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# Pulse Sequences: RARE and Simulations

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M229 Advanced Topics in MRI

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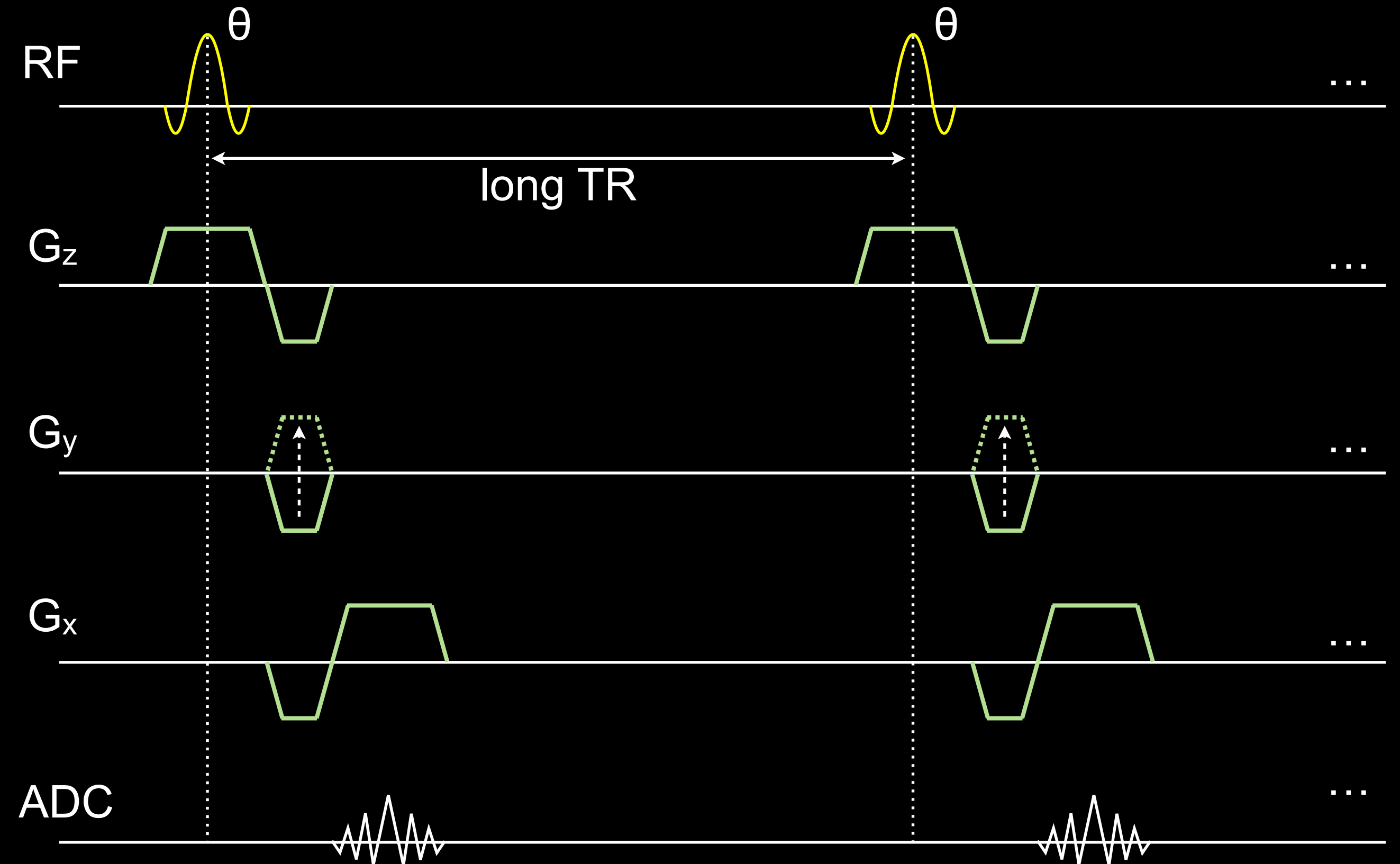
# Class Business

- Office hours
  - Instructor: Fri 10-11 am
  - TA for HW1: 4/8, 4/15, 4/22 Thu 8-10 am
- Homework 1 due on 4/23 Fri
- Final project
  - Start thinking
  - Discuss over email or during office hours
  - Discussion in class on 4/22 Thu

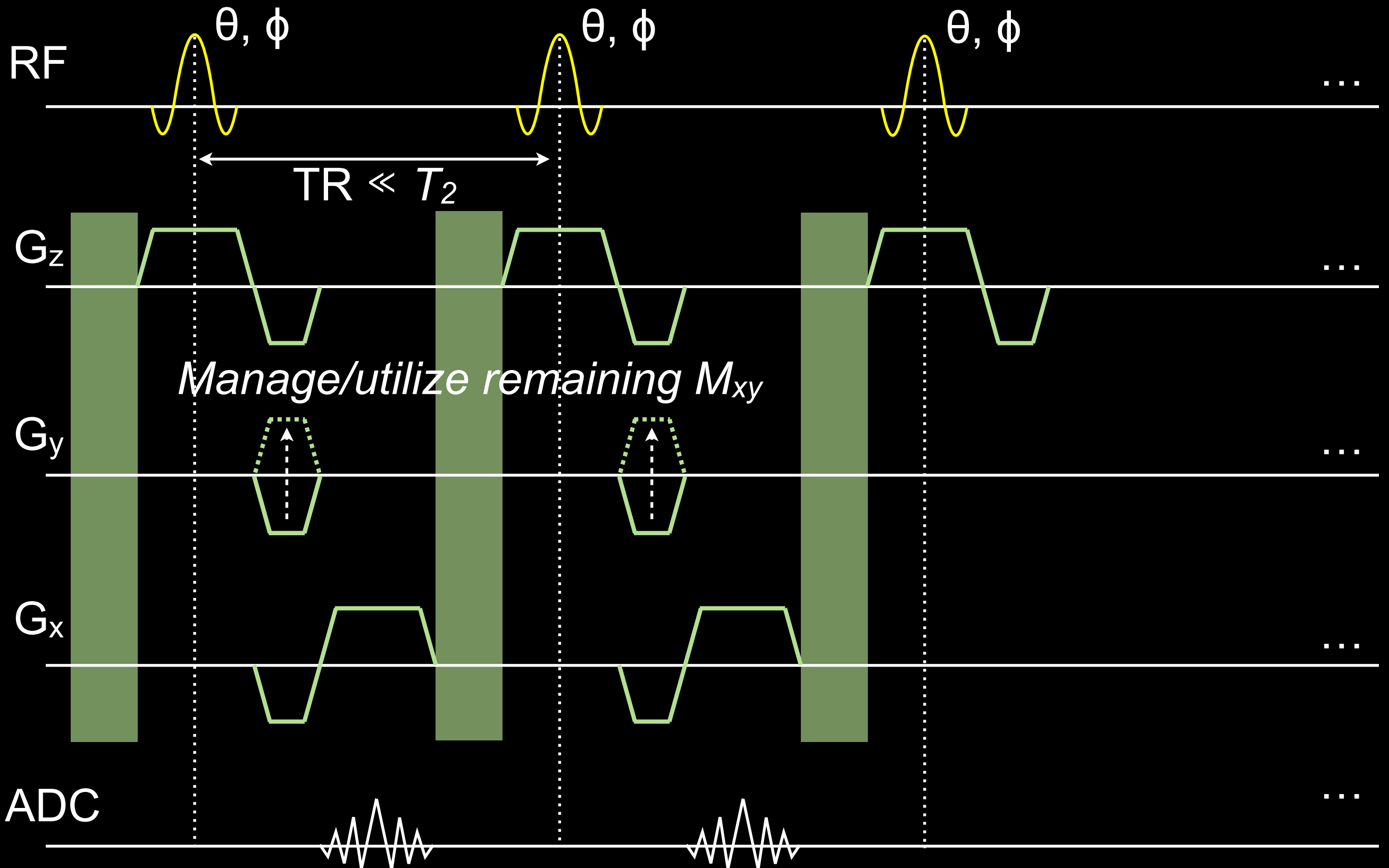
# Outline

- Rapid GRE
  - Review
- RARE (aka FSE, TSE)
- Pulse sequence simulations
  - MATLAB Bloch simulations
  - Homework 1

# Gradient Echo



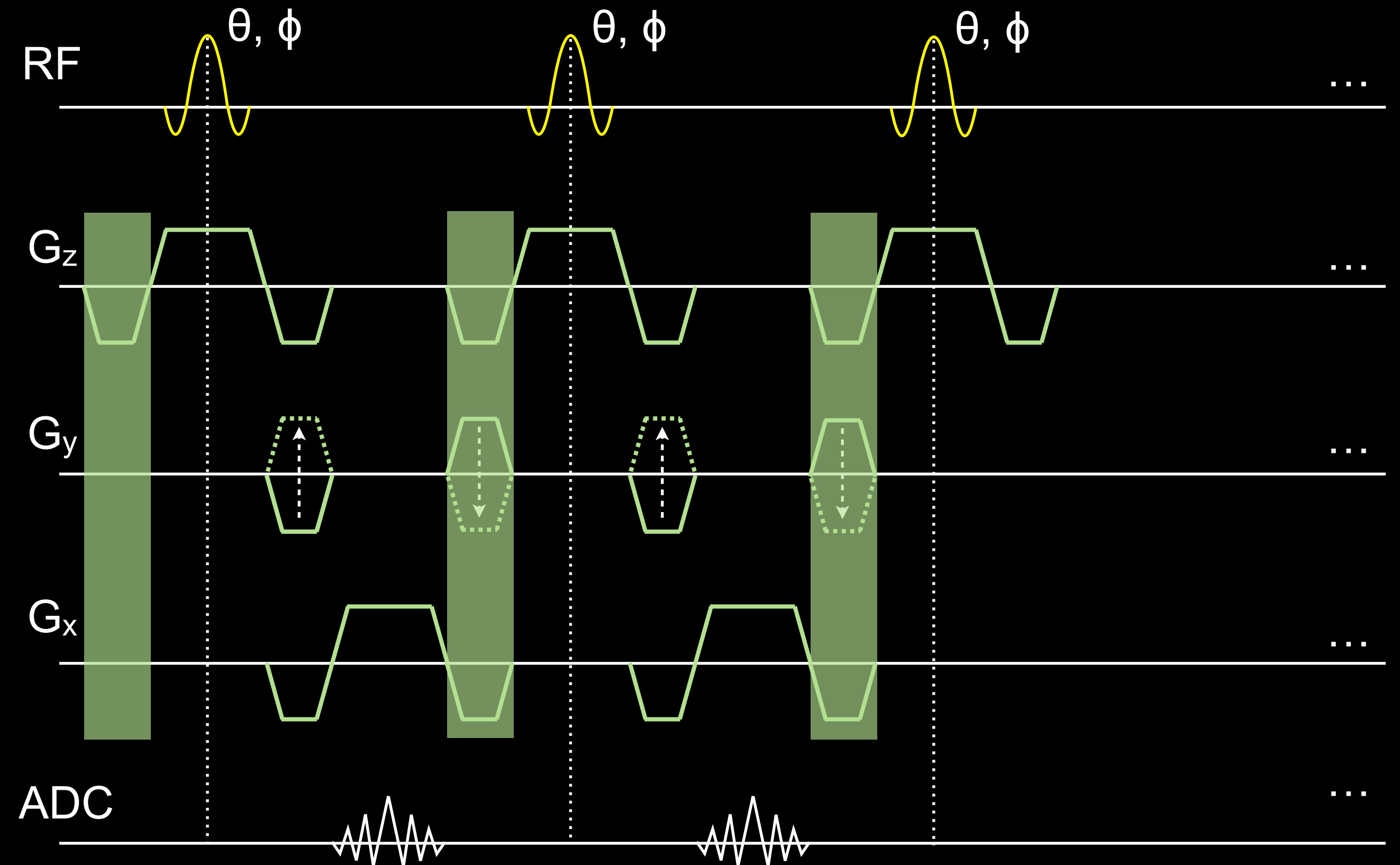
# Rapid Gradient Echo



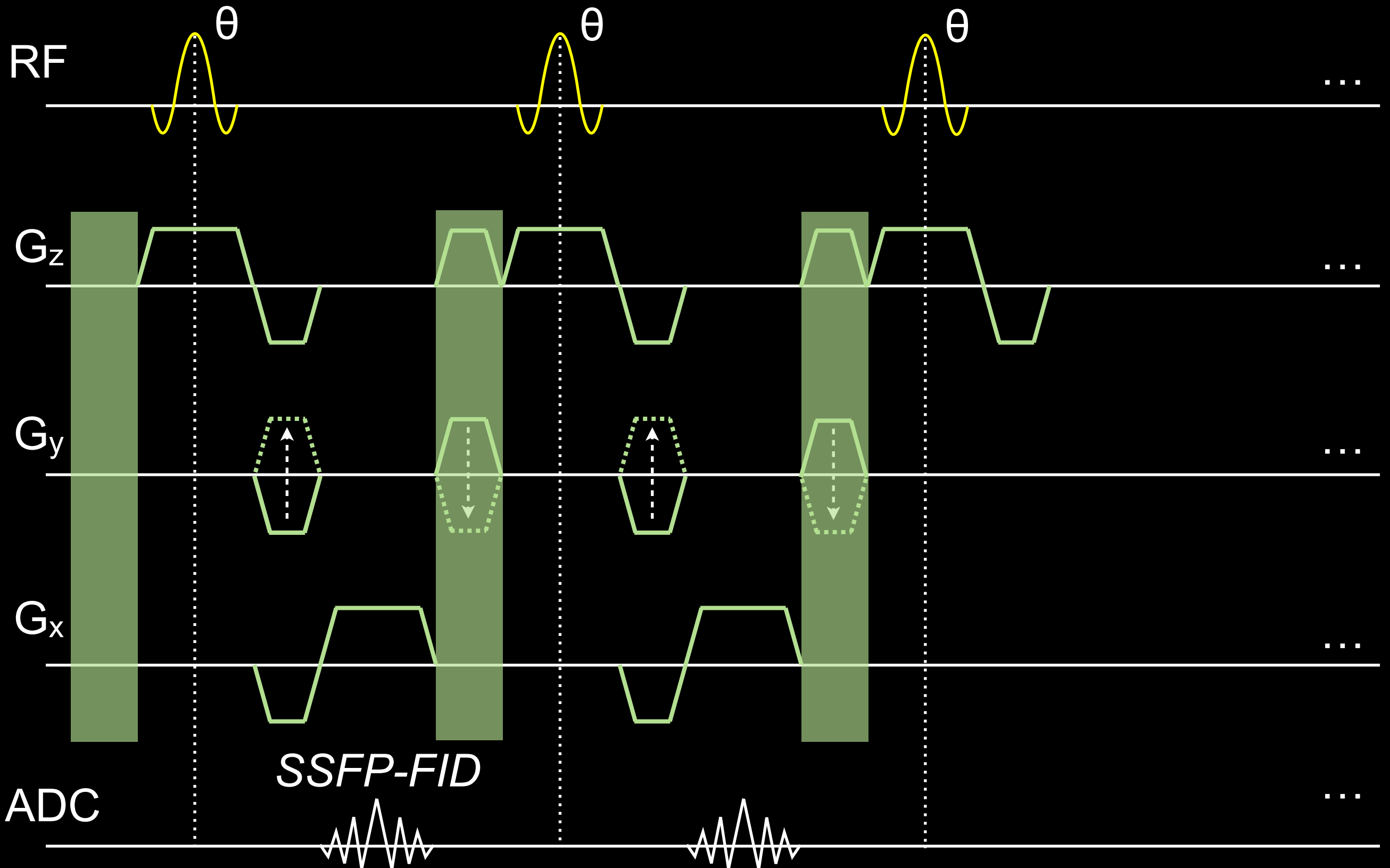
# Rapid Gradient Echo

- Rapid imaging with  $TR \ll T_2 < T_1$
- Steady state
  - Involves a mixture of  $M_z$  and  $M_{xy}$
  - Necessary and sufficient conditions:
    1. Constant RF flip angle  $\theta$
    2. Constant TR
    3. Constant dephasing  $\beta$  between RF pulses
    4. RF phase  $\phi_n = a + bn + cn^2$

# Balanced SSFP



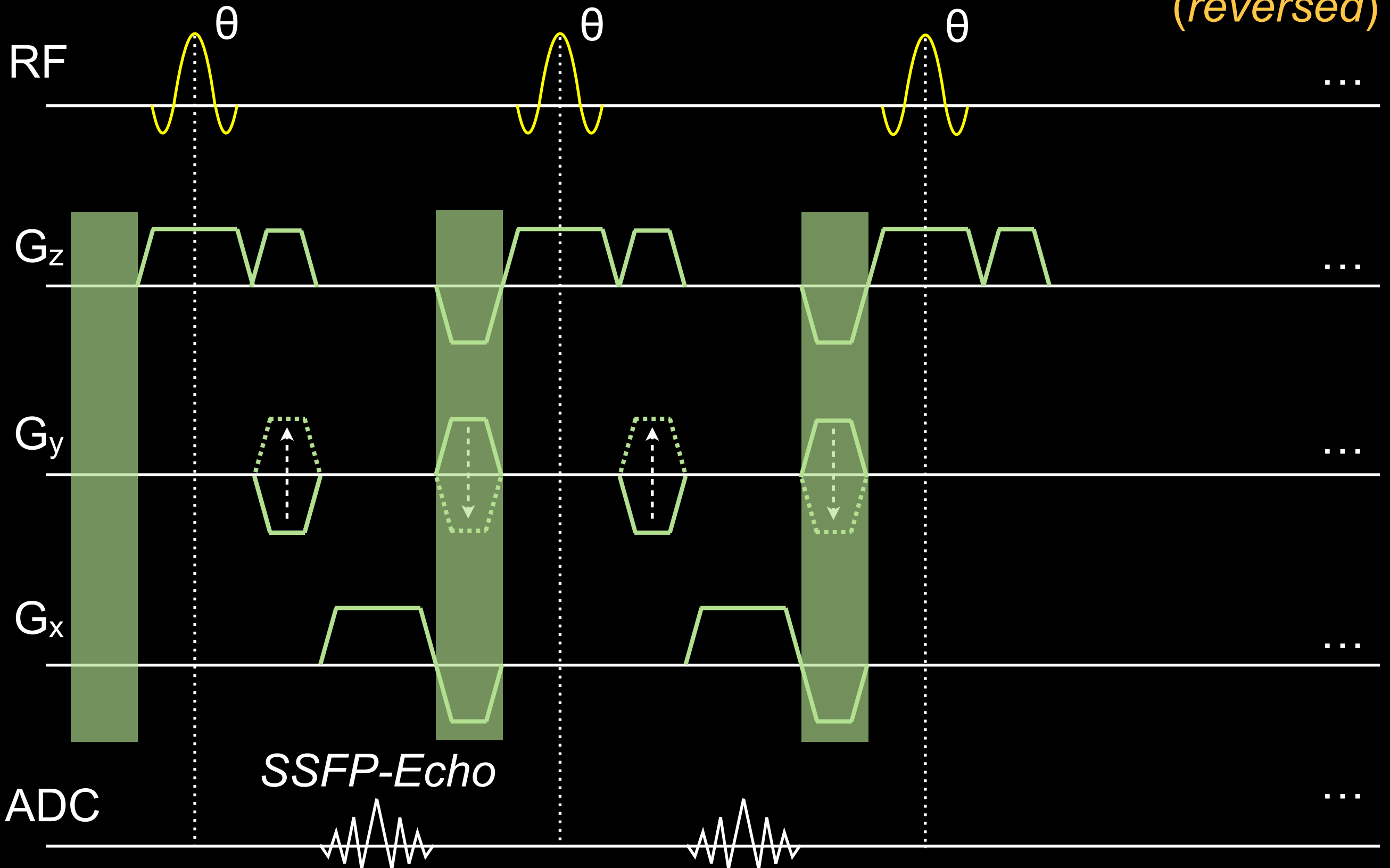
# Gradient-spoiled GRE



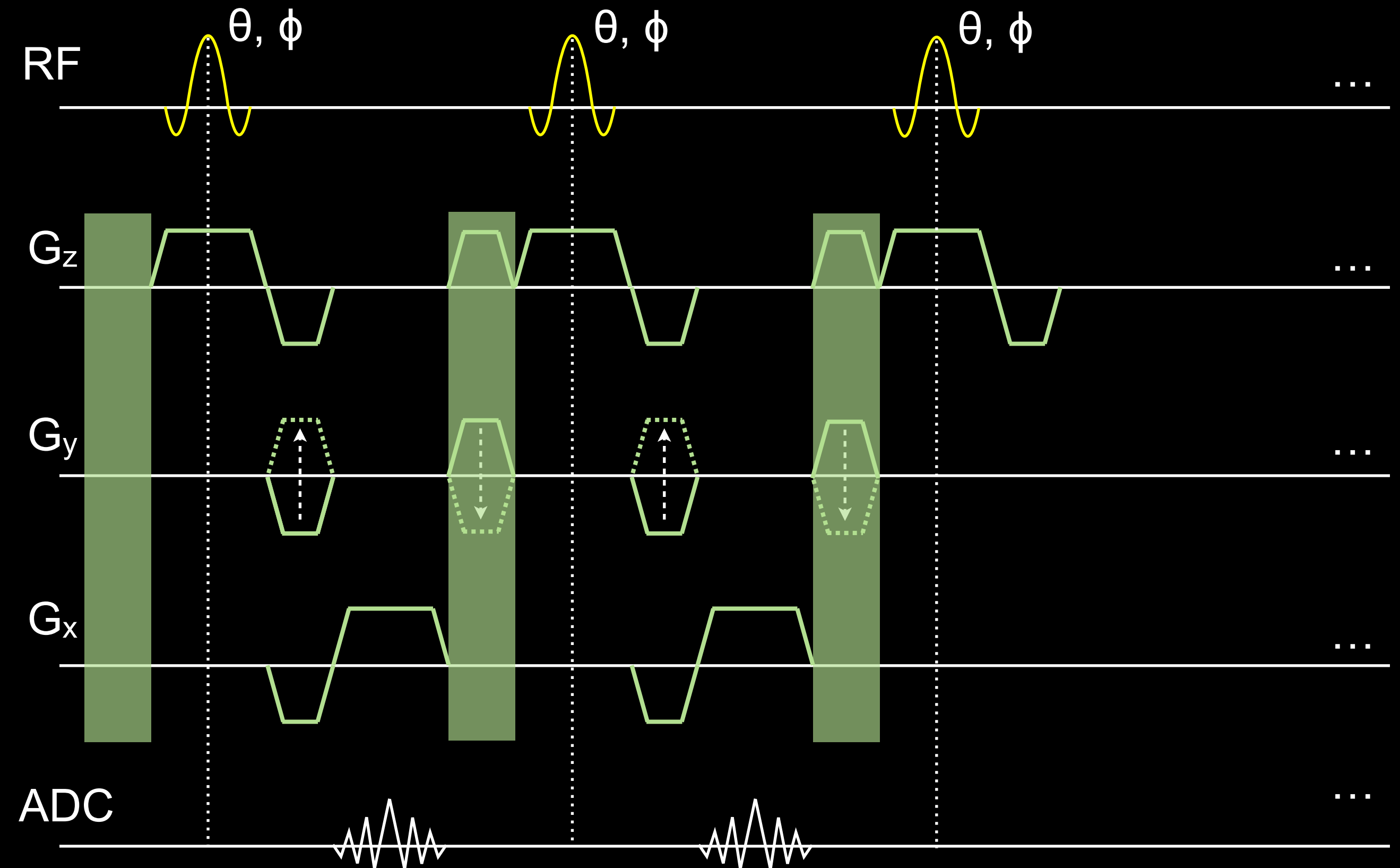


# Gradient-spoiled GRE

*(reversed)*



# Gradient & RF-spoiled GRE

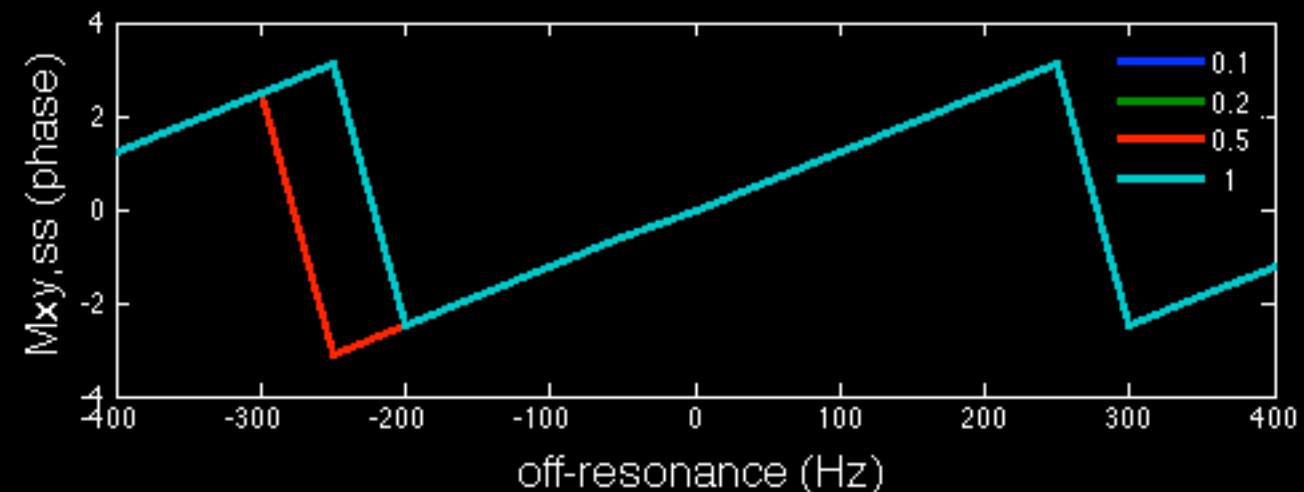
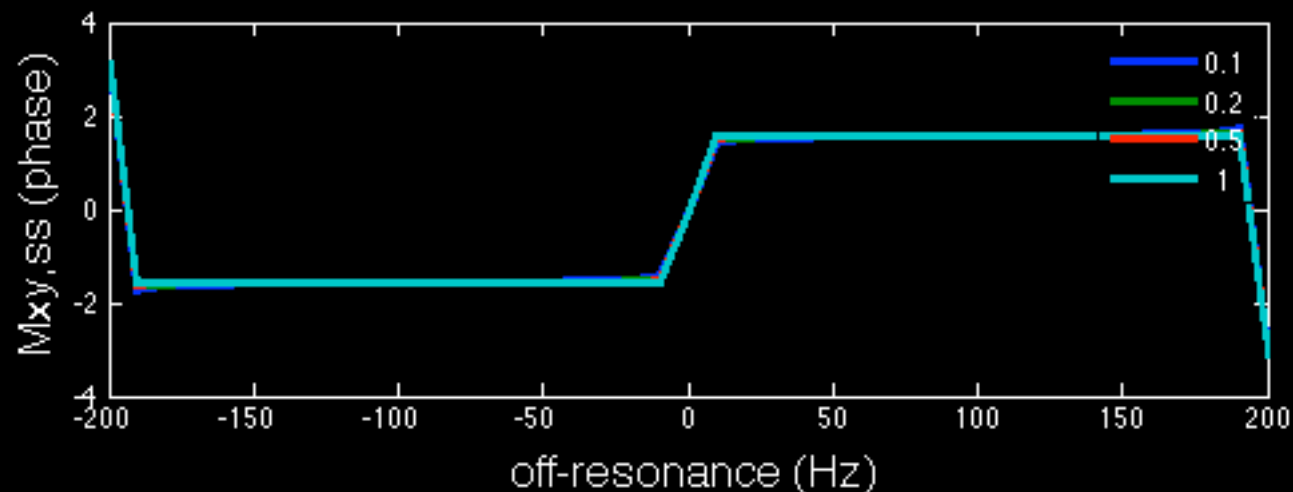
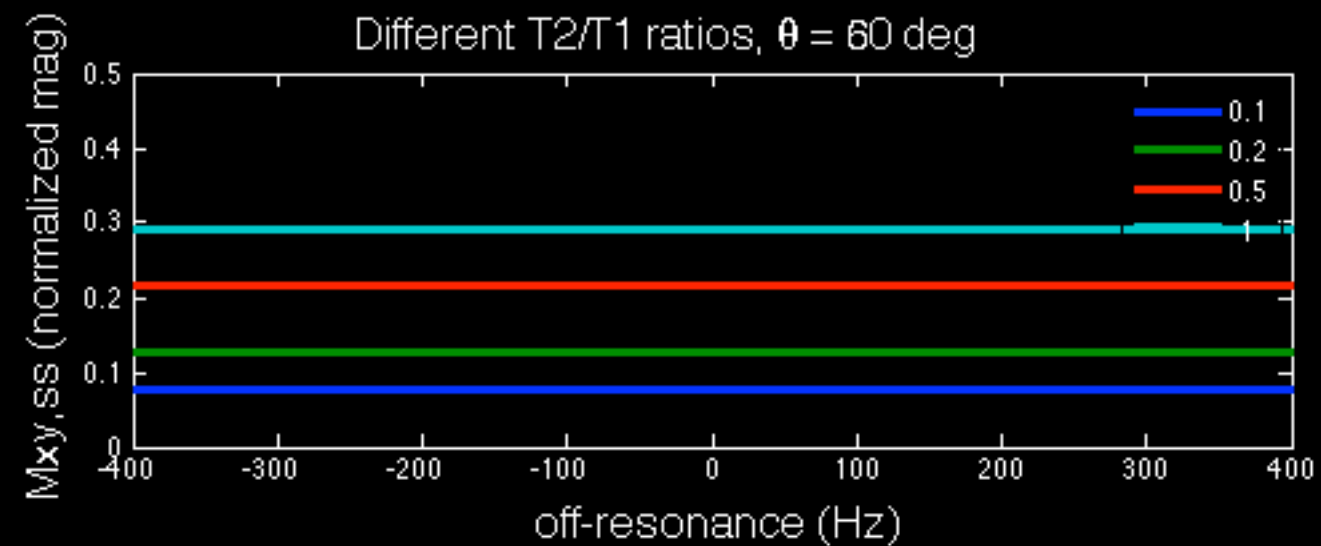
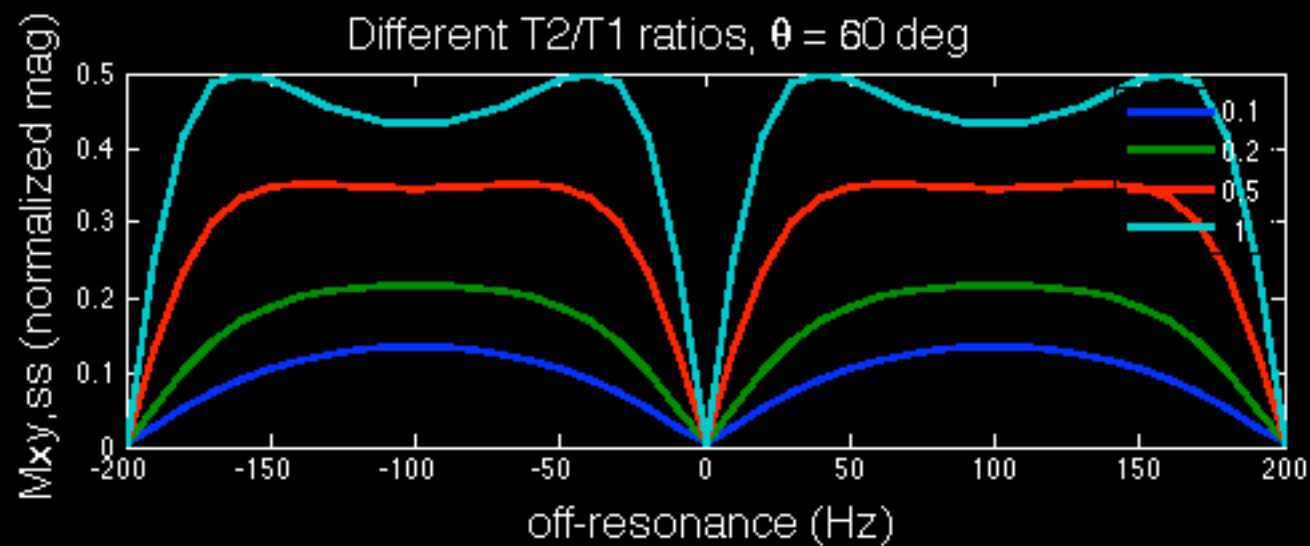


# Gradient-spoiled GRE

SS signal as a function of off-resonance:

*bSSFP*

*GRE (SSFP-FID)*



$T_1 = 1000$  ms,  $T_2 = 100, 200, 500, 1000$  ms

# Gradient and RF-spoiled GRE

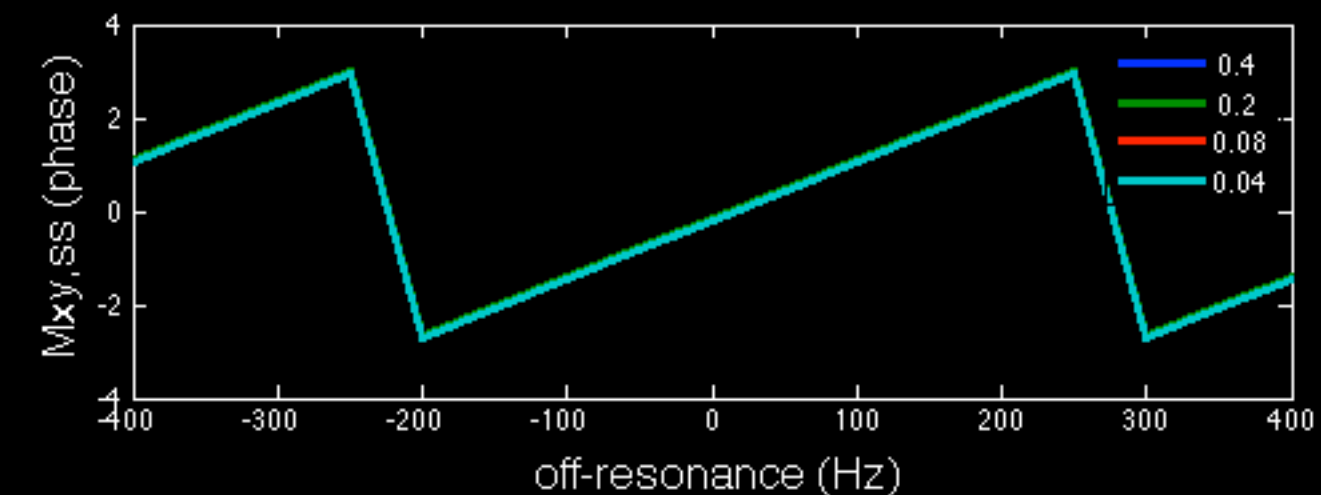
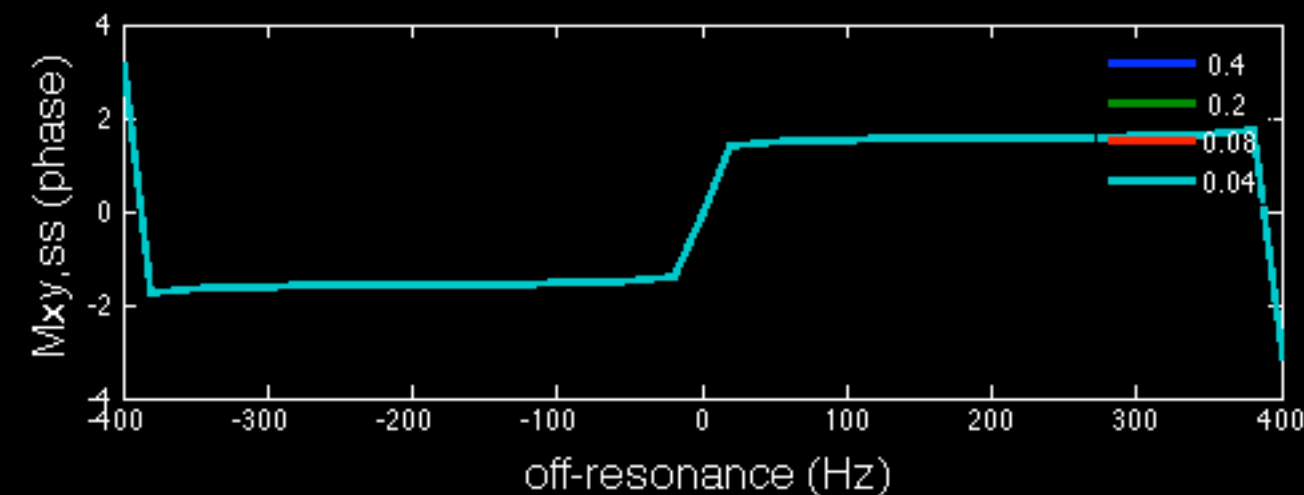
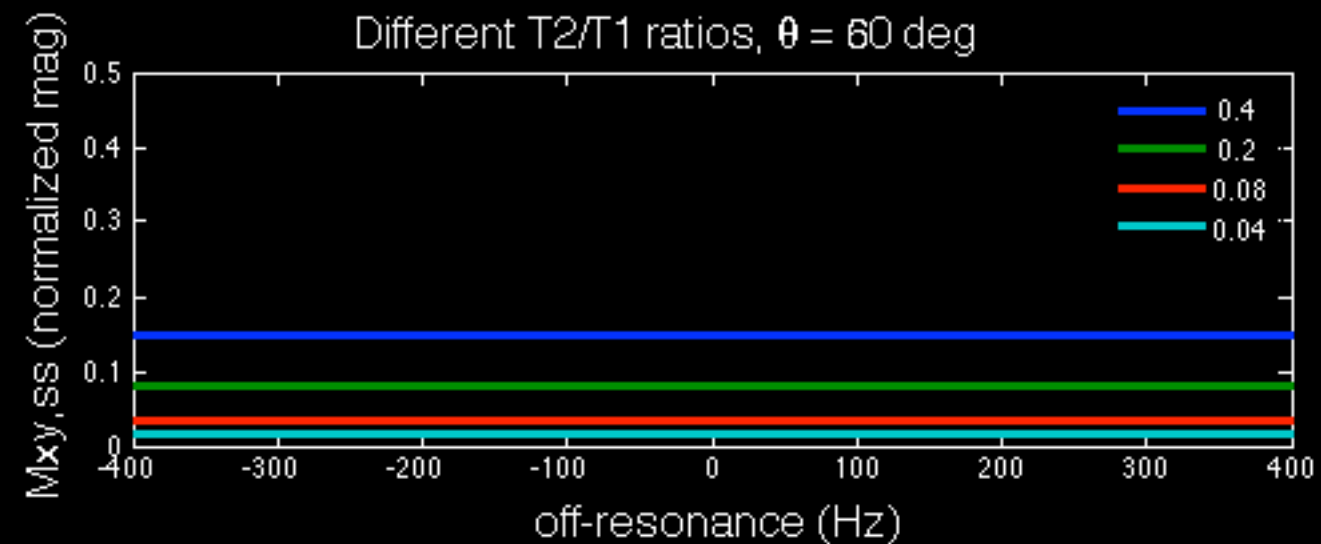
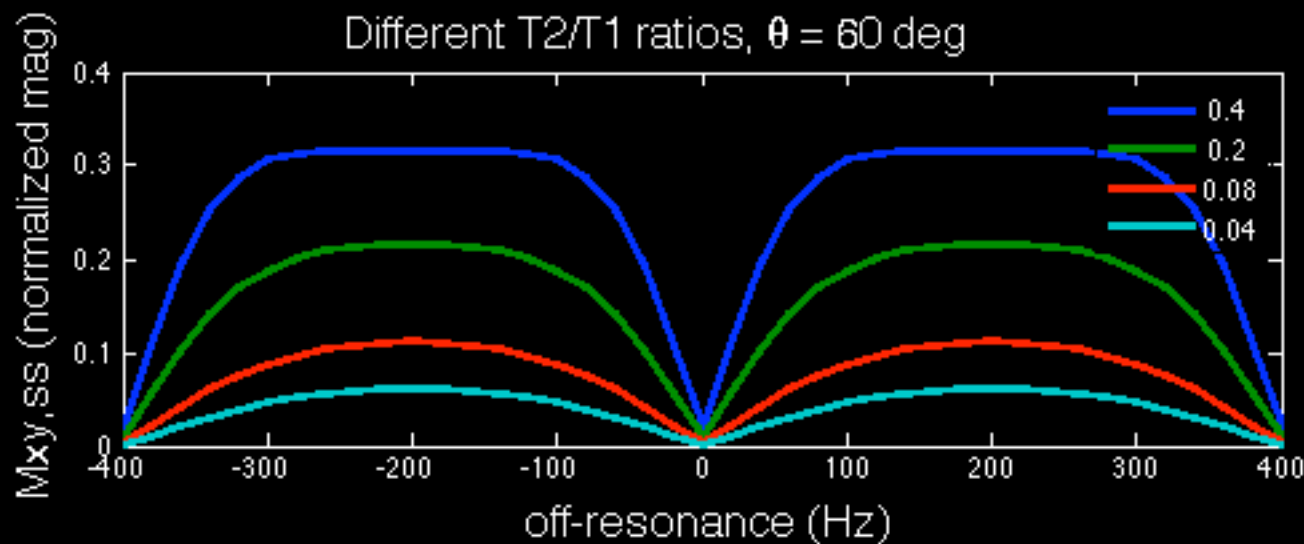
- RF spoiling (quadratic)
  - $\phi_n = \phi_{n-1} + n\phi_0 = (1/2)\phi_0(n^2 + n + 2)$
  - typically  $\phi_0 = 50^\circ$  or  $117^\circ$
  - ADC phase each TR also needs to match  $\phi_n$
- $T_1$ -weighted contrast
  - approaches contrast of ideally spoiled GRE
  - at expense of reduced SNR  
(removes T2w contributions)

# Gradient and RF-spoiled GRE

SS signal as a function of off-resonance:

*bSSFP*

*Spoiled GRE*



$T_1 = 100, 200, 500, 1000$  ms,  $T_2 = 40$  ms

# Rapid GRE - Comparison

Pulse Sequence		Mxy	Contrast	SNR	Artifacts
Balanced SSFP	bSSFP	retained	$T_2/T_1$	high	banding
Gradient-spoiled GRE	SSFP-FID	averaged	$T_2/T_1$	mid	motion
	SSFP-Echo	averaged	$T_2+T_2/T_1$	mid	motion
Gradient and RF-spoiled GRE	Spoiled GRE	cancelled	$T_1; T_2^*$	low	minimal

SS transition

# Why RARE (TSE)?

- Basic spin echo (SE) MRI is slow
  - TR on the order of 500 - 5000 ms
  - Data acquisition of one k-space line per TR, readout duration of 10 ms or less
  - Could acquire more lines before complete  $T_2$  decay of  $M_{xy}$

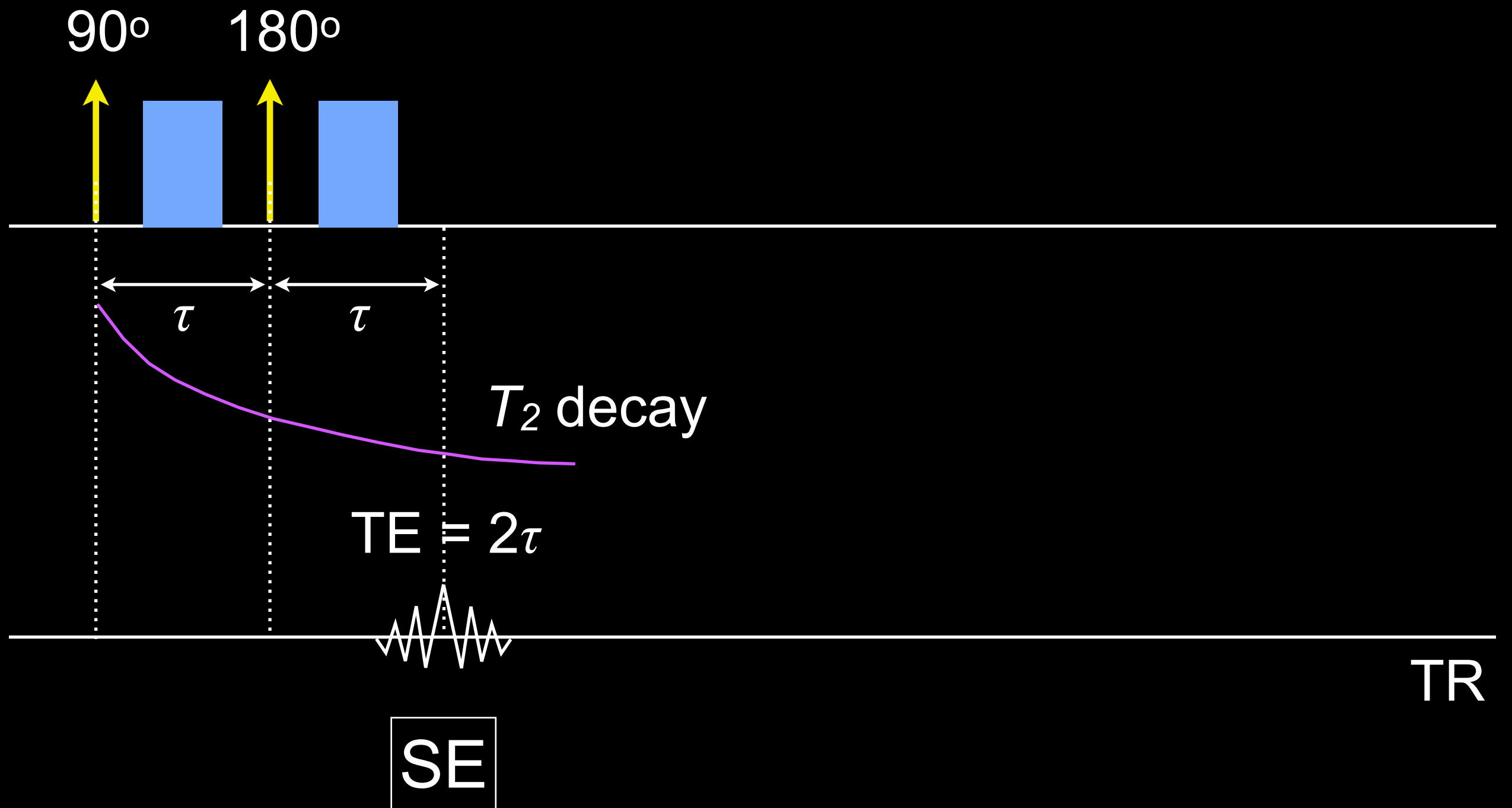
# RARE (TSE) MRI

- Rapid Acquisition with Relaxation Enhancement (RARE)<sup>1</sup>, aka Fast Spin-Echo (FSE) or Turbo Spin-Echo (TSE)
- Has virtually replaced SE for multiple clinical applications, esp. T2w imaging
- Challenging at high field ( $\geq 3$  T)

<sup>1</sup>Hennig J et al., *MRM* 1986



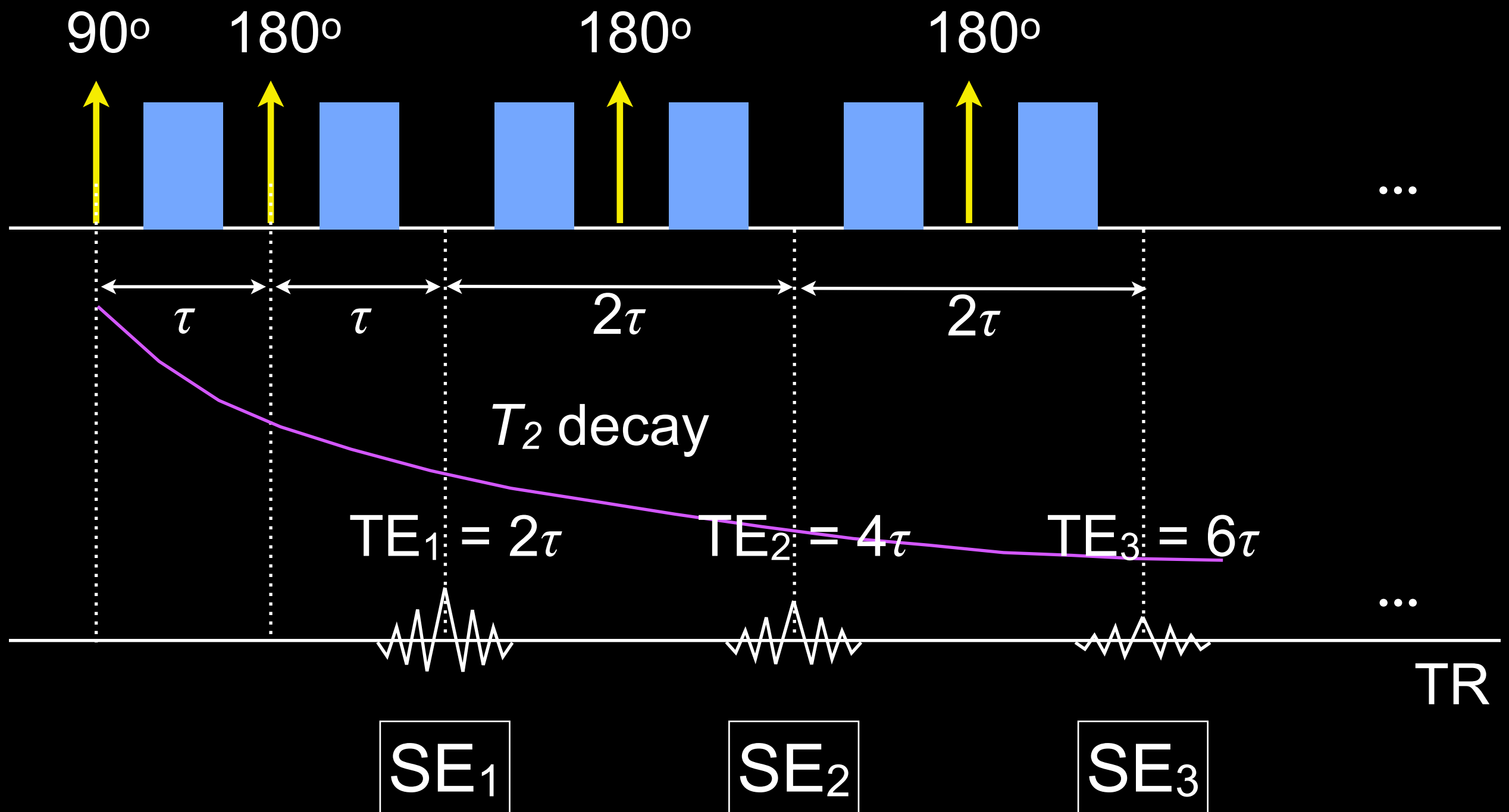
# Spin Echo



# Spin Echo

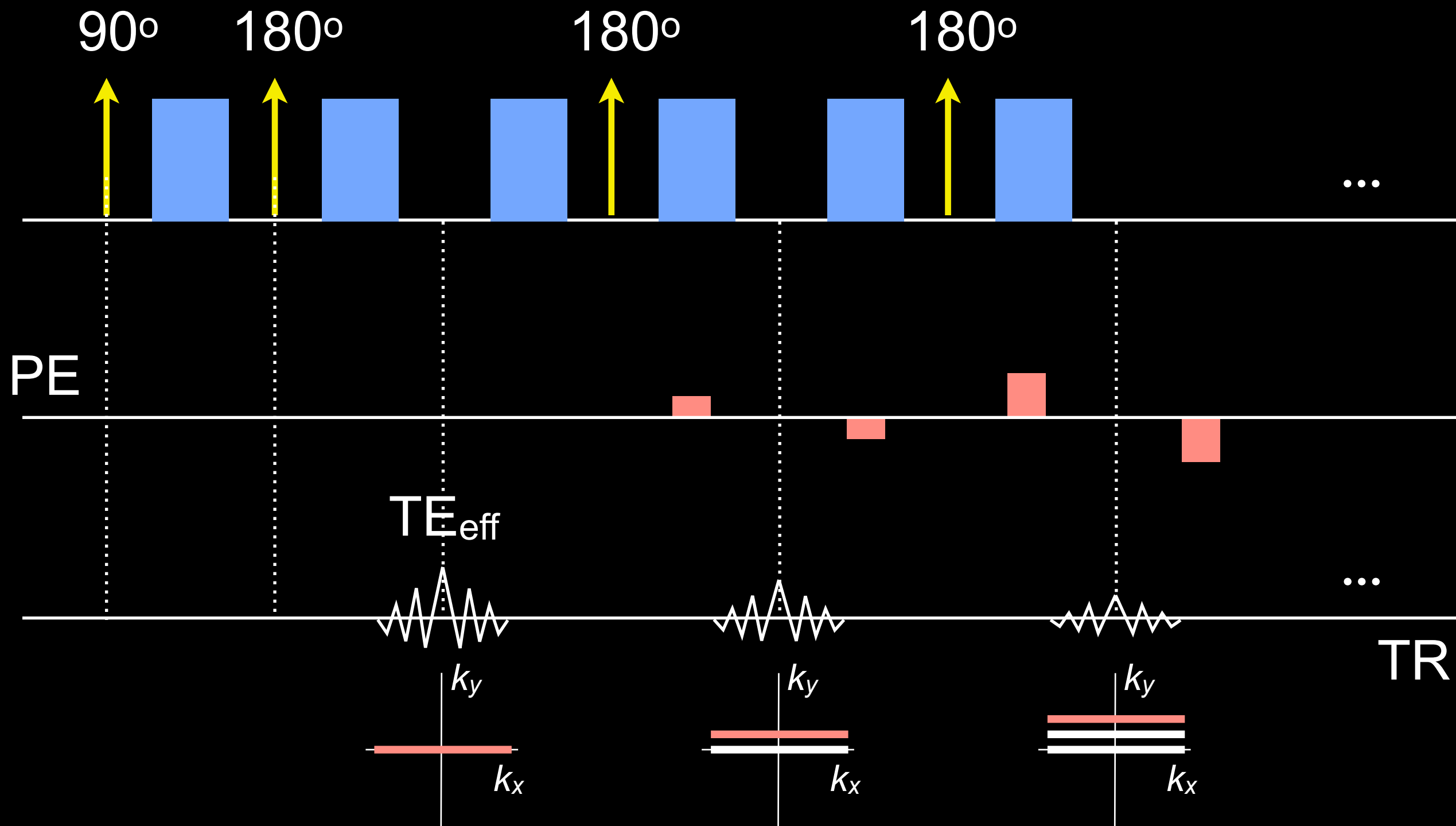
- Image contrast
  - Based on TE, TR
  - T1w, T2w, PDw
  - Can augment with prep pulses
- Scan time
  - $T_{SE} = N_{pe} \times TR$
  - TR = 1000 ms,  $N_{pe} = 256$ :  $T_{SE} = 4+$  min
  - usually combined with 2D multislice acq

# Multi-echo Spin Echo



Can perform  $T_2$  mapping.

# RARE (Turbo Spin Echo)



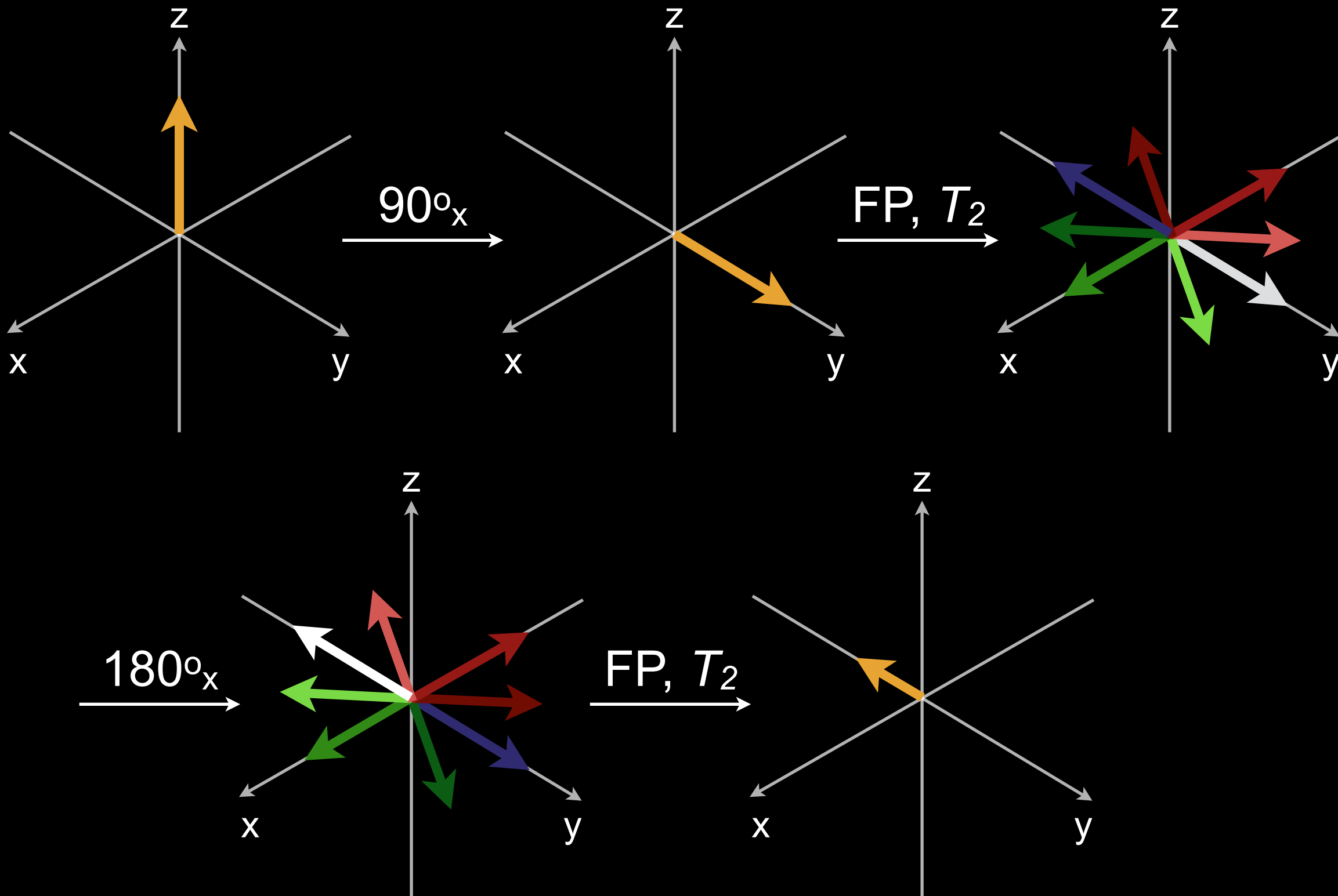
# CPMG Conditions

- Carr-Purcell-Meiboom-Gill conditions
  - ensure echoes only occur at desired positions in the sequence, and
  - signals at each position have the same phase
- $90^\circ_x - \tau - 180^\circ_y - 2\tau - 180^\circ_y - 2\tau - 180^\circ_y \dots$
- Constant phase accrual btwn pulses
  - Same area for crusher pairs
  - Phase encode rewinder

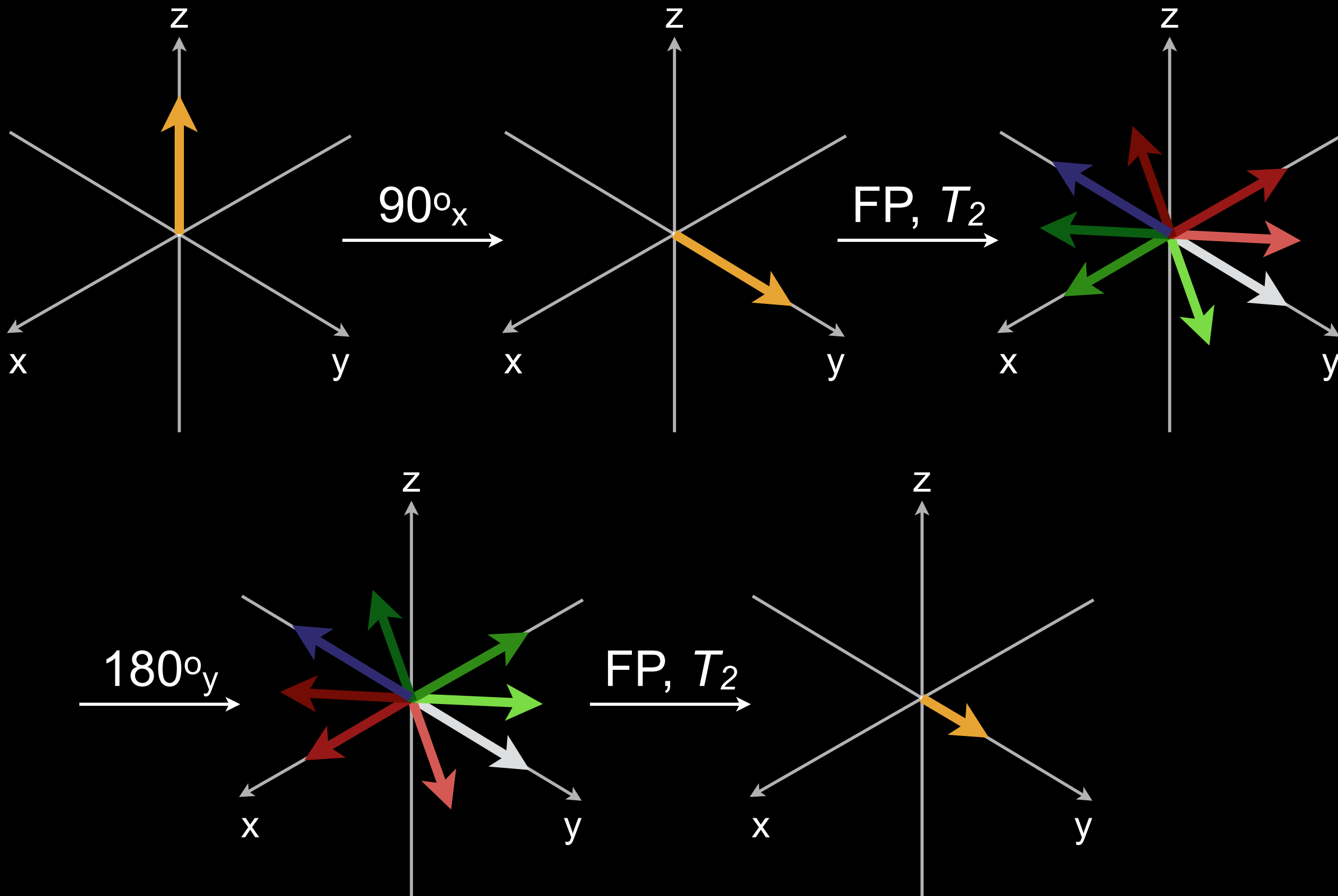
# CPMG Conditions

- When satisfied
  - SE and STE coincide (same phase)
  - secondary SE and FID are crushed
- Moving spins can violate CPMG

# Spin Echo: $90^\circ_x - 180^\circ_x$

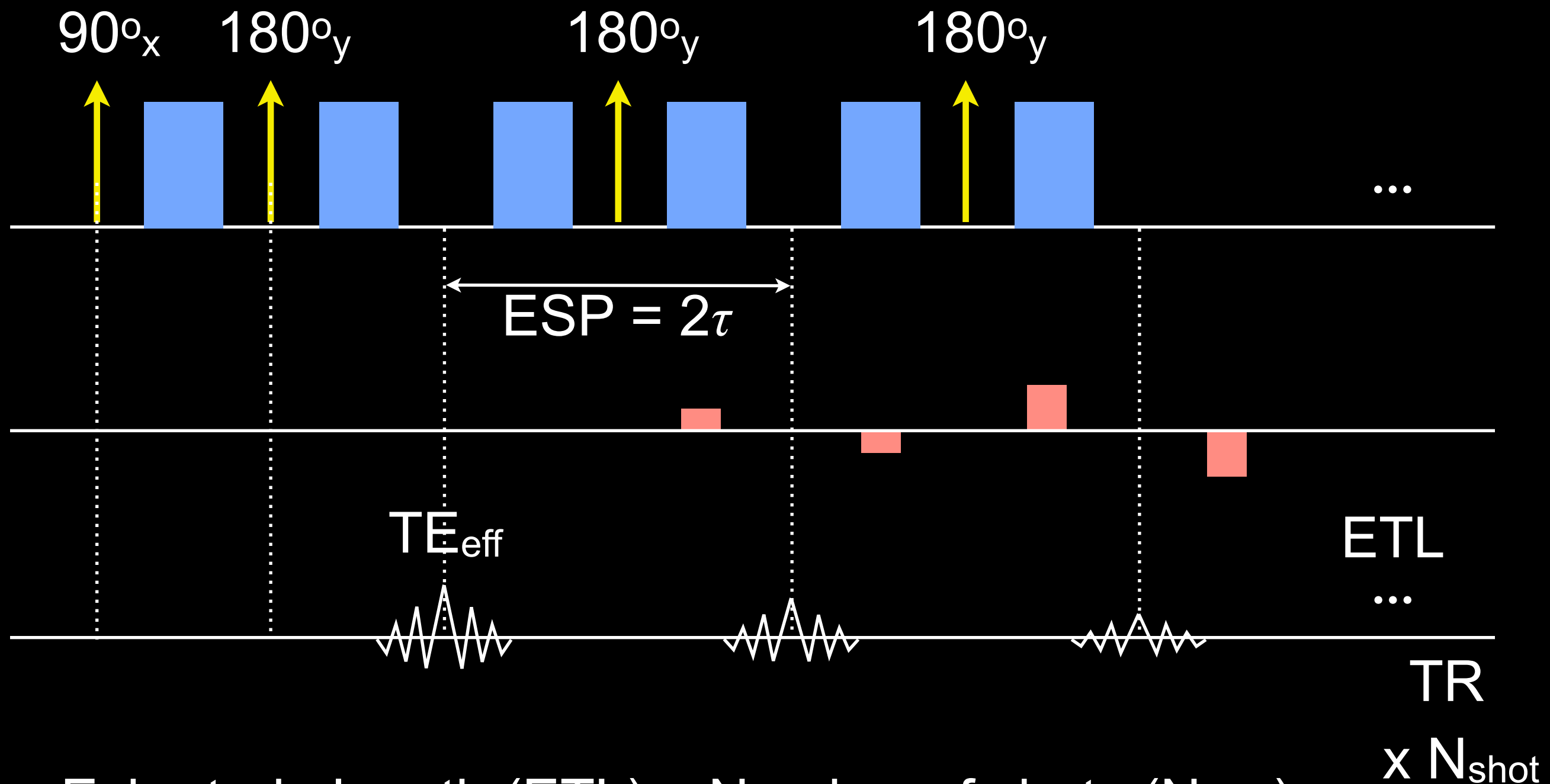


# Spin Echo: $90^\circ_x - 180^\circ_y$





# TSE Sequence Params



Echo train length (ETL)

Number of shots ( $N_{shot}$ )

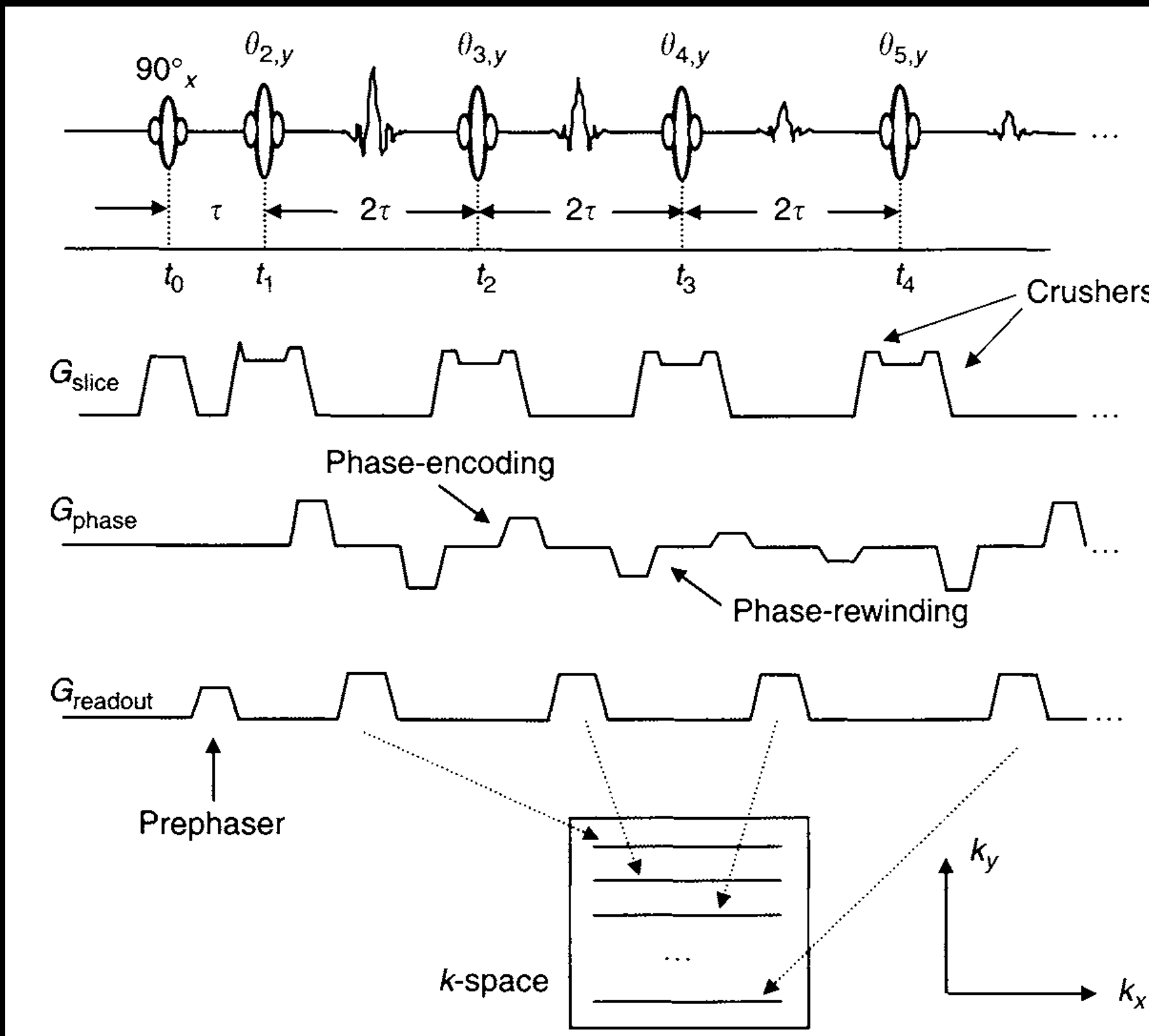
Echo spacing (ESP)

Effective TE ( $TE_{eff}$ )

# TSE Sequence Params

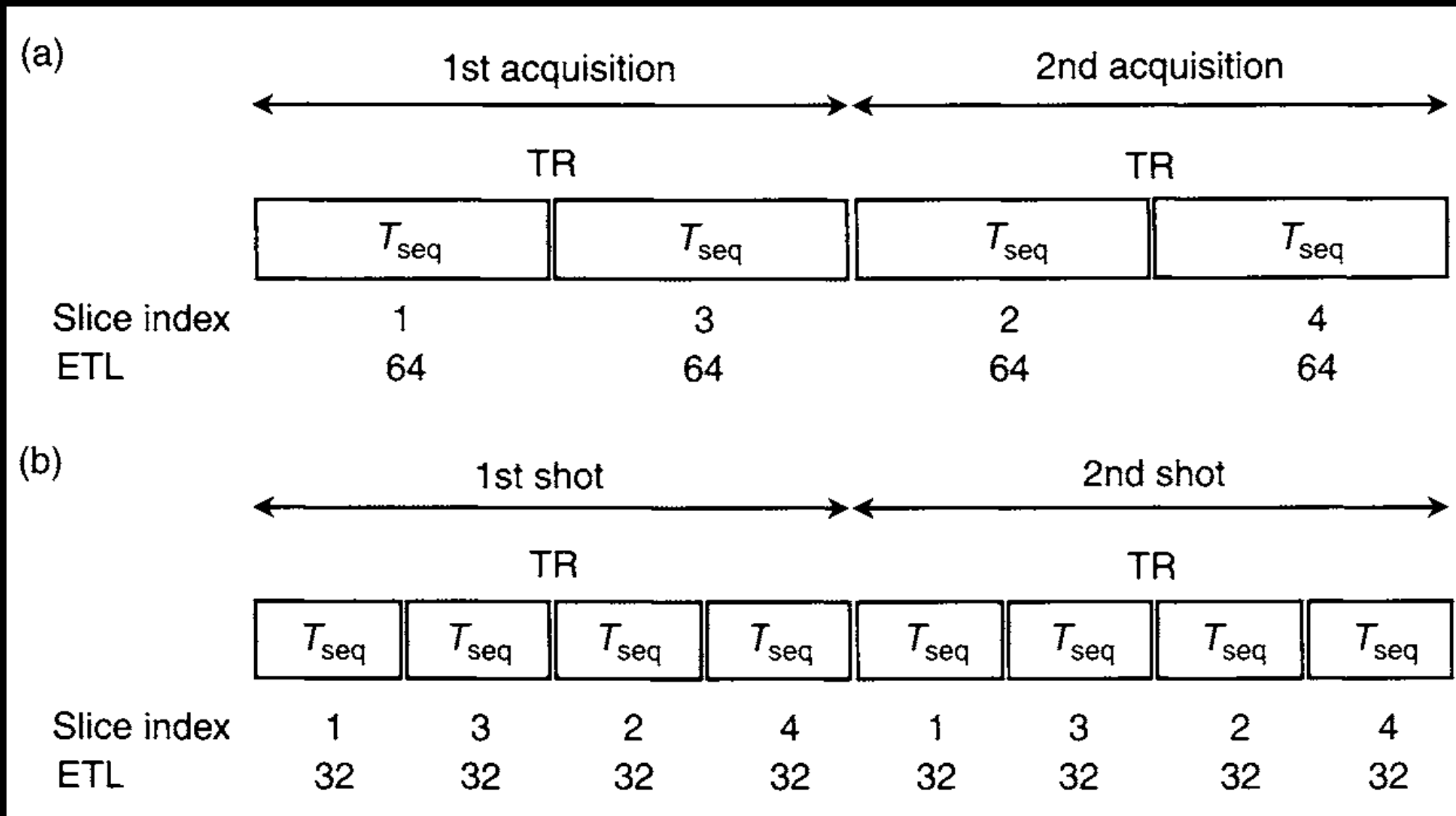
- ETL typically 4-16
  - Can't be too high, due to  $T_2$  decay
- ESP typically <10 ms
  - Must accommodate RF, gradients, ADC
  - Short ESP facilitates high ETL
- Example: readout until  $S = 0.2 S_0$ 
  - $S = S_0 * \exp(-t/T_2)$ ; assume  $T_2 = 100$  ms
  - $t = 160.9$  ms
  - ESP = 8 ms; ETL = 20
  - ESP = 4 ms; ETL = 40

# 2D RARE Sequence

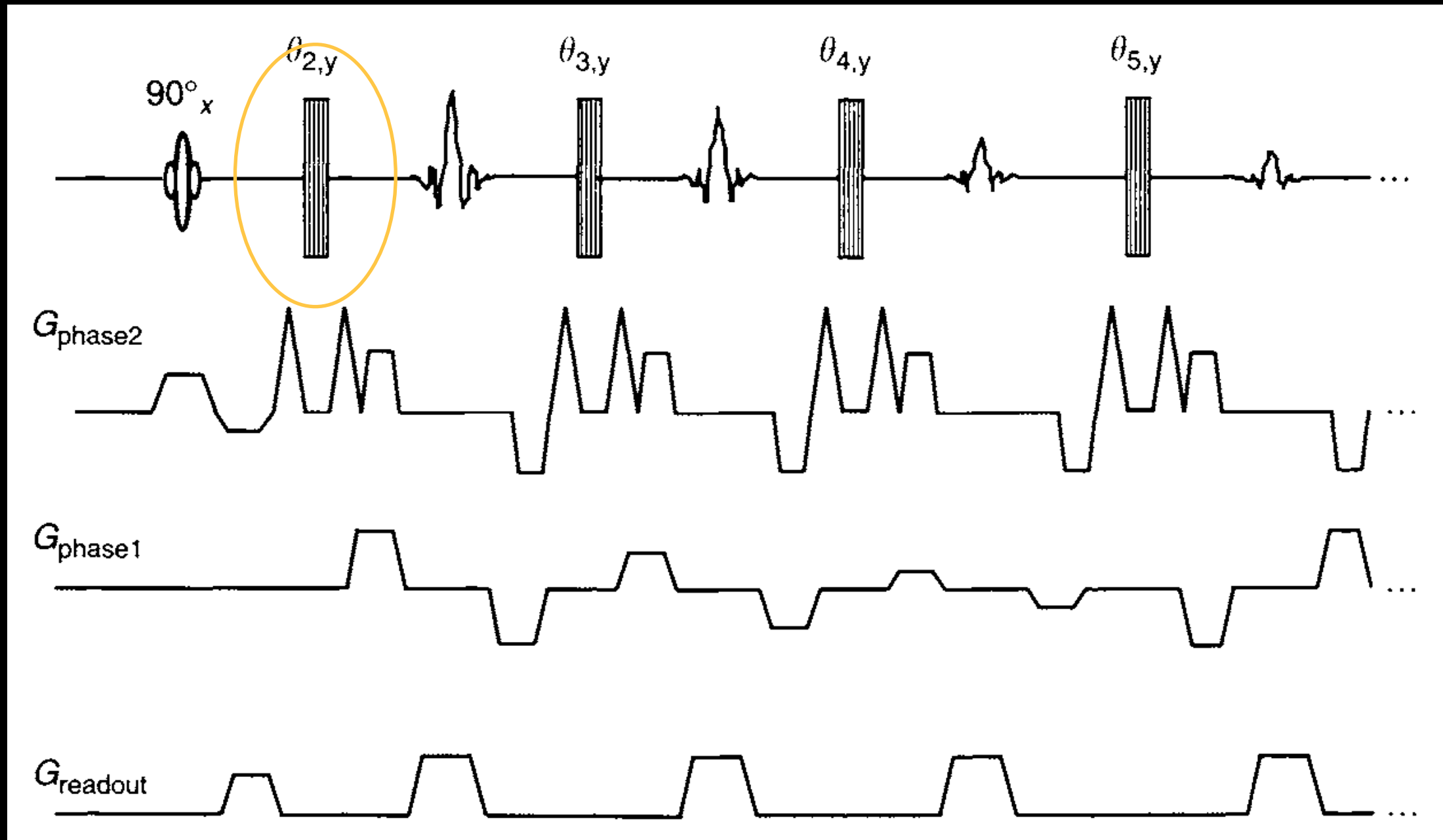


# 2D RARE Sequence

## Interleaved 2D Multi-Slice Acquisition



# 3D RARE Sequence

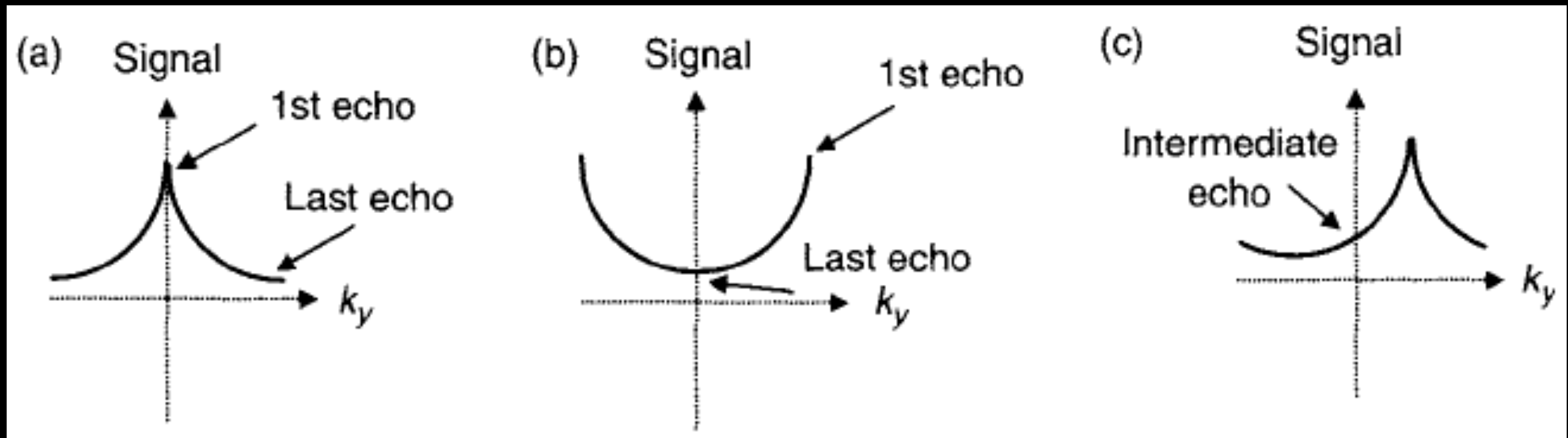


# TSE Scan Time

- Scan time
  - Recall  $T_{SE} = N_{pe} \times TR_{SE}$
  - $N_{shot} = N_{pe} / ETL$
  - $T_{TSE} = N_{shot} \times TR_{TSE} = (T_{SE} / ETL) \times (TR_{TSE}/TR_{SE})$
- Example: 2D single slice
  - $N_{pe} = 256$ ;  $ETL = 16$ ;  $N_{shot} = 16$
  - $TR = 1000$  ms:  $T_{TSE} = 16$  sec
- Example: 3D volume
  - $N_{pe} = 256 \times 256$ ;  $ETL = 32$ ;  $N_{shot} = 2048$
  - $TR = 1000$  ms:  $T_{TSE} = 34$  min

# TSE Image Contrast

- $TE_{\text{eff}}$ , TR
  - T1w, T2w, PDw
  - PE ordering affects  $TE_{\text{eff}}$



# TSE Image Contrast

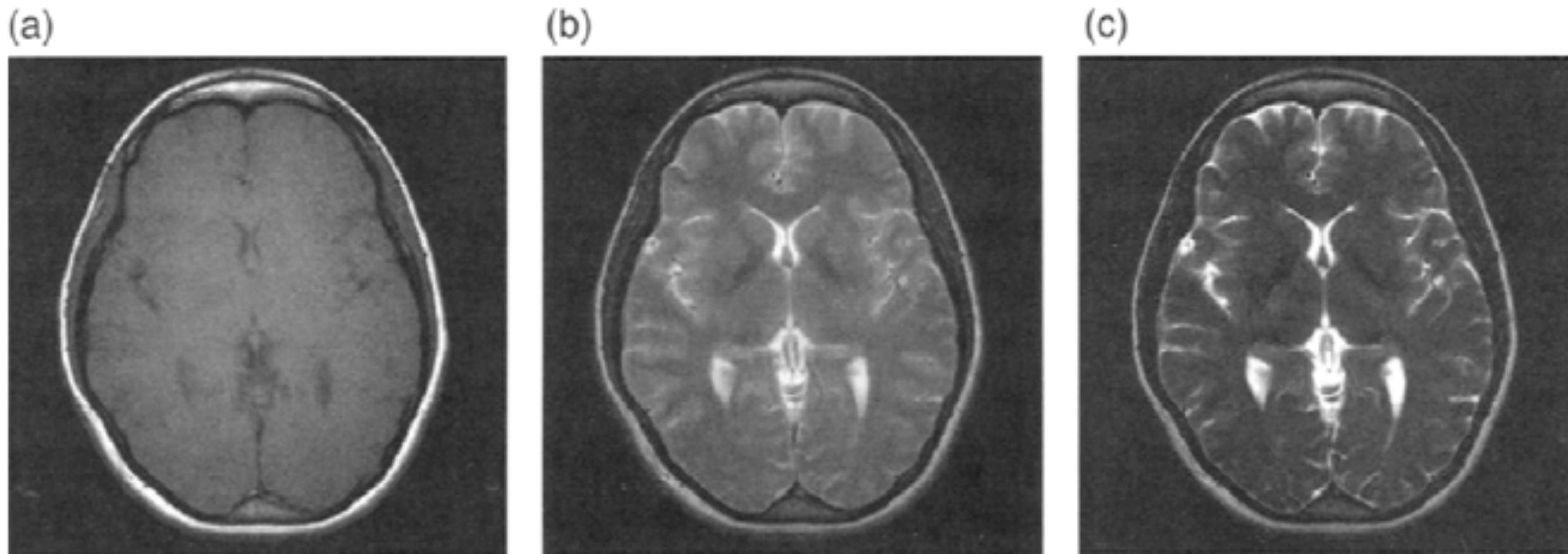


FIGURE 16.48 By using different echoes to sample the k-space center, considerably different image contrast can be obtained from a RARE sequence. (a)  $T_1$ -weighted image with  $TE = 11$  ms,  $TR = 480$  ms, and  $N_{\text{etl}} = 8$ . (b) Moderately  $T_2$ -weighted image with  $TE = 77$  ms,  $TR = 4000$  ms, and  $N_{\text{etl}} = 16$ . (c) Heavily  $T_2$ -weighted image with  $TE = 176$  ms,  $TR = 4000$  ms, and  $N_{\text{etl}} = 16$ .

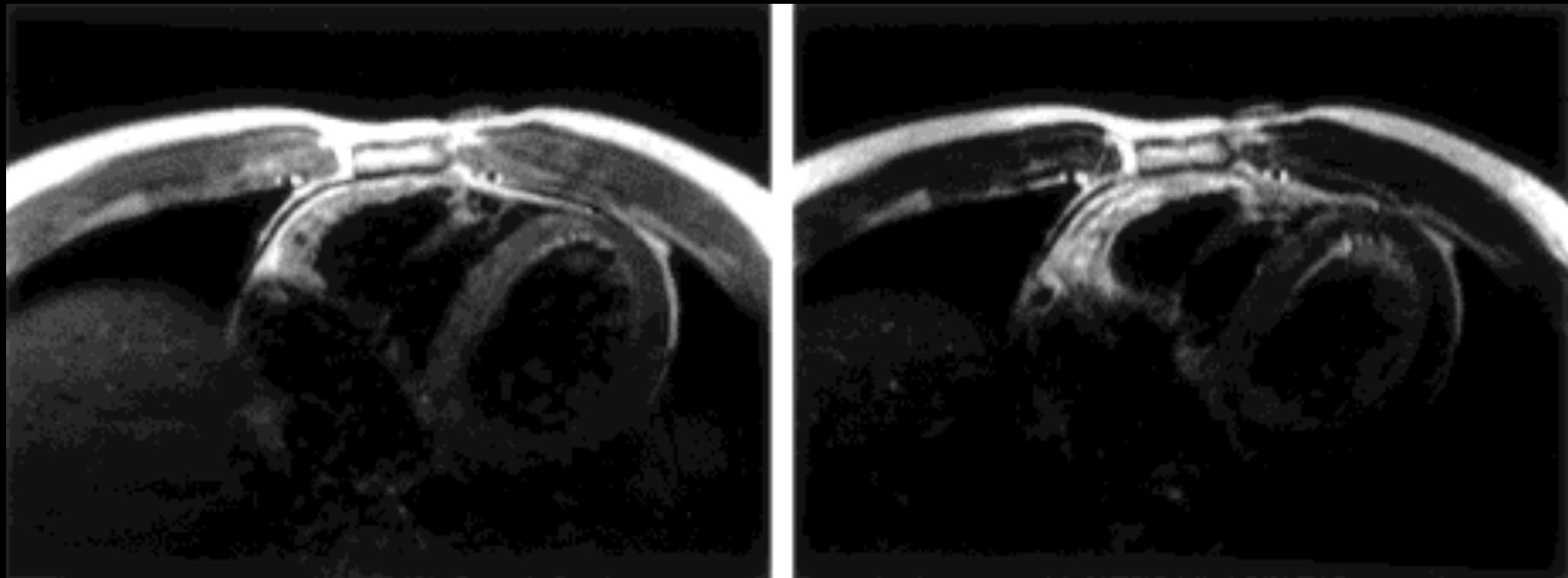


# TSE Image Contrast

- Dual-echo PDw+T2w in same TR
- Mag-prep modules (IR, SR, FS, etc.)
- Inherent flow suppression
  - only static spins see multiple 180s
  - “dark/black blood” imaging

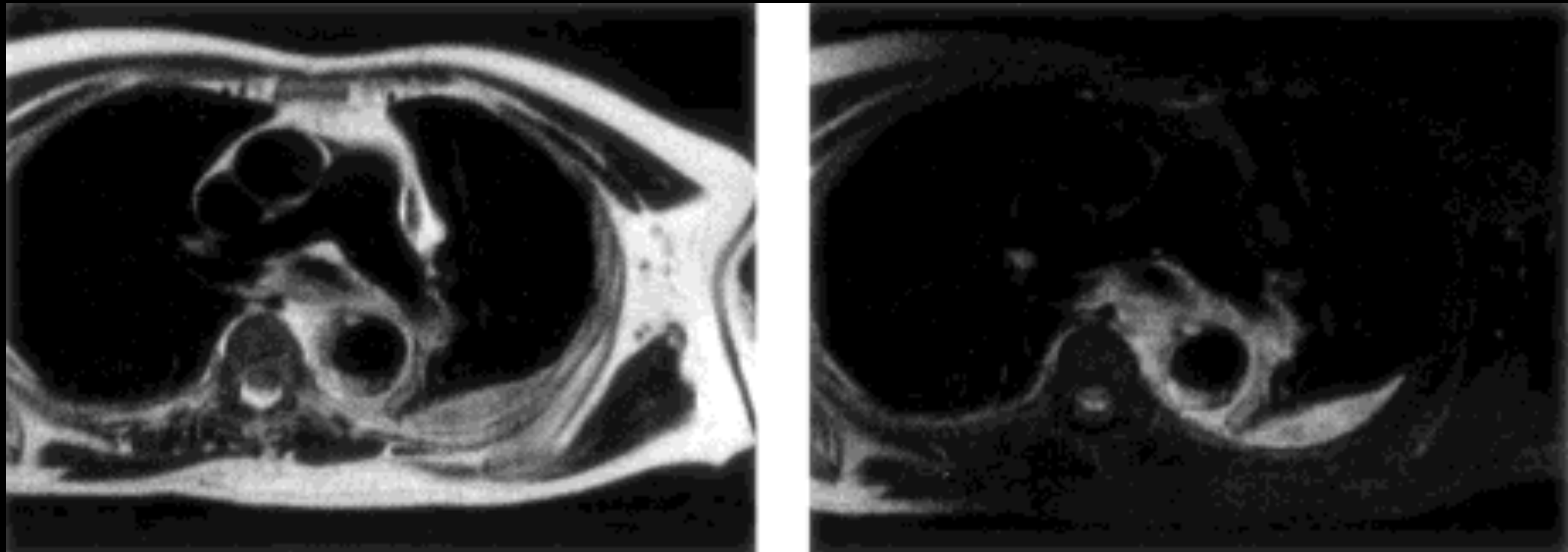
# TSE Image Contrast

Dark Blood from Spin Echo



# TSE Image Contrast

Dark Blood from Double Inversion-Recovery TSE

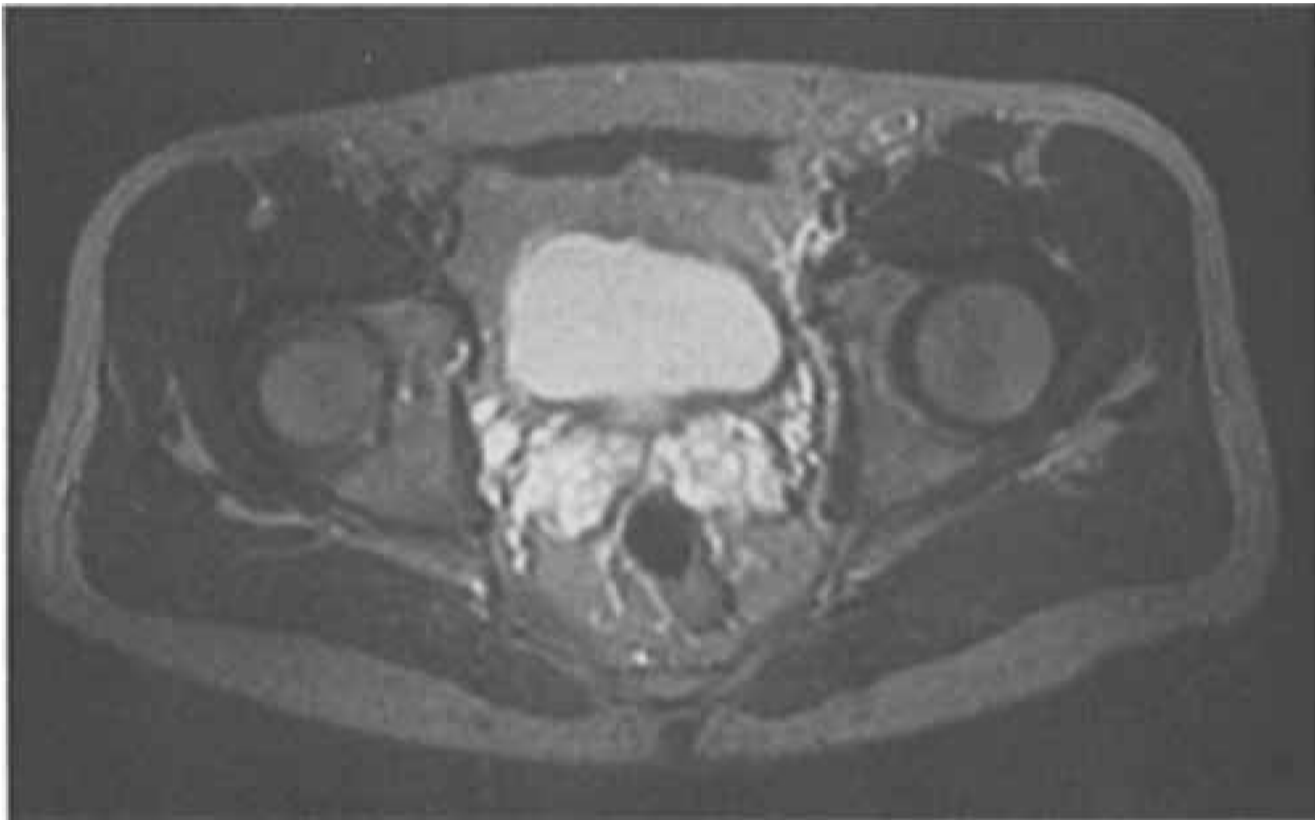


# TSE Image Contrast

- Bright fat
  - J-coupling of protons in lipids (CH<sub>3</sub>-CH<sub>2</sub>-);  
 $f_{CS} \sim 25 \text{ Hz}$ ,  $f_J \sim 7 \text{ Hz @ } 1.5 \text{ T}$
  - $S = S_0 * \exp(-t/T_2) * \cos(n_{ech} \pi f_J ESP)$
  - Shortening of apparent  $T_2$  (in SE)
  - J-coupling negligible when  
 $ESP \leq 1/[2 \text{ sqrt}(f_{CS}^2 + f_J^2)] \sim 20 \text{ ms @ } 1.5 \text{ T}$
  - In TSE, short ESP avoids attenuation by J-coupling, thus brighter fat signal

# TSE Image Contrast

Spin Echo



Turbo Spin Echo



*Bright Fat*

# TSE Image Contrast

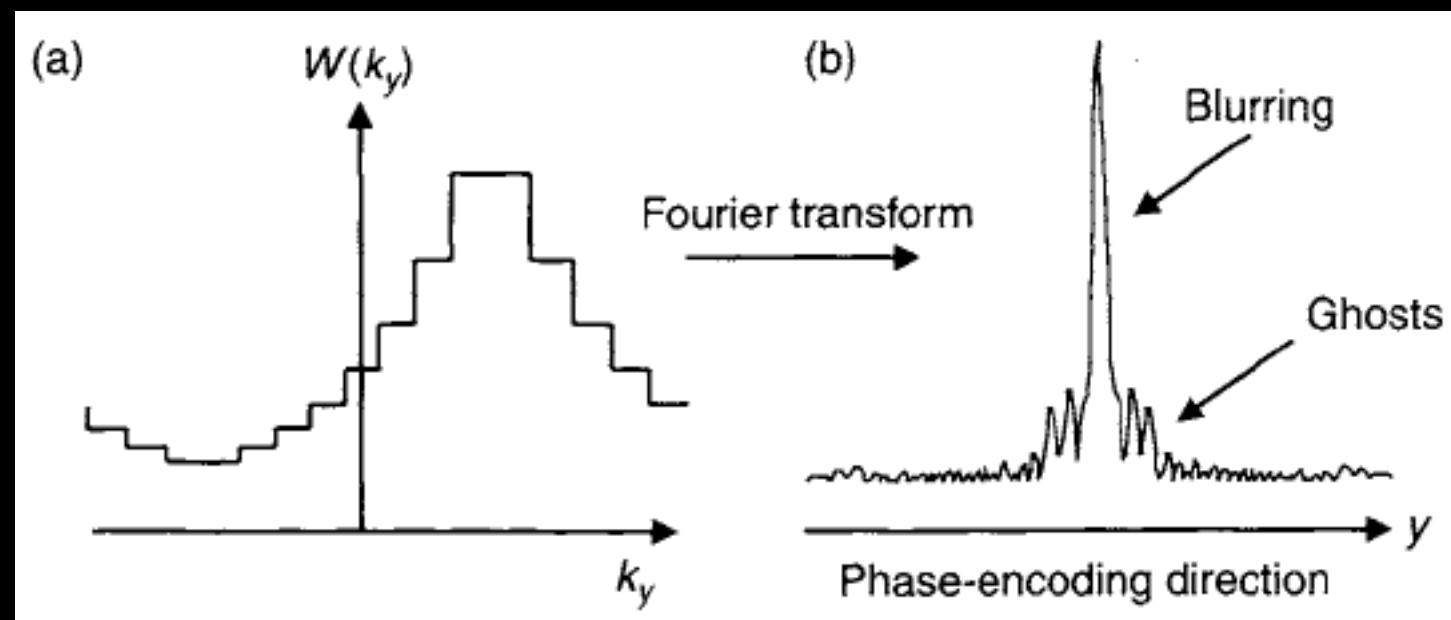
- Magnetization transfer
  - MT effect
  - multiple refocusing pulses in TSE
  - off-resonance excitation in other slices; can lead to MT-induced signal loss

# TSE Advantages

- Image contrast very similar to SE
- Robust to off-resonance effects (SE)
- Much faster scan than SE

# TSE Challenges

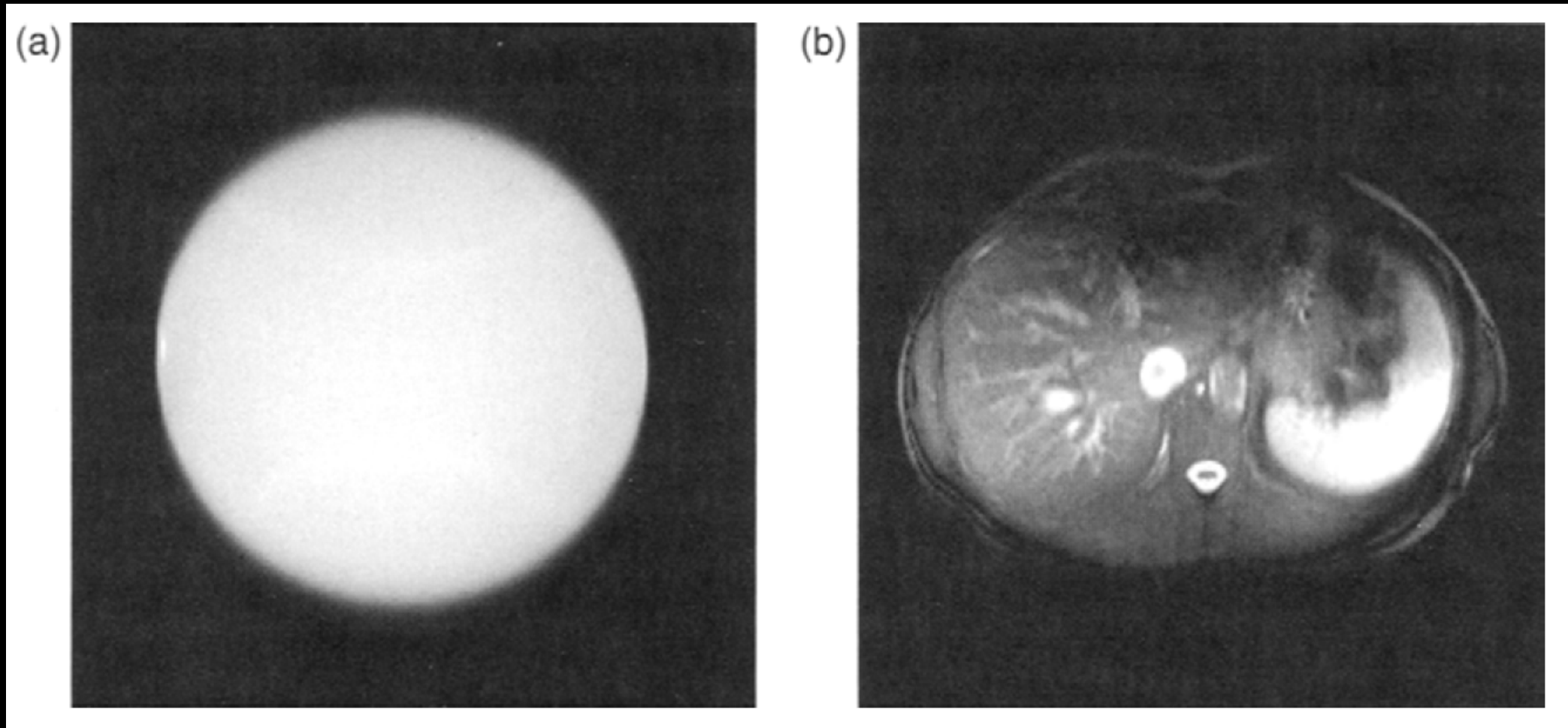
- Blurring; edge enhancement; ghosting;
  - attention to PE ordering and ETL





# TSE Challenges

T<sub>2</sub> blurring (PE) in single-shot TSE



# TSE Challenges

- RF power deposition increased
  - Specific Absorption Rate (SAR) W/kg;  
 $SAR \propto \theta^2 (B_0)^2$
  - use reduced refocusing flip angles,  
e.g.,  $\theta = 130^\circ$  instead of  $180^\circ$

# Extensions and Variations

- Partial echo
- Multi-echo
- Mag-prep

# Extensions and Variations

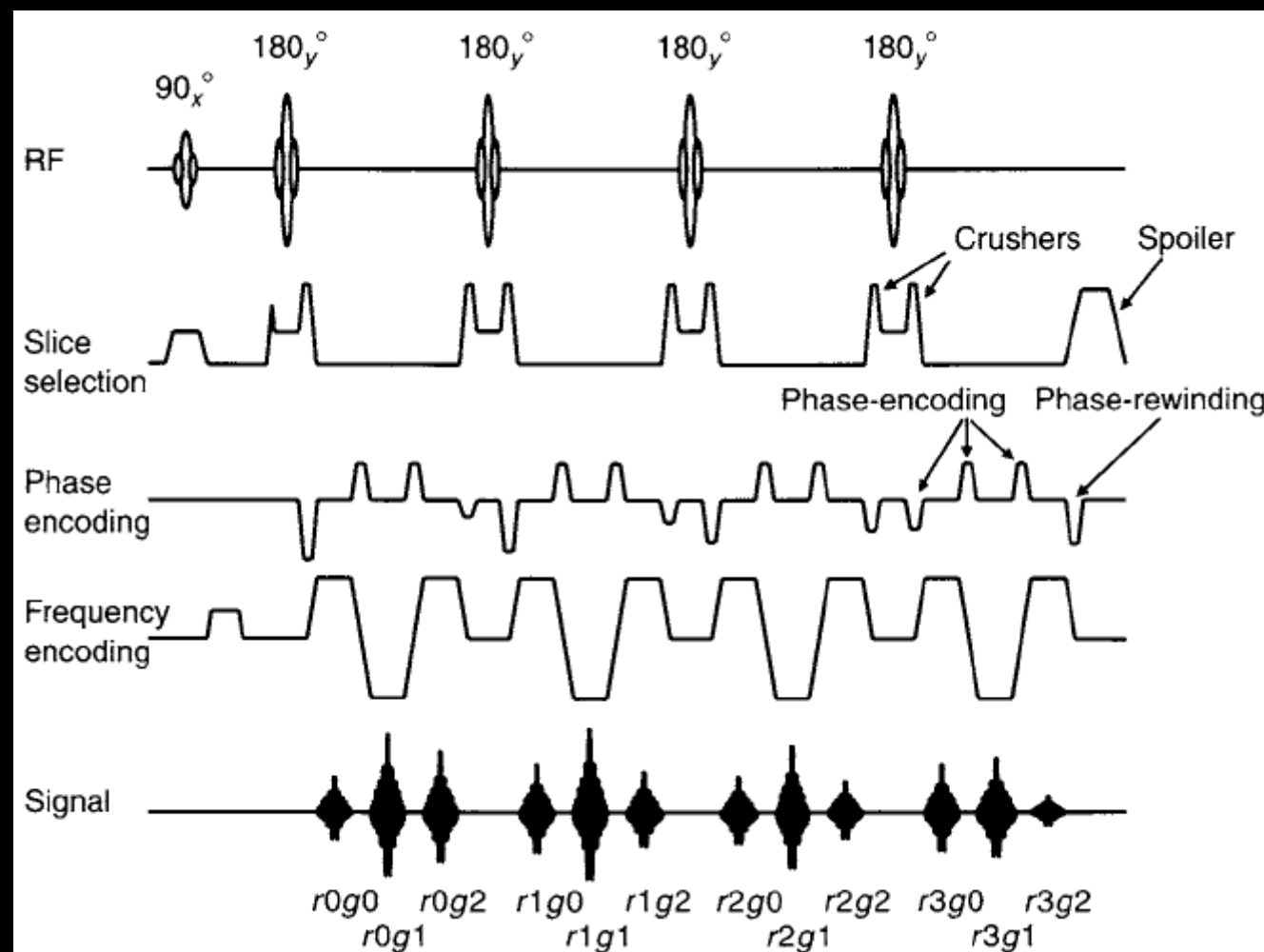
- Partial Fourier
  - Sample ~half of k-space data, reconstruct assuming Hermitian symmetry (real-valued MR images)
  - reduce refocusing pulses, reduce SAR
  - better control of  $TE_{\text{eff}}$
- Parallel imaging
  - Undersample k-space data, reconstruct using information from multiple coils
  - reduce refocusing pulses, reduce SAR

# Related Sequences

- TSE + non-Cartesian trajectories
  - radial, rings, spiral, cylinders, etc.
- TSE-Dixon to separate bright fat
- Half-Fourier acquired single-shot turbo spin echo (HASTE)
- Variable flip angle 3D TSE (SPACE, CUBE, etc.) to manage SAR, ETL

# Related Sequences

Gradient And Spin Echo (GRASE)<sup>1</sup>,  
aka Turbo gradient spin echo (TGSE)



<sup>1</sup>Oshio K et al., *MRM* 1991

Bernstein et al., *Handbook of MRI Pulse Sequences*, Ch 16.2

# Clinical Applications

- The bread and butter sequence!
  - Brain
  - Body
  - Cardiac
  - Musculoskeletal
  - and more ...

# More About TSE

- FID, SE, secondary SE, Stimulated Echoes (STE) ...
- Practical conditions
  - Reduced refocusing pulse angles
  - Non-uniform slice profiles
  - $B_1$  inhomogeneity



# Summary

- RARE (Turbo Spin Echo)
  - efficient use of  $M_{xy}$
  - shares robustness of SE
  - core clinical sequence
  - challenges with SAR
- Multiple RF pulses -> multiple echoes
  - generalized view of MR pulse sequences
- EPG next time!

# Pulse Sequence Simulations

# Outline

- Bloch Equation Simulations
  - basic operations (matrix form)
  - MATLAB implementation
  - examples: rapid GRE
  - homework

# Bloch Simulation

- Bloch Equations
  - RF excitation
  - $T_1, T_2$  decay
  - free precession
  - gradient pulse

# Bloch Simulation

Rotation:

$$R_x(\theta) = \begin{bmatrix} 1 & 0 & 0 \\ 0 & \cos \theta & \sin \theta \\ 0 & -\sin \theta & \cos \theta \end{bmatrix} \quad R_y(\theta) = \begin{bmatrix} \cos \theta & 0 & -\sin \theta \\ 0 & 1 & 0 \\ \sin \theta & 0 & \cos \theta \end{bmatrix}$$

$$R_z(\theta) = \begin{bmatrix} \cos \theta & \sin \theta & 0 \\ -\sin \theta & \cos \theta & 0 \\ 0 & 0 & 1 \end{bmatrix}$$

```
function Rx=xrot(phi)
Rx = [1 0 0; 0 cos(phi) -sin(phi); 0 sin(phi) cos(phi)];
```

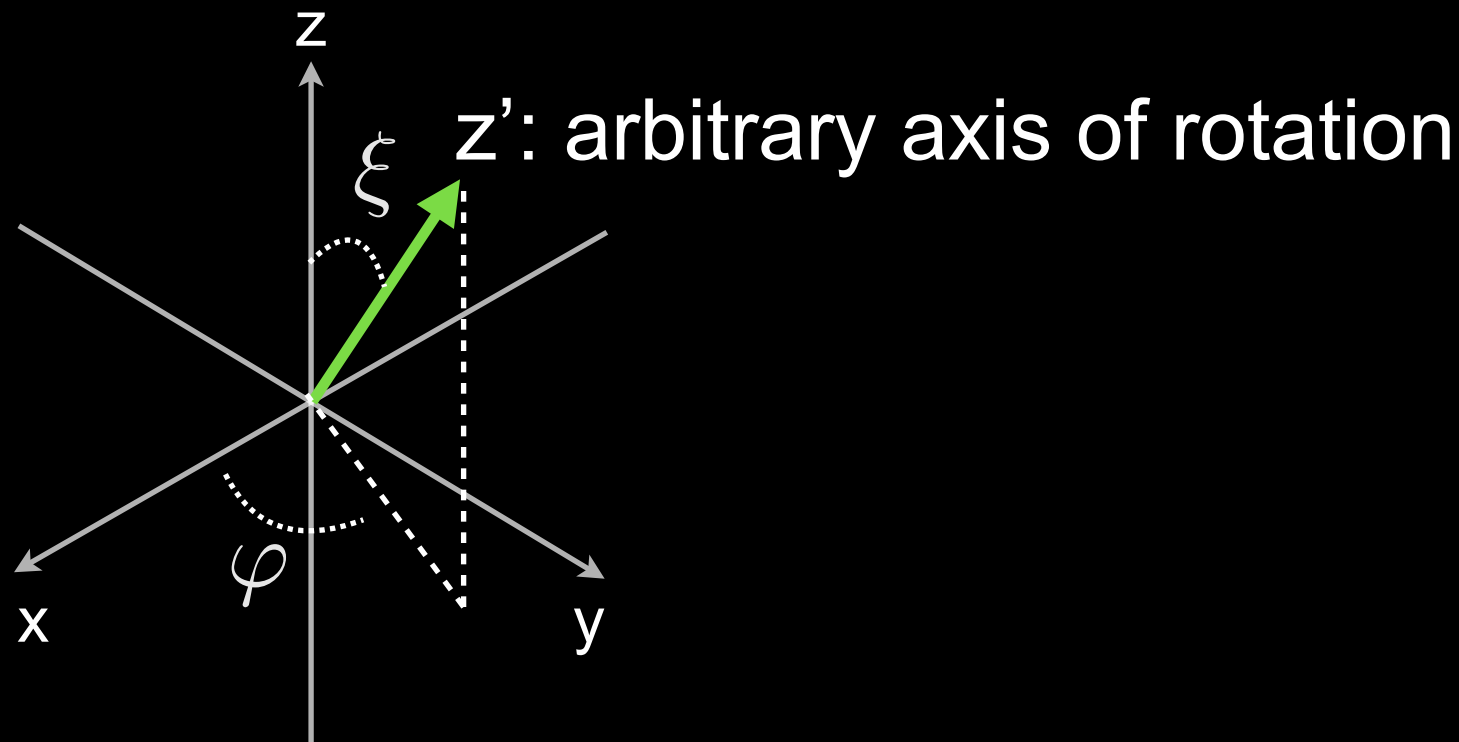
# Bloch Simulation

Free precession:

$$R_z(\omega_0 t) = \begin{bmatrix} \cos \omega_0 t & \sin \omega_0 t & 0 \\ -\sin \omega_0 t & \cos \omega_0 t & 0 \\ 0 & 0 & 1 \end{bmatrix}$$

# Bloch Simulation

General Rotation:



$$R_{\{\varphi, \xi\}}(\theta) = R_z(-\varphi)R_y(-\xi)R_z(\theta)R_y(\xi)R_z(\varphi)$$

# Bloch Simulation

Relaxation + Free Precession:

$$M(t) = \begin{bmatrix} e^{-t/T_2} & 0 & 0 \\ 0 & e^{-t/T_2} & 0 \\ 0 & 0 & e^{-t/T_1} \end{bmatrix} R_z(\Delta\omega t) M(0) + \begin{bmatrix} 0 \\ 0 \\ M_0(1 - e^{-t/T_1}) \end{bmatrix}$$

$AM(0) + B$

```
function [Afp,Bfp]=freeprecess(T,T1,T2,df)
% T, T1, T2 in ms
% df in Hz

% Relaxation
M0 = 1;
A = [exp(-T/T2) 0 0; 0 exp(-T/T2) 0; 0 0 exp(-T/T1)];
B = M0*[0 0 1-exp(-T/T1)]';

% df in Hz
phi = 2*pi * df*T*10^-3; %omega = 2pi * f, in radians
Rz = zrot( phi );

Afp = A*Rz;
% Bfp = B*Rz;
% same as:
Bfp = B;
```



# Bloch Simulation

- Transient state; steady state
- Different seq/tissue params
- Brian's MATLAB Bloch sim tutorial
  - <http://www-mrsrl.stanford.edu/~brian/bloch/>

# Bloch Simulation

- Example 1: Gradient Echo (long TR)
  - xrot.m, yrot.m, zrot.m, throt.m
  - freeprecess.m
  - Sim\_SatRecovery.m
  - add gradient rewinders / spoilers, RF phase cycling to simulate rapid GRE sequences

# Bloch Simulation

- Example 2: Balanced SSFP
  - xrot.m, yrot.m, zrot.m, throt.m
  - freeprecess.m
  - sssignal.m
  - BalancedSSFP\_freqresp.m
  
  - consider different flip angle,  $T_1$ ,  $T_2$
  - change TR and look at freq response

# Bloch Simulation

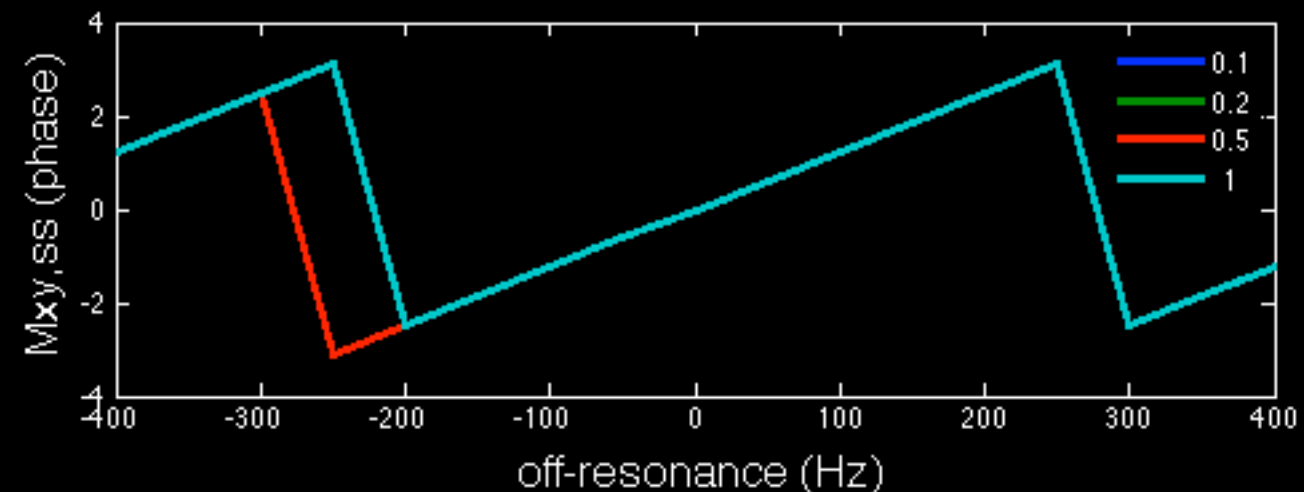
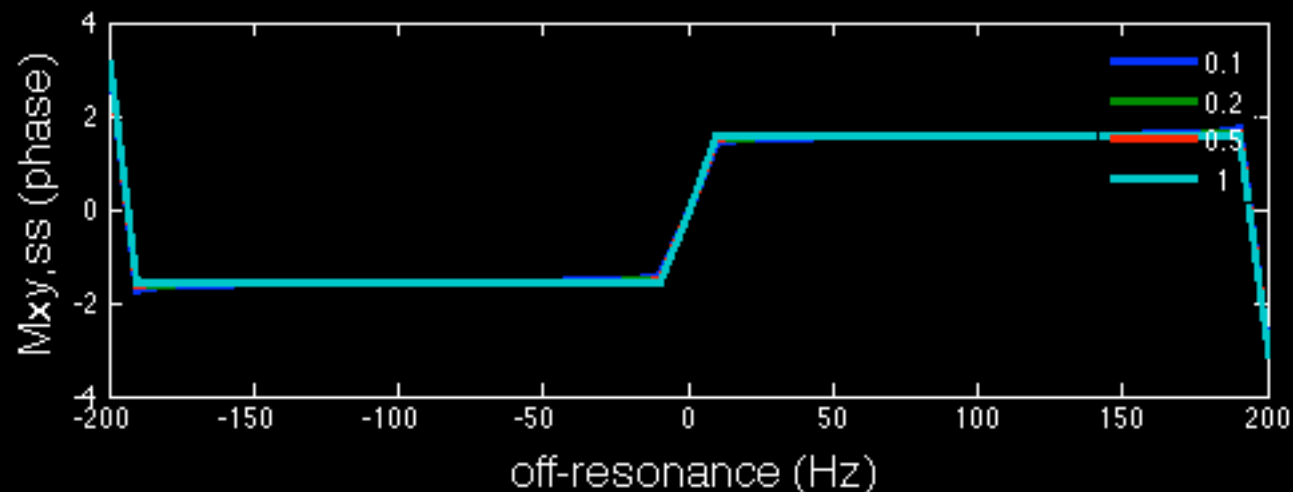
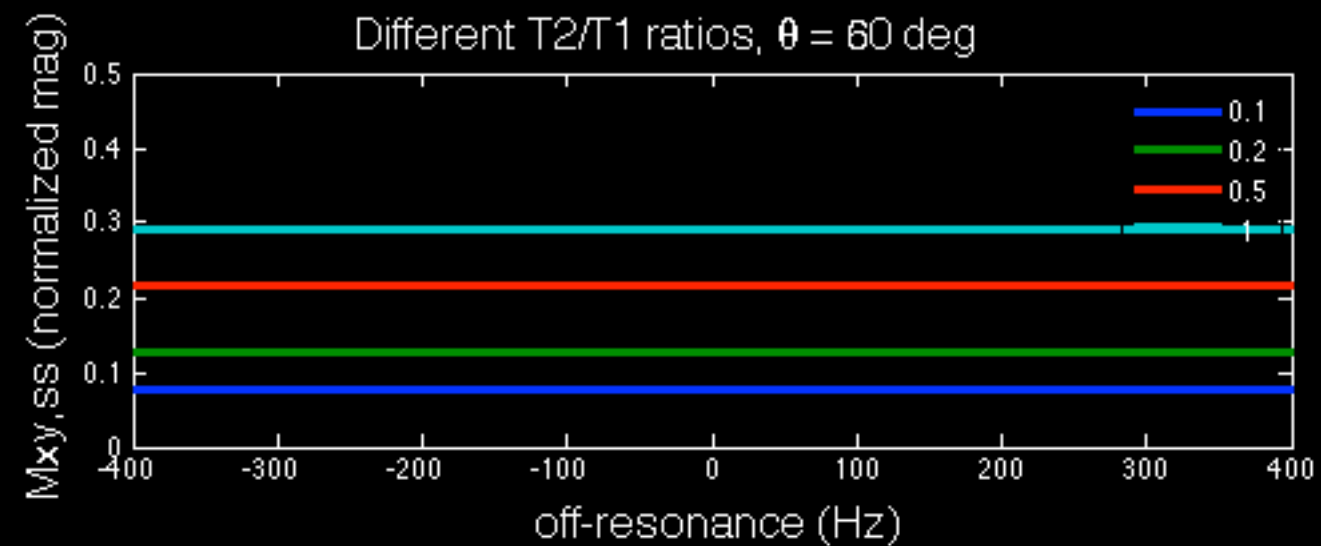
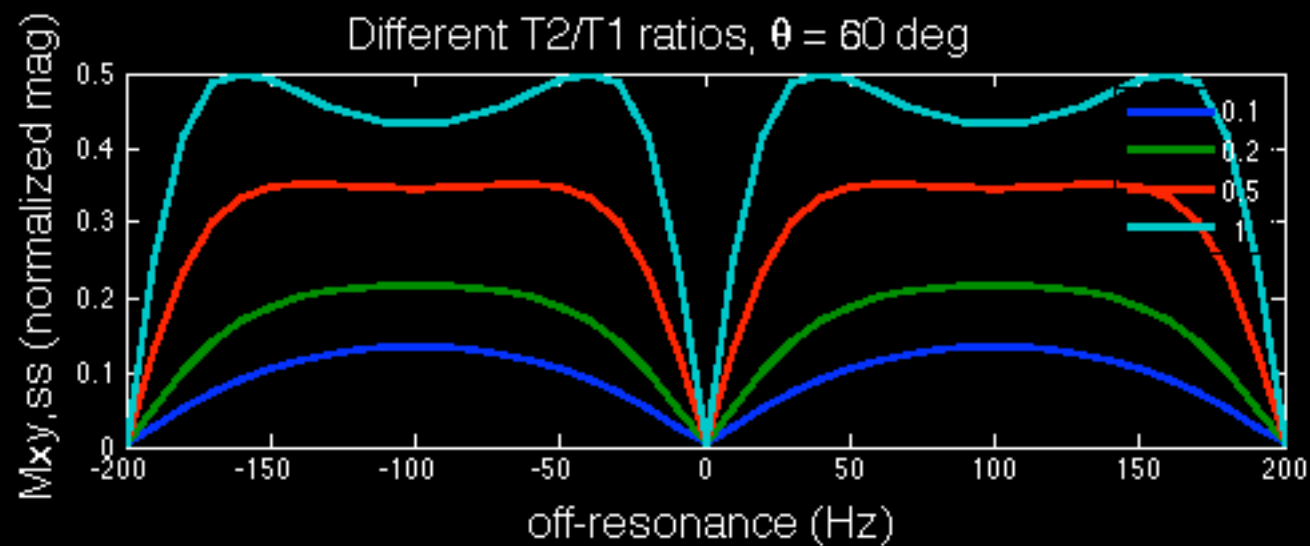
- Homework 1, part 1A
  - Steady state for bSSFP, SSFP-FID and SSFP-Echo

# Gradient-spoiled GRE

SS signal as a function of off-resonance:

*bSSFP*

*GRE (SSFP-FID)*



$T_1 = 1000$  ms,  $T_2 = 100, 200, 500, 1000$  ms

# Gradient-spoiled GRE

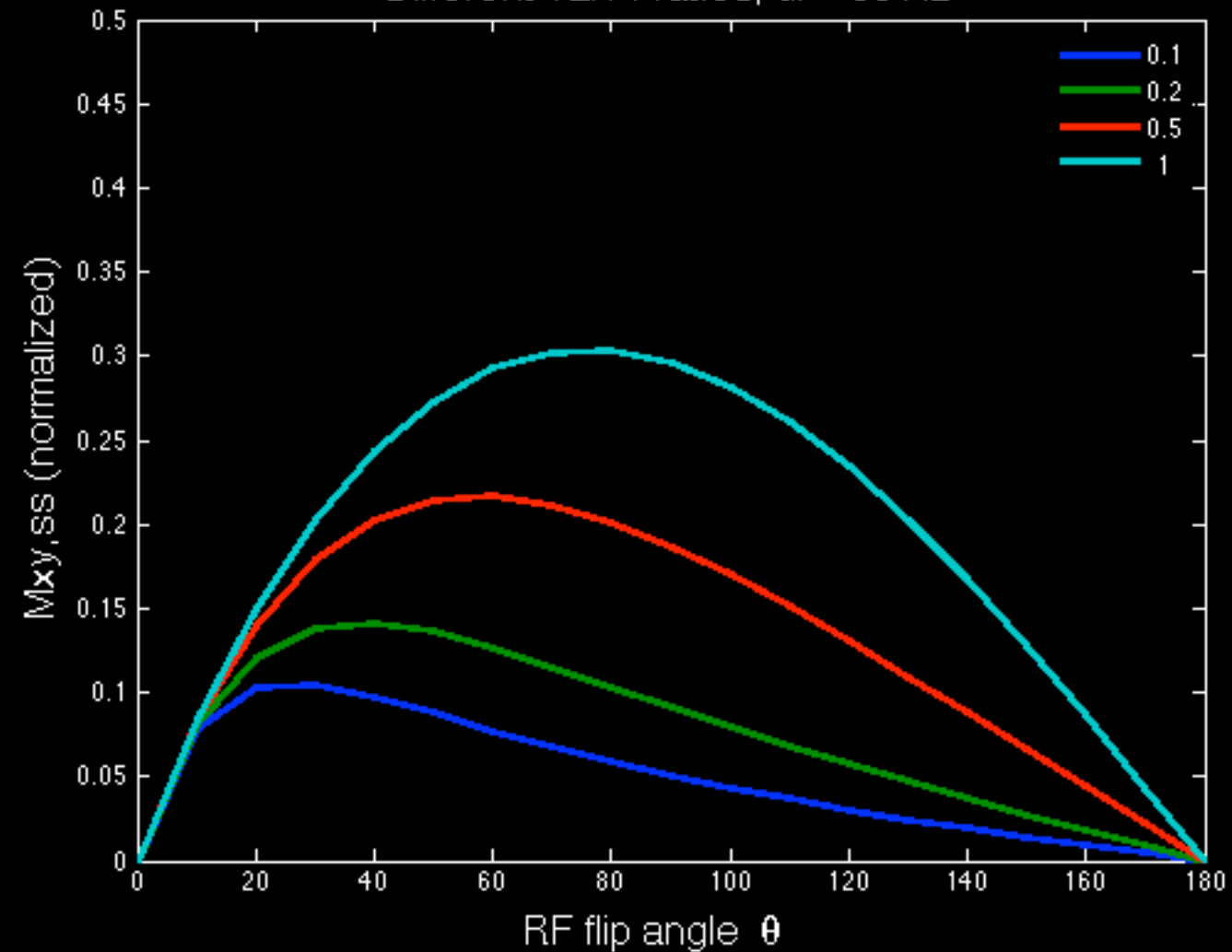
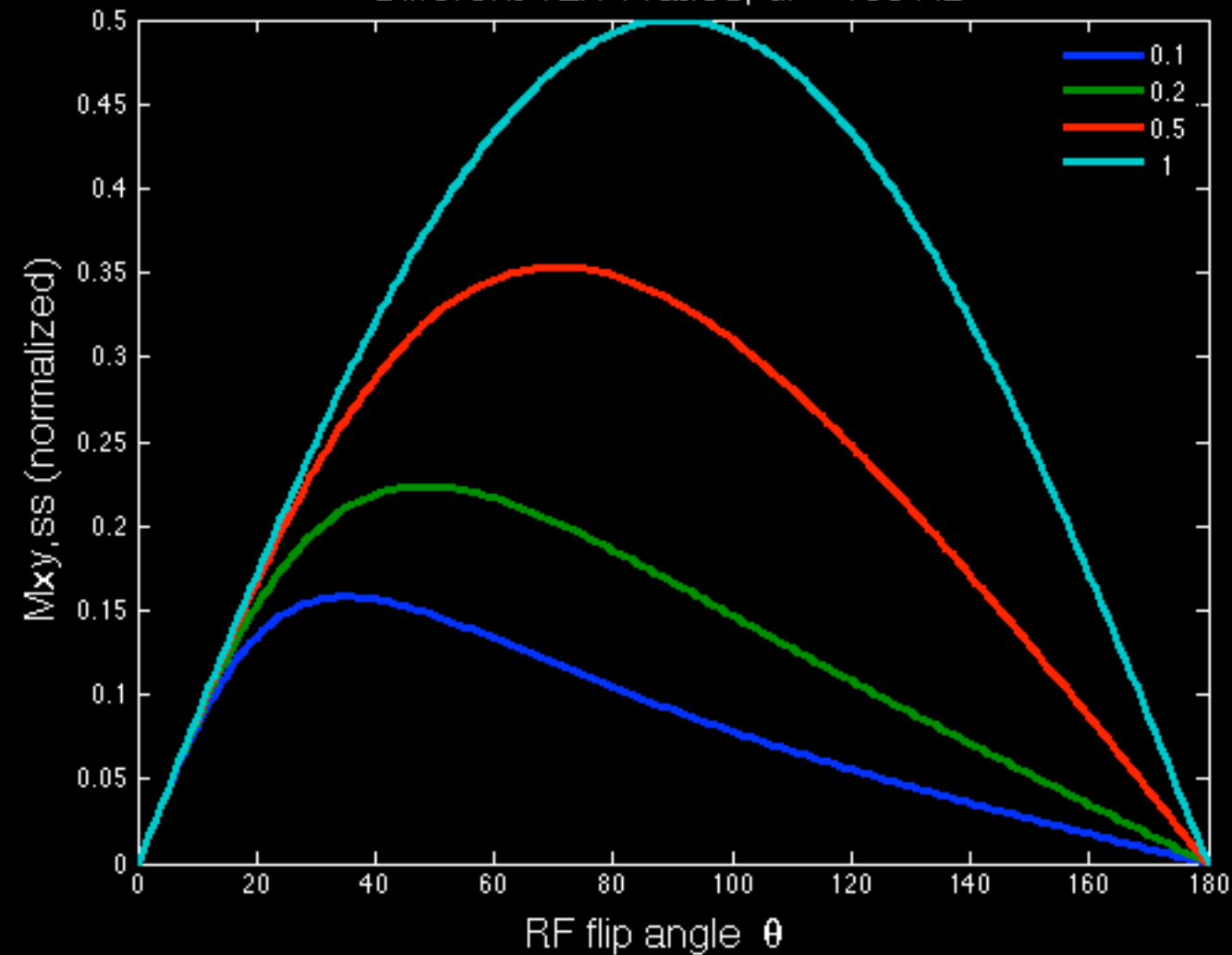
SS signal as a function of flip angle:

*bSSFP*

*GRE (SSFP-FID)*

Different T2/T1 ratios, df = 100 Hz

Different T2/T1 ratios, df = 50 Hz



$T_1 = 1000 \text{ ms}$ ,  $T_2 = 100, 200, 500, 1000 \text{ ms}$

# Gradient-spoiled GRE

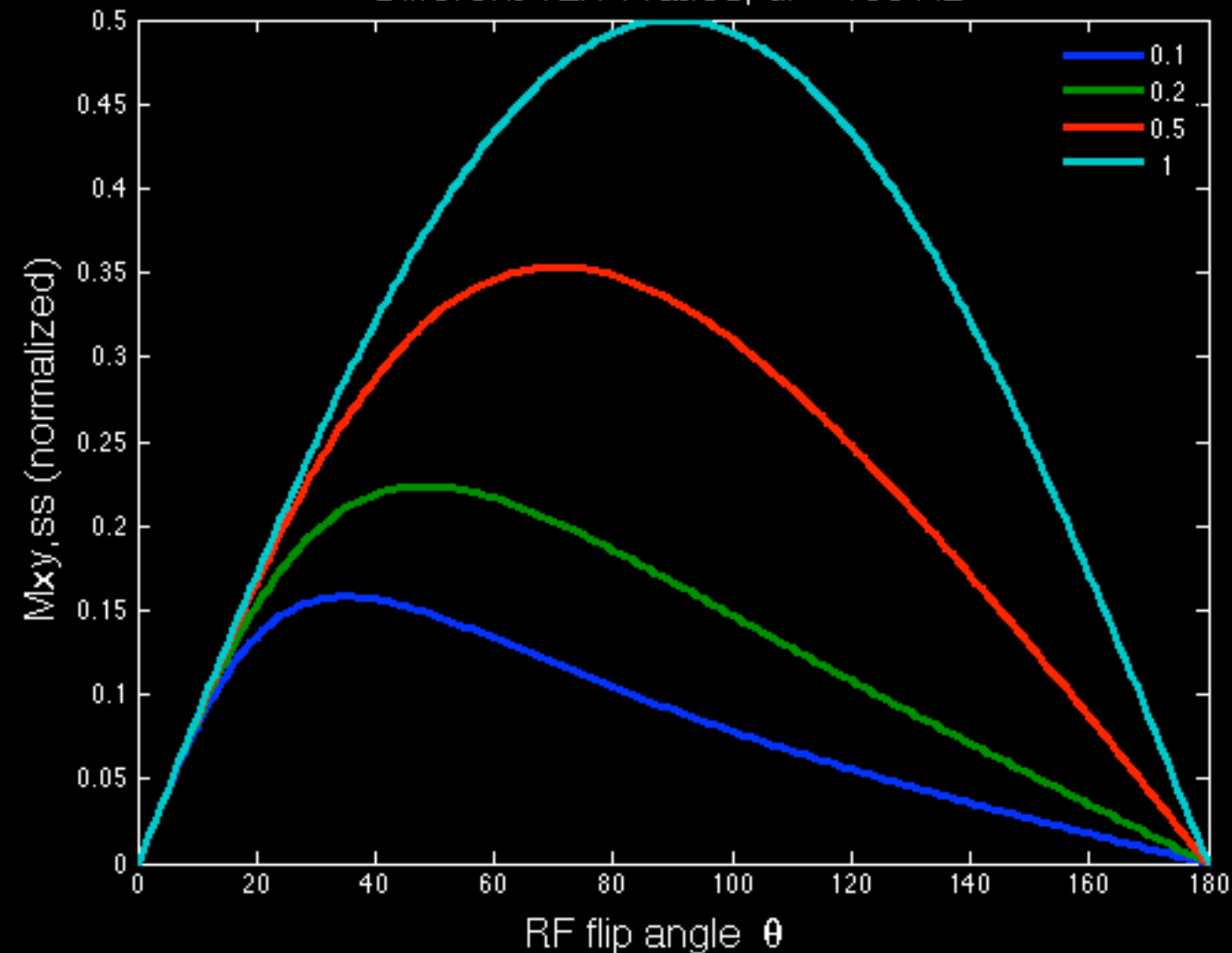
(reversed)

SS signal as a function of flip angle:

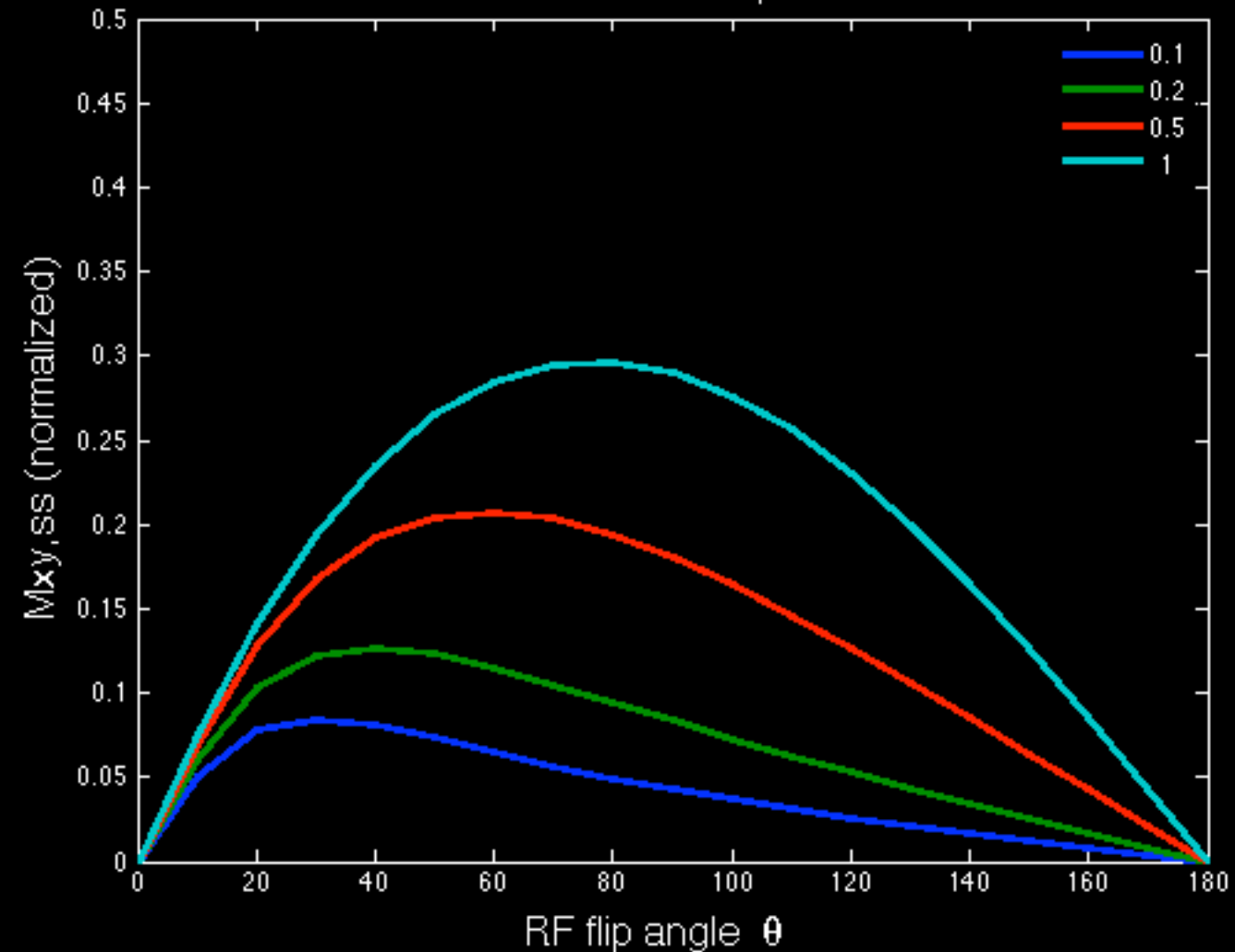
*bSSFP*

*GRE (SSFP-Echo)*

Different T2/T1 ratios, df = 100 Hz



Different T2/T1 ratios, df = 50 Hz



$T_1 = 1000$  ms,  $T_2 = 100, 200, 500, 1000$  ms

# Bloch Simulation

- Homework 1, part 1B
  - Transition to steady state for bSSFP
  - catalyzation schemes



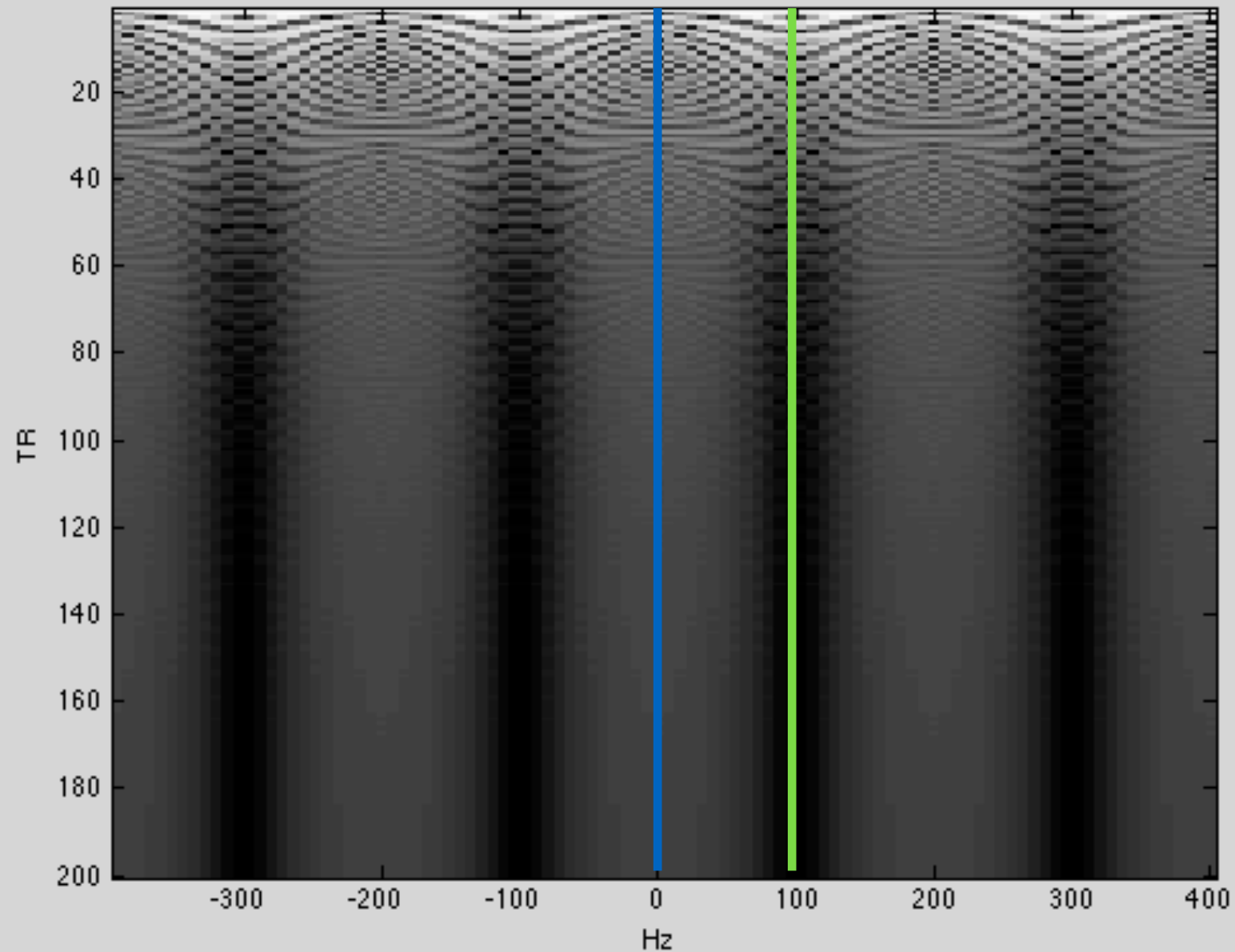
# Balanced SSFP

Transition to steady state:

$TR = 5 \text{ ms}$

$\Delta\phi = \pi$

$\theta = 60^\circ$



$T_1 = 600 \text{ ms}, T_2 = 100 \text{ ms}$

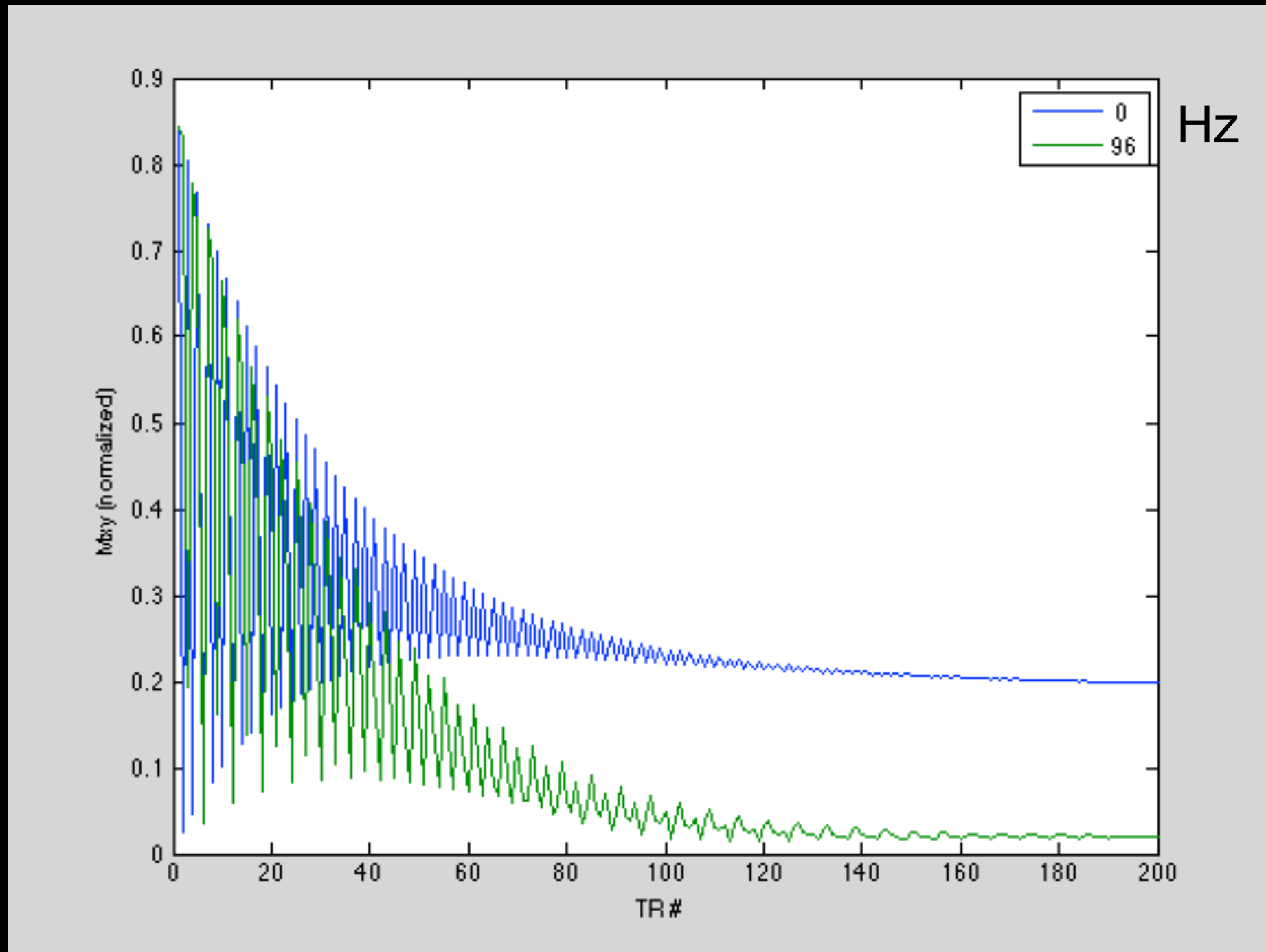
# Balanced SSFP

Transition to steady state:

TR = 5 ms

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$\theta = 60^\circ$



$T_1 = 600\text{ ms}, T_2 = 100\text{ ms}$

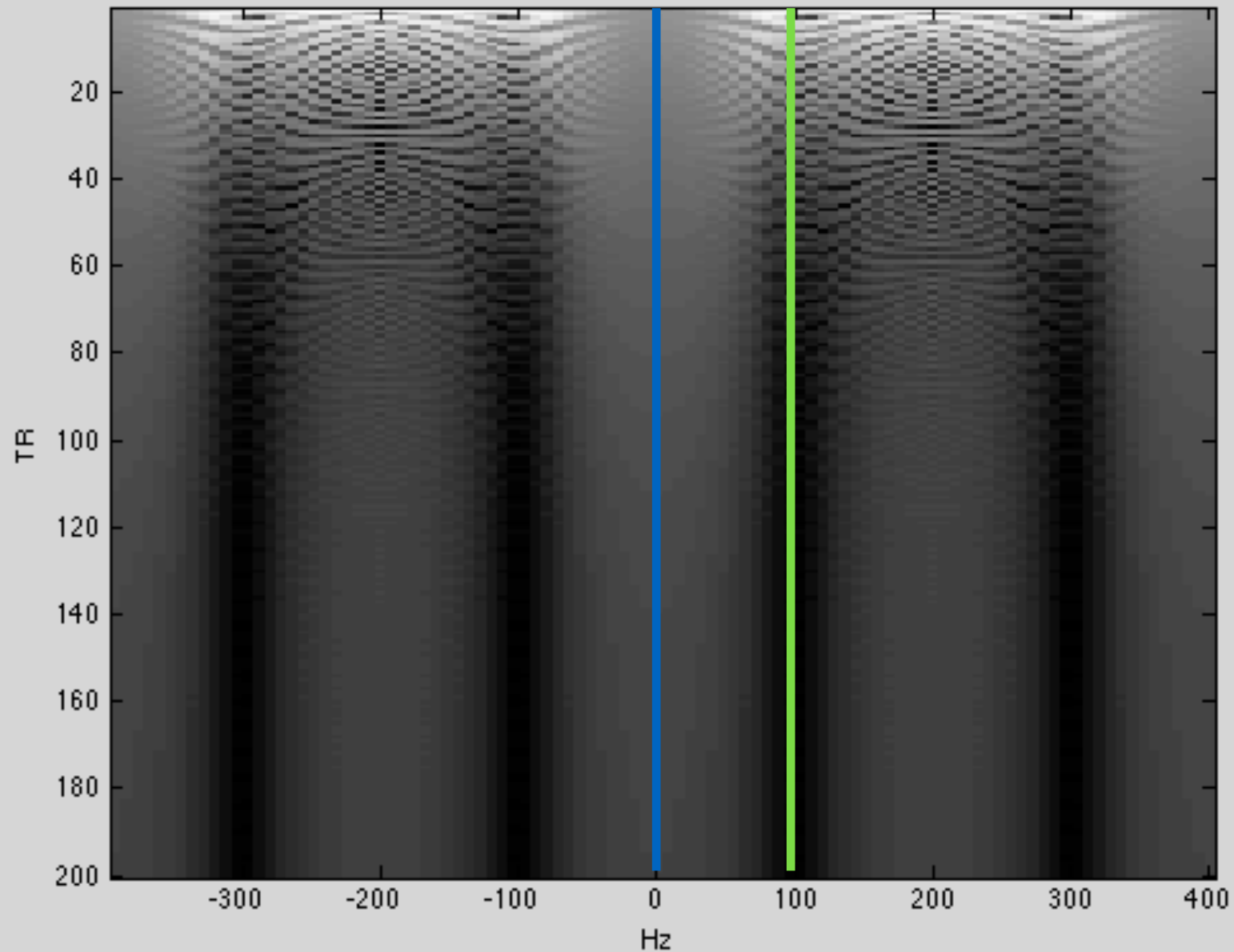
# Balanced SSFP

Transition to steady state ( $\theta/2$  -TR/2 prep):

TR = 5 ms

$\Delta\phi = \pi$

$\theta = 60^\circ$



$T_1 = 600$  ms,  $T_2 = 100$  ms

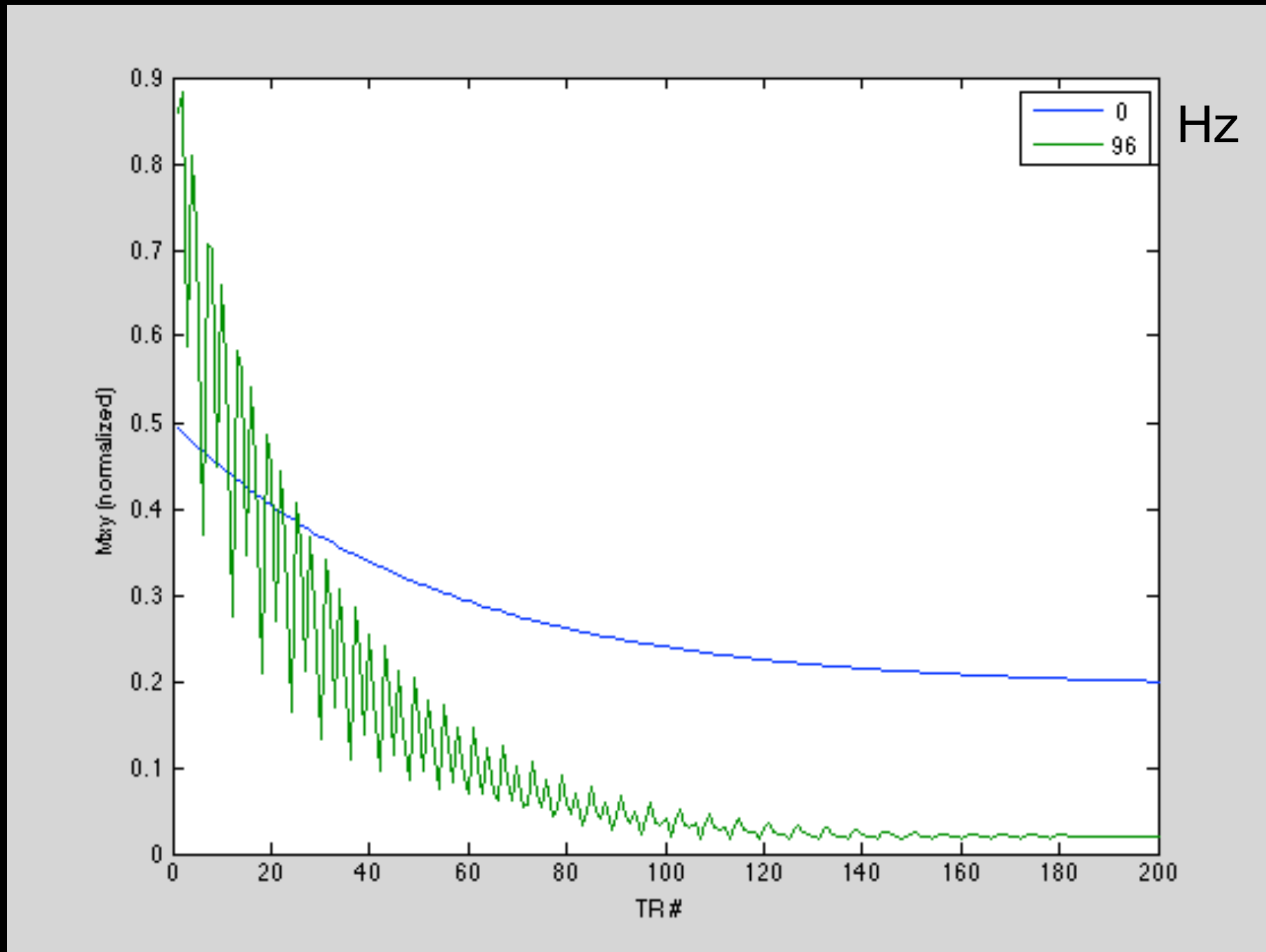
# Balanced SSFP

Transition to steady state ( $\theta/2$  -TR/2 prep):

TR = 5 ms

$\Delta\phi = \pi$

$\theta = 60^\circ$



$T_1 = 600$  ms,  $T_2 = 100$  ms

# Balanced SSFP

- Linear ramp-up catalyzation
  - initial train of  $\theta \cdot [1:N]/N$  (same TR)
  - Example:  
 $\theta = 60^\circ$ ,  $N = 5$   
ramp up pulses  $\theta_{lin} = [12^\circ, 24^\circ, 36^\circ, 48^\circ, 60^\circ]$

# Homework 1

- Pulse Sequence Simulations
  - 1. Bloch: Steady state comparison, bSSFP transient state and catalyzation
  - 2. EPG: SSFP-FID, RF-spoiled GRE
- Due 5 pm, 4/23 Fri by email
  - PDF and MATLAB code

# Thanks!

- Web resources
  - ISMRM 2010 Edu: Miller, Weigel
  - ISMRM 2011 Edu: Miller, Weigel
- Further reading
  - Bernstein et al., Handbook of MRI Sequences
  - Haacke et al., Magnetic Resonance Imaging
  - Scheffler, Concepts in MR 1999; 11:291-304
  - Hennig, JMR 1988; 78:397-407

# Thanks!

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- Next lecture
  - EPG and MATLAB demo

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