

Image Reconstruction

Parallel Imaging I

M229 Advanced Topics in MRI

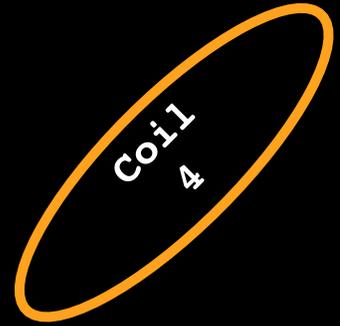
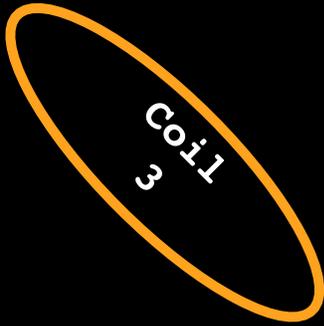
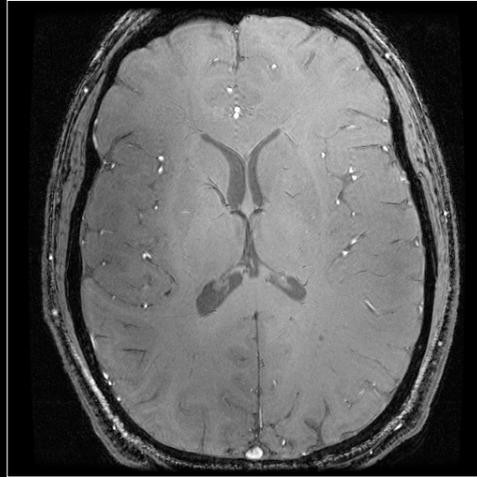
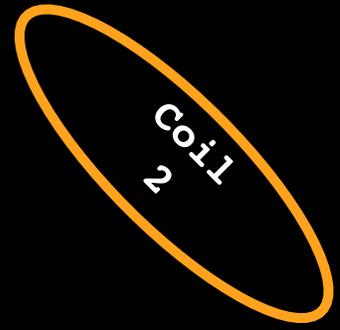
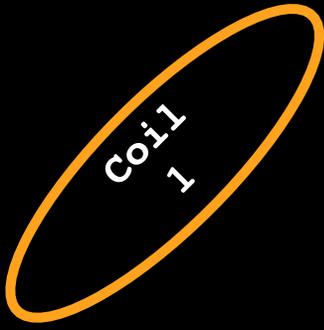
Kyung Sung, Ph.D.

2019.05.23

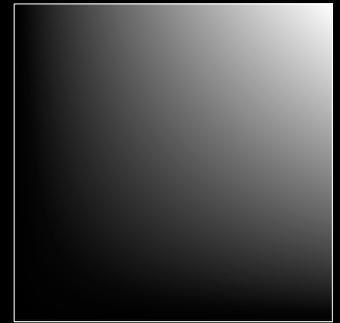
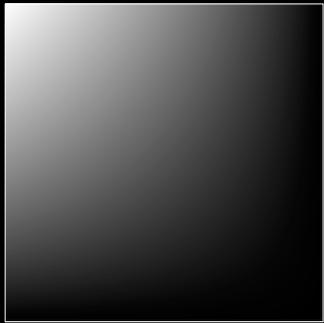
Today's Topics

- Multicoil reconstruction
- Parallel imaging
 - Image domain methods:
 - SENSE
 - k-space domain methods:
 - SMASH
 - GRAPPA (next time)

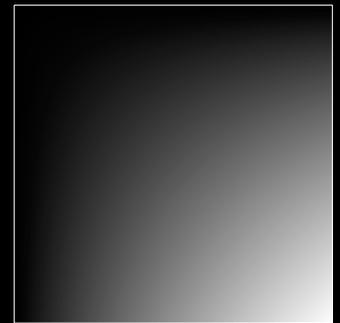
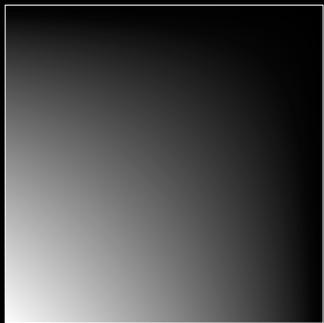
Multi-coil Arrays



Multi-coil Sensitivity



$$\| \vec{B}(\vec{r}) \|$$



Multi-coil Reconstruction

- Each coil has a complete image of whole FOV and an amplitude and phase sensitivity

$$C_l(\vec{x}) \quad l = 1, 2, \dots, L$$

- Coils are coupled, so noise is correlated

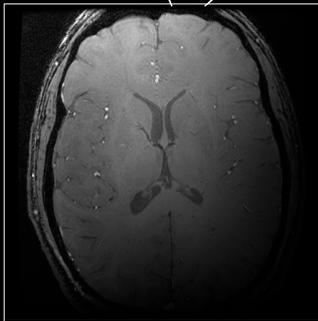
$$E[n_i n_j] = \Psi$$

- Received data from coil l :

$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x}) + n_l(\vec{x})$$

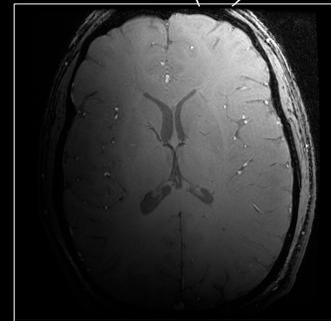
- Given $m_l(x)$, how do we reconstruct $m(x)$?

$m_1(x)$

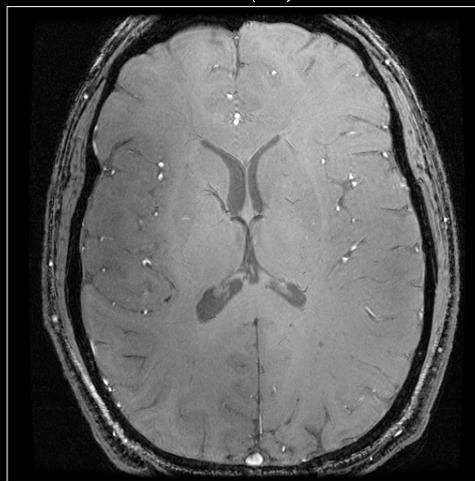


Multi-coil Images

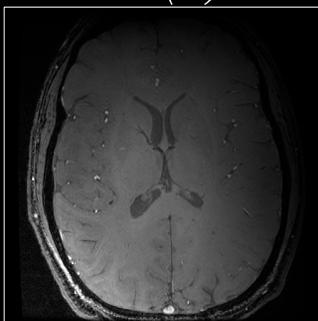
$m_2(x)$



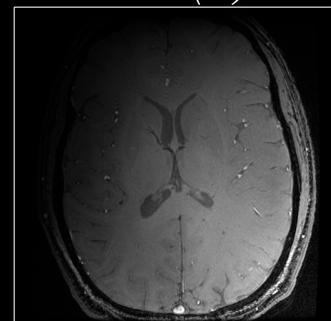
$m_s(x)$



$m_3(x)$



$m_4(x)$



Multi-coil Reconstruction

For a particular voxel \vec{x}

$$\begin{pmatrix} m_1(\vec{x}) \\ m_2(\vec{x}) \\ \vdots \\ m_L(\vec{x}) \end{pmatrix} = \begin{pmatrix} C_1(\vec{x}) \\ C_2(\vec{x}) \\ \vdots \\ C_L(\vec{x}) \end{pmatrix} m(\vec{x}) + \begin{pmatrix} n_1(\vec{x}) \\ n_2(\vec{x}) \\ \vdots \\ n_L(\vec{x}) \end{pmatrix}$$

OR

$$\begin{matrix} m_s(\vec{x}) & = & C m(\vec{x}) & + & n \\ L \times 1 & & L \times 1 & & L \times 1 \end{matrix}$$

Minimum Variance Estimate

$$\hat{m}(\vec{x}) = \underbrace{(C^* \Psi^{-1} C)^{-1}}_{1 \times 1} \underbrace{C^* \Psi^{-1}}_{1 \times L} \underbrace{m_s(\vec{x})}_{L \times 1}$$

Covariance (variance)

$$COV(\hat{m}(\vec{x})) = C^* \Psi^{-1} C$$

What if Ψ is $\sigma^2 I$?

$$\hat{m}(\vec{x}) = \underbrace{(C^* C)^{-1}}_{\text{Intensity}} \underbrace{C^*}_{\text{Phase}} m_s(\vec{x})$$

Intensity Phase
Correction Correction

Approximate Solution

- Often we don't know $C_l(x)$, but

$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x})$$

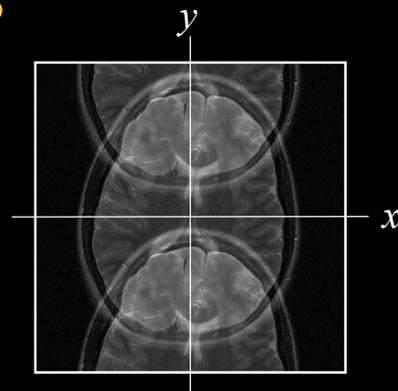
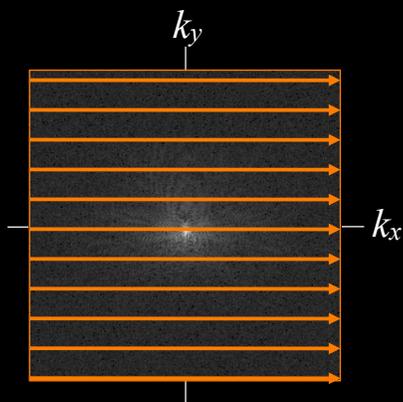
- Approximate solution:

$$\hat{m}_{SS}(\vec{x}) = \sqrt{\sum_l m_l^*(\vec{x})m_l(\vec{x})}$$

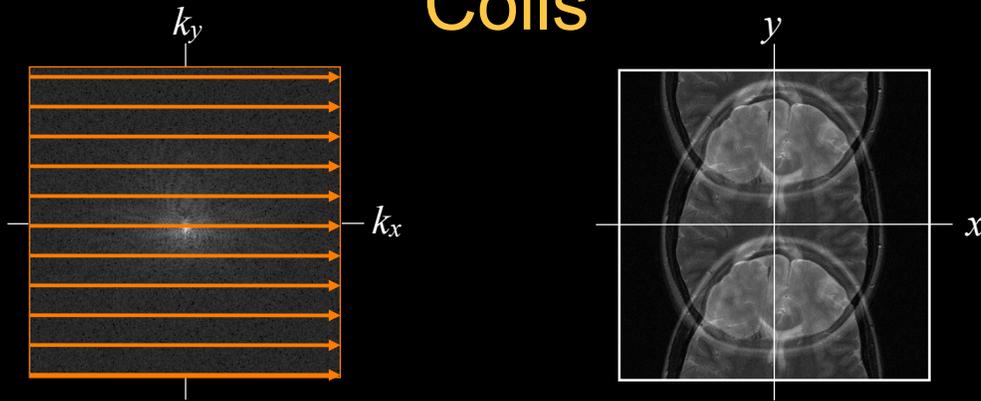
- For SNR > 20, within 10% of optimal solution

PB Roemer et al. MRM 1990

Accelerate Imaging with Array Coils



Accelerate Imaging with Array Coils



- Parallel Imaging
 - Coil elements provide some localization
 - Undersample in k-space, producing aliasing
 - Sort out in reconstruction

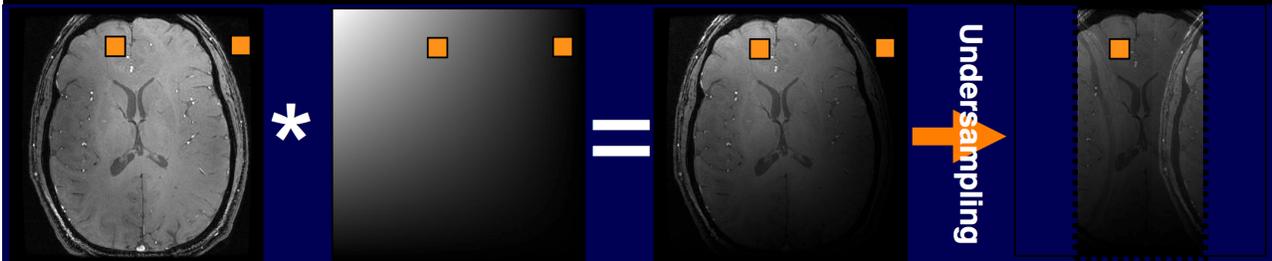
Parallel Imaging

- Many approaches:
 - Image domain - SENSE
 - k-space domain - SMASH, GRAPPA
 - Hybrid - ARC
- We will focus on two:
 - SENSE: optimal if you know coil sensitivities
 - GRAPPA: autocalibrating / robust

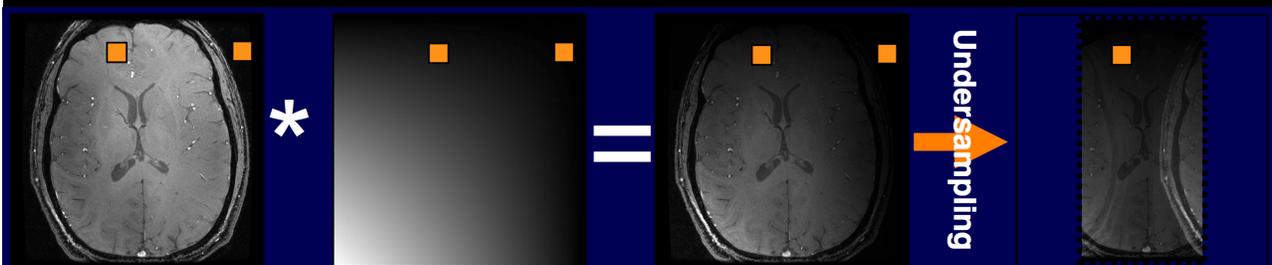
Parallel Imaging (SENSE)

Cartesian SENSE

$$m_1(\vec{x}_1) = C_1(\vec{x}_1)m(\vec{x}_1) + C_1(\vec{x}_2)m(\vec{x}_2)$$



$$m_2(\vec{x}_1) = C_2(\vec{x}_1)m(\vec{x}_1) + C_2(\vec{x}_2)m(\vec{x}_2)$$



$$\begin{pmatrix} m_1(\vec{x}_1) \\ m_2(\vec{x}_1) \\ \vdots \\ m_L(\vec{x}_1) \end{pmatrix} = \begin{pmatrix} C_1(\vec{x}_1) & C_1(\vec{x}_2) \\ C_2(\vec{x}_1) & C_2(\vec{x}_2) \\ \vdots & \vdots \\ C_L(\vec{x}_1) & C_L(\vec{x}_2) \end{pmatrix} \begin{pmatrix} m(\vec{x}_1) \\ m(\vec{x}_2) \end{pmatrix} + \begin{pmatrix} n_1(\vec{x}_1) \\ n_2(\vec{x}_1) \\ \vdots \\ n_L(\vec{x}_1) \end{pmatrix}$$

Aliased Images
Sensitivity at Source Voxels
Source Voxels

OR

$$\begin{matrix} & & 2 \times 1 \\ m_s = & C & m + n \\ L \times 1 & L \times 2 & L \times 1 \end{matrix}$$

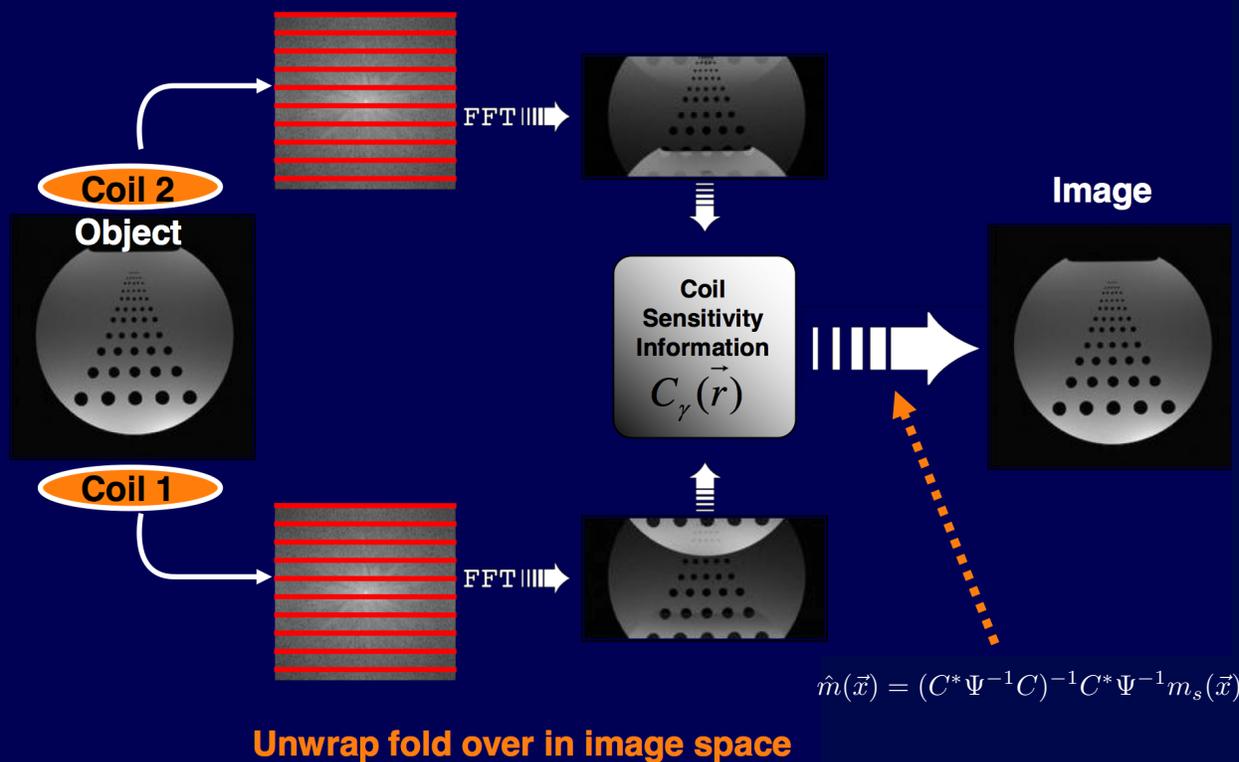
$$\hat{m}(\vec{x}) = \underbrace{(C^* \Psi^{-1} C)^{-1}}_{2 \times 2} \underbrace{C^* \Psi^{-1}}_{2 \times L} \underbrace{m_s(\vec{x})}_{L \times 1}$$

L aliased reconstruction resolves 2 image pixels

For an N x N image, we solve (N/2 x N)
2 x 2 inverse systems

For an acceleration factor R, we solve (N/R x N)
R x R inverse systems

SENSE Reconstruction



SNR Cost

- How large can R be?
- Two SNR loss mechanisms
 - Reduced scan time
 - Condition of the SENSE decomposition
- SNR Loss

$$SNR_{SENSE} = \frac{SNR}{g\sqrt{R}}$$

Geometry Reduced
Factor Scan Time

Geometry Factor

- Covariance for a fully sampled image (variance of one voxel):

$$\chi_F = \frac{1}{n_F} (C_F^* \Psi^{-1} C_F)^{-1}$$

- Covariance for a reduced encoded image:

$$\chi_R = \frac{1}{n_R} (C_R^* \Psi^{-1} C_R)^{-1}$$

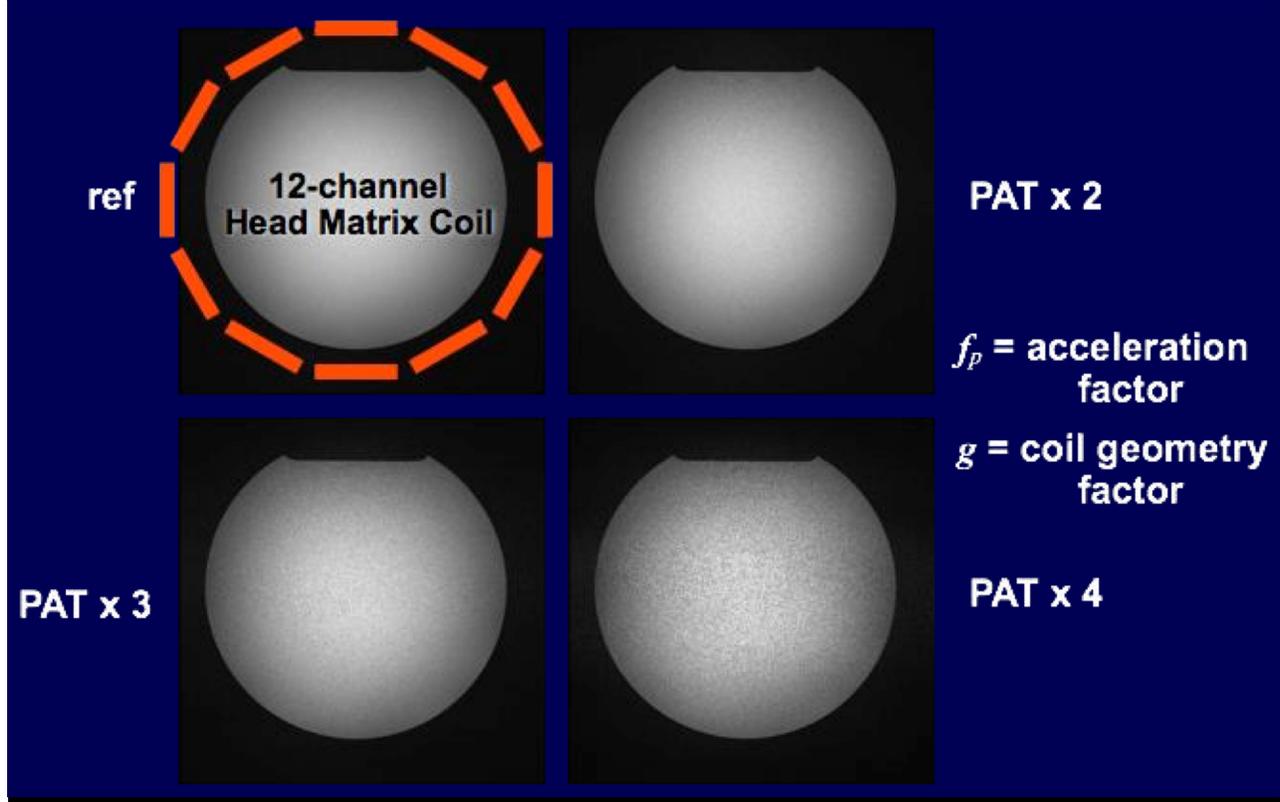
To the board ...

Geometry Factor

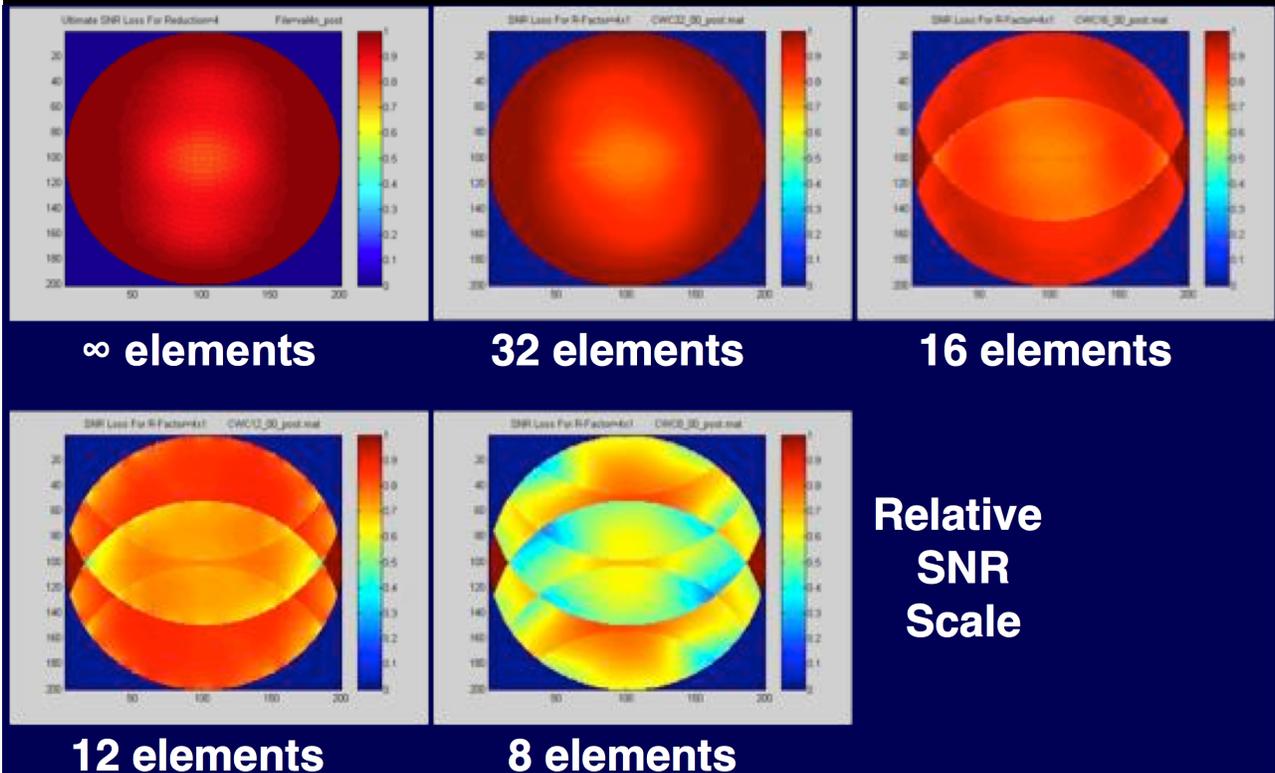
- g-factor is critical since it depends on:
 - Acceleration
 - Spatial position
 - Aliasing direction
 - Coil geometry
- Minimizing g-factor drives system design
- Sense coils are different from traditional array coils

To the board ...

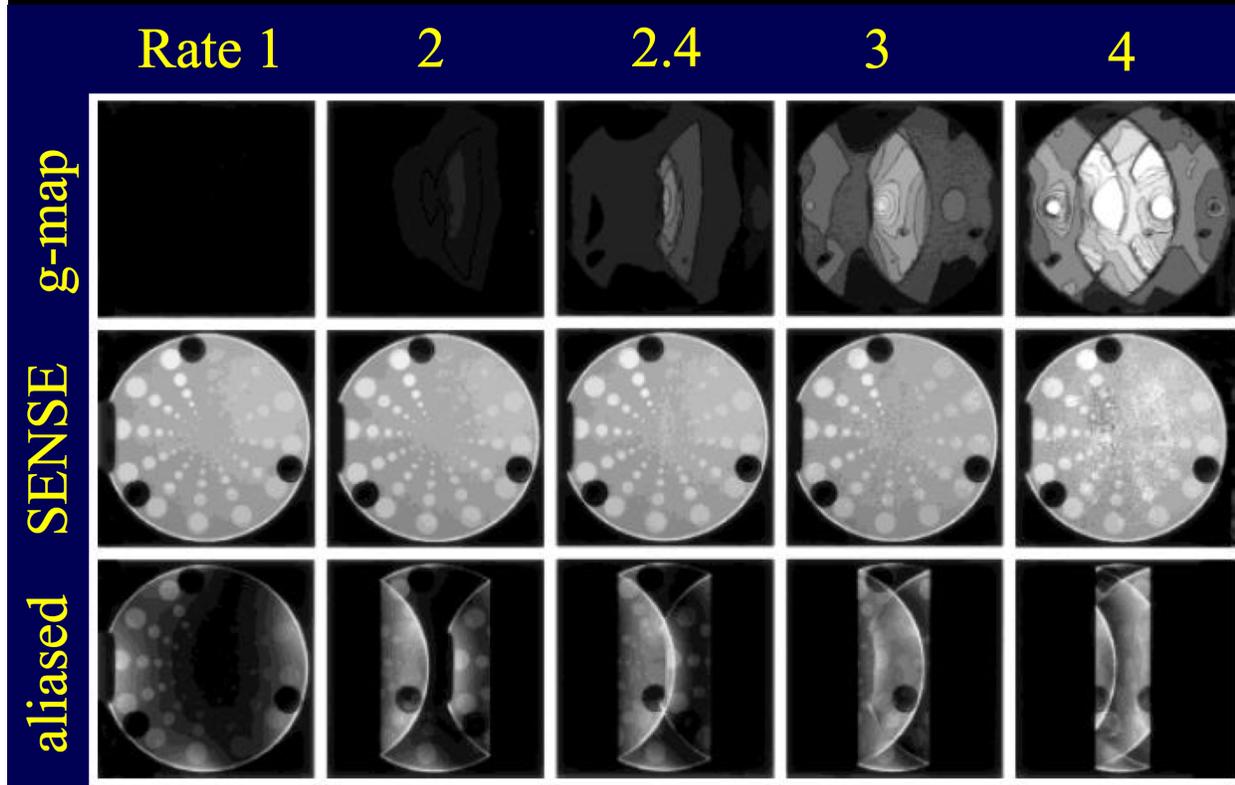
Parallel Imaging Tradeoffs



1/g-factor Map for R=4

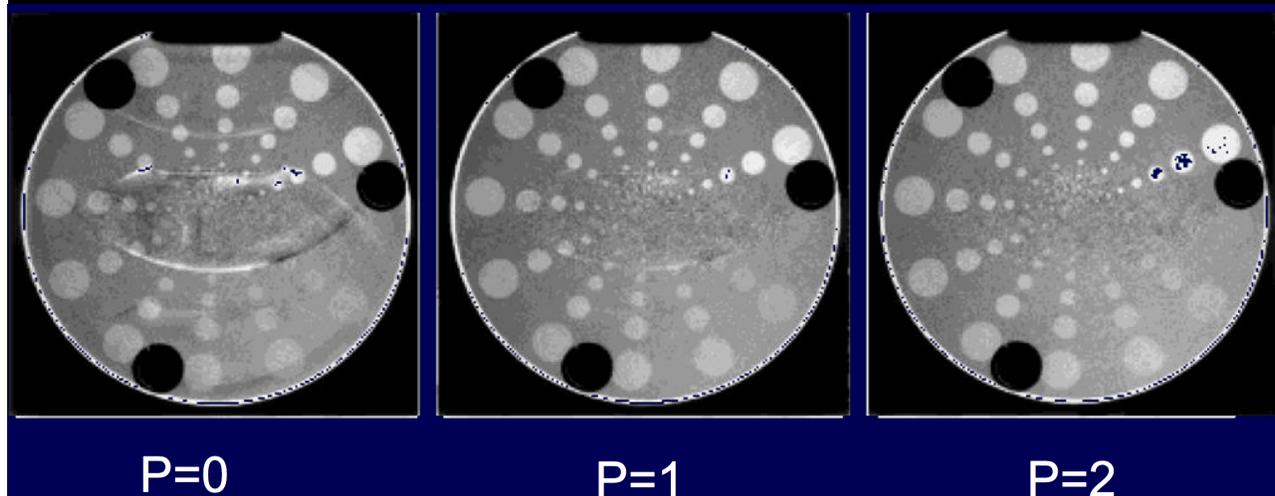


g-factor and its impact on images



Dependence on Coil Sensitivity

- Images reconstructed using coil sensitivity maps with different order P of polynomial fitting



Parallel Imaging (SMASH)

SMASH

- Simultaneous Acquisition of Spatial Harmonics (SMASH) uses linear combinations of acquired k-space data from multiple coils to generate multiple data sets with offsets in k-space

Phase Encoding by Amplitude Modulation

- Signal Equation:

$$S(k_x, k_y) = \int \int C(x, y) \rho(x, y) e^{-ik_x x - ik_y y} dx dy$$

$\rho(x, y)$ = spin density

$C(x, y)$ = receiver coil sensitivity

Phase Encoding by Amplitude Modulation

$$S(k_x, k_y) = \int \int C(x, y) \rho(x, y) e^{-ik_x x - ik_y y} dx dy$$

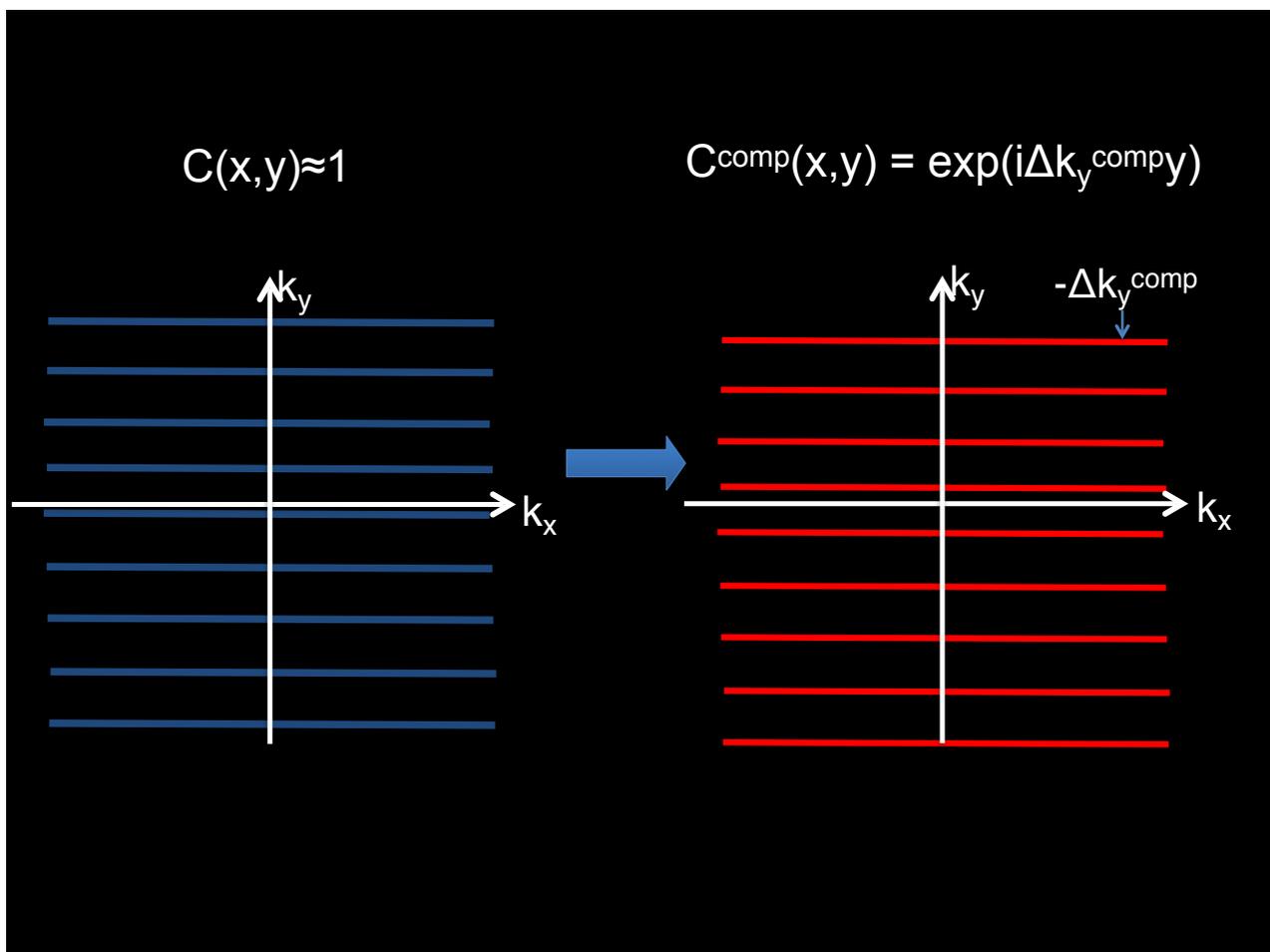
- If $C(x, y) \approx 1$ (relatively homogeneous coil sensitivity), $S(k_x, k_y) = \text{FT}\{\rho(x, y)\}$
- But coils often do not have uniform sensitivity, and usually there is a fall-off of sensitivity with distance from the coil

Phase Encoding by Amplitude Modulation

- Use the arrangement of coils to construct sinusoidal sensitivity profiles
 - Sensitivity profiles are combination of multiple coils, whose signals are combined to produce the desired sinusoidal sensitivity

$$\begin{aligned}C^{comp}(y) &= \cos(\Delta k_y^{comp} y) + i \sin(\Delta k_y^{comp} y) \\ &= e^{i\Delta k_y^{comp} y}\end{aligned}$$

The wavelength could be $\lambda = 2\pi/\Delta k_y = \text{FOV}$



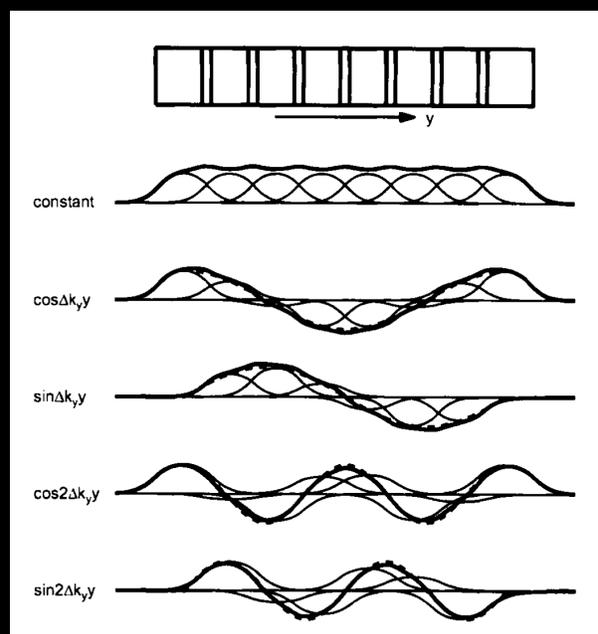
Spatial Harmonic Generation Using Coil Arrays

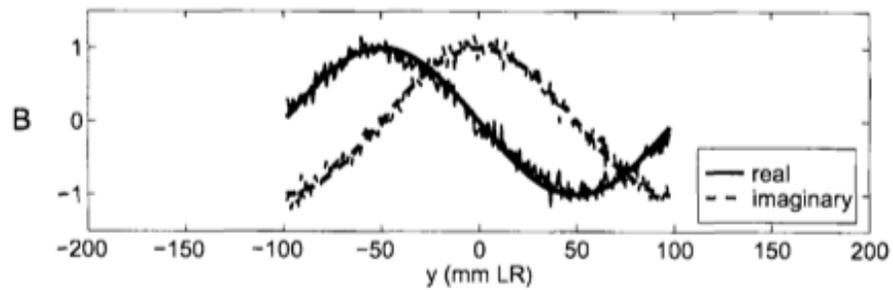
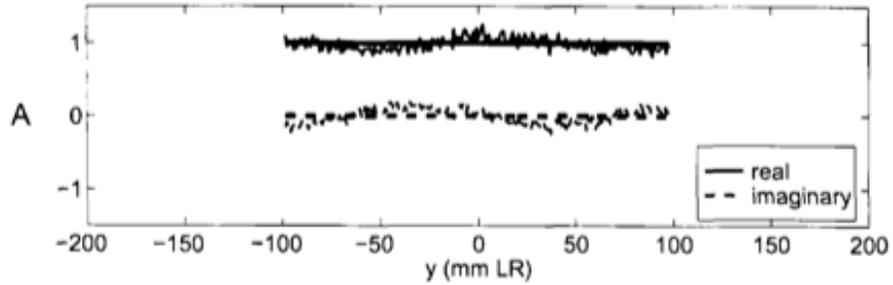
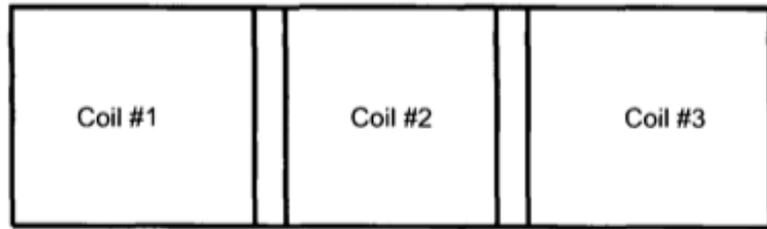
$$C_m^{comp}(y) = \sum_j a_{j,m} C_j(y) = e^{-i2\pi m \Delta k_y y}$$

- Linear surface coil array sensitivities C_j are combined with linear weights, $a_{j,m}$, to produce composite sinusoidal sensitivity
- Composite sensitivities are arranged to be spatial harmonics
- m is an integer, chosen to be a desired harmonic

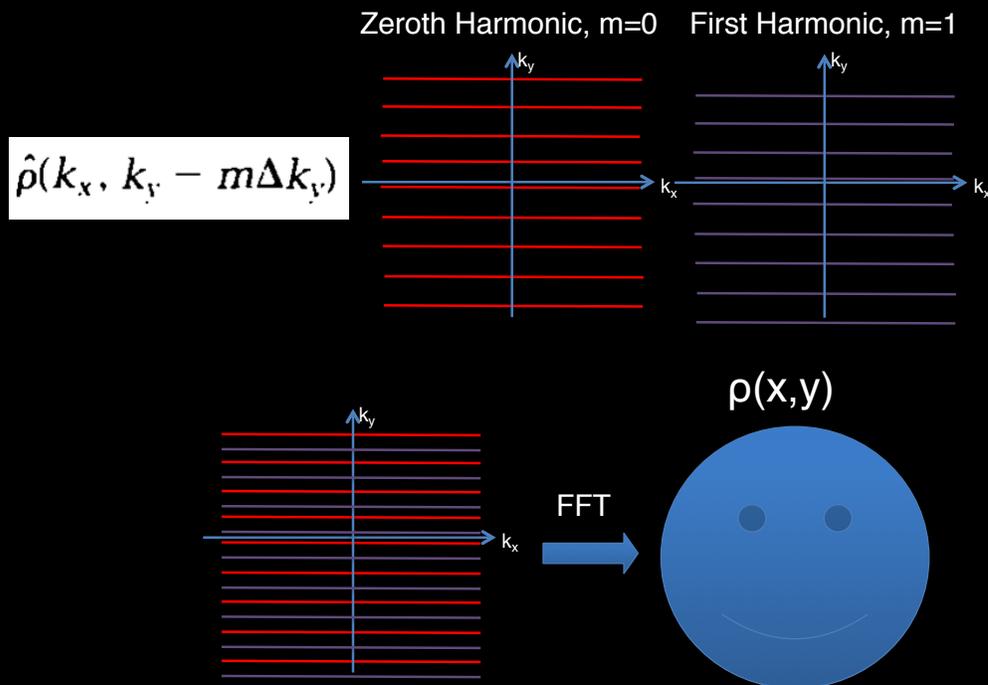
Theory: Spatial Harmonics

- 8 coil array
- Gaussian coil sensitivity distribution used
- $m = 0, 1, -1, 2, -2$
- Each spatial harmonic generated is shifted by $-m\Delta k_y$

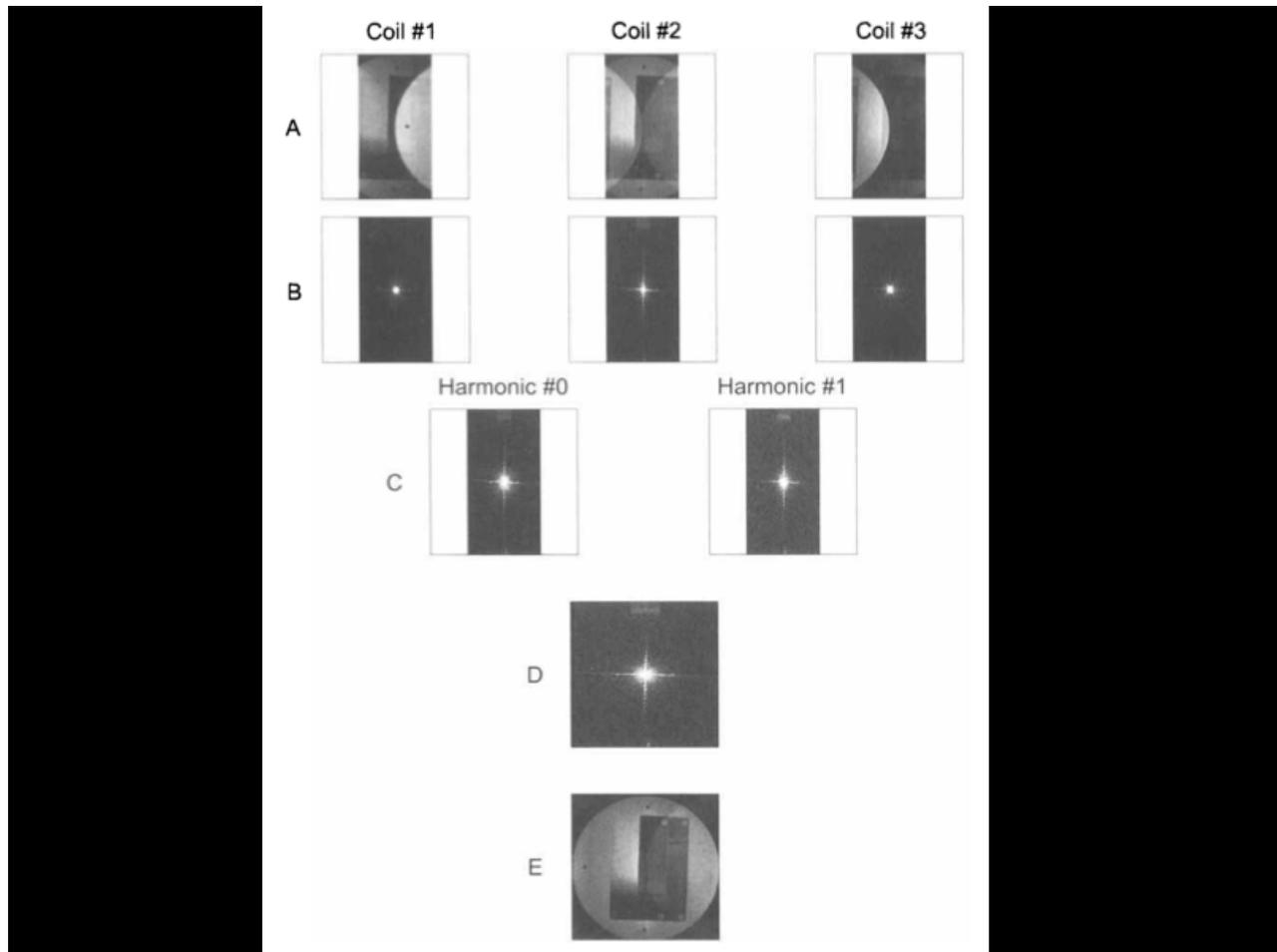
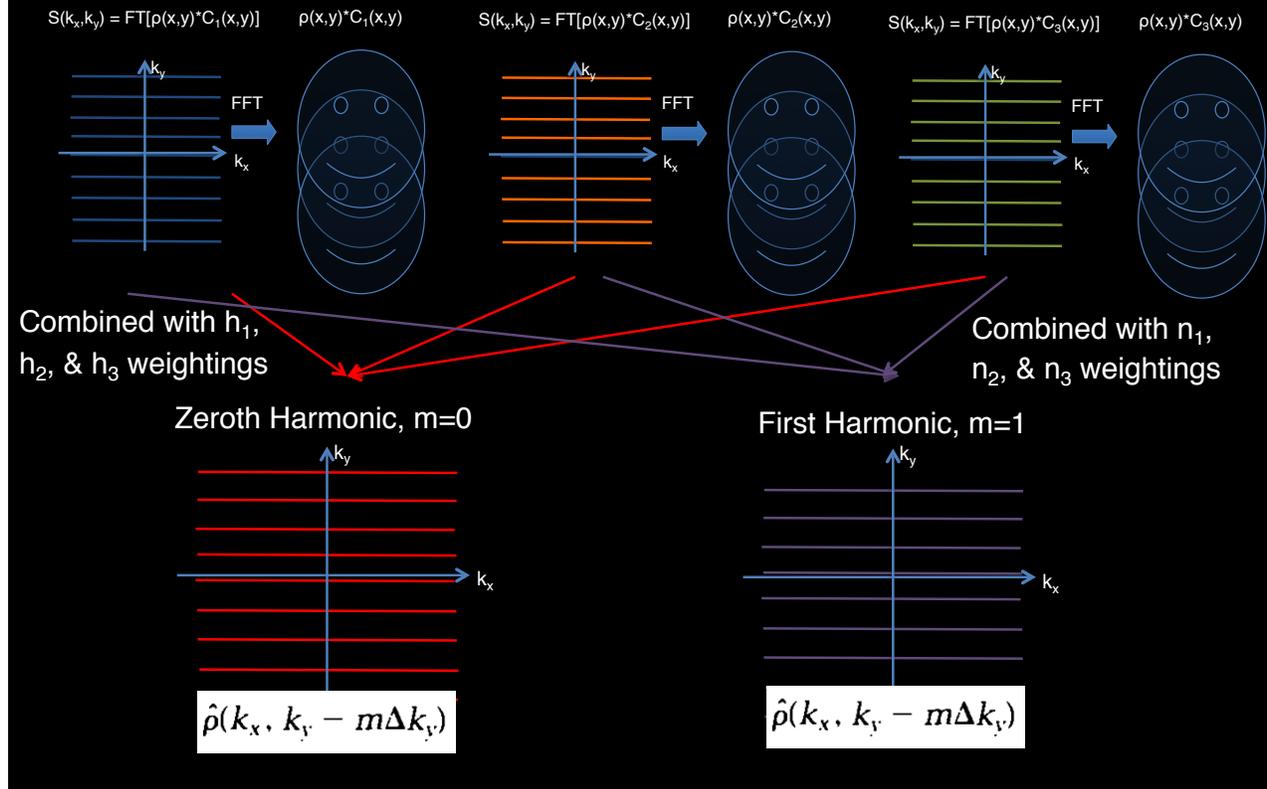




Interleave the Harmonics

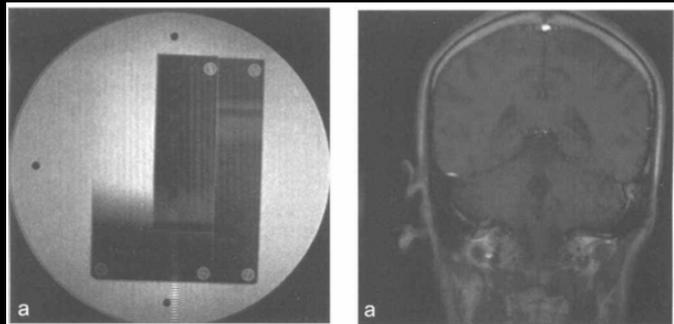


SMASH Reconstruction

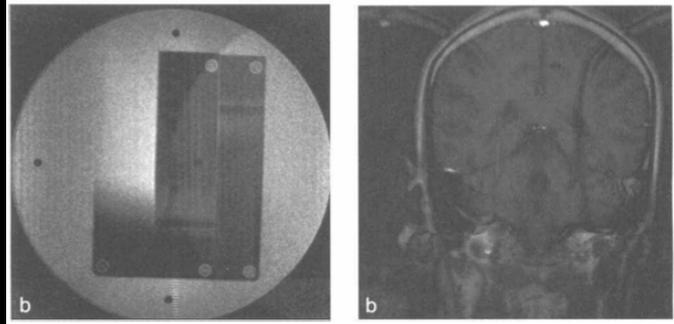


Three-Element Array

Reference images



SMASH images



Four-Element Array

Reference images



SMASH images



Key Points of SMASH

- k-space lines are synthesized by combining signals from multiple coils such that it creates a partial replacement for a phase encoding gradient
- Decreases acquisition time by 1/N
 - N is the number of generated spatial Harmonics

$$\sum_j a_{j,m} C_j(y) = e^{-i2\pi \Delta k_y y}$$

Sodickson et al. MRM 1997

Summary

- Parallel imaging utilizes coil sensitivities to increase the speed of MRI
- Cases for parallel imaging
 - Higher patient throughput,
 - Real-time imaging/Interventional imaging
 - Motion suppression
- Cases against parallel imaging
 - SNR starving applications

Further Reading

- Multi-coil Reconstruction
 - <http://onlinelibrary.wiley.com/doi/10.1002/mrm.1910160203/abstract>
- SENSE
 - <http://www.ncbi.nlm.nih.gov/pubmed/10542355>
- SMASH
 - <http://www.ncbi.nlm.nih.gov/pubmed/9324327>
- Parallel Imaging Overview
 - <http://www.ncbi.nlm.nih.gov/pubmed/17374908>

Thanks!

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