

# Image Reconstruction

## *Parallel Imaging I*

M229 Advanced Topics in MRI

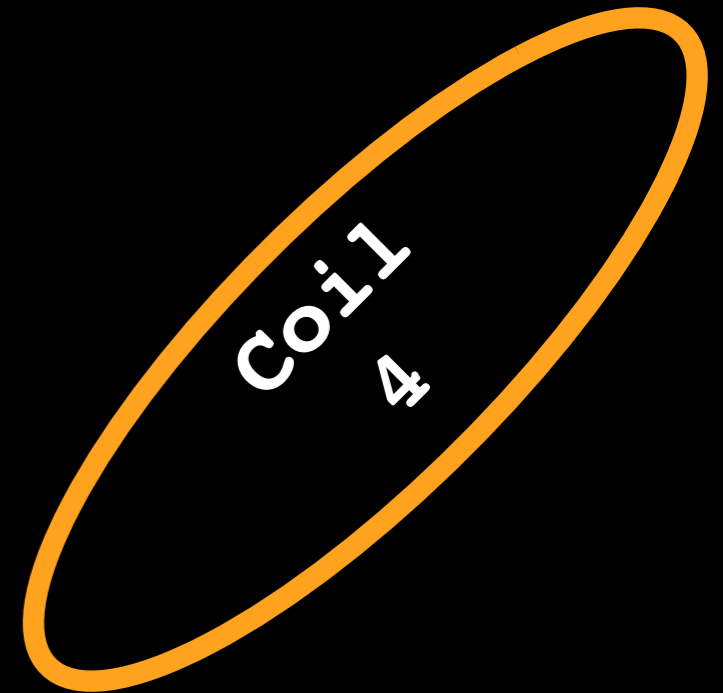
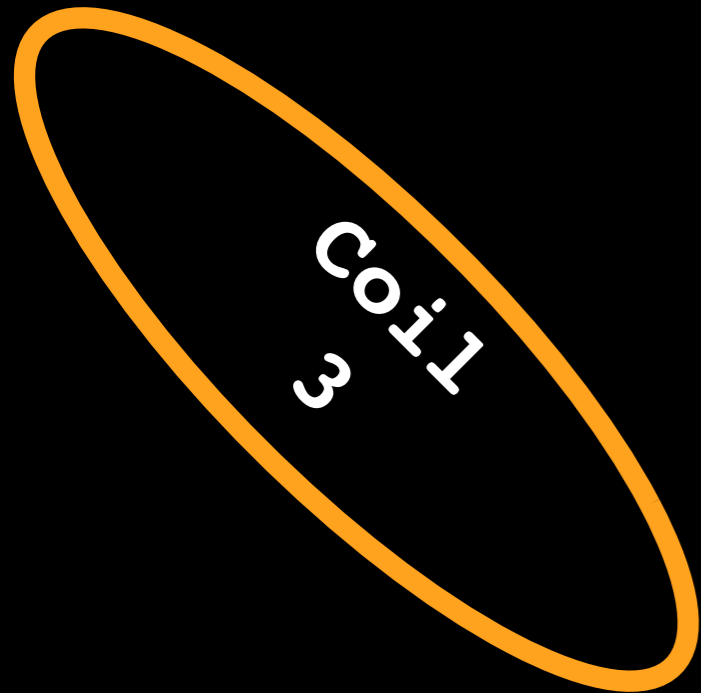
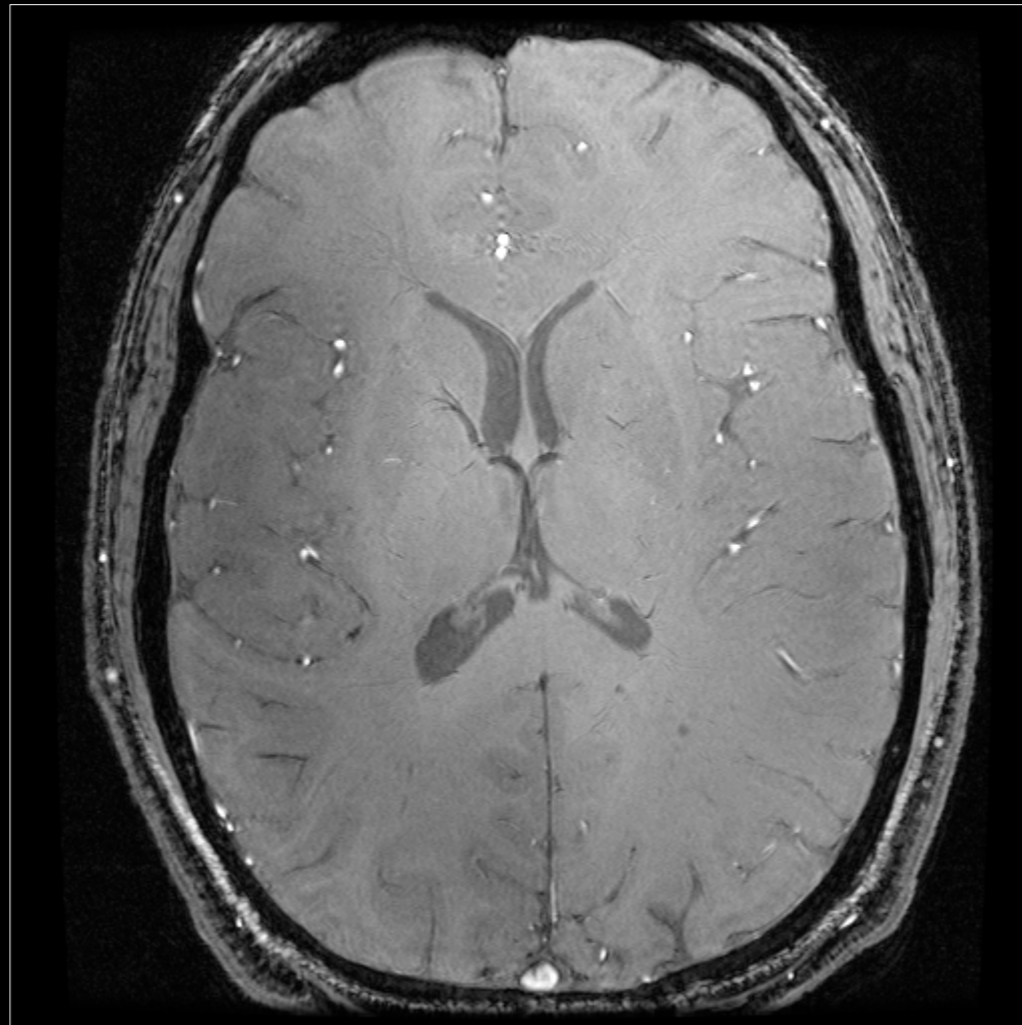
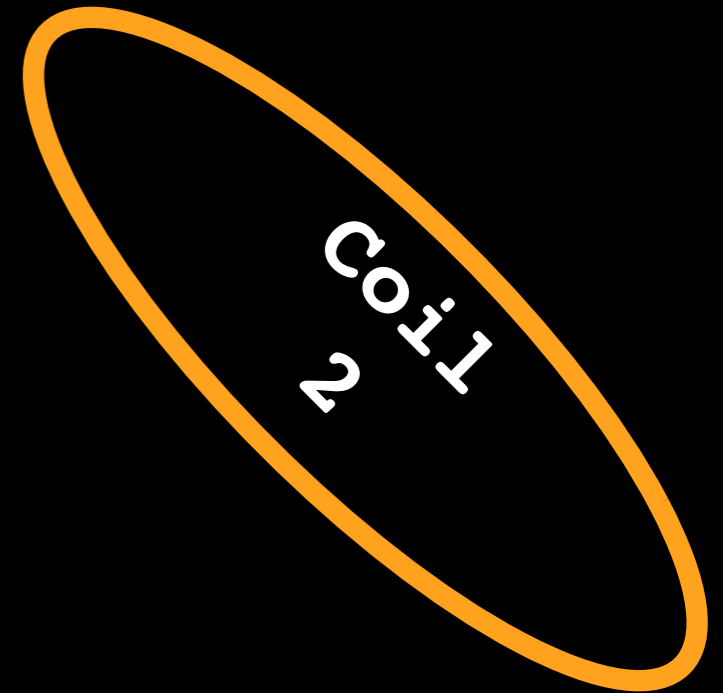
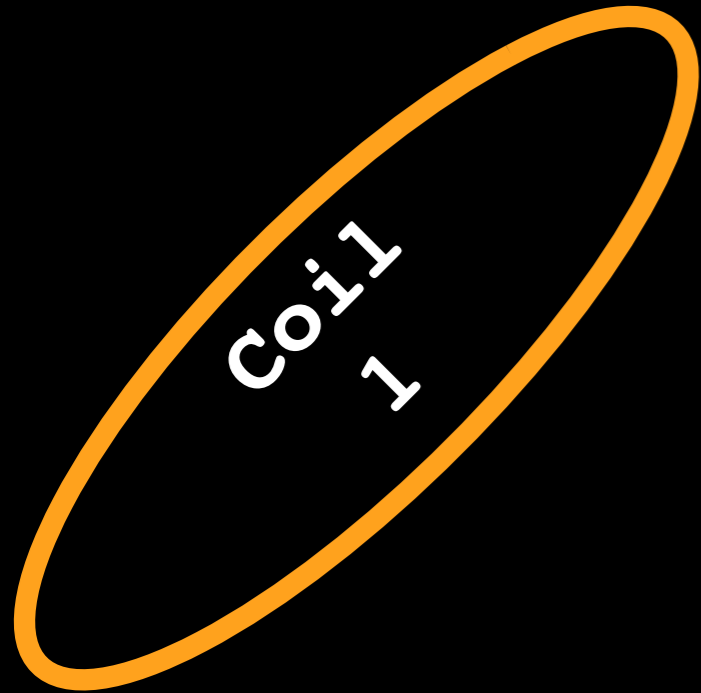
Kyung Sung, Ph.D.

2020.05.19

# Today's Topics

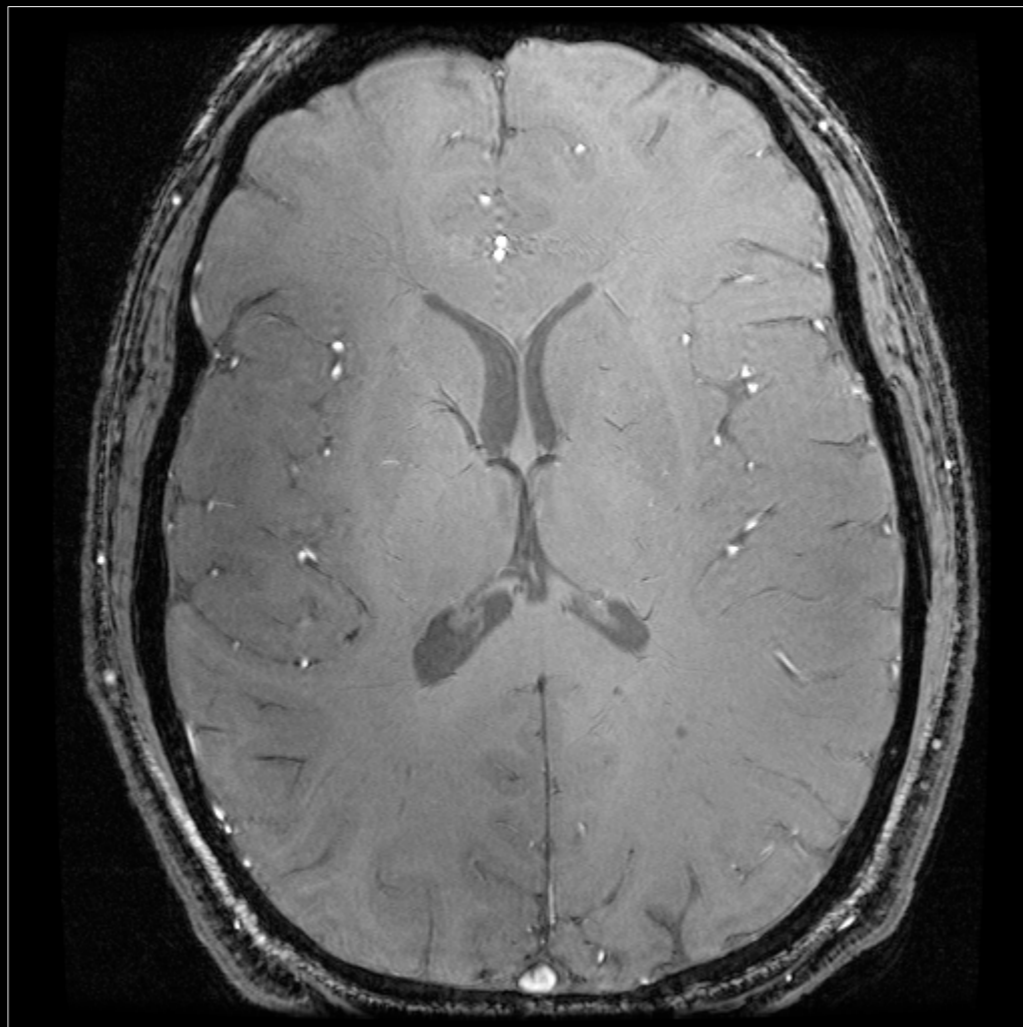
- Multicoil reconstruction
- Parallel imaging
  - Image domain methods:
    - SENSE
  - k-space domain methods:
    - SMASH
    - GRAPPA (next time)

# Multi-coil Arrays



# Multi-coil Sensitivity

$$\| \vec{B}(\vec{r}) \|$$



# Multi-coil Reconstruction

- Each coil has a complete image of whole FOV and an amplitude and phase sensitivity

$$C_l(\vec{x}) \quad l = 1, 2, \dots, L$$

- Coils are coupled, so noise is correlated

$$E[n_i n_j] = \Psi$$

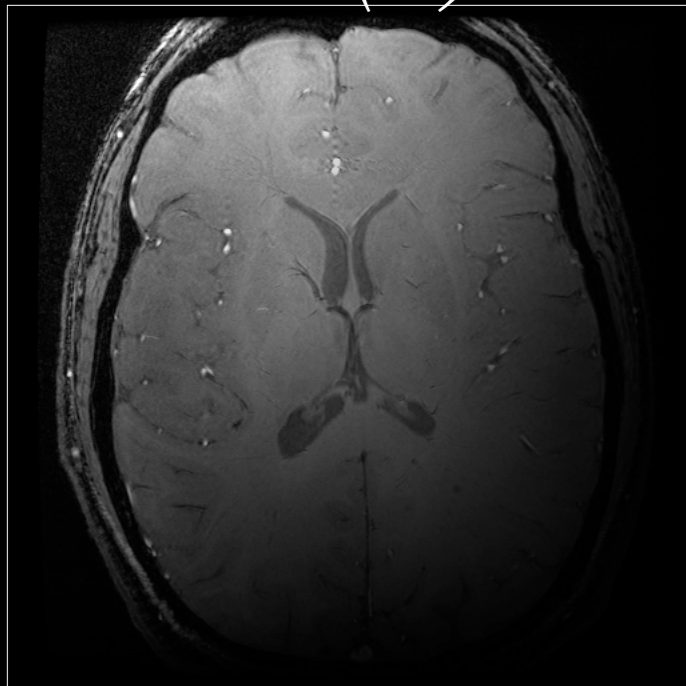
- Received data from coil  $l$ :

$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x}) + n_l(\vec{x})$$

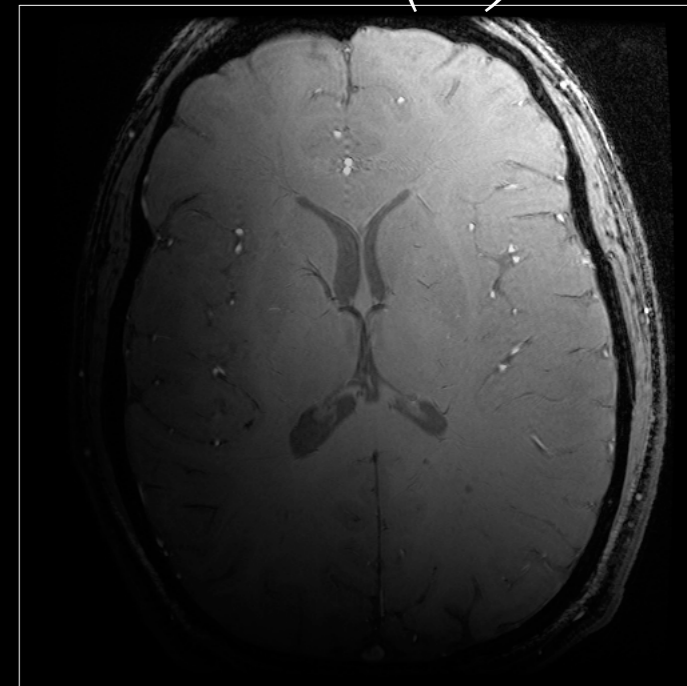
- Given  $m_l(x)$ , how do we reconstruct  $m(x)$ ?

# Multi-coil Images

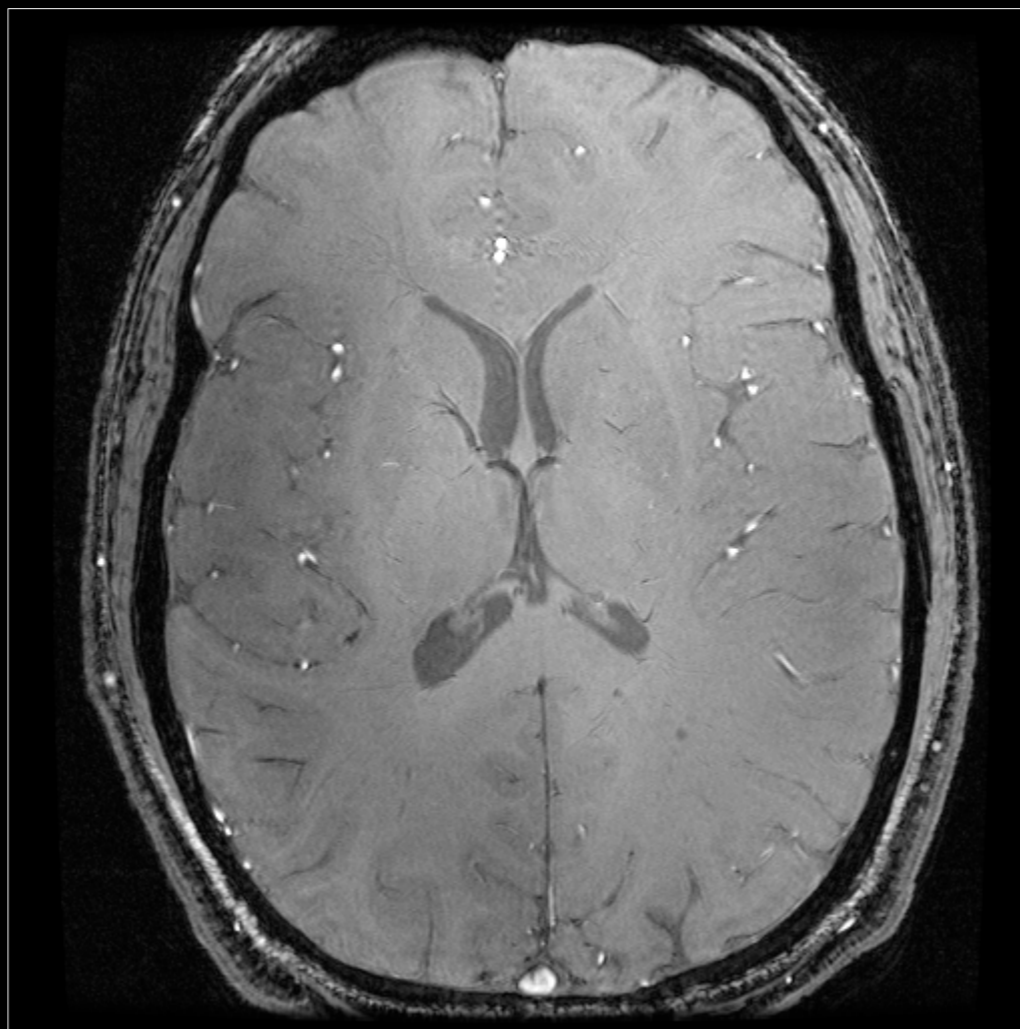
$m_1(x)$



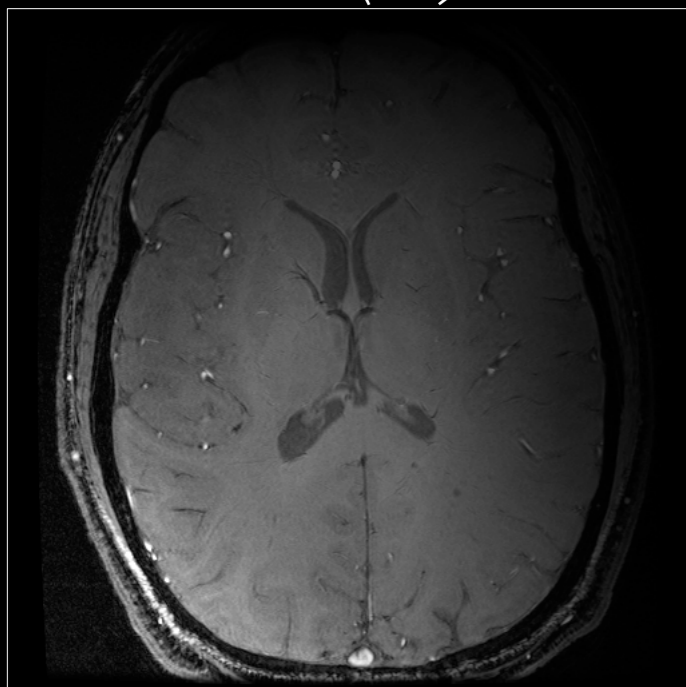
$m_2(x)$



$m_s(x)$



$m_3(x)$



$m_4(x)$



# Multi-coil Reconstruction

For a particular voxel  $\vec{x}$

$$\begin{pmatrix} m_1(\vec{x}) \\ m_2(\vec{x}) \\ \vdots \\ m_L(\vec{x}) \end{pmatrix} = \begin{pmatrix} C_1(\vec{x}) \\ C_2(\vec{x}) \\ \vdots \\ C_L(\vec{x}) \end{pmatrix} m(\vec{x}) + \begin{pmatrix} n_1(\vec{x}) \\ n_2(\vec{x}) \\ \vdots \\ n_L(\vec{x}) \end{pmatrix}$$

OR

$$\begin{array}{ccccc} \underline{m_s(\vec{x})} & = & \underline{C} \underline{m(\vec{x})} & + & \underline{n} \\ \mathbf{L \times 1} & & \mathbf{L \times 1} & & \mathbf{L \times 1} \end{array}$$

# Minimum Variance Estimate

$$\hat{m}(\vec{x}) = \underbrace{(C^* \Psi^{-1} C)^{-1}}_{1 \times 1} \underbrace{C^* \Psi^{-1}}_{1 \times L} \underbrace{m_s(\vec{x})}_{L \times 1}$$

Covariance (variance)

$$COV(\hat{m}(\vec{x})) = C^* \Psi^{-1} C$$

What if  $\Psi$  is  $\sigma^2 I$ ?

$$\hat{m}(\vec{x}) = \underbrace{(C^* C)^{-1}}_{\text{Intensity}} \underbrace{C^*}_{\text{Phase}} m_s(\vec{x})$$

Intensity Correction      Phase Correction



# Approximate Solution

- Often we don't know  $C_l(x)$ , but

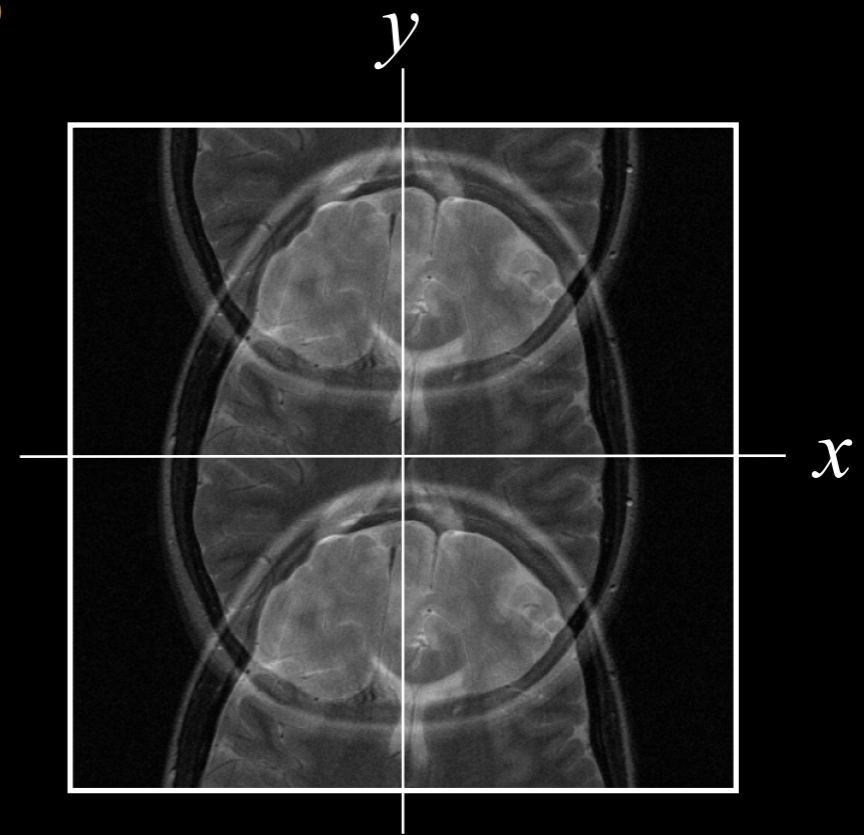
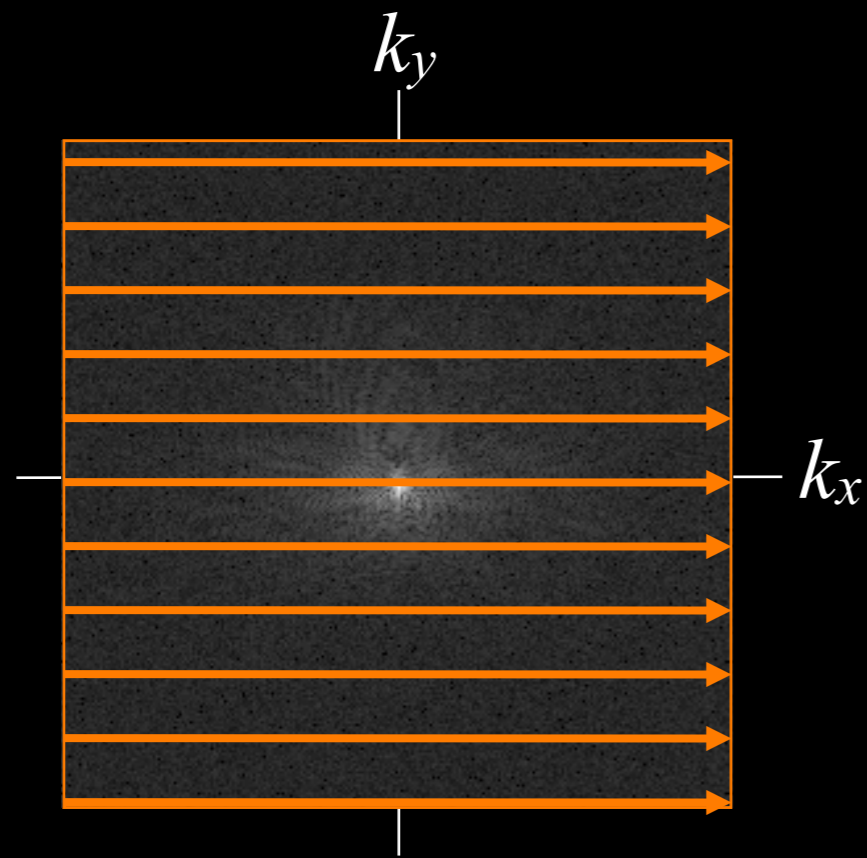
$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x})$$

- Approximate solution:

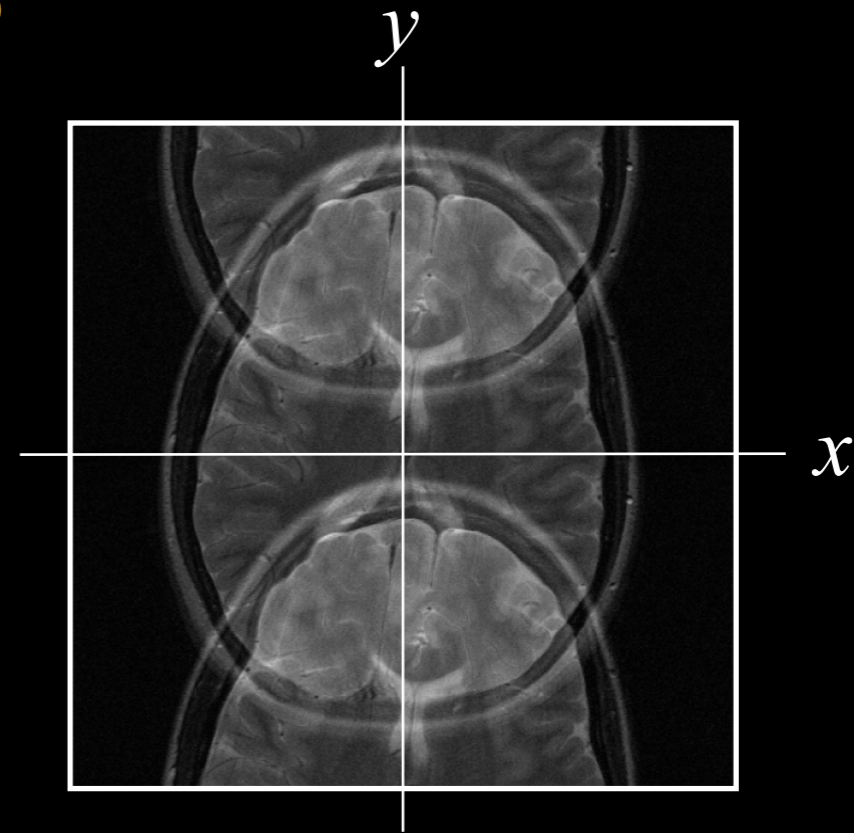
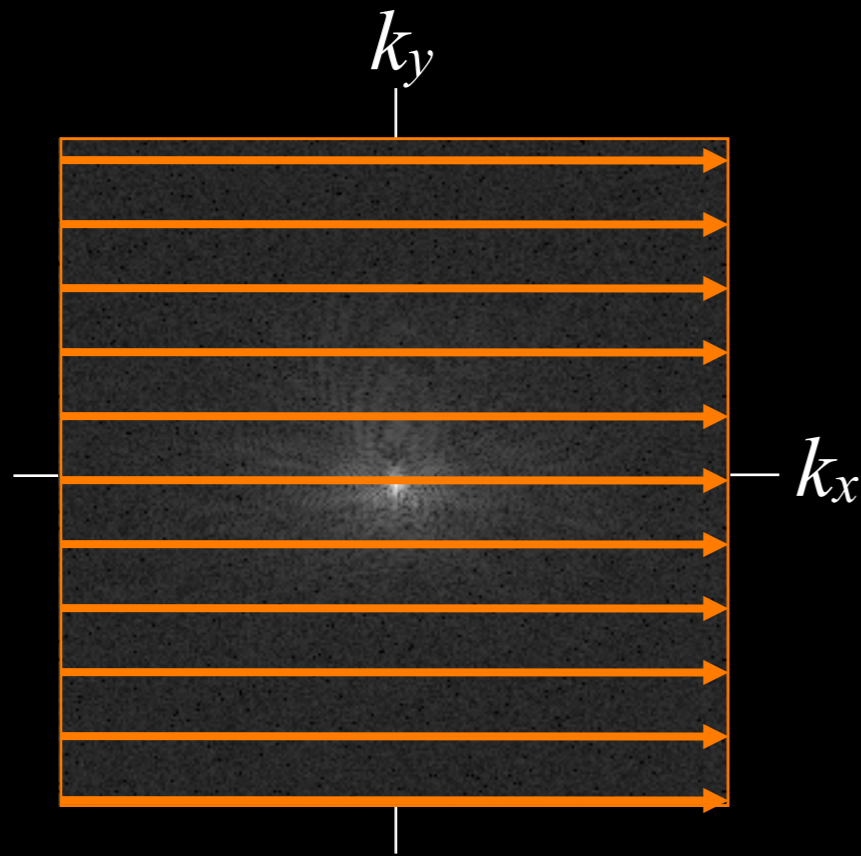
$$\hat{m}_{SS}(\vec{x}) = \sqrt{\sum_l m_l^*(\vec{x})m_l(\vec{x})}$$

- For SNR > 20, within 10% of optimal solution

# Accelerate Imaging with Array Coils



# Accelerate Imaging with Array Coils



- Parallel Imaging
  - Coil elements provide some localization
  - Undersample in k-space, producing aliasing
  - Sort out in reconstruction

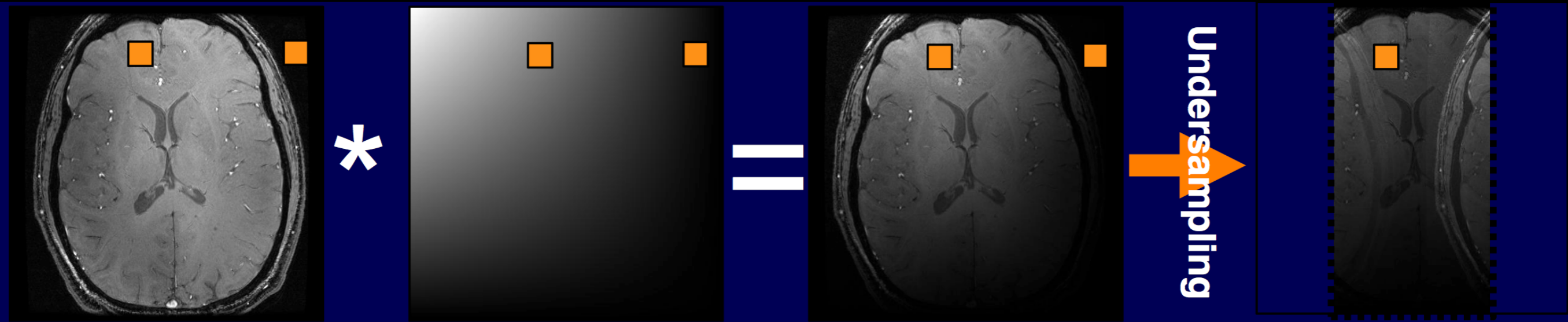
# Parallel Imaging

- Many approaches:
  - Image domain - SENSE
  - k-space domain - SMASH, GRAPPA
  - Hybrid - ARC
  
- We will focus on two:
  - SENSE: optimal if you know coil sensitivities
  - GRAPPA: autocalibrating / robust

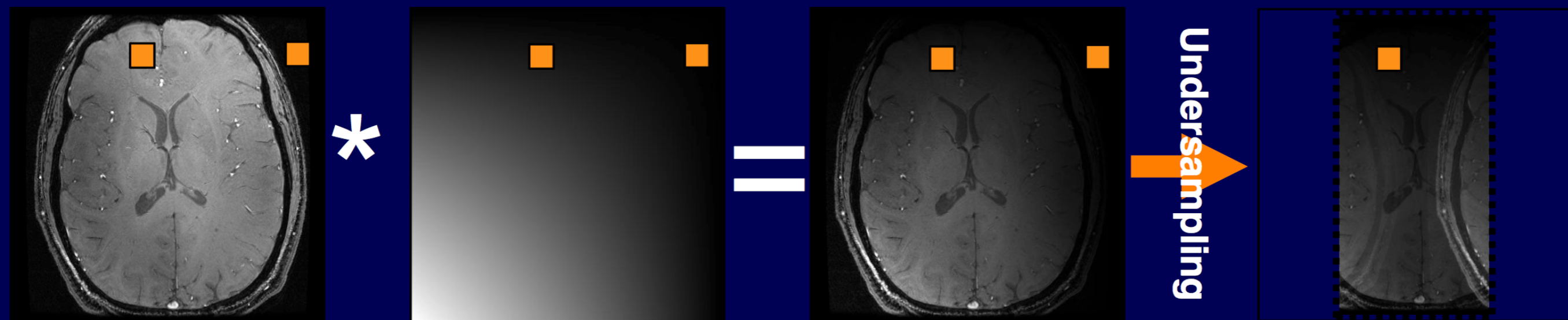
# Parallel Imaging (SENSE)

# Cartesian SENSE

$$m_1(\vec{x}_1) = C_1(\vec{x}_1)m(\vec{x}_1) + C_1(\vec{x}_2)m(\vec{x}_2)$$



$$m_2(\vec{x}_1) = C_2(\vec{x}_1)m(\vec{x}_1) + C_2(\vec{x}_2)m(\vec{x}_2)$$



$$\begin{pmatrix} m_1(\vec{x}_1) \\ m_2(\vec{x}_1) \\ \vdots \\ m_L(\vec{x}_1) \end{pmatrix} = \begin{pmatrix} C_1(\vec{x}_1) & C_1(\vec{x}_2) \\ C_2(\vec{x}_1) & C_2(\vec{x}_2) \\ \vdots & \vdots \\ C_L(\vec{x}_1) & C_L(\vec{x}_2) \end{pmatrix} \begin{pmatrix} m(\vec{x}_1) \\ m(\vec{x}_2) \end{pmatrix} + \begin{pmatrix} n_1(\vec{x}_1) \\ n_2(\vec{x}_1) \\ \vdots \\ n_L(\vec{x}_1) \end{pmatrix}$$

Aliased  
Images

Sensitivity at  
Source Voxels

Source  
Voxels

OR

$$\begin{matrix} & & 2 \times 1 \\ m_s = & C & m + n \\ L \times 1 & L \times 2 & L \times 1 \end{matrix}$$

$$\hat{m}(\vec{x}) = \underbrace{(C^* \Psi^{-1} C)^{-1}}_{2 \times 2} \underbrace{C^* \Psi^{-1}}_{2 \times L} \underbrace{m_s(\vec{x})}_{L \times 1}$$

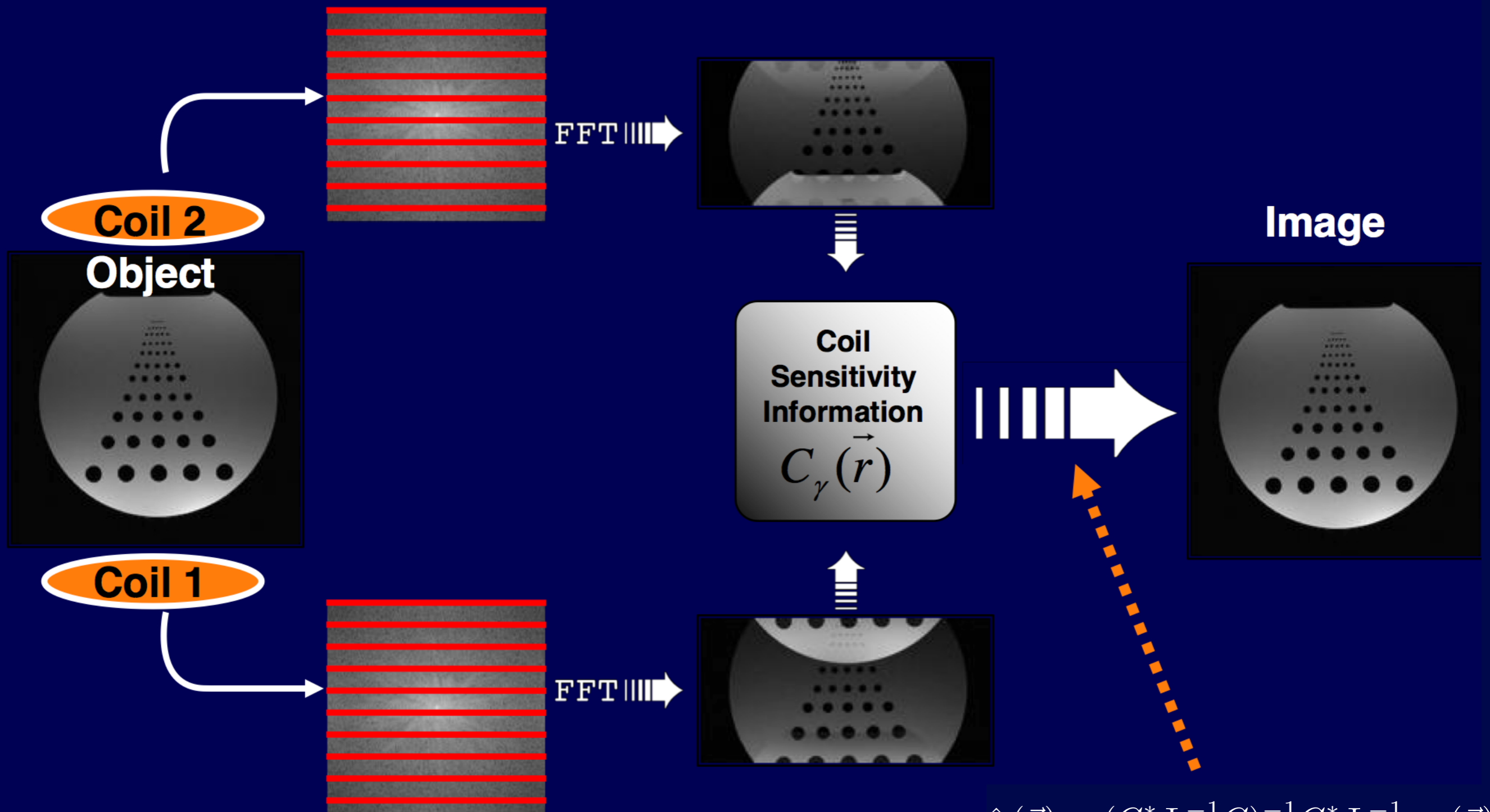
L aliased reconstruction resolves 2 image pixels

For an  $N \times N$  image, we solve  $(N/2 \times N)$   
 $2 \times 2$  inverse systems

For an acceleration factor  $R$ , we solve  $(N/R \times N)$   
 $R \times R$  inverse systems



# SENSE Reconstruction



$$\hat{m}(\vec{x}) = (C^* \Psi^{-1} C)^{-1} C^* \Psi^{-1} m_s(\vec{x})$$

**Unwrap fold over in image space**

# SNR Cost

- How large can R be?
- Two SNR loss mechanisms
  - Reduced scan time
  - Condition of the SENSE decomposition
- SNR Loss

$$SNR_{SENSE} = \frac{SNR}{g\sqrt{R}}$$

Geometry Reduced  
Factor Scan Time

# Geometry Factor

- Covariance for a fully sampled image (variance of one voxel):

$$\chi_F = \frac{1}{n_F} (C_F^* \Psi^{-1} C_F)^{-1}$$

- Covariance for a reduced encoded image:

$$\chi_R = \frac{1}{n_R} (C_R^* \Psi^{-1} C_R)^{-1}$$

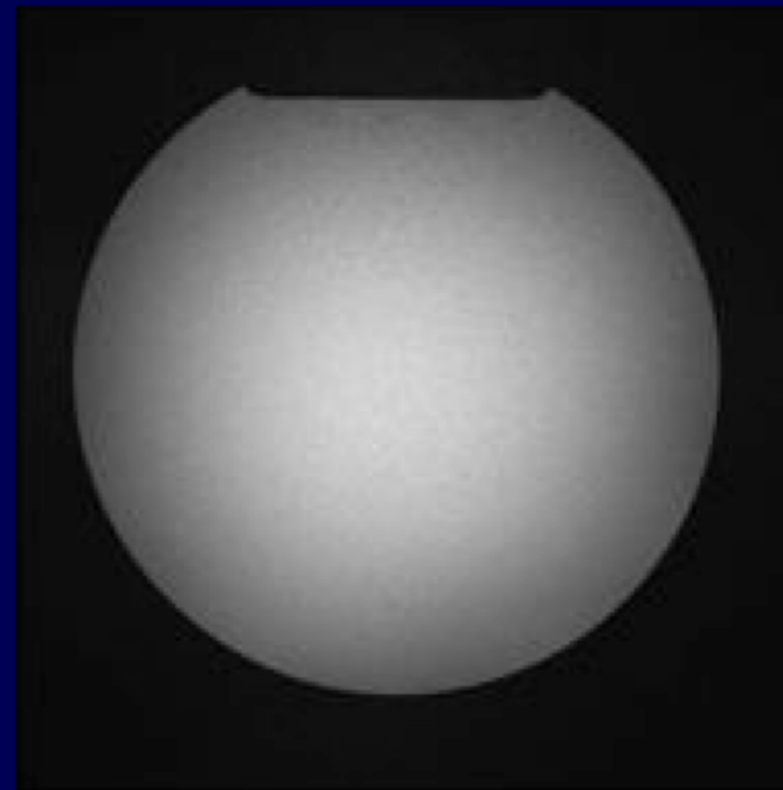
To the board ...

# Geometry Factor

- g-factor is critical since it depends on:
  - Acceleration
  - Spatial position
  - Aliasing direction
  - Coil geometry
- Minimizing g-factor drives system design
- Sense coils are different from traditional array coils

To the board ...

# Parallel Imaging Tradeoffs

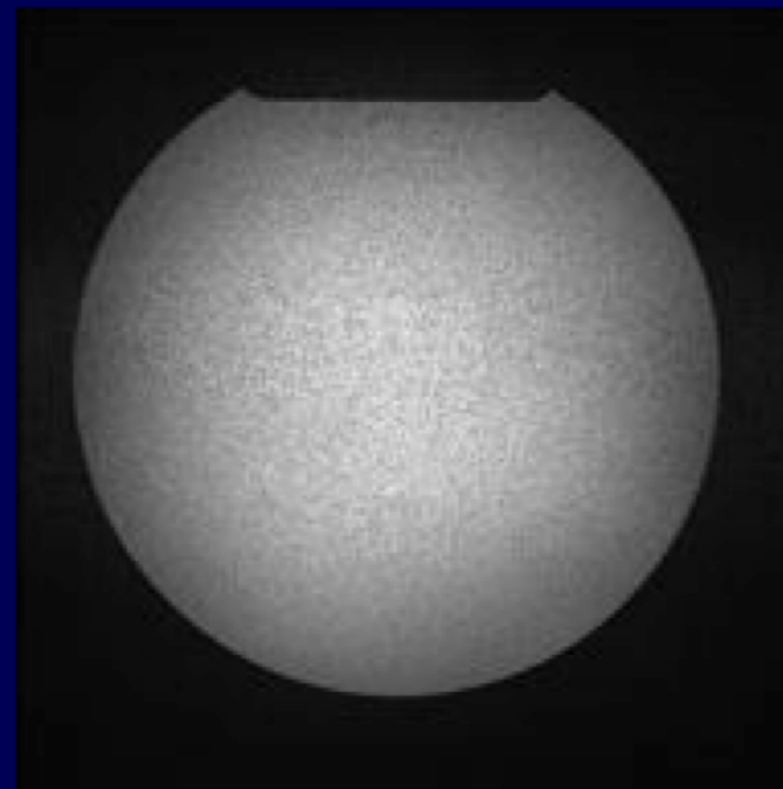
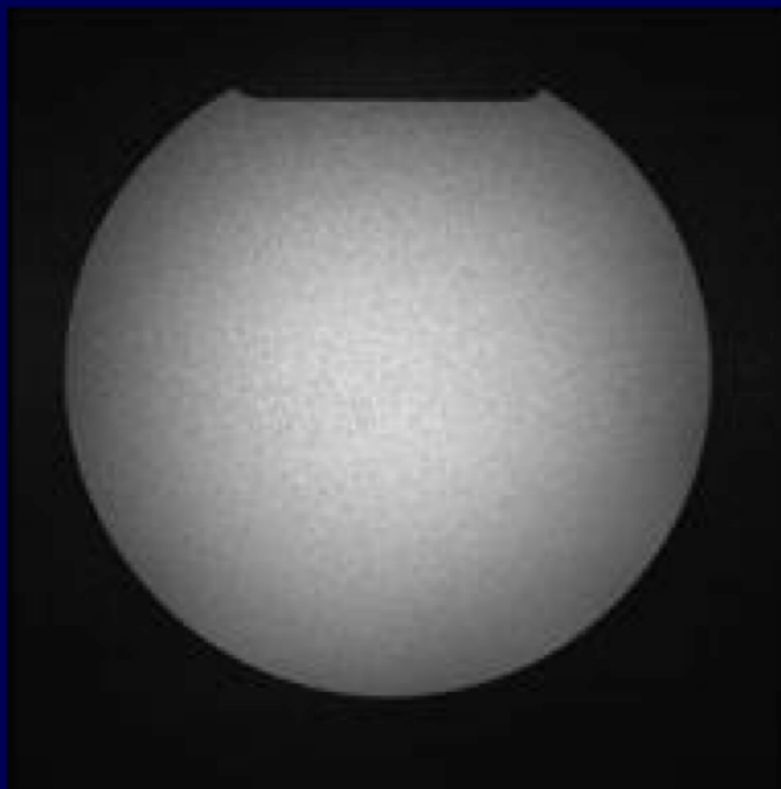


PAT x 2

$f_p$  = acceleration  
factor

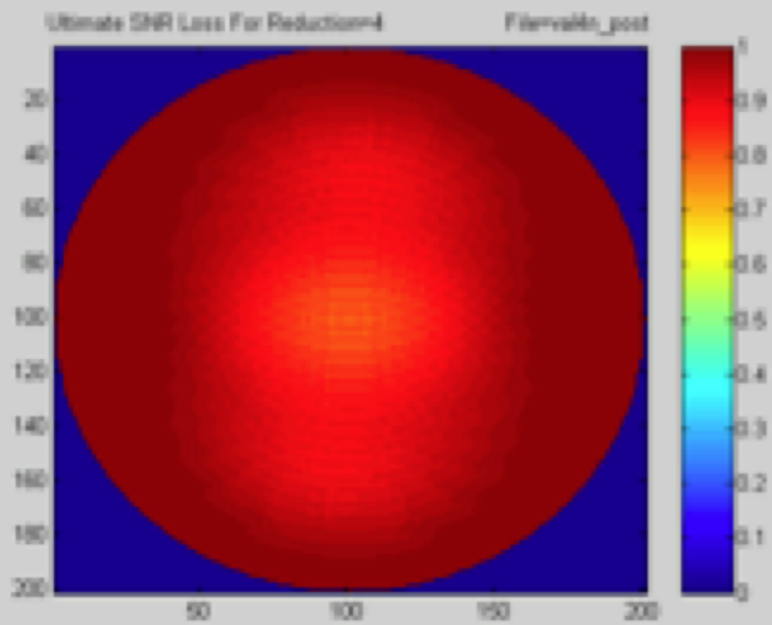
$g$  = coil geometry  
factor

PAT x 3

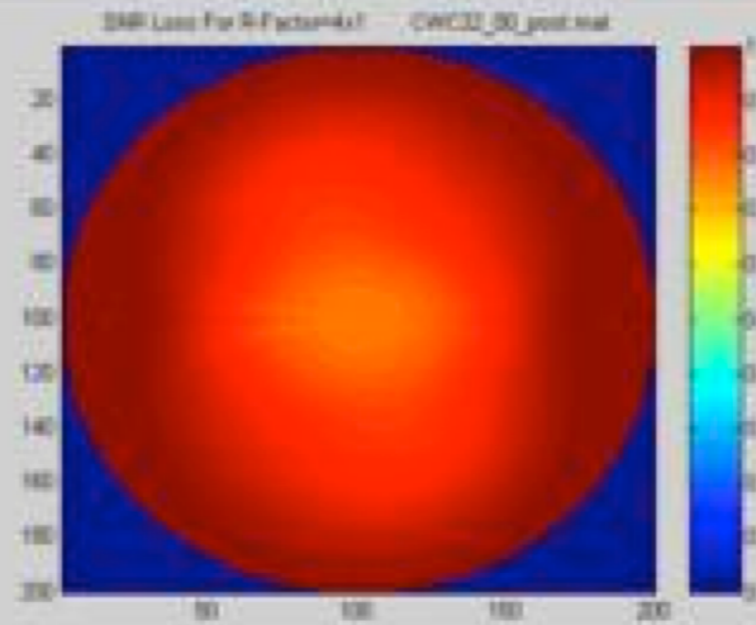


PAT x 4

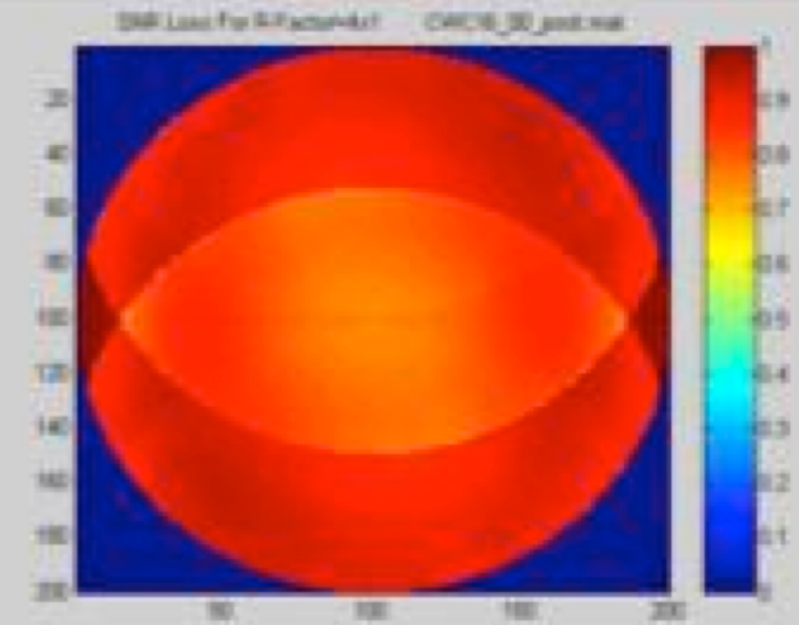
# 1/g-factor Map for R=4



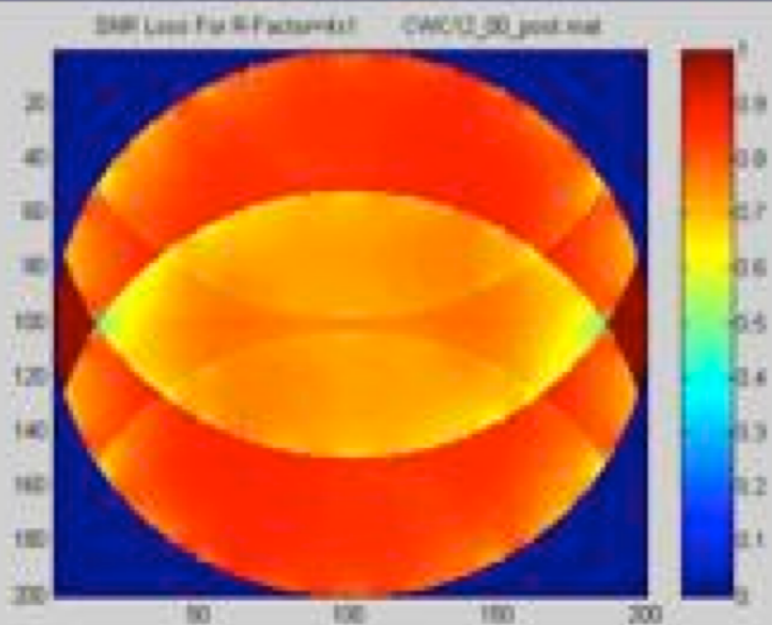
$\infty$  elements



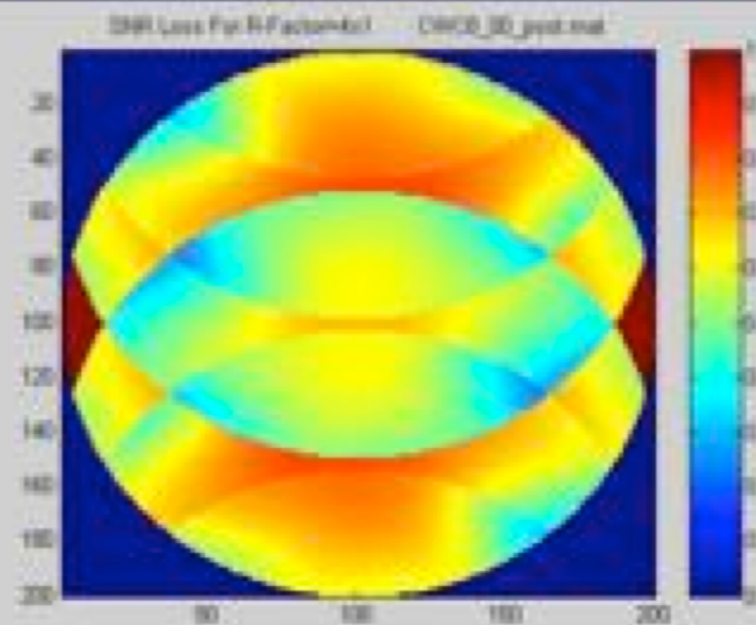
32 elements



16 elements



12 elements



8 elements

Relative  
SNR  
Scale



# g-factor and its impact on images

Rate 1

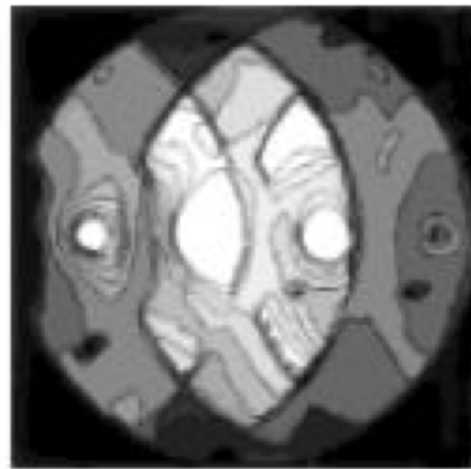
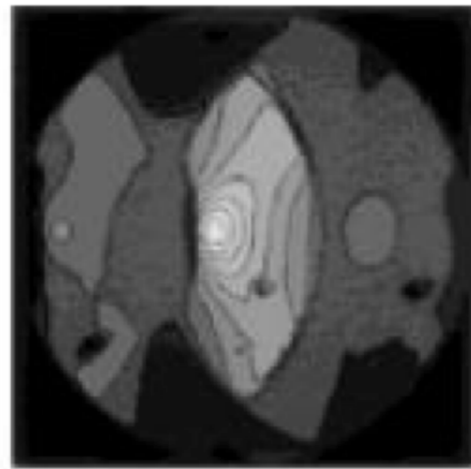
2

2.4

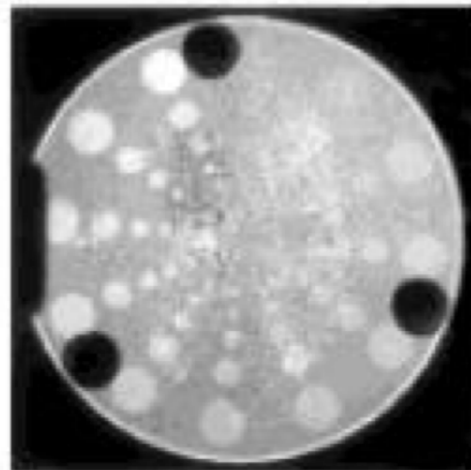
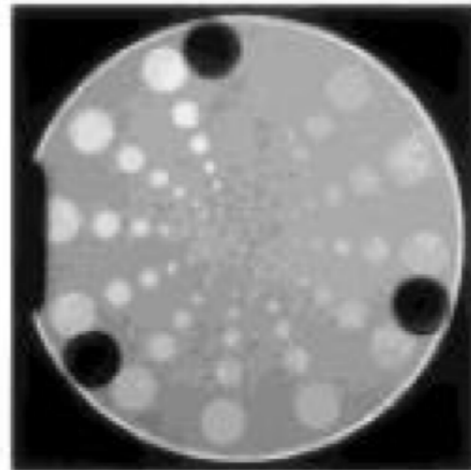
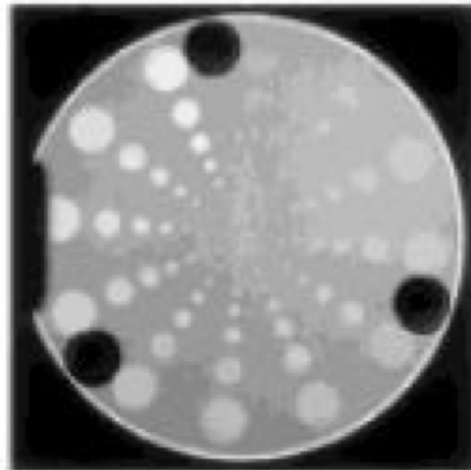
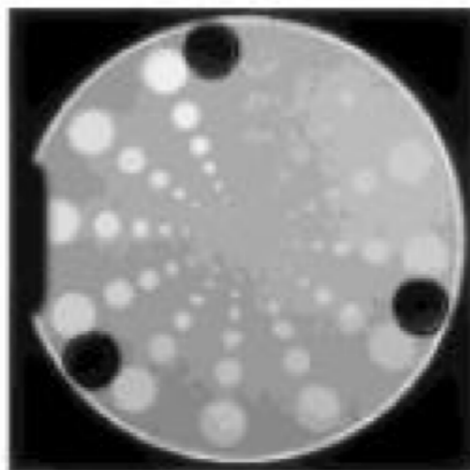
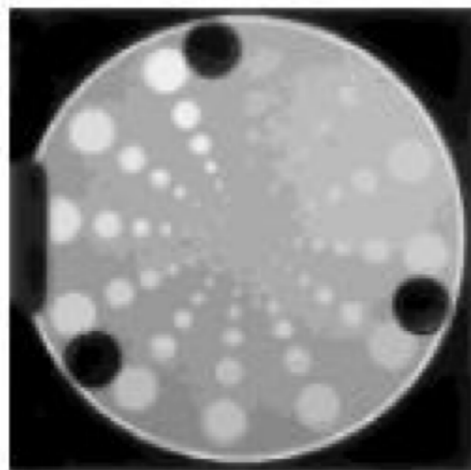
3

4

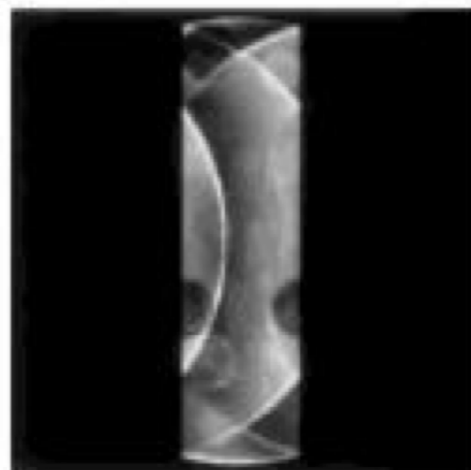
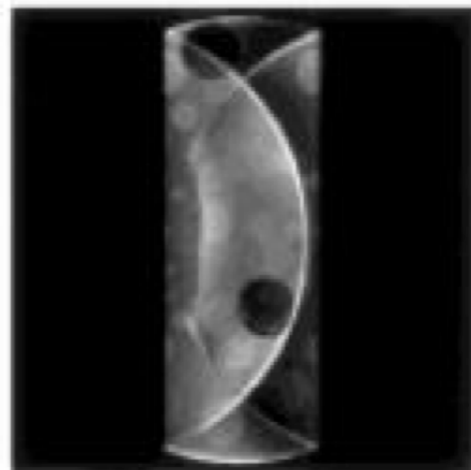
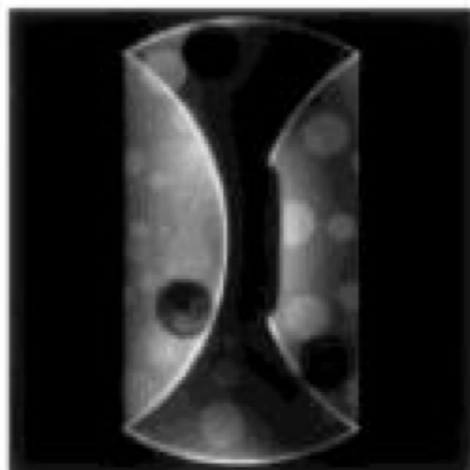
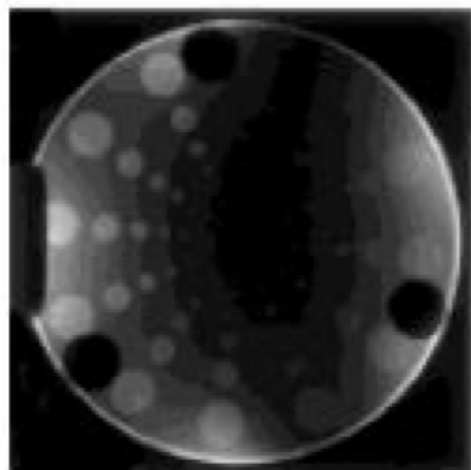
g-map



SENSE

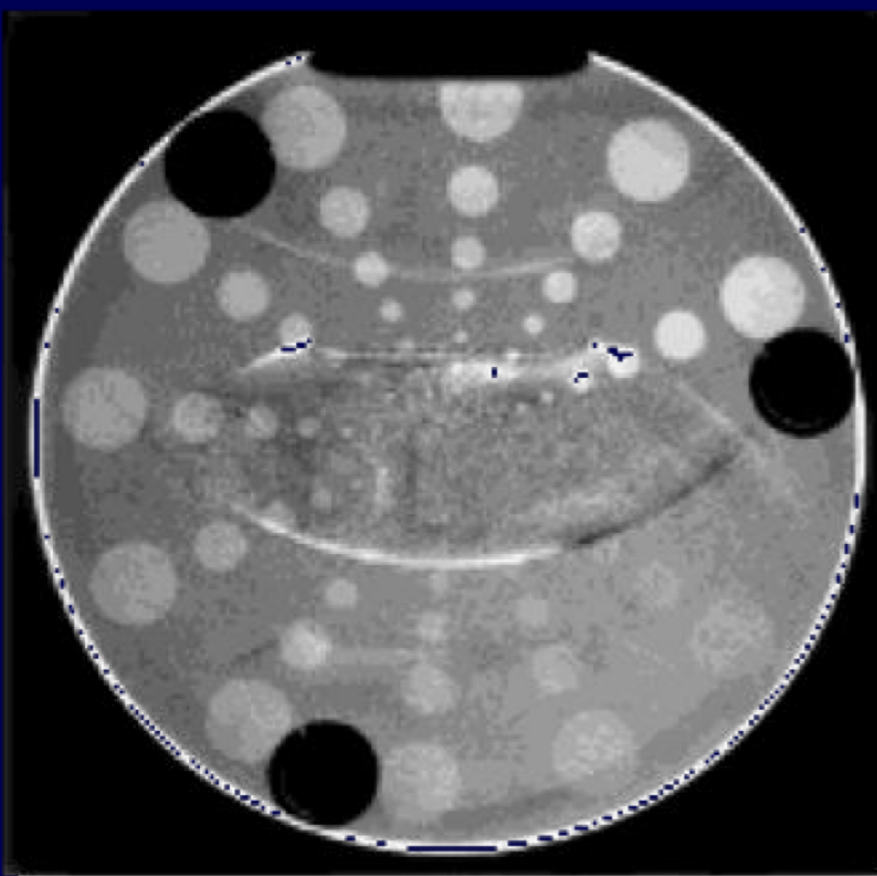


aliased

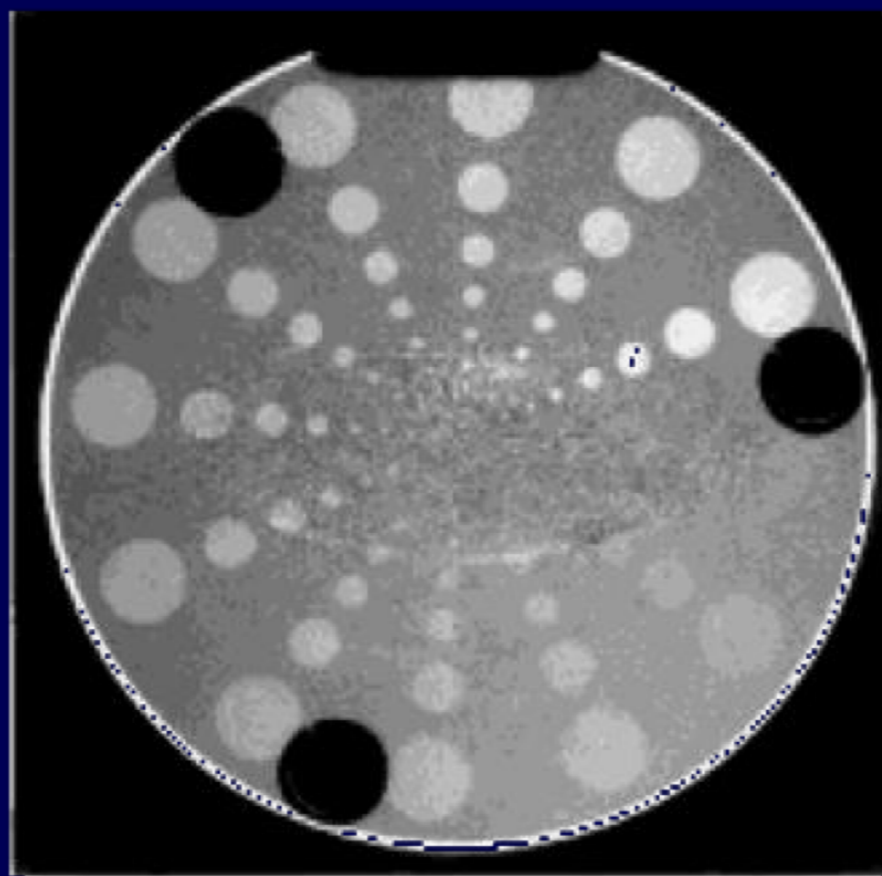


# Dependence on Coil Sensitivity

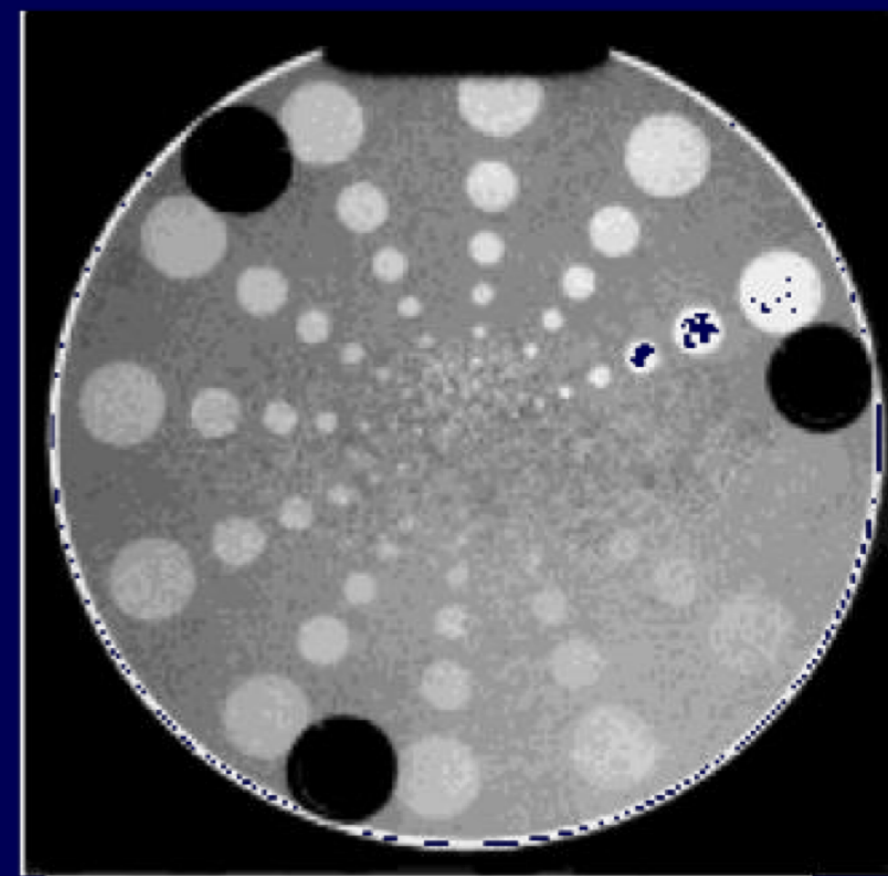
- Images reconstructed using coil sensitivity maps with different order  $P$  of polynomial fitting



$P=0$



$P=1$



$P=2$

# Parallel Imaging (SMASH)

# SMASH

- Simultaneous Acquisition of Spatial Harmonics (SMASH) uses linear combinations of acquired k-space data from multiple coils to generate multiple data sets with offsets in k-space

# Phase Encoding by Amplitude Modulation

- Signal Equation:

$$S(k_x, k_y) = \iint C(x, y) \rho(x, y) e^{-ik_x x - ik_y y} dx dy$$

$\rho(x, y)$  = spin density

$C(x, y)$  = receiver coil sensitivity

# Phase Encoding by Amplitude Modulation

$$S(k_x, k_y) = \iint C(x, y) \rho(x, y) e^{-ik_x x - ik_y y} dx dy$$

- If  $C(x, y) \approx 1$  (relatively homogeneous coil sensitivity),  $S(k_x, k_y) = \text{FT}\{\rho(x, y)\}$
- But coils often do not have uniform sensitivity, and usually there is a fall-off of sensitivity with distance from the coil

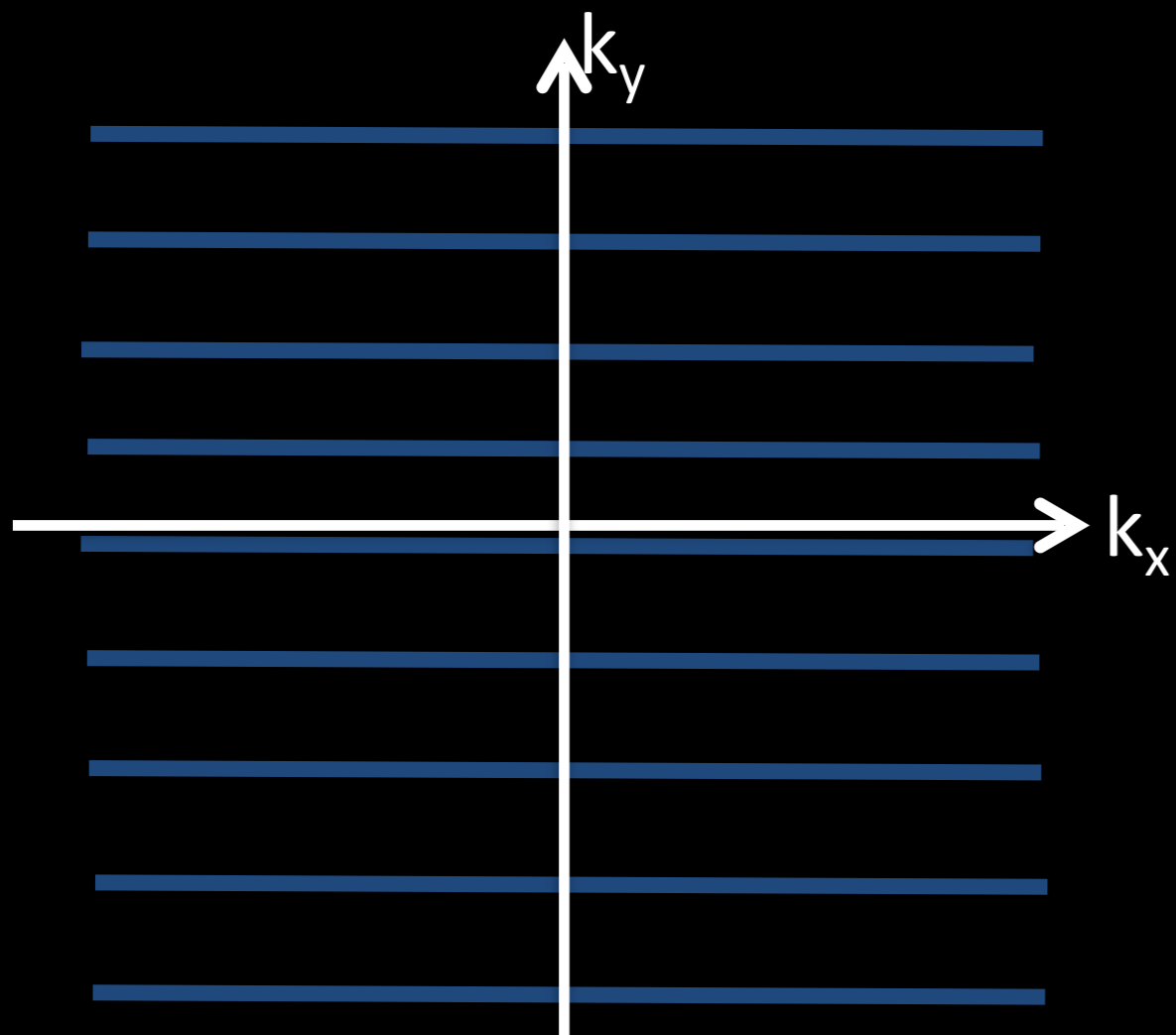
# Phase Encoding by Amplitude Modulation

- Use the arrangement of coils to construct sinusoidal sensitivity profiles
  - Sensitivity profiles are combination of multiple coils, whose signals are combined to produce the desired sinusoidal sensitivity

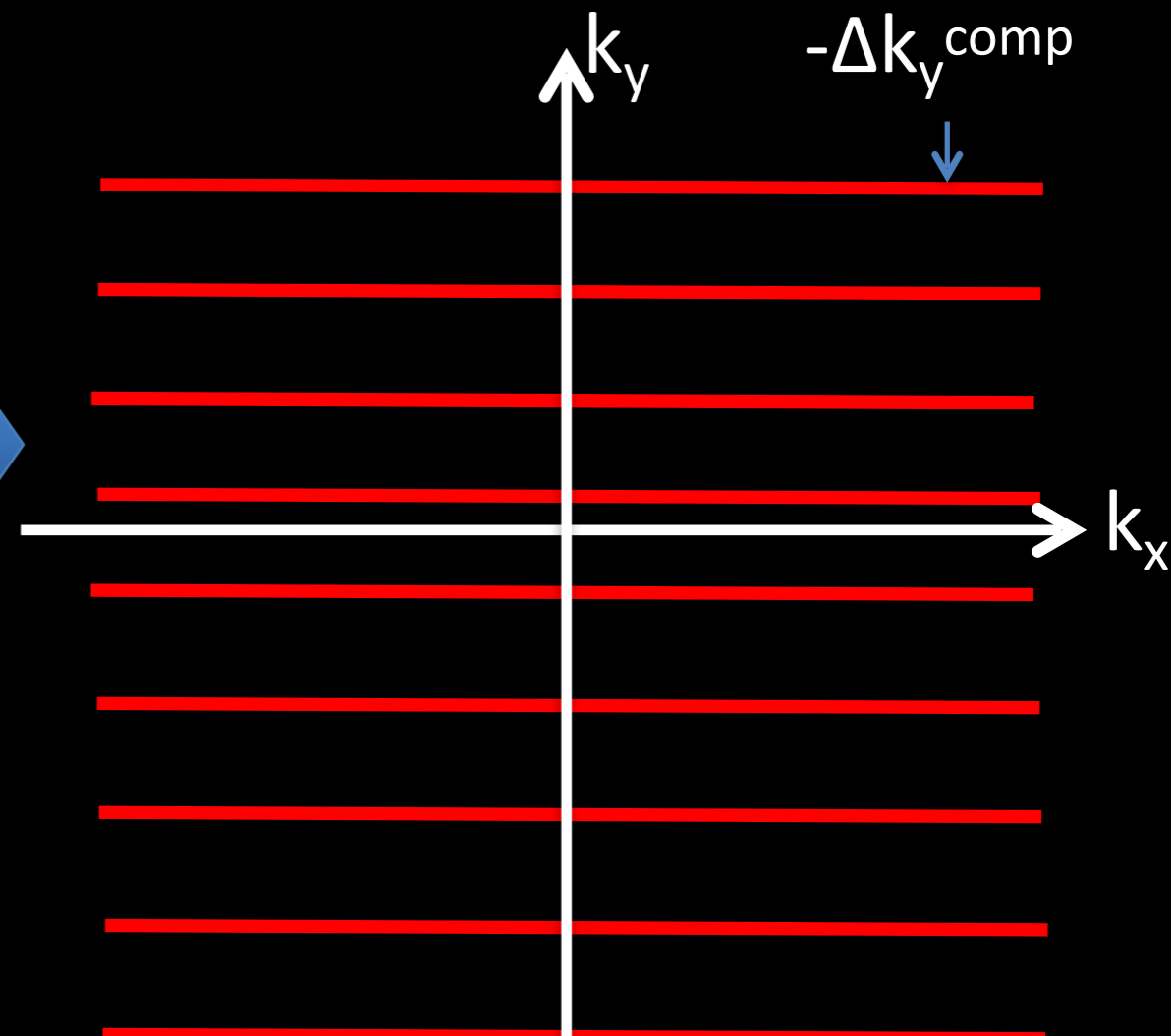
$$\begin{aligned} C^{comp}(y) &= \cos(\Delta k_y^{comp} y) + i \sin(\Delta k_y^{comp} y) \\ &= e^{i \Delta k_y^{comp} y} \end{aligned}$$

The wavelength could be  $\lambda = 2\pi/\Delta k_y = \text{FOV}$

$$C(x,y) \approx 1$$



$$C^{\text{comp}}(x,y) = \exp(i\Delta k_y^{\text{comp}} y)$$





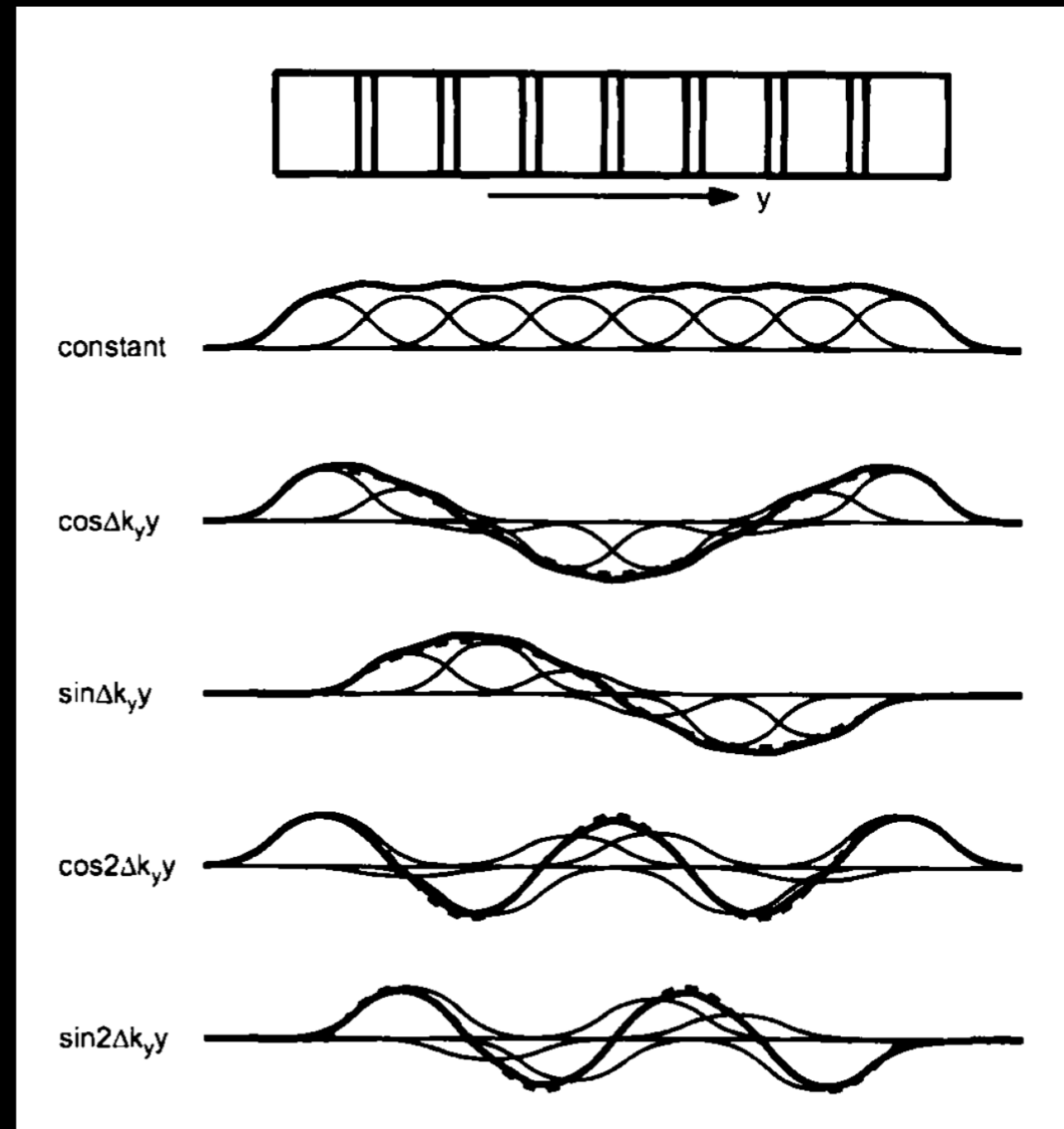
# Spatial Harmonic Generation Using Coil Arrays

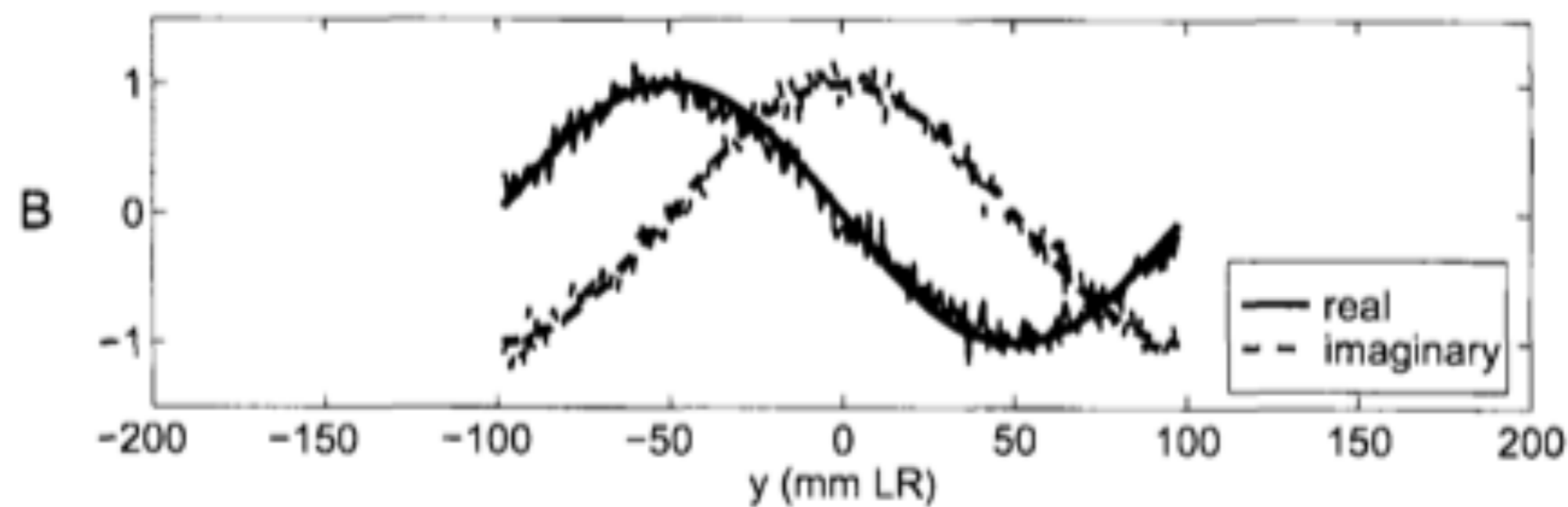
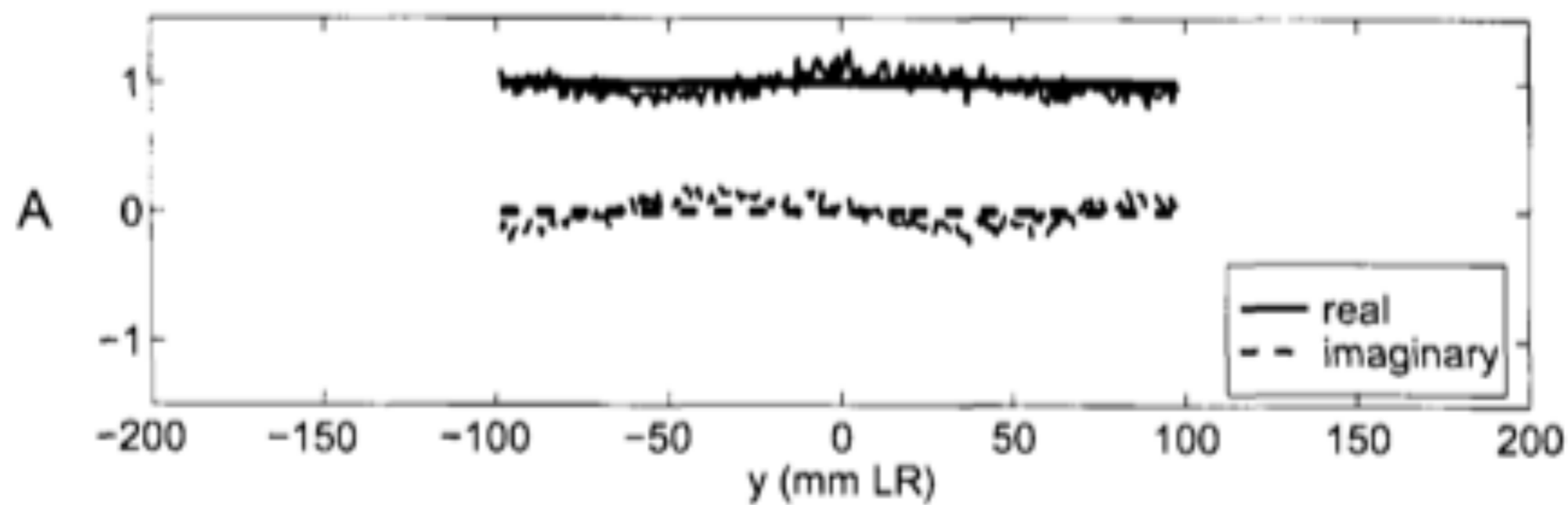
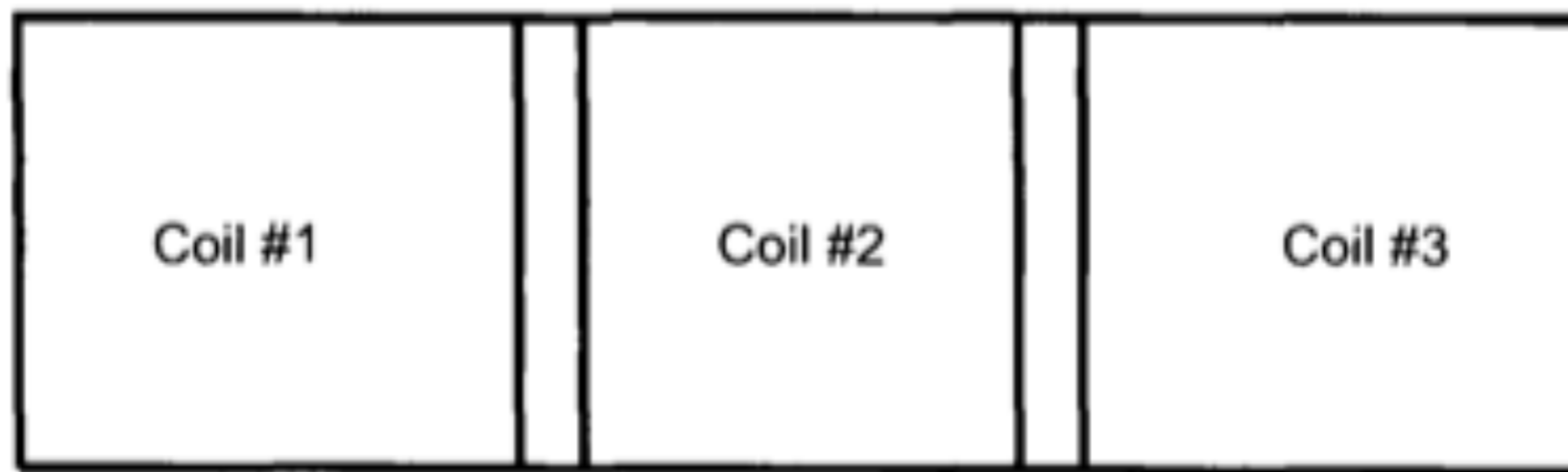
$$C_m^{comp}(y) = \sum_j a_{j,m} C_j(y) = e^{-i2\pi m \Delta k_y y}$$

- Linear surface coil array sensitivities  $C_j$  are combined with linear weights,  $a_{j,m}$ , to produce composite sinusoidal sensitivity
- Composite sensitivities are arranged to be spatial harmonics
- $m$  is an integer, chosen to be a desired harmonic

# Theory: Spatial Harmonics

- 8 coil array
- Gaussian coil sensitivity distribution used
- $m = 0, 1, -1, 2, -2$
- Each spatial harmonic generated is shifted by  $-m\Delta k_y$

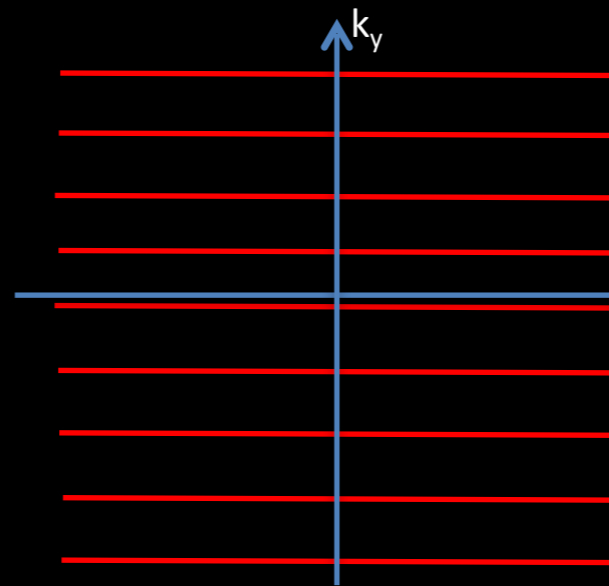




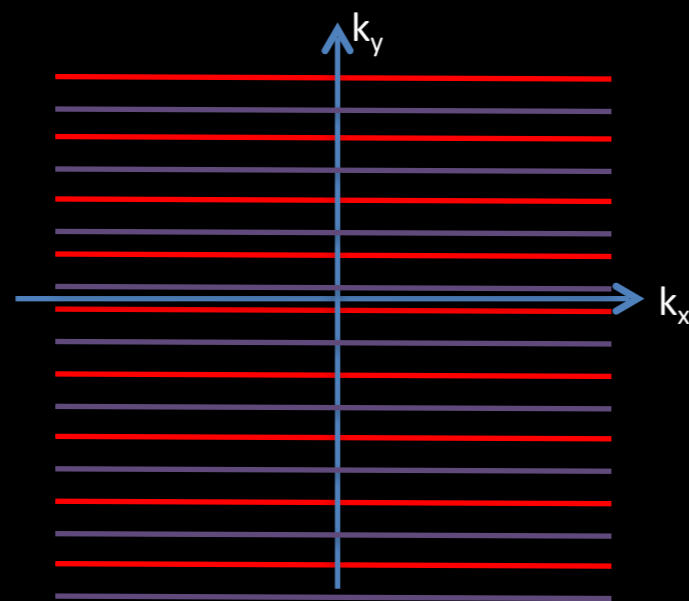
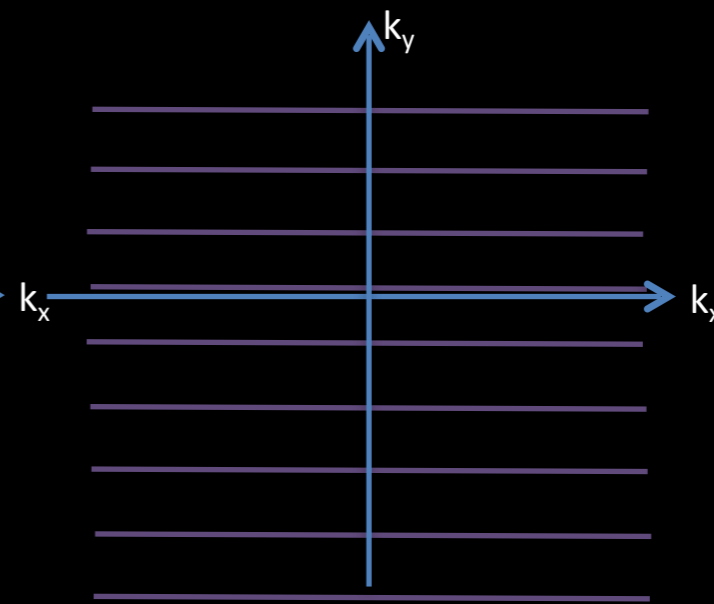
# Interleave the Harmonics

$$\hat{\rho}(k_x, k_y - m\Delta k_y)$$

Zeroth Harmonic,  $m=0$



First Harmonic,  $m=1$



FFT



$\rho(x,y)$



# SMASH Reconstruction

$$S(k_x, k_y) = \text{FT}[\rho(x, y) * C_1(x, y)]$$

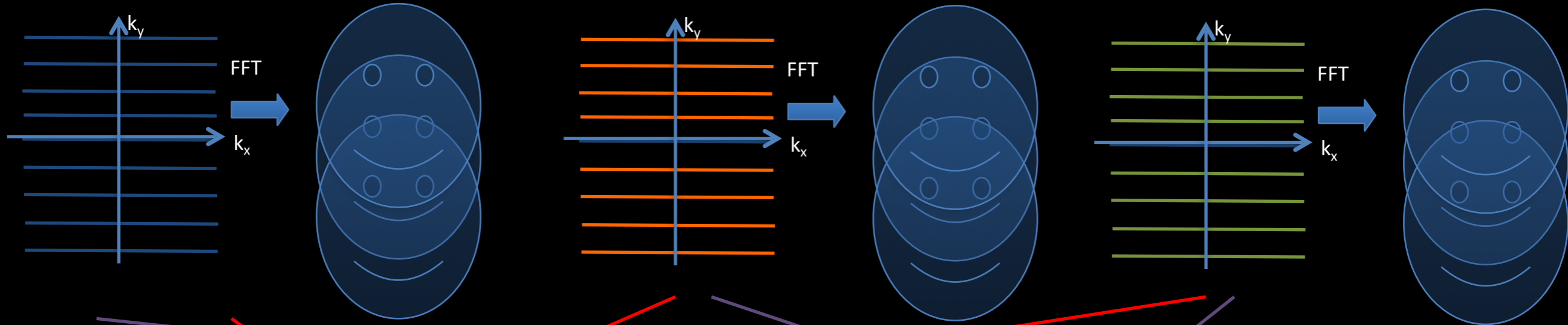
$$\rho(x, y) * C_1(x, y)$$

$$S(k_x, k_y) = \text{FT}[\rho(x, y) * C_2(x, y)]$$

$$\rho(x, y) * C_2(x, y)$$

$$S(k_x, k_y) = \text{FT}[\rho(x, y) * C_3(x, y)]$$

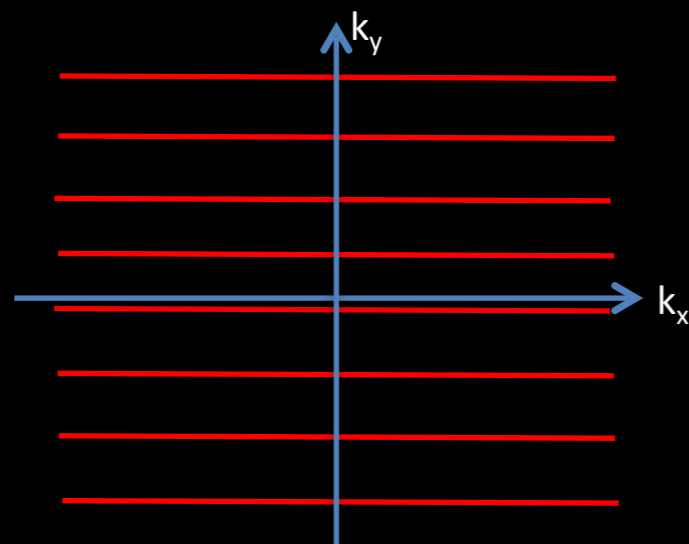
$$\rho(x, y) * C_3(x, y)$$



Combined with  $h_1, h_2,$   
&  $h_3$  weightings

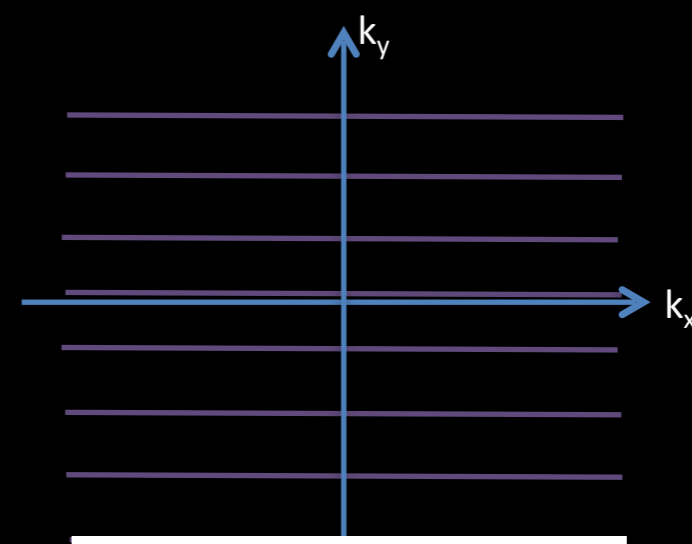
Combined with  $n_1, n_2,$   
&  $n_3$  weightings

Zeroth Harmonic,  $m=0$



$$\hat{\rho}(k_x, k_y - m\Delta k_y)$$

First Harmonic,  $m=1$



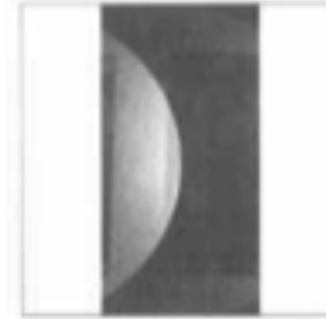
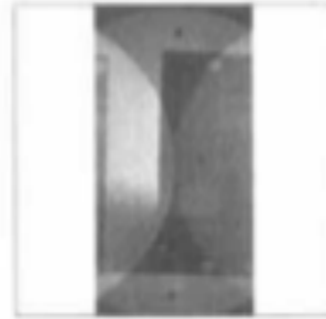
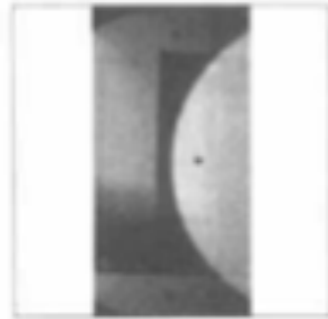
$$\hat{\rho}(k_x, k_y - m\Delta k_y)$$

Coil #1

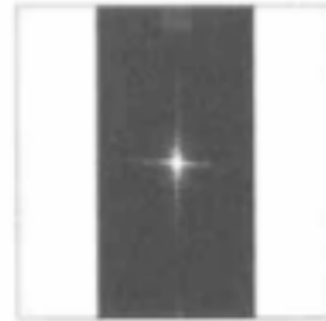
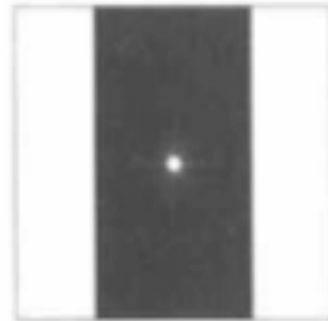
Coil #2

Coil #3

A



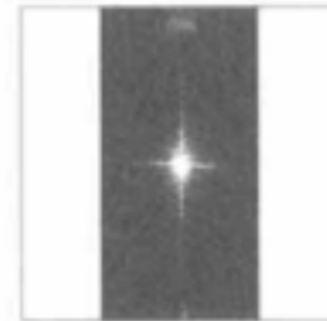
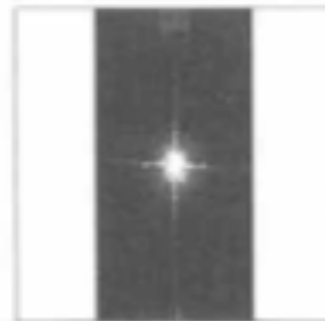
B



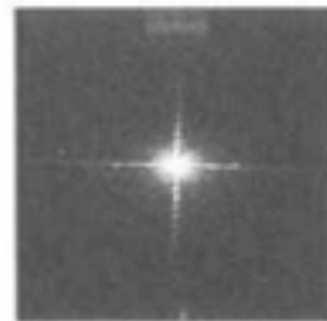
Harmonic #0

Harmonic #1

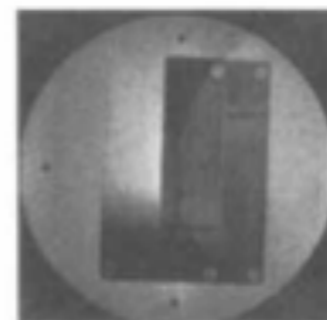
C



D

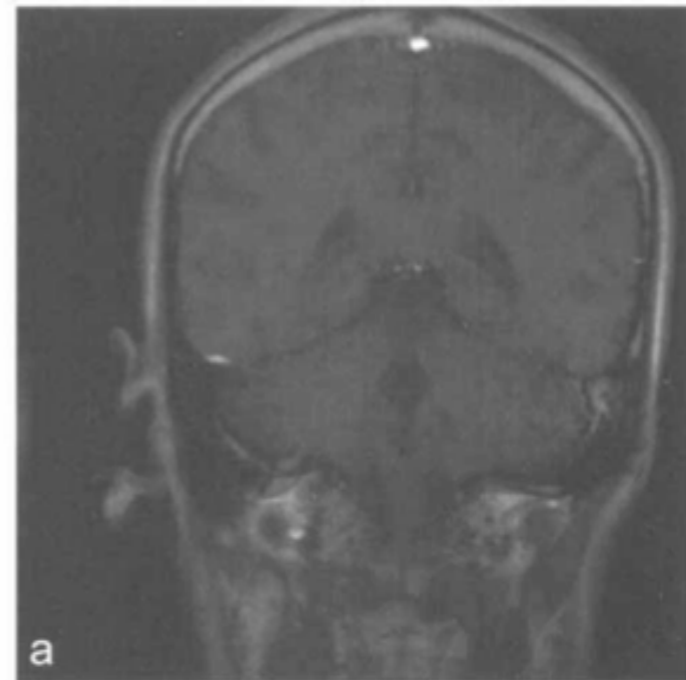
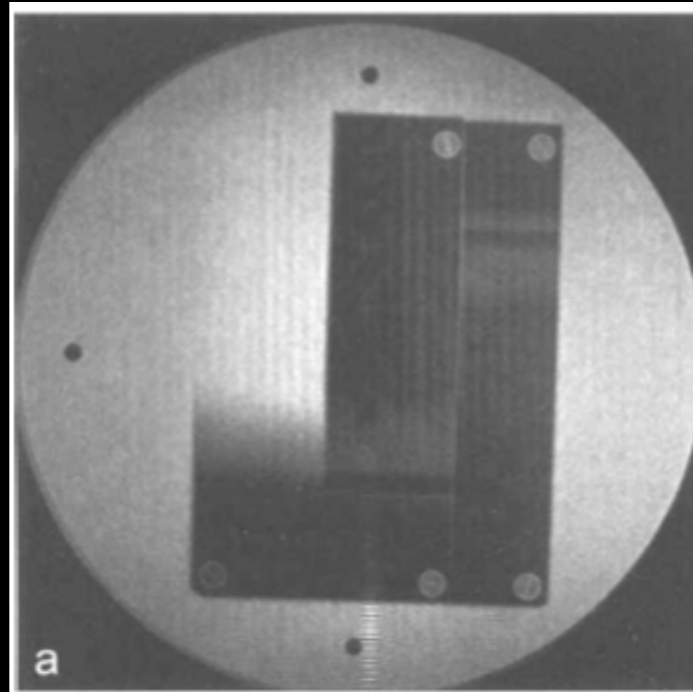


E

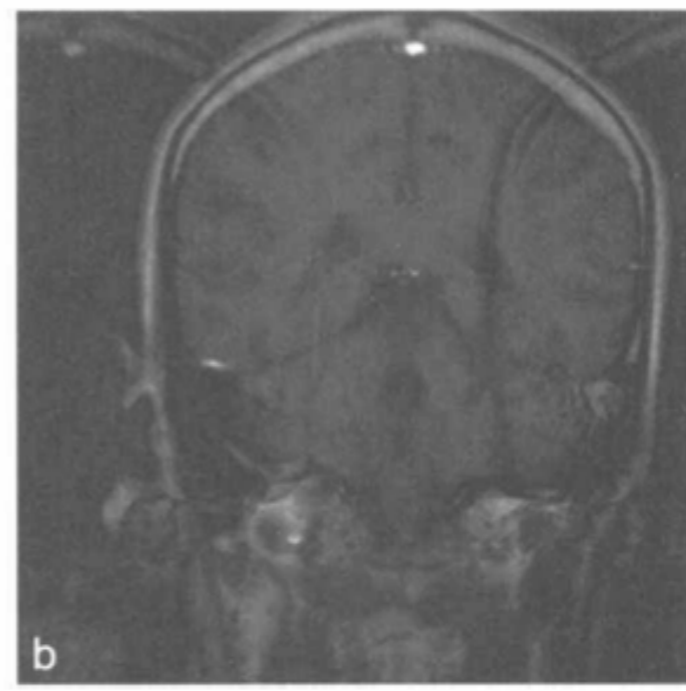
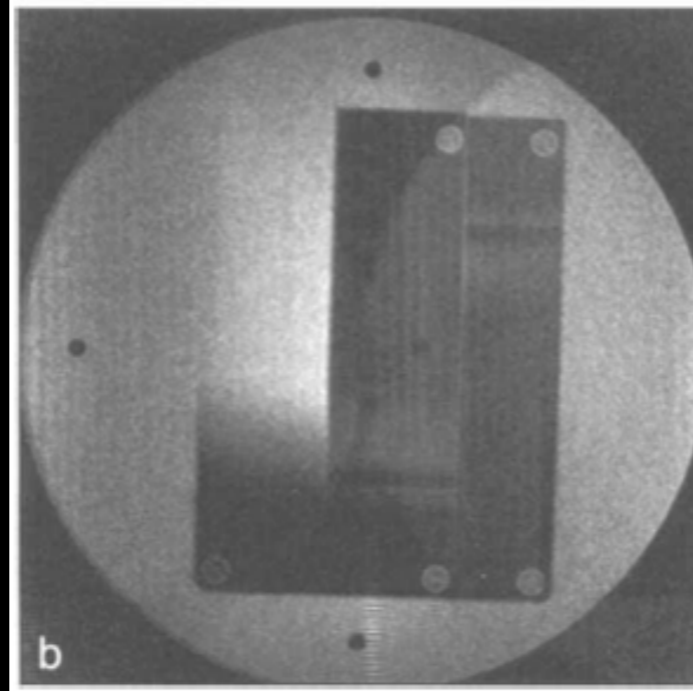


# Three-Element Array

Reference  
images

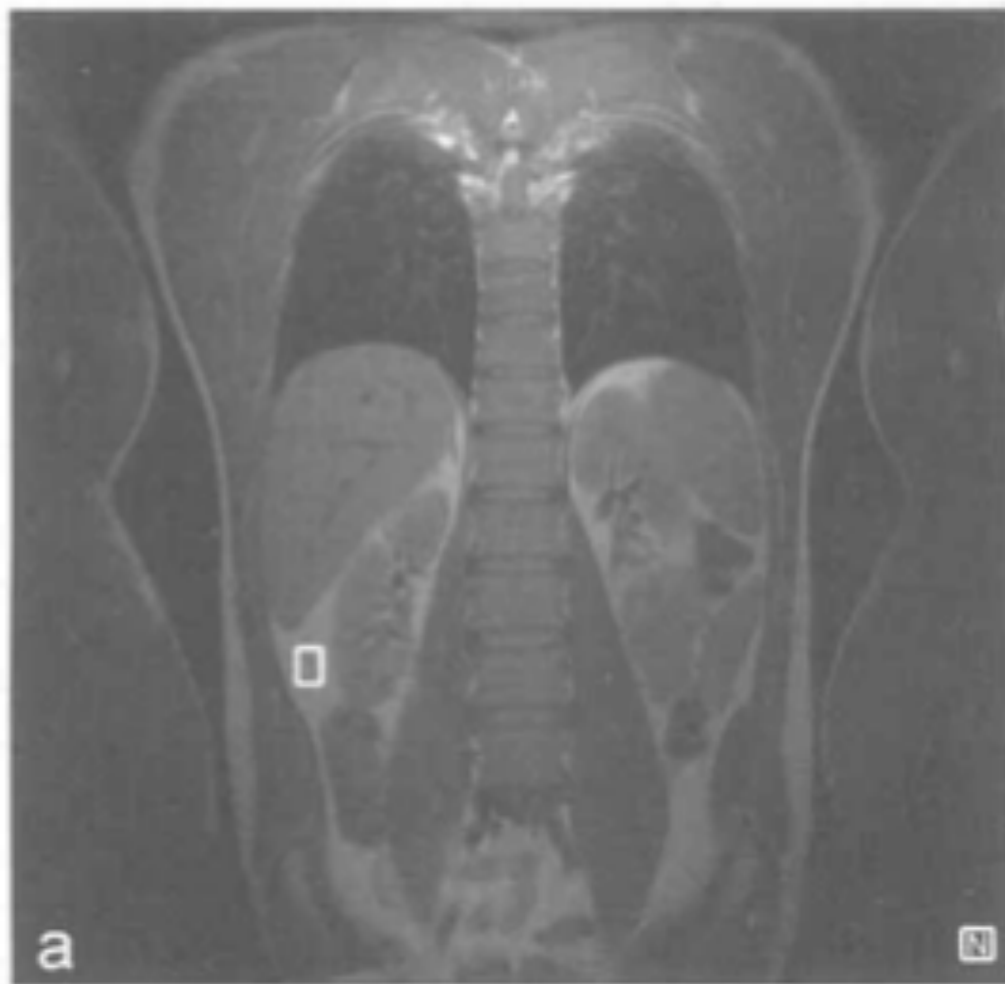


SMASH  
images



# Four-Element Array

Reference images



SMASH images





# Key Points of SMASH

- k-space lines are synthesized by combining signals from multiple coils such that it creates a partial replacement for a phase encoding gradient
- Decreases acquisition time by 1/N
  - N is the number of generated spatial Harmonics

$$\sum_j a_{j,m} C_j(y) = e^{-i2\pi \Delta k_y y}$$

# Summary

- Parallel imaging utilizes coil sensitivities to increase the speed of MRI
- Cases for parallel imaging
  - Higher patient throughput,
  - Real-time imaging/Interventional imaging
  - Motion suppression
- Cases against parallel imaging
  - SNR starving applications

# Further Reading

- Multi-coil Reconstruction
  - <http://onlinelibrary.wiley.com/doi/10.1002/mrm.1910160203/abstract>
- SENSE
  - <http://www.ncbi.nlm.nih.gov/pubmed/10542355>
- SMASH
  - <http://www.ncbi.nlm.nih.gov/pubmed/9324327>
- Parallel Imaging Overview
  - <http://www.ncbi.nlm.nih.gov/pubmed/17374908>

# Thanks!

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