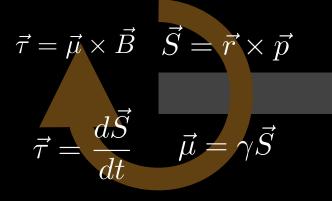
### **Bloch Equations and Relaxation**

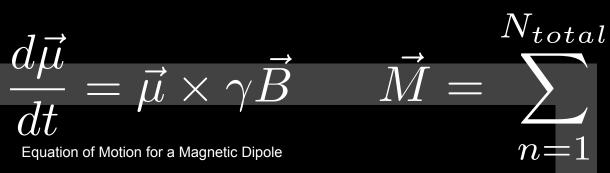
#### M219 - Principles and Applications of MRI Kyung Sung, Ph.D. 1/23/2023

# **Course Overview**

- Course website
  - https://mrrl.ucla.edu/pages/m219
- 2023 course schedule
  - https://mrrl.ucla.edu/pages/m219\_2023
- Assignments
  - Homework #1 due on 1/30
  - Homework #2 will be out on 1/30
- Office hours, Fridays 10-12pm
  - In-person (Ueberroth, 1417B)
  - Zoom is also available

# Last Time...





$$M_x(t) = M_x^0 \cos(\gamma B_0 t) + M_y^0 \sin(\gamma B_0 t)$$
  

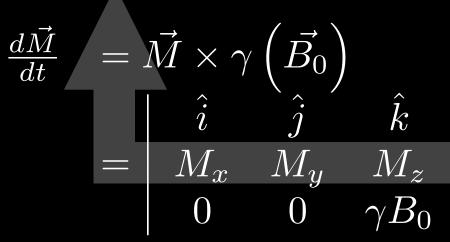
$$M_y(t) = -M_x^0 \sin(\gamma B_0 t) + M_y^0 \cos(\gamma B_0 t)$$
  

$$M_z(t) = M_z^0$$

$$\frac{d\vec{M}}{dt} = \vec{M} \times \gamma \vec{B}$$

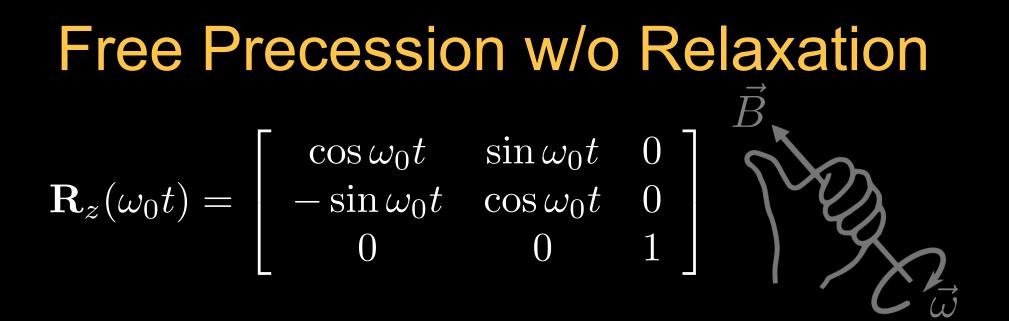
Equation of Motion for the bulk magnetization.

 $=B_0\vec{k}$ 





 $ec{\mu}_n$ 



#### Precession is left-handed (clockwise).

 $\vec{M}(t) = \mathbf{R}_z(\omega_0 t) \vec{M}^0$ 

#### Basic RF Pulse $\overrightarrow{B} = \overrightarrow{B}_0 + \overrightarrow{B}_1(t)$ $\vec{B}_1(t) = B_1^e(t)[\cos(\omega_{RF}t + \theta)\hat{i} - \sin(\omega_{RF}t + \theta)\hat{j}]$ $B_{1}^{e}(t)$ pulse envelope function $\omega_{RF}$ excitation carrier frequency Ĥ initial phase angle

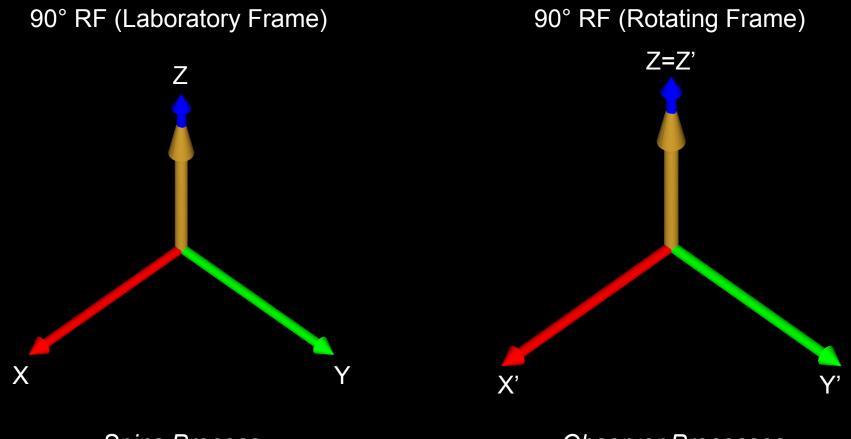
 $B_1$  is perpendicular to  $B_0$ .

$$\overrightarrow{B}_0 = B_0 \hat{k}$$

**Rotating Frame** 

## Lab vs. Rotating Frame

• The rotating frame simplifies the mathematics and permits more intuitive understanding.



Spins Precess

**Observer Precesses** 

*Note*: Both coordinate frames share the same z-axis.

# Combined B<sub>0</sub> & B<sub>1</sub> Effects

 $\frac{d\vec{M}}{dt} = \vec{M} \times \gamma \vec{B}$  $= \vec{M} \times \gamma \left( \vec{B_0} + \vec{B_1} \right)$ 

#### **Relationship Between Lab and Rotating Frames**

$$\frac{d\vec{M}}{dt} = \vec{M} \times \gamma \vec{B}$$

Rotating Frame Definitions $\vec{M}_{rot} \equiv \begin{bmatrix} M_{x'} \\ M_{y'} \\ M_{z'} \end{bmatrix}$  $\vec{B}_{rot} \equiv \begin{bmatrix} B_{x'} \\ B_{y'} \\ B_{z'} \end{bmatrix}$ 

$$B_{z'} \equiv B_z$$
$$M_{z'} \equiv M_z$$

$$\vec{M}_{lab}(t) = R_Z(\omega_{RF}t) \cdot \vec{M}_{rot}(t)$$

 $\overrightarrow{B}_{lab}(t) = R_Z(\omega_{RF}t) \cdot \overrightarrow{B}_{rot}(t)$ 

Bulk magnetization components in the rotating frame.

Applied B-field components in the rotating frame.

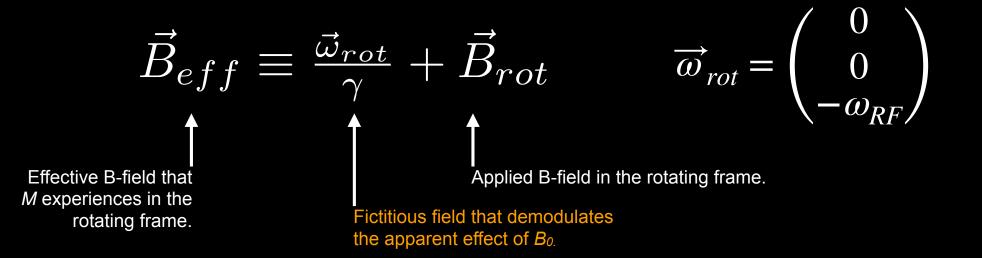
$$\frac{d\vec{M}}{dt} = \vec{M} \times \gamma \vec{B} \qquad \Longrightarrow \quad \frac{d\vec{M}_{rot}}{dt} = \vec{M}_{rot} \times \gamma \vec{B}_{eff}$$

# **Bloch Equation (Rotating Frame)**

$$\frac{d\vec{M}}{dt} = \vec{M} \times \gamma \vec{B}$$

Equation of motion for an ensemble of spins (isochromats). [Laboratory Frame]

$$\frac{d\vec{M}_{rot}}{dt} = \vec{M}_{rot} \times \gamma \left( \frac{\vec{\omega}_{rot}}{\gamma} + \vec{B}_{rot} \right) \overset{\text{Equation of motion for an}}{\underset{[\text{Rotating Frame}]}{\text{Equation of motion for an}}}$$

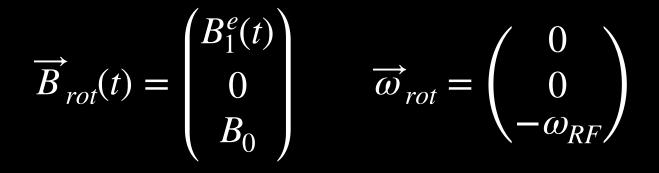




**Bloch Equation (Rotating Frame)**  $\vec{B}(t) = B_0 \hat{k} + B_1^e(t) [\cos(\omega_{RF}t + \theta)\hat{i} - \sin(\omega_{RF}t + \theta)\hat{j}]$  $\vec{B}_{lab}(t) = \begin{pmatrix} B_1^e(t)\cos(\omega_{RF}t + \theta) \\ -B_1^e(t)\sin(\omega_{RF} + \theta) \\ B_0 \end{pmatrix} \qquad \vec{B}_{rot}(t) = \begin{pmatrix} B_1^e(t)\cos\theta \\ -B_1^e(t)\sin\theta \\ B_0 \end{pmatrix}$  $\vec{B}_{eff} \equiv \frac{\vec{\omega}_{rot}}{\gamma} + \vec{B}_{rot} \qquad \vec{\omega}_{rot} = \begin{pmatrix} 0 \\ 0 \\ -\omega_{RF} \end{pmatrix}$ Effective B-field that Applied B-field in the rotating frame. M experiences in the Fictitious field that demodulates rotating frame. the apparent effect of  $B_{0}$ .

# Bloch Equation (Rotating Frame) $\vec{B}_{eff} \equiv \frac{\vec{\omega}_{rot}}{\gamma} + \vec{B}_{rot}$

Assume no RF phase ( $\theta = 0$ )



$$\vec{B}_{eff}(t) = \begin{pmatrix} B_1^e(t) \\ 0 \\ B_0 \\ & \omega_{RF} \\ B_0 \\ & \gamma \end{pmatrix}$$

#### **Relationship Between Lab and Rotating Frames**

$$\frac{d\vec{M}}{dt} = \vec{M} \times \gamma \vec{B}$$

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Bulk magnetization components in the rotating frame.

Applied B-field components in the rotating frame.

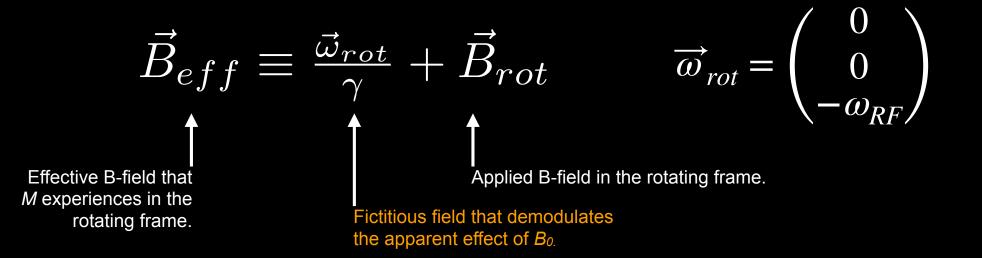
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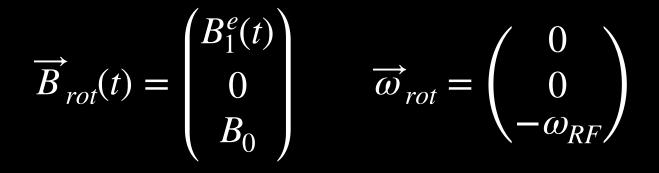




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Assume no RF phase ( $\theta = 0$ )



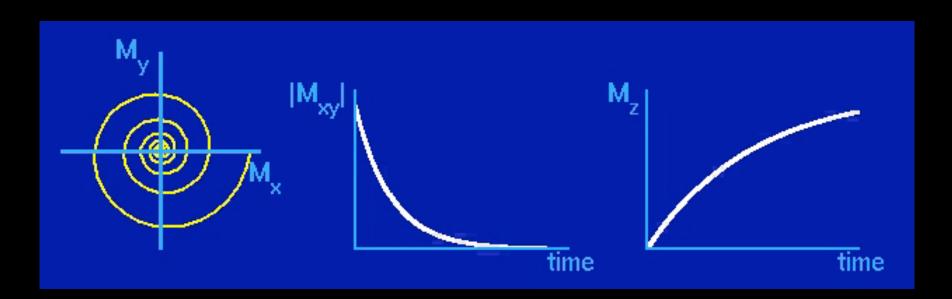
$$\vec{B}_{eff}(t) = \begin{pmatrix} B_1^e(t) \\ 0 \\ B_0 \\ & \omega_{RF} \\ B_0 \\ & \gamma \end{pmatrix}$$

To the Board

T<sub>1</sub> & T<sub>2</sub> Relaxation

#### Relaxation

- Magnetization returns exponentially to equilibrium:
  - Longitudinal recovery time constant is T1
  - Transverse decay time constant is T2
- Relaxation and precession are independent



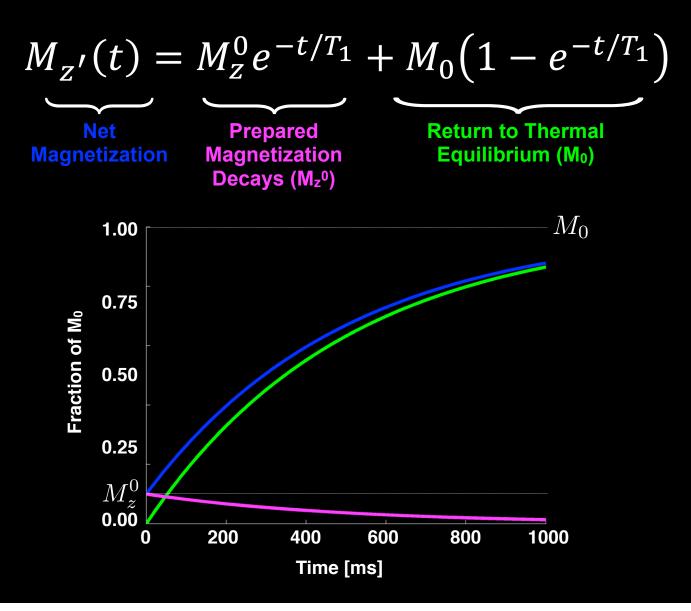
## T<sub>1</sub> Relaxation

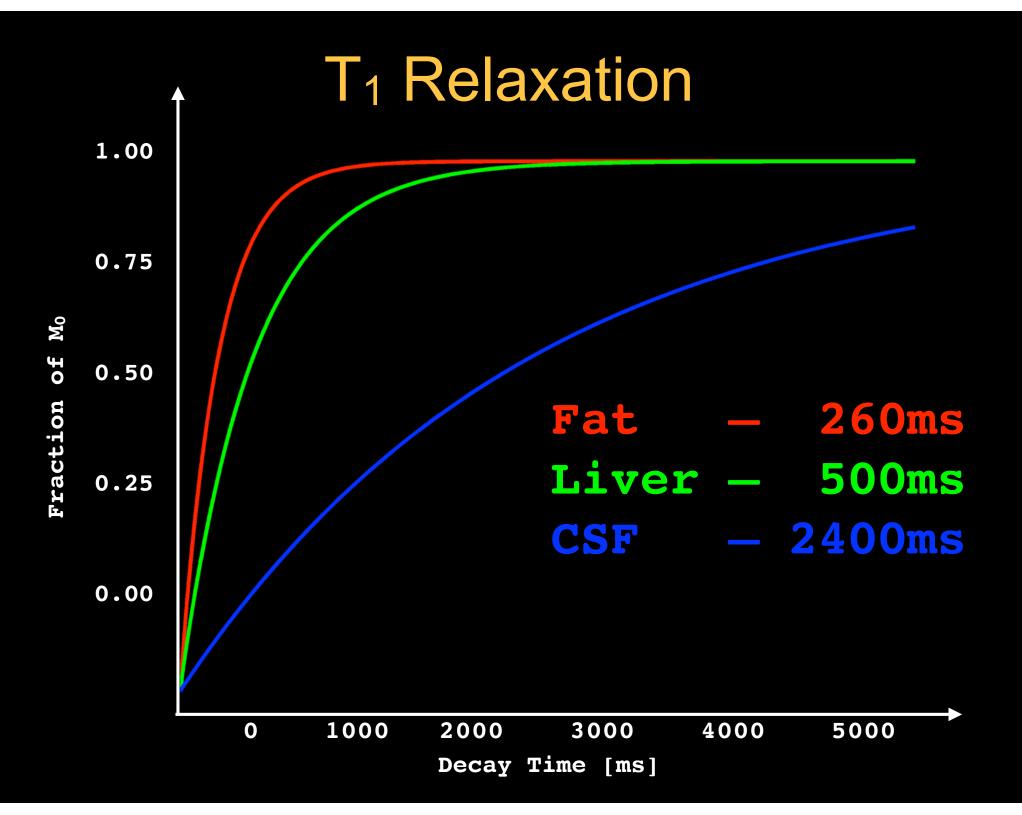
- Longitudinal or spin-lattice relaxation
  - Typically, (10s ms) < T1 < (100s ms)
- T1 is long for
  - Small molecules (water)
  - Large molecules (proteins)
- T1 is short for
  - Fats and intermediate-sized molecules
- T1 increases with increasing B0
- T1 decreases with contrast agents

#### Short $T_1s$ are bright on $T_1$ -weighted image

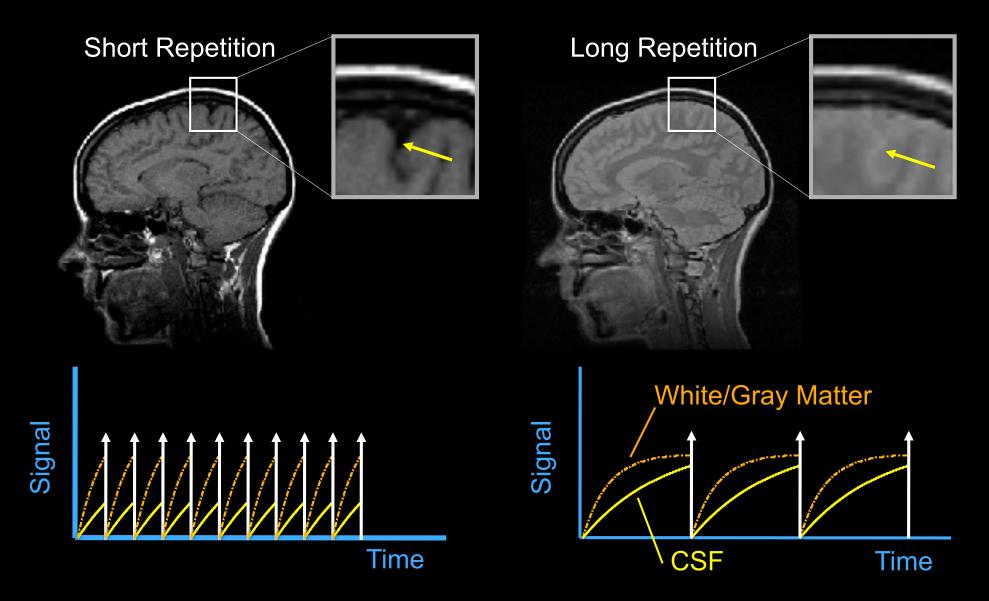
# T<sub>1</sub> Relaxation

Free Precession in the Lab or Rotating Frame with Relaxation





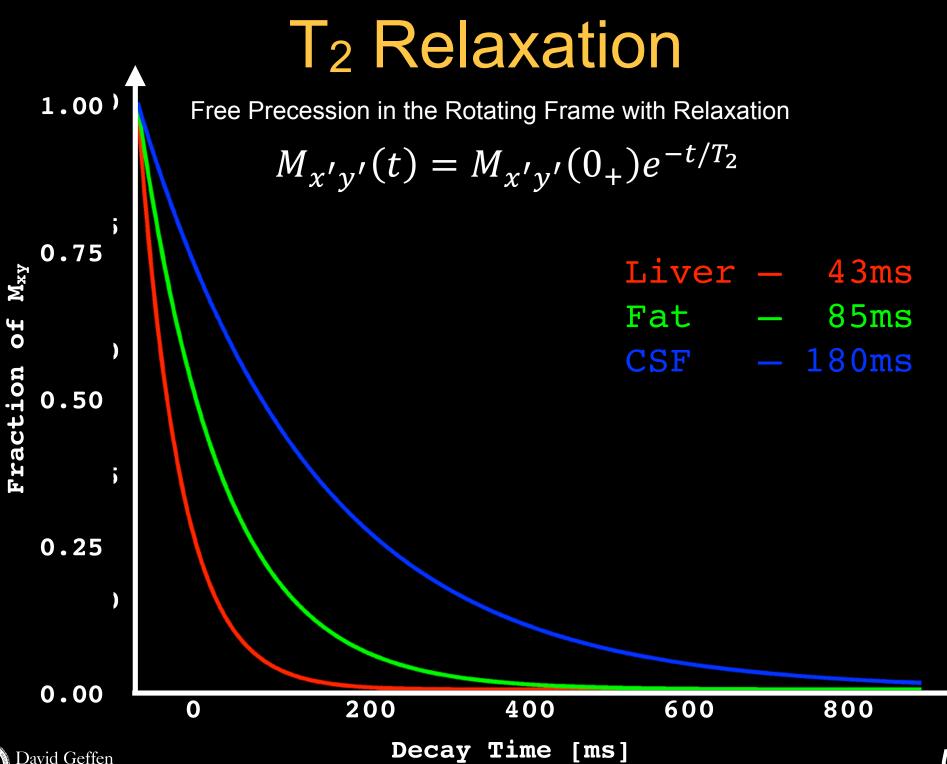
## T<sub>1</sub> Contrast



## T<sub>2</sub> Relaxation

- Transverse or spin-spin relaxation
  - Molecular interaction causes spin dephasing
  - Typically, T2 < (10s ms)</p>
- Increasing molecular size, decrease T2
  - Fat has a short T2
- Increasing molecular mobility, increases T2
  - Liquids (CSF, edema) have long T2s
- Increasing molecular interactions, decreases T2
  - Solids have short T2s
- T2 relatively independent of B0

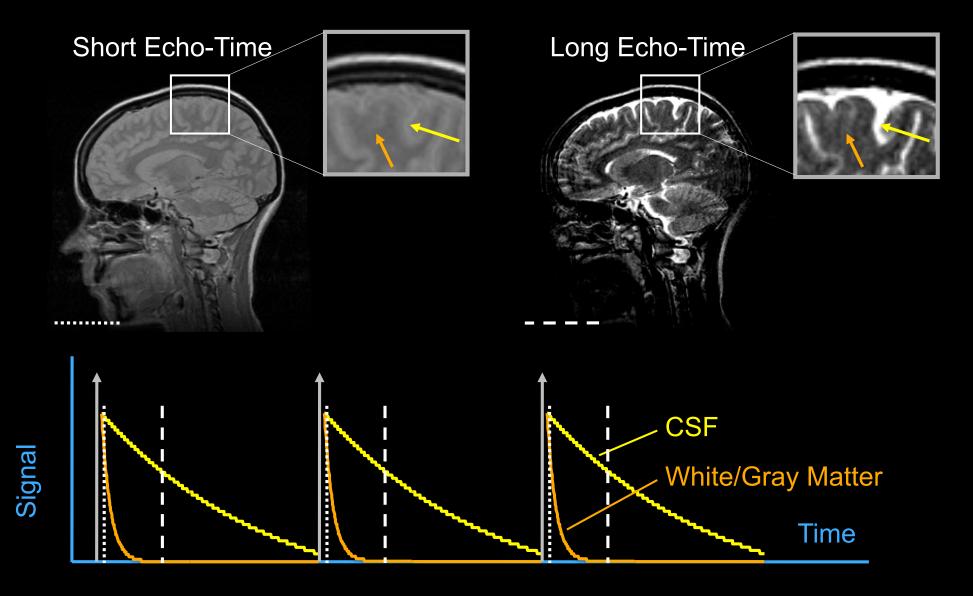
#### Long T<sub>2</sub> is bright on T<sub>2</sub> weighted image



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#### T2 Contrast



## T<sub>1</sub> and T<sub>2</sub> Values @ 1.5T

Tissue	$\mathbf{T}_1$ [ms]	<b>T</b> <sub>2</sub> [ms]
gray matter	925	100
white matter	790	92
muscle	875	47
fat	260	85
kidney	650	58
liver	500	43
CSF	2400	180

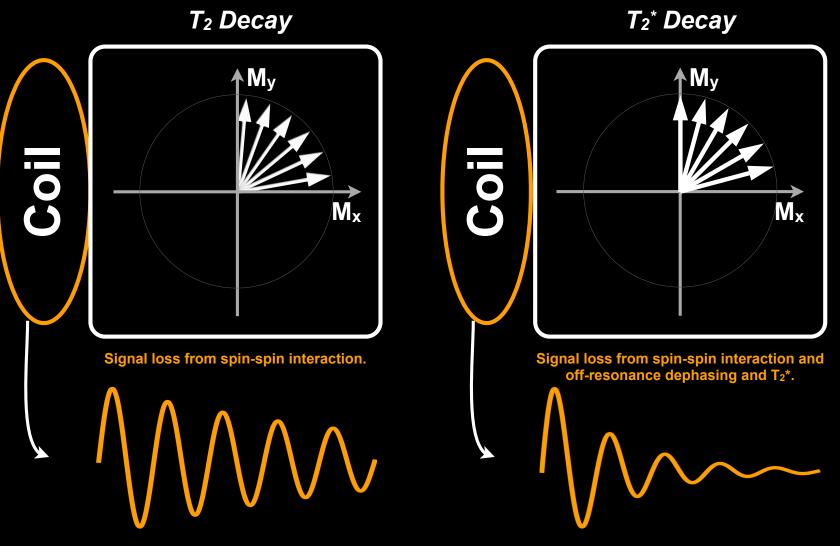
Each tissue has "unique" relaxation properties, which enables "soft tissue contrast".

## T<sub>2</sub>\* Relaxation

# $\frac{1}{T_2^*} = \frac{1}{T_2} + \gamma \Delta B_0$

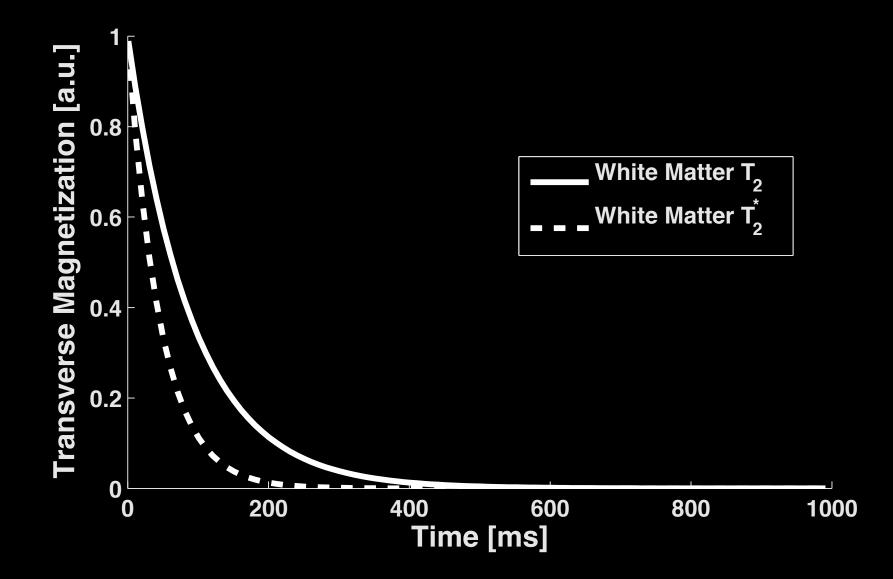
- T<sub>2</sub>\* is "observed" transverse relaxation time constant
- T<sub>2</sub>\* consists of <u>irreversible spin-spin (T<sub>2</sub>)</u> <u>dephasing</u> and <u>reversible intravoxel spin de-</u> <u>phasing</u> due to off-resonance
- Sources of off-resonance:
  - B<sub>0</sub> inhomogeneity
  - susceptibility differences (e.g. air spaces)





 $T_2^*$  is signal loss from spin dephasing and  $T_2$ 

T2\*<T2 (always!)



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SHEET 2 OF 2

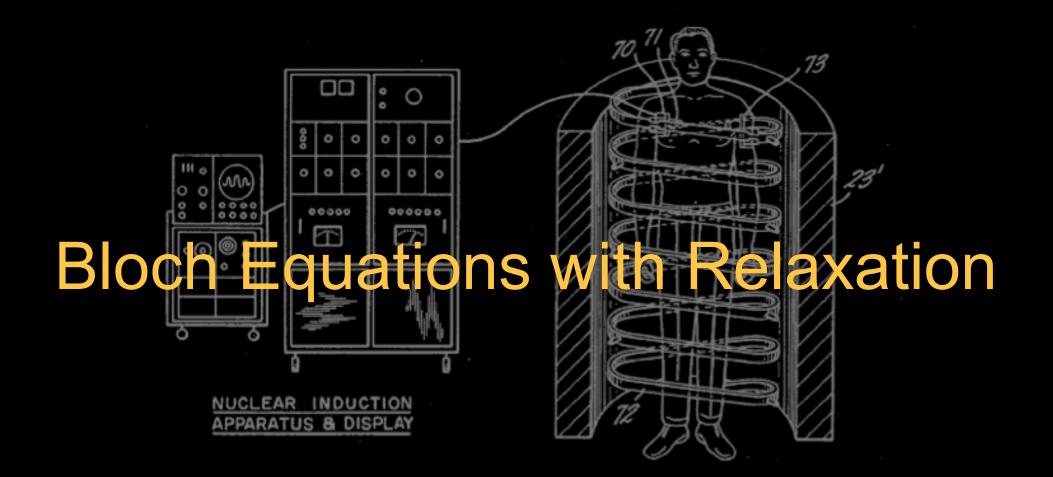


FIG. 2





# **Bloch Equations with Relaxation**

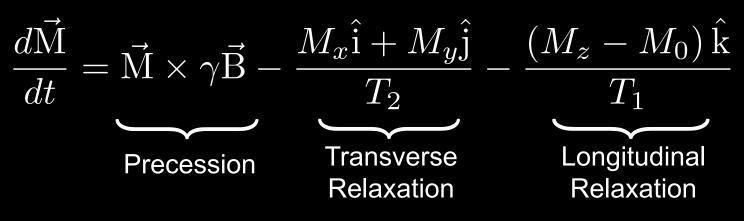
$$\frac{d\vec{\mathbf{M}}}{dt} = \vec{\mathbf{M}} \times \gamma \vec{\mathbf{B}} - \frac{M_x \hat{\mathbf{i}} + M_y \hat{\mathbf{j}}}{T_2} - \frac{(M_z - M_0) \hat{\mathbf{k}}}{T_1}$$

- Differential Equation

   Ordinary, Coupled, Non-linear
- No analytic solution, in general.
  - Analytic solutions for simple cases.
  - Numerical solutions for all cases.
- Phenomenological
  - Exponential behavior is an approximation.



# **Bloch Equations - Lab Frame**

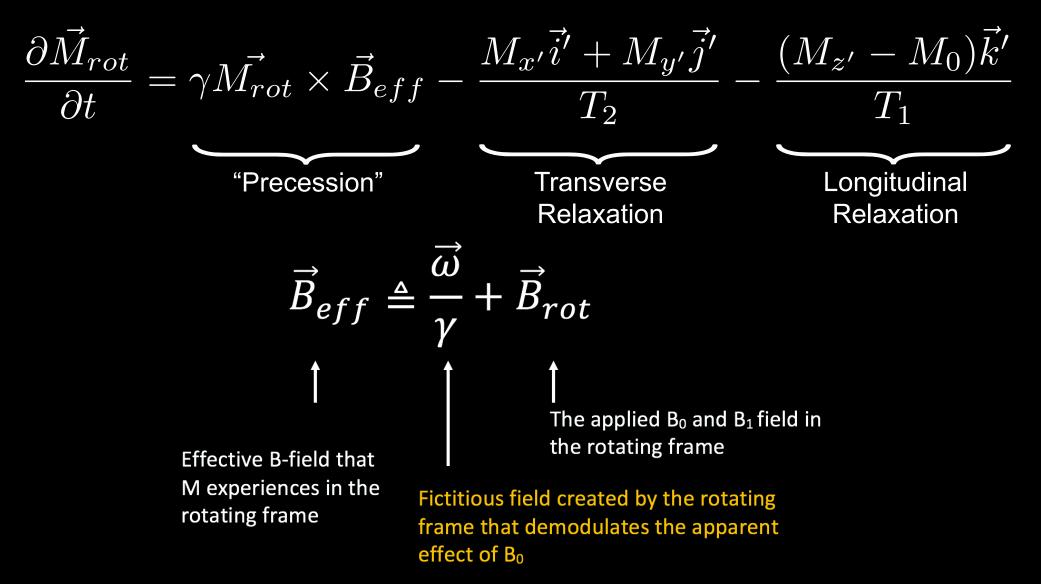


- Precession
  - Magnitude of M unchanged
  - Phase (rotation) of M changes due to B
- Relaxation
  - T<sub>1</sub> changes are slow O(100ms)
  - T<sub>2</sub> changes are fast O(10ms)
  - Magnitude of M can be ZERO
- Diffusion
  - Spins are thermodynamically driven to exchange positions.
    - Bloch-Torrey Equations





# **Bloch Equations – Rotating Frame**







Free Precession in the Rotating Frame with Relaxation

#### Free Precession in the Rotating Frame

$$\frac{\partial \vec{M}_{rot}}{\partial t} = \gamma \vec{M}_{rot} \times \vec{B}_{eff} - \frac{M_{x'}\vec{i'} + M_{y'}\vec{j'}}{T_2} - \frac{(M_{z'} - M_0)\vec{k'}}{T_1}$$

$$\vec{B}_{eff} \triangleq \frac{\vec{\omega}}{\gamma} + \vec{B}_{rot}$$

$$\vec{\omega}_{rot} = \vec{\omega} = -\gamma \mathbf{B}_0 \hat{k} \qquad \vec{\mathbf{B}}_{rot} = \mathbf{B}_0 \hat{k}$$

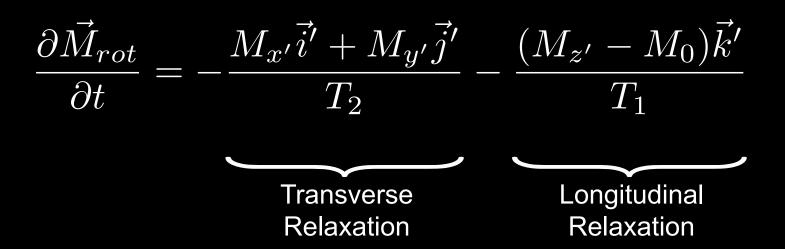
 $\vec{B}_{eff} = \vec{0}$   $\frac{\partial \vec{M}_{rot}}{\partial t} = -\frac{M_{x'}\vec{i'} + M_{y'}\vec{j'}}{T_2} - \frac{(M_{z'} - M_0)\vec{k'}}{T_1}$ 



The precessional term drops out in the rotating frame.



## Free Precession in the Rotating Frame



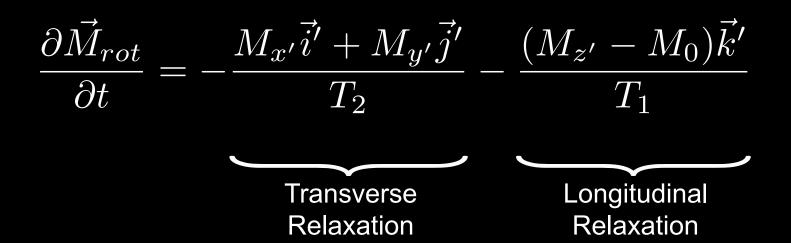
- No precession
- T<sub>1</sub> and T<sub>2</sub> Relaxation
- Drop the diffusion term
- System or first order, linear, separable ODEs!



The precessional term drops out in the rotating frame.



#### Free Precession in the Rotating Frame



**Solution:** 

$$M_{z'}(t) = M_z^0 e^{-t/T_1} + M_0 (1 - e^{-t/T_1})$$
$$M_{x'y'}(t) = M_{x'y'}(0_+) e^{-t/T_2}$$



The precessional term drops out in the rotating frame.



Forced Precession in the Rotating Frame with Relaxation

#### Forced Precession in the Rot. Frame with Relaxation

$$\begin{aligned} \frac{\partial \vec{M}_{rot}}{\partial t} &= \gamma \vec{M_{rot}} \times \vec{B}_{eff} - \frac{M_{x'}\vec{i'} + M_{y'}\vec{j'}}{T_2} - \frac{(M_{z'} - M_0)\vec{k'}}{T_1} \\ \vec{B}_{eff} \triangleq \frac{\vec{\omega}}{\gamma} + \vec{B}_{rot} \\ \vec{\omega}_{rot} &= \vec{\omega} = -\gamma B_0 \hat{k} \quad \vec{B}_{rot} = B_0 \hat{k} + B_1^e(t) \hat{i'} \\ \vec{B}_{eff} &= B_1^e(t) \hat{i'} \end{aligned}$$



The precessional term *does not* drop out in the rotating frame.



#### Forced Precession in the Rot. Frame with Relaxation

$$\frac{\partial \vec{M}_{rot}}{\partial t} = \gamma \vec{M}_{rot} \times \vec{B}_{eff} - \frac{M_{x'}\vec{i'} + M_{y'}\vec{j'}}{T_2} - \frac{(M_{z'} - M_0)\vec{k'}}{T_1}$$
$$\vec{B}_{eff} = B_1^e(t)\hat{i'}$$

- B1 induced nutation
- T<sub>1</sub> and T<sub>2</sub> Relaxation

David Geffen

- Drop the diffusion term
- System or first order, linear, coupled PDEs!
- When does this equation apply?



# Forced Precession in the Rotating Frame with Relaxation

- RF pulses are short
  - $-100\mu s$  to 5ms
- Relaxation time constants are long
  - $-T_1 O(100s) ms$
  - $-T_2 O(10s) ms$
- Complicated Coupling
- Best suited for simulation





# Free? Forced? Relaxation?

- We've considered all combinations of:
  - Free and forced precession
  - With and without relaxation
  - Laboratory and rotating frames
- Which one's concern M219 the most?
  - Free precession in the rotating frame with relaxation
  - Forced precession in the rotating frame without relaxation.
- We can, in fact, simulate all of them...







- Related reading materials
  - Nishimura Chap 4 and 5

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