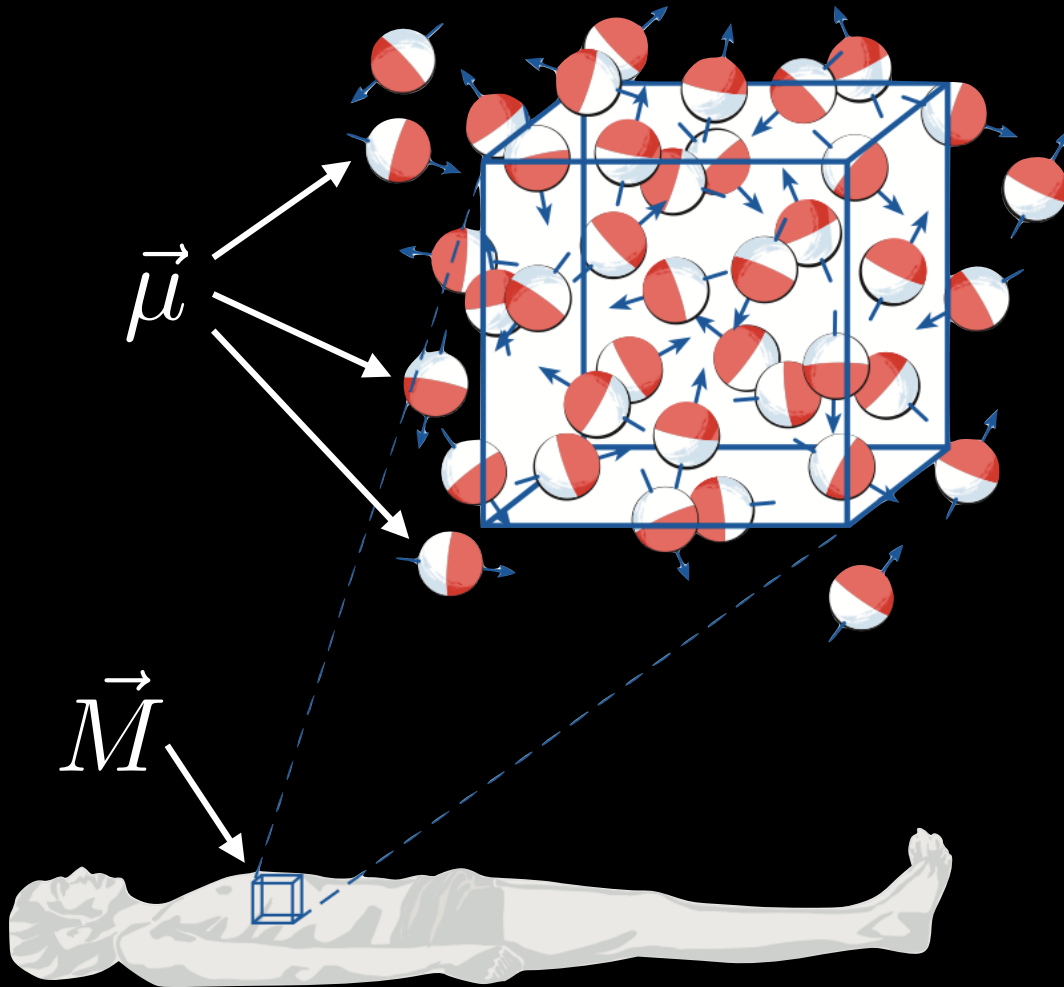
Spin + Charge \Rightarrow Magnetic Moment $\Rightarrow \vec{\mu}$ [$\text{J}\cdot\text{T}^{-1}$ or $\text{kg}\cdot\text{m}^2/\text{s}^2/\text{T}$]

“a measure of the strength of the system's net magnetic source”
--http://en.wikipedia.org/wiki/Magnetic_moment



Hydrogen nuclei have magnetic dipole moments.

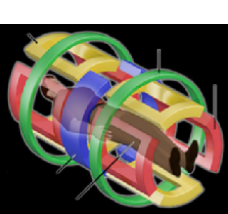
Bulk Magnetization



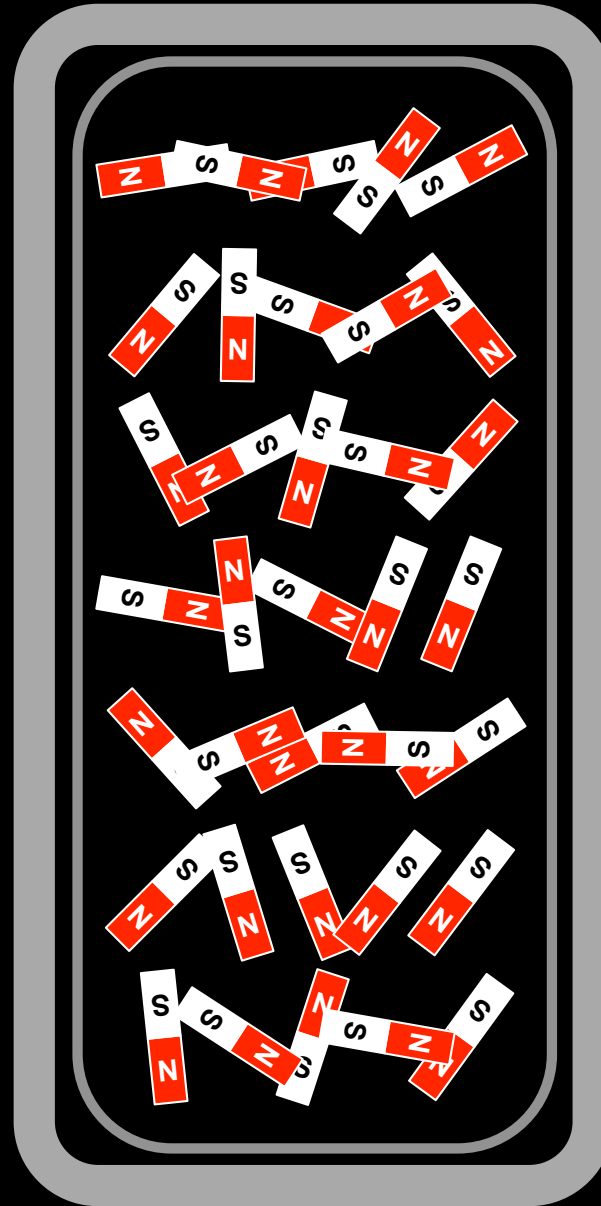
$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n$$

$N_{total} = 0.24 \times 10^{23}$ spins in a $2 \times 2 \times 10$ mm voxel

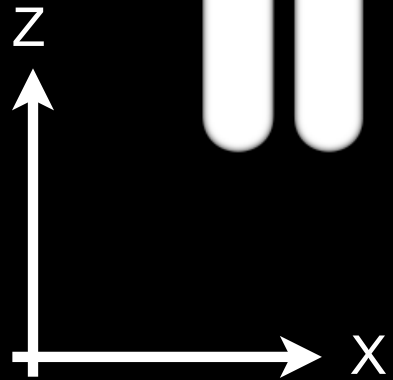
But not all spins contribute to our measured signal...

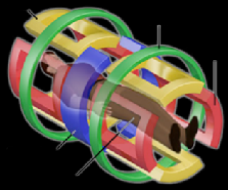


B₀ Field OFF

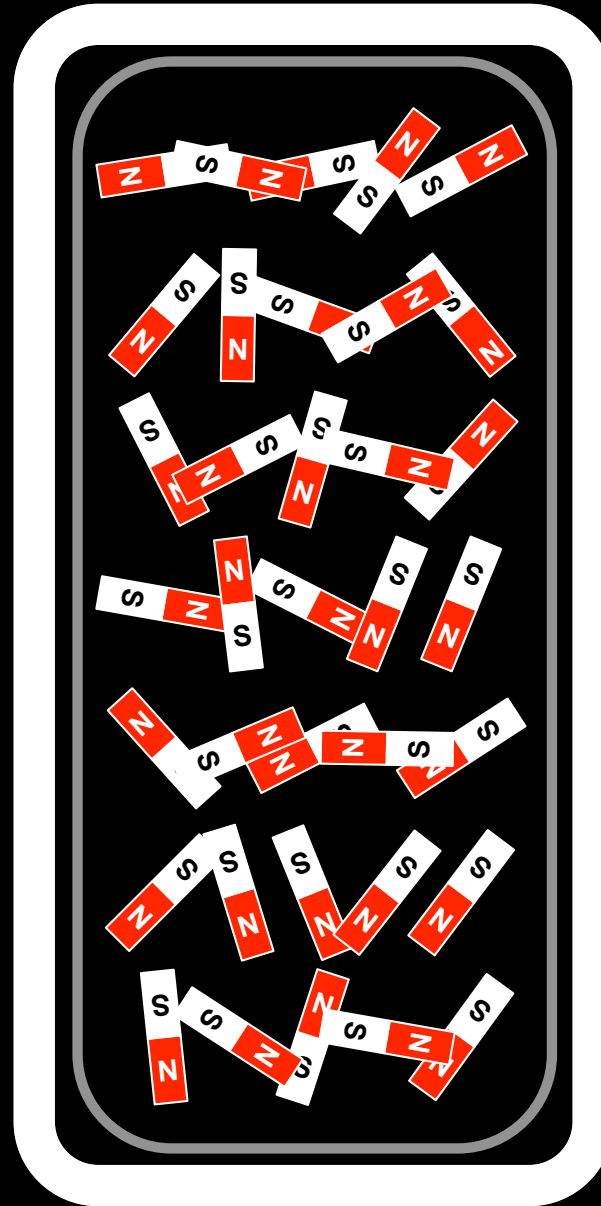


$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = 0$$



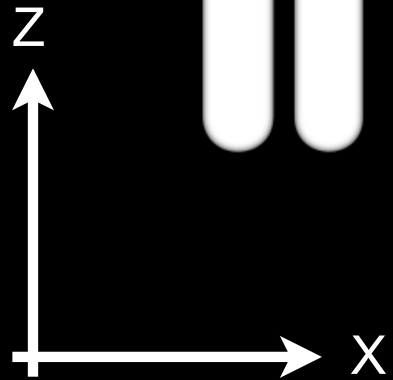


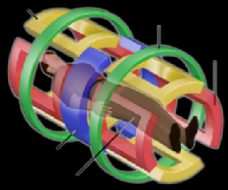
B₀ Field ON



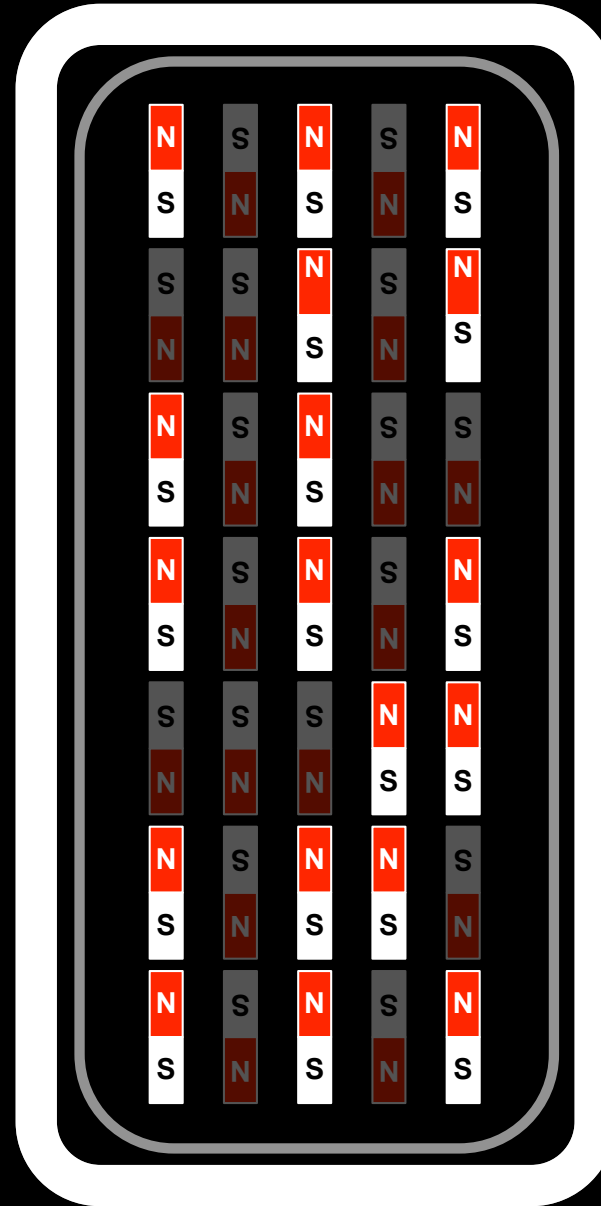
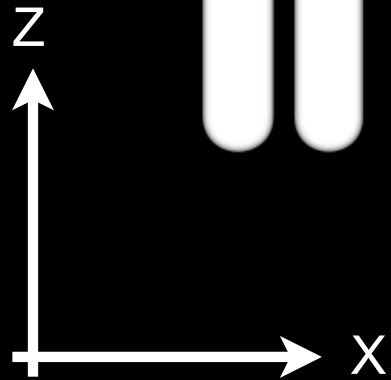
$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = M_z$$

B₀ polarizes the spins and generates bulk magnetization.







B₀ Field ON



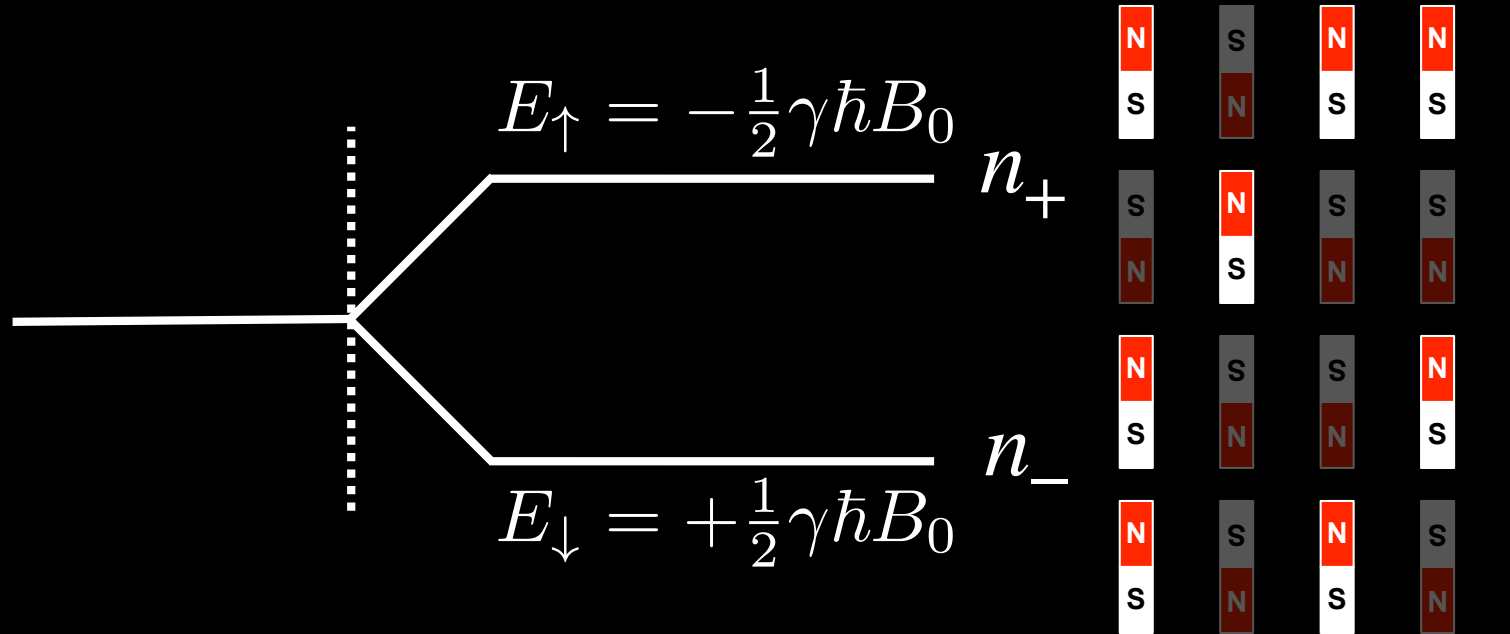
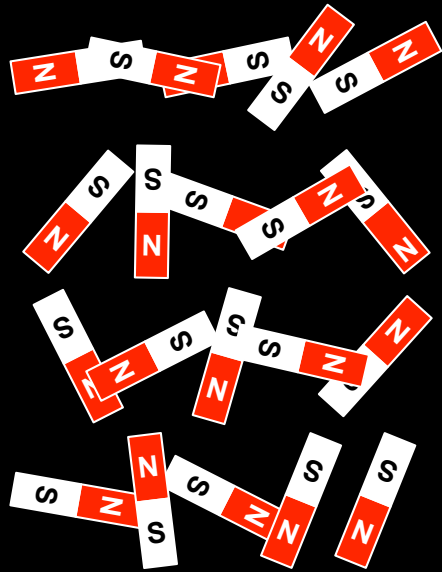
$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = M_z$$

 Spin-Up

 Spin-Down

Only a very small number are spin-up relative to spin-down.

Zeeman Splitting



B_0 is off

B_0 is on

n_+ = Spin-Up State, Low Energy

n_- = Spin-Down State, High Energy



Zeeman Splitting

- The spin population difference in the two spin states is related to their energy difference. According to the well-known Boltzmann distribution:

$$\frac{n_-}{n_+} = e^{-\Delta E/\kappa T}$$

$$\Delta E = \gamma \hbar B_0$$

κ = Boltzmann constant

T = Absolute temperature of the spin system

- At 1.5T, $\frac{n_-}{n_+} = 0.999993$

- Imaging is based on weak polarization (enough for imaging)

Main Field (B_0) - Principles

- B_0 is a strong magnetic field
 - >1.5T
 - Z-oriented

$$\vec{B}_0 = B_0 \vec{k}$$

- B_0 generates bulk magnetization (\vec{M})
 - More B_0 , more

$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n$$

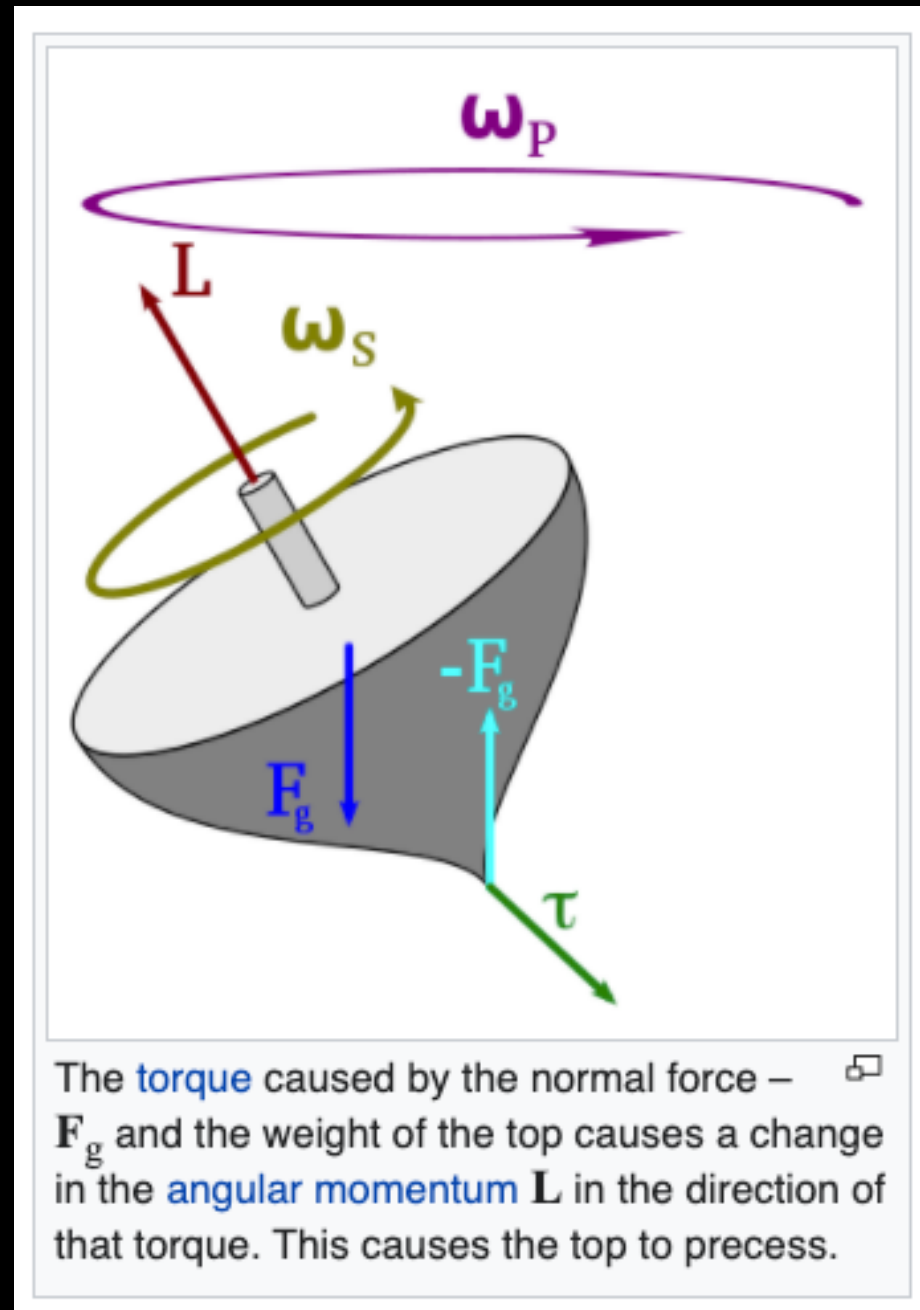
- B_0 forces \vec{M} to precess
 - Larmor Equation

$$\omega = \gamma B$$

Spin vs. Precession

- **Spin**
 - Intrinsic form of angular momentum
 - Quantum mechanical phenomena
 - No classical physics counterpart
 - Except by hand-waving analogy...
- **Precession**
 - **Spin+Mass+Charge** give rise to precession

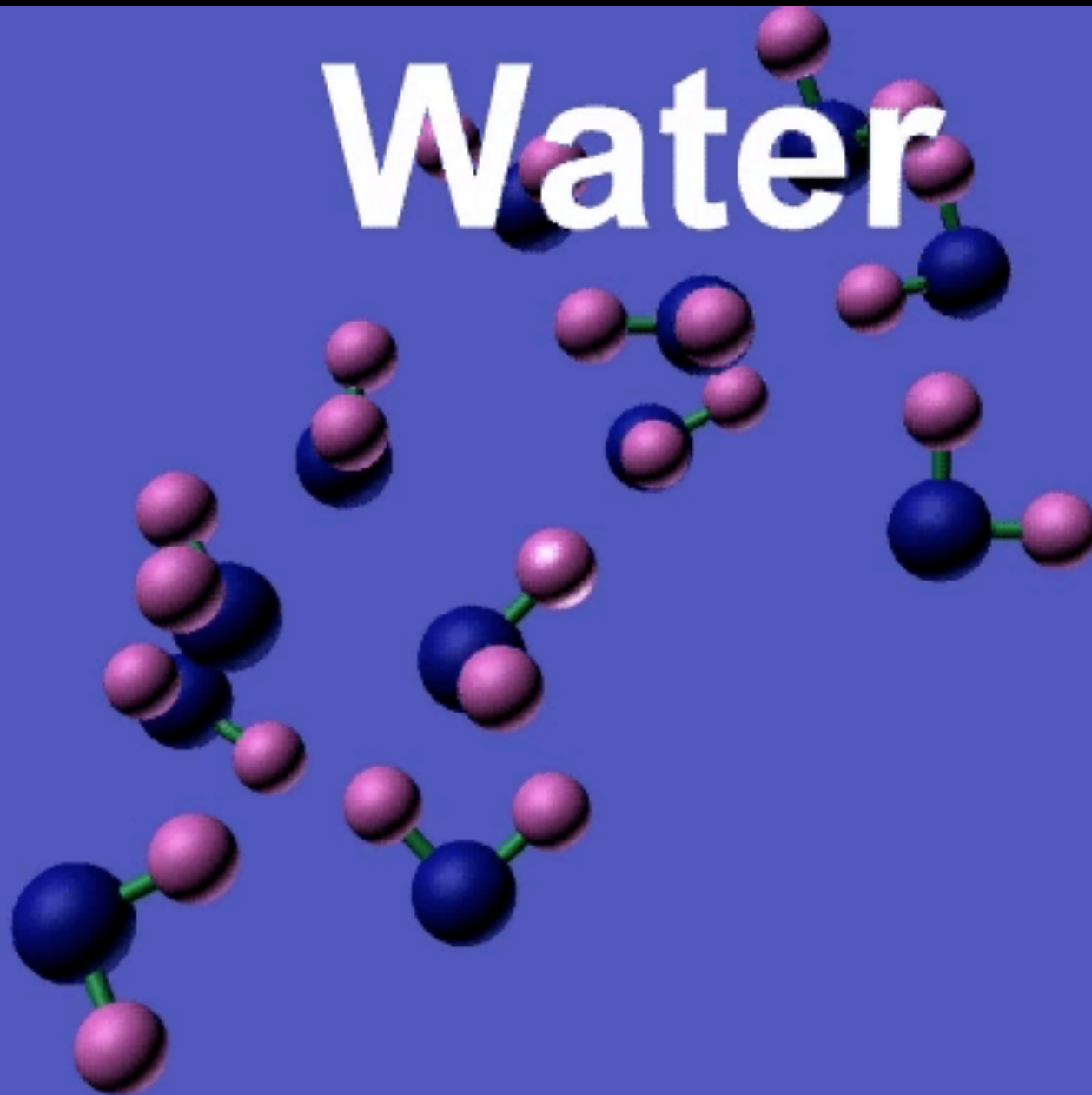
Precession



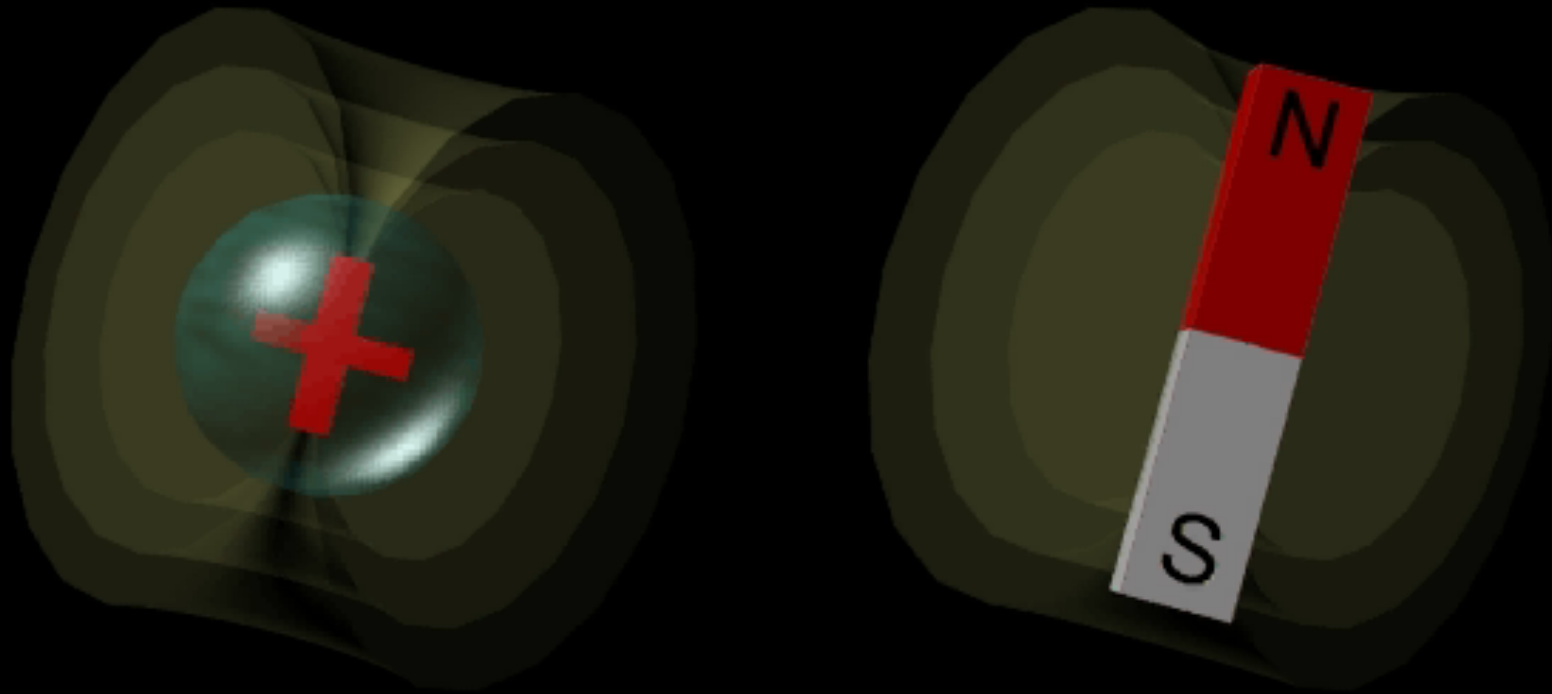
Nuclear Magnetic Resonance

NMR Phenomena

Water



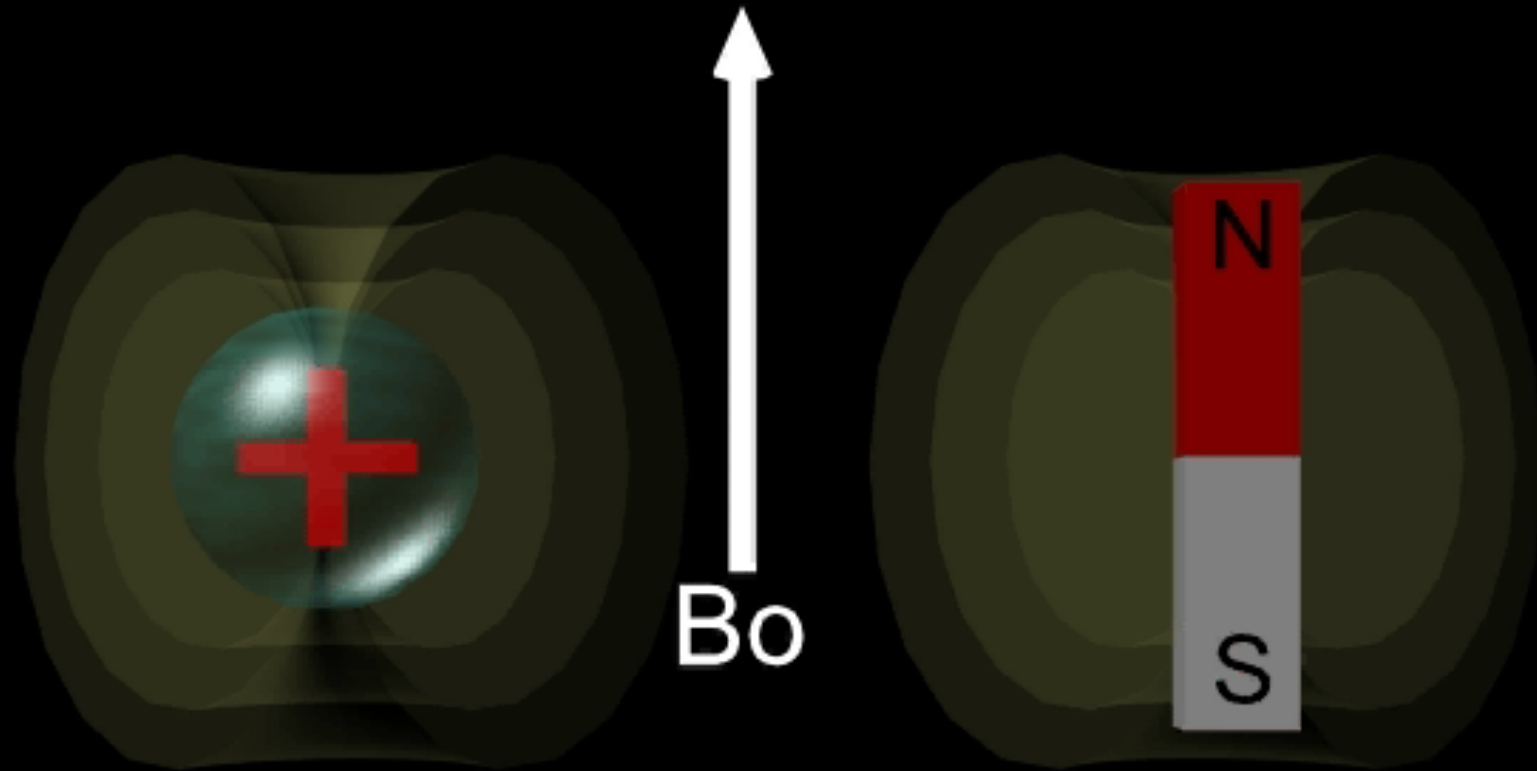
Magnetic Moment



Charge }
Spin } Magnetic
Moment

Protons behave like small magnets because of spin and charge.

Magnetic Moment



Charge }
Spin } Magnetic
Moment

Protons (small magnets) align with an external magnetic field (B_0).

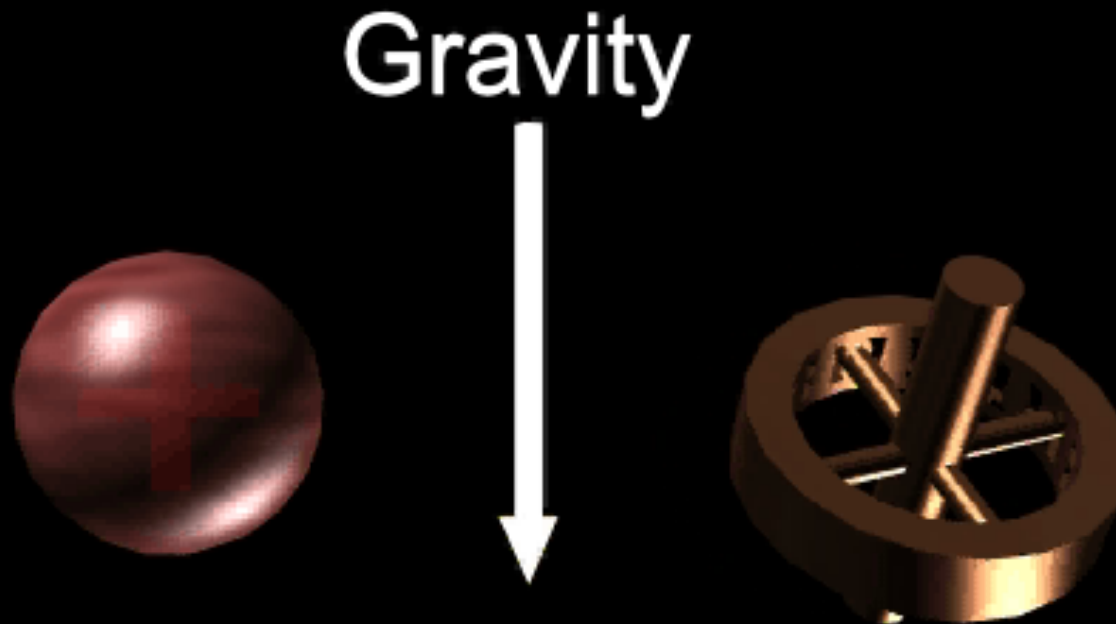
Angular Momentum



Spin
Mass } Angular
Momentum

Protons have angular momentum because of spin and mass.

Precession (Top Analogy)



Precession

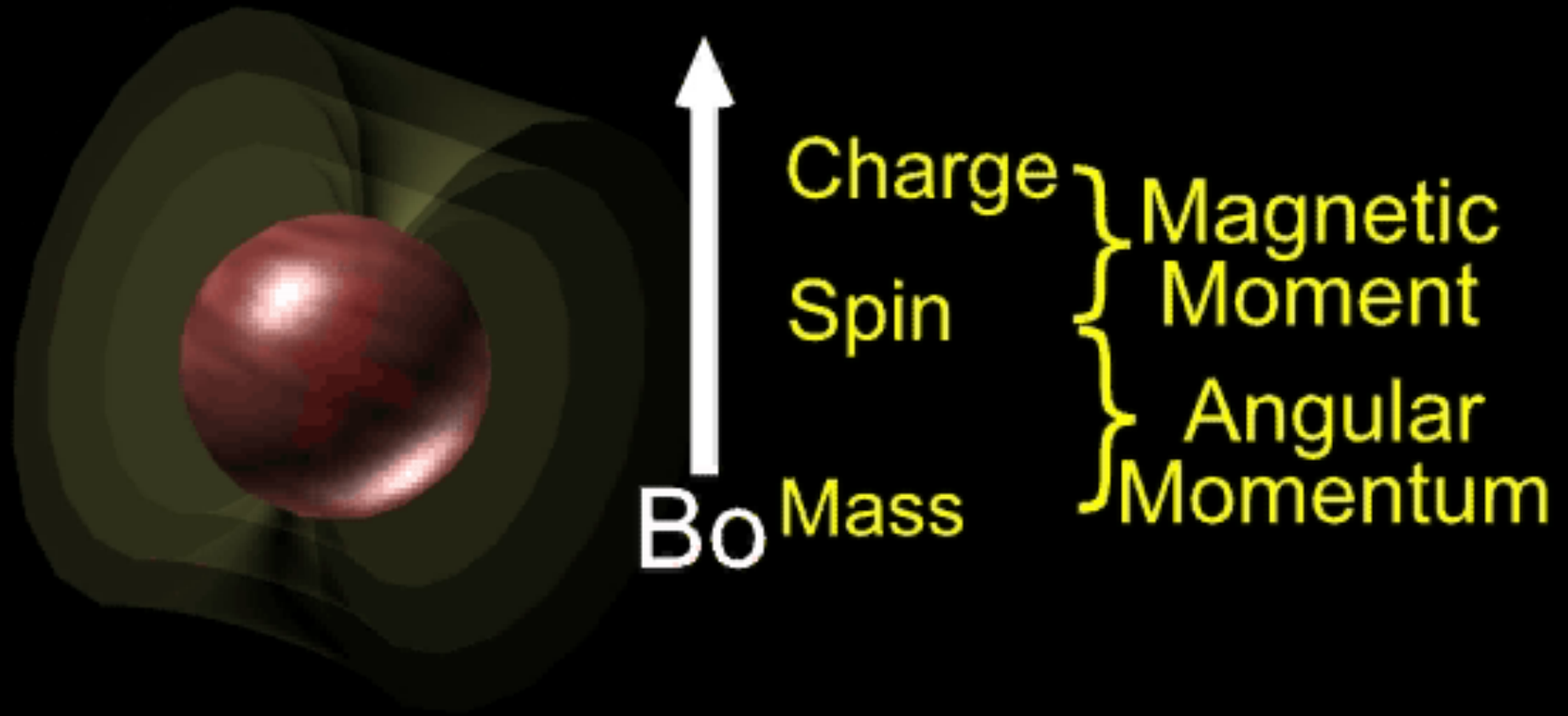
Spin

Mass

} Angular
} Momentum

A spinning top precesses in a gravitational field.
A spinning proton precesses in a magnetic (B_0) field.

Larmor Frequency

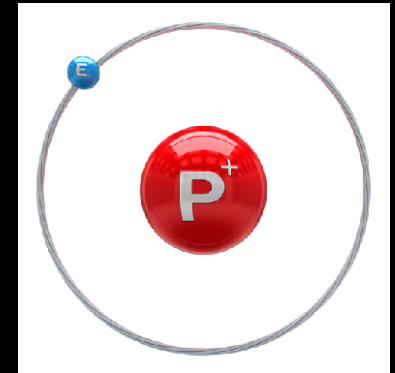


$$\text{Larmor Frequency} = \omega = \gamma B_0$$

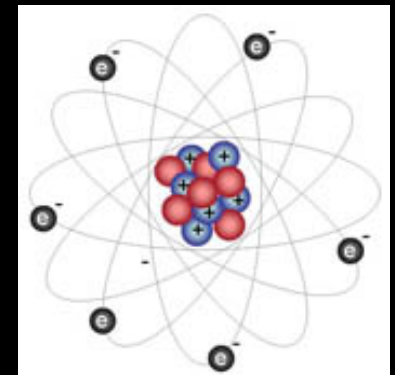
The frequency of precession is the Larmor frequency.

NMR Active Nuclei

- Spin + Charge + Mass \Rightarrow NMR Active
 - Spin? *Intrinsic* form of angular momentum.
- Nuclei have spin angular momentum if:
 - Odd atomic mass (# protons+neutrons)
And/Or
 - Odd atomic number (# of protons)
- Spin angular momentum
 - Leads to precession
 - Spin \neq precession (a top spins *and* precesses)
- Frequency of precession (**Larmor Frequency**)
 - Gyromagnetic Ratio (γ)
 - Physical constant
 - Unique for each NMR active nuclei



Hydrogen



Carbon-13

What is so special about ^1H ? Spin, charge, and mass!

Larmor Equation

- Spin≠Precession
 - Protons *intrinsically* have spin
 - Protons *precess* in the presence of a B-field
- Larmor frequency increases with:
 - Larger B_0
 - Higher gyromagnetic ratio
 - Higher frequencies produce stronger signals...

$$\omega = \gamma B_0$$

NMR Active Nuclei

Isotope	Spin [I]	Gyromagnetic Ratio [MHz/T]	Relative Sensitivity	Natural Abundance	Absolute Sensitivity
^1H	$1/2$	42.57	1	0.9980	$9.98\text{E-}01$
^2H	1	6.54	$9.65\text{E-}06$	0.0002	$1.93\text{E-}09$
^{12}C	0	---	---	0.9890	---
^{13}C	$1/2$	10.71	0.016	0.0110	$1.76\text{E-}04$
^{14}N	1	3.08	0.001	0.9960	$9.96\text{E-}04$
^{15}N	$1/2$	-4.32	0.001	0.0040	$4.00\text{E-}06$
^{16}O	0	---	---	0.9890	---
^{17}O	$5/2$	-5.77	0.029	0.0004	$1.16\text{E-}05$
^{19}F	$1/2$	40.05	0.83	1.0000	$8.30\text{E-}01$
^{23}Na	$3/2$	11.26	0.093	1.0000	$9.30\text{E-}02$
^{31}P	$1/2$	17.24	0.066	1.0000	$6.60\text{E-}02$

The **relative sensitivity** is at constant magnetic field and equal number of nuclei
The **absolute sensitivity** is the relative sensitivity multiplied by natural abundance

Quiz: NMR - True or False?

1. Electron spin is the key to NMR
2. MRI is *nothing* without spin, charge, and mass
3. All atomic nuclei are NMR active.
4. Spin and precession are the same.
5. Higher fields lead to faster precession

Quiz: Main Field - True or False?

1. B_0 is rare earth permanent magnet.
2. 1 Tesla=1000 Gauss.
3. Higher fields increase polarization, which contributes to better image quality
4. Exams at higher fields have lower SAR.
5. ^1H always precesses at the same Larmor frequency.

Questions?

- Related reading materials
 - Nishimura Chap 3 and 4

Kyung Sung, Ph.D.

KSung@mednet.ucla.edu

<http://mrrl.ucla.edu/sunglab>